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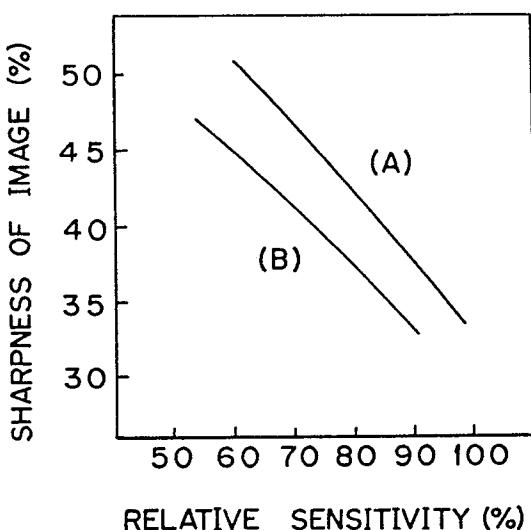
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⑯ Radiation image conversion panel.

⑯ A radiation image conversion panel comprising a support and at least one phosphor layer comprising a binder and a phosphor dispersed therein. Examples of the conversion panel include a radiographic intensifying screen and a radiation image storage panel. The sharpness of image provided by the conversion panel and the adhesion between the phosphor layer and the support are both remarkably improved by providing onto the surface of the support a great number of pits having a mean depth of at least 1 μ m, a maximum depth of more than 1 to 100 μ m, and a mean diameter at the opening of at least 1 μ m.



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RADIATION IMAGE CONVERSION PANEL

This invention relates to a radiation image conversion panel such as a radiographic intensifying screen or a radiation image storage panel, and a process for the preparation of the same. More particularly, this invention relates to a radiation image conversion panel comprising a support and at least one phosphor layer comprising a binder and phosphor dispersed therein, and a process for the preparation of the same.

The radiographic intensifying screen is generally employed in close contact with one or both surfaces of an X-ray film for enhancing the photographic sensitivity of the film in a variety of radiographies such as medical radiography and industrial radiography. The radiographic intensifying screen consists essentially of a support and a phosphor layer provided thereonto. Further, a transparent film is generally provided onto the free surface of the phosphor layer to keep the phosphor layer from chemical and physical deterioration.

The phosphor layer comprises a binder and a phosphor dispersed therein. The phosphor is in the form of small particles, and emits light of high luminance when excited by radiation such as X-rays. The light of high luminance emitted by the phosphor is in proportion to the dose of radiation energy transmitted through an object. The X-ray film positioned in close contact with the intensifying screen is exposed to the

light emitted by the phosphor layer, as well as being exposed directly to the radiation energy transmitted through the object. Accordingly, the X-ray film receives radiation energy enough for formation of the radiation image 5 of the object, even if the radiation is applied to the object at a relatively small dose.

In view of the above-described characteristics of the radiographic intensifying screen, it is desired that the screen shows a high radiographic speed, as 10 well as provides excellent image characteristics such as sharpness and graininess. For the reason, various proposals have been previously given for the improvement of radiographic speed and image characteristics of the radiographic intensifying screen.

15 For instance, United States Patent No. 4,207,125 describes an X-ray intensifying screen including an anti-reflecting surface at the back side of the luminous layer in which a plurality of randomly positioned leaflets extend from the surface, in which the layer 20 is typically formed of a microstructured layer of boehmite, a hydrated aluminum oxide.

United States Patent No. 4,236,061 describes an image intensifying screen comprising an antireflecting surface formed by subjecting a substantially planner 25 aluminum surface on a support layer to a steam treatment to convert the aluminum surface to a microstructured surface of boehmite, a hydrated aluminum oxide, having a plurality of randomly positioned leaflets extending from the surface.

30 The radiographic intensifying screen also is ought to be so mechanically strong enough to keep itself from separation between the support and the phosphor layer when receives mechanical shocks such as bending in the course of radiographic procedures. The intensifying 35 screen is chemically and physically resistant to radiographic rays, whereby the screen is employable for a

long period even under the conditions of repeated uses. For this reason, the screen ought to be resistant to mechanical shocks given in the procedure for changing an X-ray film or other procedures so that it is 5 free from separation between the support and the phosphor layer.

Accordingly, a primary object of the present invention is to provide a radiographic intensifying screen improved in the sharpness, and a process for the preparation of the same. 10

Another object of the invention is to provide a radiographic intensifying screen improved in the mechanical strength, particularly, strength in the adhesion between the support and the phosphor layer, and a process for the preparation of the same. 15

There is provided by the invention a radiographic intensifying screen comprising a support and at least one phosphor layer comprising a binder and a phosphor dispersed therein, in which the support is provided 20 on the surface facing the phosphor layer with a great number of pits having a mean depth of at least 1 μm , a maximum depth of more than 1 μm to 100 μm , and a mean diameter at the opening of at least 1 μm .

The radiographic intensifying screen of the invention 25 can be prepared by a process comprising applying hard solid particles onto the surface of the support at high speed to form the pits.

The present invention is now described hereinafter more in detail.

According to the invention, a radiographic intensifying screen producing on a radiographic film an image prominently improved in the sharpness, as well 30 as being highly improved in the adhesion between the support and the phosphor layer, is obtained by providing a great number of pits having the specifically 35 determined size onto the surface of the support on the

side facing the phosphor layer.

When radiation such as X-rays having passed through an object impinges upon the phosphor layer of a radiographic intensifying screen, the phosphor particles contained in the phosphor layer are excited upon absorbing the radiation energy and immediately emits light of a wavelength in the visible or near ultra-violet region which is different from the wavelength of the introduced radiation. The so emitted light advances in all directions, and a part of the light enters directly into a photosensitive layer of the film placed in contact with the screen so as to contribute the formation of a photographic image on the film. Another part of the light advances in the direction towards the interface between the phosphor layer and the support, and is reflected by the support surface to enter into the photosensitive layer through the phosphor layer, also contributing the formation of the photographic image. In the case of using a radiographic intensifying screen comprising a simply plane interface having no protrusions and depressions between the phosphor layer and the support, the reflection of light is done as the mirror plane reflection, whereby the reflected light enters into the film at an angle higher than the angle of the light directly entering into the film. Accordingly, the reflected light causes formation of an obscure image on the film, resulting in marked deterioration of the sharpness of image.

According to study of the present inventors, the deterioration of image formed on the radiographic film can be effectively prevented by providing a great number of pits having the specifically determined size, that is, a mean depth of at least 1 μm , a maximum depth of more than 1 μm to 100 μm , and a mean diameter at the opening of at least 1 μm , onto a surface of the support facing the phosphor layer, that is, the interface therebetween.

The pits provided onto the surface of the support, as described above, further serves for enhancing the adhesion between the support and the phosphor layer, so that substantially no separation takes place in a normal procedure for handling the intensifying screen.

The radiographic intensifying screen of the present invention can be prepared in the manner as described below.

The support for constituting the intensifying screen of the invention can be prepared by the use of material selected from those known or employed in the preparation of various radiographic intensifying screens. Examples of the support material include plastic films such as films of cellulose acetate, polyester, polyethylene terephthalate, polyamide, polyimide, triacetate, and polycarbonate; metal sheets such as aluminum foil and aluminum alloy foil; ordinary papers; baryta paper; resin-coated papers; pigment papers containing titanium dioxide or the like; and papers sized with polyvinyl alcohol or the like. In other words, there is no specific limitation on the material of the support, as far as the material can accept on the surface the formation of pits specified in the description given hereinbefore. In view of easiness in formation of these pits on the surface, as well as characteristics of a radiographic intensifying screen prepared therefrom, a plastic film is preferably employed as the support material. The plastic film may contain a light-absorbing material such as carbon black, or may contain a light-reflecting material such as titanium dioxide. The former is appropriate for preparing a radiographic intensifying screen belonging to the acutance (high sharpness) type, while the latter is appropriate for preparing a radiographic intensifying screen belonging to the high speed type.

In the preparation of a conventional radiographic

intensifying screen, one or more of additional layers are optionally provided between the support and the phosphor layer. For instance, a subbing layer or an adhesive layer may be provided by coating a polymer

5 material such as gelatin over the surface of the support on the side to receive the phosphor layer. Otherwise, a light-reflecting layer or a light-absorbing layer may be provided by introducing a polymer material layer containing a light-reflecting material such as titanium

10 dioxide or a light-absorbing material such as carbon black, respectively. Otherwise, a metal foil may be provided onto the surface of the support to receive the phosphor layer so as to remove scattered radiation in the radiographic intensifying screen to be employed in

15 the industrial radiography. Such a metal foil can be chosen from lead foil, lead alloy foil, tin foil, and the like. Any one or more of these additional layers may be provided to the radiographic intensifying screen of the invention.

20 A great number of the pits specified herein can be provided onto the surface of support in an optionally chosen manner. Preferably, these pits are provided by a process comprising applying hard solid particles such as grits and sands onto the surface of

25 support at high speed. The above-mentioned process is called "grit blasting" or "sand blasting". The hard solid particles can be applied onto the surface of support as such. Otherwise, a surface of an additional layer such as a subbing layer, light-reflecting layer,

30 light-absorbing layer, or metal layer, can be subjected to the high speed blasting of hard solid particles. The materials of the hard solid particles employable for the sand blasting or grit blasting are known in the art. For instance, metal particles, metal

35 oxide particles, or other inorganic material particles can be employed. The size of the hard solid particles

and the conditions for carrying out the above-mentioned process for the provision of the pits can be determined according to those known in the art.

In the case using the radiographic intensifying screen of the invention in contact with a radiographic film, a part of the light that is emitted by the phosphor upon receiving radiation having passed through an object and then advances toward the surface of the support layer (the interface between the phosphor layer and the support) is reflected diffusely by the surface provided with a great number of the pits having the specific dimension, whereby most of the reflected light is absorbed by the phosphor layer, not reaching the photo-sensitive layer of the radiographic film placed in contact therewith. Accordingly, the sharpness of the image produced on the radiographic film is prominently enhanced.

Moreover, as described hereinbefore, the provision of a great number of pits having dimensions in the ranges defined herein onto the surface of the support improves the adhesion between the phosphor layer and the support of the radiographic intensifying screen.

In contrast, if pits provided onto the support surface have dimension substantially deviated from the ranges defined as hereinbefore for the present invention, the prominent improvement both in the sharpness of a formed image and adhesion between the phosphor layer and the support are hardly attained.

If the pits are smaller than those defined hereinbefore, most of the light reflected by the support surface probably is not diffused and rather straightly advances toward the radiographic film, whereby no substantial improvement in the sharpness of image can be attained. Also unattainable is substantial enhancement of the adhesion between the phosphor layer and the support.

If the pits are larger than those defined herein-

before, the phosphor layer with plane surrace and even phase conditions are hardly prepared on the support, giving unfavorable factors to the intensifying screen.

The pits provided onto the surface of the support of the radiographic intensifying screen according to the present invention preferably have a mean depth of 1 - 10 μm , inclusive, more preferably 1 - 5 μm , inclusive; a maximum depth of more than 1 μm to 50 μm , more preferably 2 - 20 μm , inclusive; and a mean diameter at the opening of 1 - 100 μm , inclusive, more preferably 10 - 50 μm , inclusive. The radiographic intensifying screen provided onto the support surface with a great number of pits as specified above is particularly improved in the sharpness and the adhesion between the phosphor layer and the support.

Onto the surface of the support provided with a great number of the pits is provided a phosphor layer.

The phosphor layer comprises a binder and a phosphor in the form of particles dispersed therein. There are known a variety of phosphors employable for a radiographic intensifying screen. Examples of the phosphors preferably employable in the present invention include:

tungstate type phosphors such as CaWO_4 , MgWO_4 , and $\text{CaWO}_4:\text{Pb}$;

terbium activated rare earth metal oxysulfide type phosphors such as $\text{Y}_2\text{O}_2\text{S}:\text{Tb}$, $\text{Gd}_2\text{O}_2\text{S}:\text{Tb}$, $\text{La}_2\text{O}_2\text{S}:\text{Tb}$, $(\text{Y},\text{Gd})_2\text{O}_2\text{S}:\text{Tb}$, and $(\text{Y},\text{Gd})_2\text{O}_2\text{S}:\text{Tb},\text{Tm}$;

terbium activated rare earth phosphate type phosphors such as $\text{YPO}_4:\text{Tb}$, $\text{GdPO}_4:\text{Tb}$, and $\text{LaPO}_4:\text{Tb}$;

terbium activated rare earth oxyhalide type phosphors such as $\text{LaOBr}:\text{Tb}$, $\text{LaOBr}:\text{Tb},\text{Tm}$, $\text{LaOCl}:\text{Tb}$, $\text{LaOCl}:\text{Tb},\text{Tm}$, $\text{GdOBr}:\text{Tb}$, and $\text{GdOCl}:\text{Tb}$;

thulium activated rare earth oxyhalide type phosphors such as $\text{LaOBr}:\text{Tm}$ and $\text{LaOCl}:\text{Tm}$;

barium sulfate type phosphors such as $\text{BaSO}_4:\text{Pb}$, $\text{BaSO}_4:\text{Eu}^{2+}$, and $(\text{Ba},\text{Sr})\text{SO}_4:\text{Eu}^{2+}$;

divalent europium activated alkaline earth metal phosphate type phosphors such as $\text{Ba}_2(\text{PO}_4)_2:\text{Eu}^{2+}$, and $(\text{Ba},\text{Sr})_2(\text{PO}_4)_2:\text{Eu}^{2+}$;

divalent europium activated alkaline earth metal 5 fluorohalide type phosphors such as $\text{BaFCl}:\text{Eu}^{2+}$, $\text{BaFBr}:\text{Eu}^{2+}$, $\text{BaFCl}:\text{Eu}^{2+},\text{Tb}$, $\text{BaFBr}:\text{Eu}^{2+},\text{Tb}$, $\text{BaF}_2 \cdot \text{BaCl}_2 \cdot \text{KCl}:\text{Eu}^{2+}$, $\text{BaF}_2 \cdot \text{BaCl}_2 \cdot x\text{BaSO}_4 \cdot \text{KCl}:\text{Eu}^{2+}$, and $(\text{Ba},\text{Mg})\text{F}_2 \cdot \text{BaCl}_2 \cdot \text{KCl}:\text{Eu}^{2+}$;

iodide type phosphors such as $\text{CsI}:\text{Na}$, $\text{CsI}:\text{Tl}$, $\text{NaI}:\text{Tl}$, and $\text{KI}:\text{Tl}$;

10 sulfide type phosphors such as $\text{ZnS}:\text{Ag}$, $(\text{Zn},\text{Cd})\text{S}:\text{Ag}$, $(\text{Zn},\text{Cd})\text{S}:\text{Cu}$, and $(\text{Zn},\text{Cd})\text{S}:\text{Cu},\text{Al}$; and

hafnium phosphate type phosphors such as $\text{HfP}_2\text{O}_7:\text{Cu}$.

The above-described phosphors are given by no means to restrict the phosphor employable in the present invention. Any other phosphor can be optionally employed, provided that the phosphor emits light in the visible or near ultra-violet region upon exposed to radiation.

Examples of the binder contained in the phosphor layer include: natural polymers such as proteins (e.g. 20 gelatin), polysaccharides (e.g. dextran) and gum arabic; and synthetic polymers such as polyvinyl butyral, polyvinyl acetate, nitrocellulose, ethylcellulose, vinylidene chloride-vinyl chloride copolymer, polymethyl methacrylate, vinyl chloride-vinyl acetate copolymer, polyurethane, cellulose acetate butyrate, polyvinyl alcohol, and linear polyester. Particularly preferred binders 25 are nitrocellulose, linear polyester, and a mixture of nitrocellulose and linear polyester.

The phosphor layer can be formed on the support 30 in the following procedure.

The phosphor particles and binder are mixed in the presence of a sufficient amount of a solvent to prepare a coating dispersion containing the phosphor particles dispersed homogeneously in the binder solution. Examples of the solvent employable in the preparation of the coating dispersion include lower

alcohols such as methanol, ethanol, n-propanol, and n-butanol; chlorinated hydrocarbons such as methylene chloride and ethylene chloride; ketones such as acetone, methyl ethyl ketone and methyl isobutyl ketone; esters of lower alcohols with lower aliphatic acids such as methyl acetate, ethyl acetate, and butyl acetate; ethers such as dioxane, ethylene glycol monoethylether, and ethylene glycol monomethylether; and mixtures of the above-mentioned compounds.

10 The ratio between the binder and the phosphor in the coating dispersion may be determined according to the aimed characteristics of the radiographic intensifying screen and nature of the phosphor employed. Generally, the ratio therebetween is in the range of 15 from 1 : 1 to 1 : 100 (binder : phosphor, by weight), preferably 1 : 8 to 1 : 40.

20 The coating dispersion may contain a dispersing agent for assisting dispersion of the phosphor particles in the solution, a plasticizer for increasing the adhesion between the binder and the phosphor particles in the phosphor layer, and/or other additives. Examples of the dispersing agent include phthalic acid, stearic acid, capric acid, and hydrophobic surface active agents. Examples of the plasticizer include 25 phosphates such as triphenyl phosphate, tricresyl phosphate, and diphenyl phosphate; phthalates such as diethyl phthalate and dimethoxyethyl phthalate; glycolates such as ethylphthalyl ethyl glycolate and butylphthalyl butyl glycolate; and polyesters of polyethylene glycols with aliphatic dicarboxylic acids such as 30 polyester of triethylene glycol with adipic acid and polyester of diethylene glycol with succinic acid.

35 The coating dispersion containing the phosphor particles and binder prepared as above is coated evenly over the surface of the support provided with a great number of the pits having the specific dimension.

The coating procedure can be carried out by a conventional method such as a method using a doctor blade, roll coater, or knife coater.

The so coated layer is then heated slowly to dryness, so as to complete the formation of the phosphor layer on the support. The thickness of the phosphor layer varies depending upon the aimed characteristics of the intensifying screen, nature of the phosphor particles, the ratio between the binder and the phosphor particles, etc. Generally, the thickness of the phosphor layer is in the range of from 20 μm to 1 mm. The thickness in the range of 50 - 500 μm is preferred.

The phosphor layer can be provided onto the support in a different manner. For instance, the phosphor layer is independently prepared on a sheet such as a glass plate, metal plate, or plastic sheet, by the use of the aforementioned coating dispersion. The so prepared phosphor layer is then transferred onto the support by pressing the phosphor layer thereonto or laminating the phosphor layer on the support by the use of an adhesive agent.

As mentioned hereinbefore, the conventional radiographic intensifying screen generally has transparent film on the surface of the phosphor layer to protect the phosphor layer from physical and chemical deterioration. Accordingly, the radiographic intensifying screen of the present invention likewise has such a transparent film for the same purpose.

The transparent film can be provided onto the phosphor layer by coating the surface of the phosphor layer with a polymer solution containing a transparent polymer such as a cellulose derivative (e.g. cellulose acetate or nitrocellulose), or a synthetic polymer (e.g. polymethyl methacrylate, polyvinyl butyral, polyvinyl formal, polycarbonate, polyvinyl acetate, or vinyl chloride-vinyl acetate copolymer). Otherwise, a trans-

parent film prepared independently from polyethylene terephthalate, polyethylene, polyvinylidene chloride, polyamide or the like can be placed and fixed on the support by the use of an appropriate adhesive agent to 5 provide the protective film. The transparent protective film preferably has a thickness in the range of approximately 2 - 20 μm .

10 The present invention is further described by the following examples, which are by no means intended to restrict the invention.

Example 1

15 A surface of a polyethylene terephthalate film containing titanium dioxide (support, thickness 250 μm) was subjected to sand blasting employing silica sand in which more than approximately 50 % by weight of the silica particles had 100 - 150 mesh size. The sand blasting was carried out under centrifugal force by applying to the support surface the silica particles supplied from a drum rotating at a speed of 1900 r.p.m. 20 Thus, a rough surface was provided onto the support. The so prepared surface of the support was provided with a great number of pits having a mean diameter of 2 μm , a maximum depth of 7 μm , and a mean diameter at the opening of 20 μm .

25 Independently, to a mixture of a particulated terbium activated gadolinium oxysulfide phosphor ($\text{Gd}_2\text{O}_2\text{S:Tb}$) and a linear polyester resin were successively added methyl ethyl ketone and nitrocellulose (nitrofication degree 11.5 %) to prepare a phosphor 30 dispersion. To the phosphor dispersion were further added tricresyl phosphate, n-butanol and methyl ethyl ketone. The mixture was sufficiently stirred by means of a propeller agitator to obtain a homogeneous coating dispersion having a viscosity of 25 - 35 PS (at 35 25°C).

The coating dispersion was applied to the sand-blasted surface of the support placed horizontally on a glass plate. The coating procedure was carried out using a doctor blade. The support coated with the dispersion thereon was then placed in an oven and heated therein at a temperature slowly varying from 25 to 100°C. Thus, a phosphor layer having the thickness of approximately 180 μm was formed on the support.

On the phosphor layer of the support was placed a transparent polyethylene terephthalate film (thickness: 12 μm ; having a polyester adhesive layer) to combine the transparent film and the phosphor layer through the adhesive layer.

Thus, a radiographic intensifying screen consisting of a support, a phosphor layer and a transparent protective film was prepared.

Comparison Example 1

The procedure of Example 1 was repeated except that no sand blasting was applied to the polyethylene terephthalate film containing titanium dioxide, to prepare a radiographic intensifying screen consisting of a support, a phosphor layer and a transparent protective film.

Comparison Example 2

The procedure of Example 1 was repeated except that the sand blasting to the surface of the support was carried out using silica sand in which more than approximately 50 % by weight of the silica particles had approximately 300 mesh size. The so processed surface of the support was provided with a great number of pits having a mean diameter of 0.2 μm , a maximum depth of 0.8 μm , and a mean diameter at the opening of 0.5 μm .

A radiographic intensifying screen consisting of a support, a phosphor layer and a transparent protective film was then prepared in the same manner

as described in Example 1.

The radiographic intensifying screens prepared in the above-described examples were evaluated on the sharpness of image and the adhesion strength of the phosphor layer to the support. The evaluation methods are given below:

5 (1) Sharpness of image

The radiographic intensifying screen was combined with an X-ray film in a cassette, and exposed to X-rays of 80 KVp through an MTF chart. The film was then developed to obtain a visible image, and the MTF value was determined. In Table 1, the MTF value is set forth as a value (%) at the spacial frequency of 2 cycle/mm. A relative radiographic speed is also set forth in Table 1.

10 (2) Adhesion strength of phosphor layer to support

The radiographic intensifying screen was cut to give a test strip (1 cm x 6 cm), and an adhesive polyester tape was stuck on the protective film of the support. The so prepared test strip was then given on the adhesive tape side a U-shaped cut having a depth reaching the interface between the phosphor layer and the support by means of a knife. The U-shaped cut was made along the longitudinal direction of the strip.

15 25 In a tensile testing machine (Tensilon UTM-11-20 manufactured by Toyo Baldwin Co., Ltd., Japan), the U-shaped cut portion and the remaining strip portion were forced to separate from each other by pulling up the tab end of the cut portion at a rate of 2 cm/min.

20 30 The adhesion strength was determined just when a 1-cm long portion of the phosphor layer was separated from the support. The strength is expressed in terms of the force F (g/cm).

The results are set forth in Table 1.

Table 1

	Ex. 1	Com. Ex. 1	Com. Ex. 2
Sharpness	0.27	0.23	0.24
Adhesion strength	300	100	120
Relative radiographic speed	≤95	100	95 - 100

Example 2

The sand blasting procedure of Example 1 was repeated except that the polyethylene terephthalate film containing titanium dioxide was replaced with a polyethylene 5 terephthalate film having the same thickness but containing carbon black. The so processed surface of the support was provided with a great number of pits having a mean diameter of 2 μm , a maximum depth of 7 μm , and a mean diameter at the opening of 20 μm .

10 Subsequently, a radiographic intensifying screen consisting of a support, a phosphor layer and a transparent protective film was prepared in the same manner as described in Example 1.

Comparison Example 3

15 The procedure of Example 2 was repeated except that no sand blasting was applied to the polyethylene terephthalate film containing carbon black, to prepare a radiographic intensifying screen consisting of a support, a phosphor layer and a transparent protective 20 film.

Each of the screens prepared in Example 2 and Comparison Example 3 was evaluated on the sharpness of image and the adhesion strength of the phosphor layer to the support in the same manner described previously.

25 The results are set forth in Table 2.

Table 2

	Ex. 2	Com. Ex. 3
Sharpness	0.34	0.28
Adhesion strength	350	140
Relative radiographic speed	95 - 100	100

Example 3

5 The procedure of Example 2 was repeated except that the particulated terbium activated gadolinium oxysulfide phosphor was replaced with a particulated divalent europium activated barium fluorobromide ($BaFBr:Eu^{2+}$) phosphor, to prepare a radiographic intensifying screen consisting of a support, a phosphor layer, and a transparent protective film.

Comparison Example 4

10 The procedure of Example 3 was repeated except that no sand blasting was applied to the polyethylene terephthalate film containing carbon black, to prepare a radiographic intensifying screen consisting of a support, a phosphor layer and a transparent protective film.

15 Each of the screens prepared in Example 3 and Comparison Example 4 was evaluated on the sharpness of image and the adhesion strength of the phosphor layer to the support in the same manner described previously. The results are set forth in Table 3.

Table 3

	Ex. 3	Com. Ex. 4
Sharpness	0.38	0.34
Adhesion strength	320	150
Relative radiographic speed	95 - 100	100

Example 4

The procedure of Example 2 was repeated except that the particulated divalent europium activated barium fluorobromide ($BaFBr:Eu^{2+}$) phosphor was replaced with 5 a calcium tungstate ($CaWO_4$) phosphor, to prepare a radiographic intensifying screen consisting of a support, a phosphor layer, and a transparent protective film.

Comparison Example 5

10 The procedure of Example 4 was repeated except that no sand blasting was applied to the polyethylene terephthalate film containing carbon black, to prepare a radiographic intensifying screen consisting of a support, a phosphor layer and a transparent protective film.

15 Each of the screens prepared in Example 4 and Comparison Example 5 was evaluated on the sharpness of image and the adhesion strength of the phosphor layer to the support in the same manner described previously.

20 The results are set forth in Table 4.

Table 4.

	Ex. 4	Com. Ex. 5
Sharpness	0.54	0.50
Adhesion strength	400	220
Relative radiographic speed	95 - 100	100

As described previously, the radiation image conversion panel of this invention includes a radiation image storage panel.

As a method of obtaining a radiation image, a radiation image recording and reproducing method described in U.S. Patents No. 3,859,527, No. 4,258,264, No. 4,236,078, and No. 4,239,968 is paid much attention. In this radiation image recording and reproducing method, there is employed a radiation image storage panel comprising a stimulable phosphor which emits light when stimulated by an electromagnetic wave such as visible light and infrared rays (referred to hereinafter as "stimulating rays") after exposure to a radiation. The term "radiation" as used herein means an electromagnetic wave or a corpuscular radiation, such as X-rays, α -rays, β -rays, γ -rays, high energy neutron rays, cathode rays, vacuum ultraviolet rays, or ultraviolet rays. The above-cited method involves steps of (1) causing the stimulable phosphor of the panel to absorb a radiation having passed through an object; (2) scanning the panel with stimulating rays to sequentially release the radiation energy stored in the panel as light emission; and (3) electrically processing the emitted light to give an image.

In the radiation image recording and reproducing method, it is desired that a radiation image is recorded and reproduced with high sensitivity, as well as that the quality of image such as sharpness obtained by the method is high.

The radiation image storage panel employable for carrying out the radiation image recording and reproducing method likewise comprises a support and at least one phosphor layer comprising a binder and a phosphor dispersed therein. However, the phosphor contained in this phosphor layer ought to be a stimulable phosphor.

The favorable effects such as the improvements

in the sharpness of image and the adhesion between the phosphor layer and the support as described for the radiographic intensifying screen are also observed on the radiation image storage panel using a support provided on the surface with a great number of pits having the specifically determined size, that is, a mean depth of at least 1 μm , a maximum depth of more than 1 μm to 100 μm , and a mean diameter at the opening of at least 1 μm . The preferred ranges of the dimension of the pits described hereinbefore with respect to the radiographic intensifying screen have been also confirmed in the radiation image storage panel.

As mentioned above, there are no substantial difference of the material and constitution of the panel (screen) between the radiographic intensifying screen and the radiation image storage panel except that the stimulable phosphor ought to be employed in the latter. Accordingly, the stimulable phosphor is specifically stated hereinbelow for description of the radiation image storage panel of the invention.

Examples of the stimulable phosphors employable in the present invention include the following phosphors.

- i) SrS:Ce,Sm , SrS:Eu,Sm , $\text{La}_2\text{O}_2\text{S:Eu,Sm}$, and $(\text{Zn,Cd})\text{S:MnX}$ wherein X is halogen, as described in U.S. Patent No. 3,859,527;
- ii) ZnS:Cu,Pb , $\text{BaO.xAl}_2\text{O}_3:\text{Eu}$ wherein \underline{x} is a number satisfying the condition of $0.8 \leq \underline{x} \leq 10$, and $\text{M}^{\text{II}}\text{O.xSiO}_2:\text{A}$ wherein M^{II} is at least one divalent metal selected from the group consisting of Mg, Ca, Sr, Zn, Cd and Ba, A is at least one element selected from the group consisting of Ce, Tb, Eu, Tm, Pb, Tl, Bi and Mn, and \underline{x} is a number satisfying the condition of $0.5 \leq \underline{x} \leq 2.5$, as described in U.S. Patent No. 4,236,078;
- iii) LnOX:xA wherein Ln is at least one element selected from the group consisting of La, Y, Gd and

Lu, X is Cl and/or Br, A is Ce and/or Tb, and x is a number satisfying the condition of $0 < x \leq 0.1$, as described in the above-mentioned U.S. Patent No. 4,236,078;

iv) $(Ba_{1-x}, M^{II}x)FX:yA$ wherein M^{II} is at least one divalent metal selected from the group consisting of Mg, Ca, Sr, Zn and Cd, X is at least one halogen selected from the group consisting of Cl, Br and I, A is at least one element selected from the group consisting of Eu, Tb, Ce, Tm, Dy, Pr, Ho, Nd, Yb and Er, and x and y are numbers satisfying the conditions of $0 \leq x \leq 0.6$ and $0 < y \leq 0.1$, respectively, as described in U.S. Patent No. 4,239,968;

v) $(Ba_{1-x-y}, Mg_x, Ca_y)FX:aEu^{2+}$ wherein X is at least one halogen selected from the group consisting of Cl, Br and I, x and y are numbers satisfying the conditions of $0 < x+y \leq 0.6$ and $xy \neq 0$, and a is a number satisfying the condition of $10^{-6} \leq a \leq 5 \times 10^{-2}$, as described in Japanese Patent Provisional Publication No. 55(1980)-12143;

vi) $BaFX:xCe,yA$ wherein X is at least one halogen selected from the group consisting of Cl, Br and I, A is at least one element selected from the group consisting of In, Ta, Gd, Sm and Zr, and x and y are numbers satisfying the conditions of $0 < x \leq 2 \times 10^{-1}$ and $0 < y \leq 5 \times 10^{-2}$, respectively, as described in U.S. Patent No. 4,261,854;

vii) $BaF_2 \cdot aBaX_2 \cdot bMe^I F \cdot cMe^{II} F_2 \cdot dMe^{III} F_3 \cdot eLn$ wherein X is at least one halogen selected from the group consisting of Cl, Br and I, Me^I is Li and/or Na, Me^{II} is at least one divalent metal selected from the group consisting of Be, Ca and Sr, Me^{III} is at least one trivalent metal selected from the group consisting of Al, Ga, Y and La, Ln is at least one element selected from the group consisting of Eu, Ce and Tb, and a, b, c, d and e are numbers satisfying the conditions of $0.90 \leq a \leq 1.05$, $0 \leq b \leq 0.9$, $0 \leq c \leq 1.2$, $0 \leq d \leq 0.03$, $10^{-6} \leq e \leq 0.03$, respectively and $b=c=d \neq 0$, as described in Japanese

Patent Provisional Publication No. 56(1981)-2385;

5 viii) complex halide phosphor in which MgF_2 is added to the above-mentioned phosphor of Japanese Patent Provisional Publication No. 56(1981)-2385, as described in Japanese Patent Provisional Publication No. 56(1981)-2386;

10 ix) $BaFX \cdot aLiX' \cdot bBeX''_2 \cdot cM^{III}X'''_3 : dA$ wherein each of X, X', X'' and X''' are at least one halogen selected from the group consisting of Cl, Br and I, M^{III} is Al and/or Ga, A is at least one element selected from the group consisting of Eu, Tb, Ce, Tm, Dy, Pr, Ho, Nd, Yb, Er, Gd, Lu, Sm and Y, and a, b, c and d are numbers satisfying the conditions of $0 \leq a \leq 0.1$, $0 \leq b \leq 0.1$, $0 \leq c \leq 0.1$, $10^{-6} \leq d \leq 0.2$, respectively and $0 \leq a+b+c \leq 0.1$, as described 15 in Japanese Patent Provisional Publication No. 56(1981)-74175; and the like.

20 The stimulable phosphor preferably is a divalent europium activated complex halide phosphor. Out of the divalent europium activated complex halide phosphor, a divalent europium activated alkaline earth metal fluorohalide phosphor is preferred. Out of the divalent europium activated alkaline earth metal fluorohalide phosphor, a divalent europium activated barium fluorohalide phosphor is preferred. Out of the divalent europium activated barium fluorohalide phosphor, a divalent europium activated barium fluorobromide ($BaFBr:Eu^{2+}$) phosphor 25 is particularly preferred.

30 From the viewpoint of practical use, the stimulable phosphor preferably is a phosphor which emits light in the wavelength region ranging from 300 nm to 600 nm when stimulated by stimulating rays in the wavelength region ranging from 450 nm to 1100 nm, particularly from 450 nm to 750 nm.

35 The radiation image storage panel of the present invention consists essentially of a phosphor layer comprising a binder and a stimulable phosphor having the aforementioned

particle size distribution and being dispersed in the binder. When the phosphor layer is self-supporting, the radiation image storage panel can consist solely thereof. However, the panel generally comprises a support and the phosphor layer provided thereonto. There is no specific limitation on the binder employed in the phosphor layer. The ratio between the amount of the binder and the amount of the phosphor generally ranges from 1:1 to 1:80 (binder : phosphor) by weight and preferably ranges from 1:5 to 1:50 by weight, and the thickness of the phosphor layer generally ranges from 20 μm to 1 mm, preferably from 100 μm to 500 μm , depending upon the purpose. There is no specific limitation on the support employed in the invention, but the support preferably employed is a plastic sheet having flexibility.

In the radiation image storage panel of the present invention, one or more layers can be optionally placed between the support and the phosphor layer, such as a light reflecting layer, a light absorbing layer and an undercoating layer (subbing layer).

Further, a protective layer is generally provided onto the phosphor layer in a thickness ranging from 3 μm to 20 μm , to chemically and physically protect the phosphor layer. Furthermore, the radiation image storage panel of the present invention can be colored with a coloring agent, to enhance the sharpness of the image, as described in Japanese Patent Provisional Publication No. 56(1981)-163500. For the same purpose, a white powder can be dispersed in the phosphor layer of the panel, as described in U.S. Patent No: 4,350,893.

It is assumed that the improvement of the sharpness of image accomplished in the storage panel is given by the fact that the stimulating rays impinged upon the phosphor layer are substantially free from the mirror reflection by the support surface which causes reduction of the sharpness, because of the provision of the pits having the specified dimension. In this case, most of the reflected light is presumably enclosed in the pit.

The radiation image storage panel of the present invention is further described by the following examples, which are by no means intended to restrict the invention.

Example 5

5 A surface of a polyethylene terephthalate film containing carbon black (support, thickness 250 μm) was subjected to sand blasting employing silica sand in which more than approximately 50 % by weight of the silica particles had 100 - 150 mesh size. The sand blasting
10 was carried out under centrifugal force by applying to the support surface the silica particles supplied from a drum rotating at a speed of 1900 r.p.m. Thus, a rough surface was provided onto the support. The so prepared surface of the support was provided with a
15 great number of pits having a mean diameter of 2 μm , a maximum depth of 7 μm , and a mean diameter at the opening of 20 μm .

Independently, to a mixture of a particulated divalent europium activated barium fluorobromide (BaFBr:Eu^{2+})
20 stimulable phosphor and a linear polyester resin were successively added methyl ethyl ketone and nitrocellulose (nitrofication degree 11.5 %) to prepare a phosphor dispersion. To the phosphor dispersion were further added tricresyl phosphate, n-butanol and methyl
25 ethyl ketone. The mixture was sufficiently stirred by means of a propeller agitator to obtain a homogeneous coating dispersion having a viscosity of 25 - 35 PS (at 25°C).

30 The coating dispersion was applied to the sand-blasted surface of the support placed horizontally on a glass plate. The coating procedure was carried out using a doctor blade. The support coated with the dispersion thereon was then placed in an oven and heated therein at a temperature slowly varying from 25 to 100°C.
35 Thus, a phosphor layer having thickness of approximately 180 μm was produced on the support.

On the phosphor layer of the support was placed a transparent polyethylene terephthalate film (thickness: 12 μm ; having a polyester adhesive layer) to combine the transparent film and the phosphor layer through the adhesive layer.

Thus, a radiation image storage panel consisting of a support, a phosphor layer and a transparent protective film was prepared.

Comparison Example 6

The procedure of Example 5 was repeated except that the sand blasting to the surface of the support was carried out using silica sand in which more than approximately 50 % by weight of the silica particles had approximately 300 mesh size. The so processed surface of the support was provided with a great number of pits having a mean diameter of 0.2 μm , a maximum depth of 0.8 μm , and a mean diameter at the opening of 0.5 μm .

A radiation image storage panel consisting of a support, a phosphor layer and a transparent protective film was then prepared in the same manner as described in Example 5.

The radiation image storage panels prepared in Example 5 and Comparison Example 6 were evaluated on the sharpness of image and the adhesion strength of the phosphor layer to the support. The evaluation methods are given below:

(1) Sharpness of image

The panel was exposed to X-rays of 80 KVp through an MTF chart made of lead, and subsequently the panel was scanned with a He-Ne laser beam. The light emitted by the phosphor layer of the panel was detected and converted to the corresponding electric signal by means of the above-mentioned photosensor. The electric signal was converted to the corresponding image signal by means of an analogue-digital converter, and the image

signal was recorded on a magnetic tape. The magnetic tape was then analyzed in a computer to produce the modulation transfer function (MTF) of the X-ray image recorded thereon. The MTF value was produced and given
5 as an MTF value (%) at the spacial frequency of 2 cycle/mm.

(2) Adhesion strength of phosphor layer to support
Same as previously described for the determination
of the adhesion strength of the radiographic intensify-
10 ing screen.

The results are set forth in Table 5. A relative
sensitivity is also set forth in Table 5.

Table 5

	Ex. 5	Com. Ex. 6
Sharpness	0.41	0.36
Adhesion strength	170	75
Relative sensitivity	84	85

Example 6

The procedure of Example 5 was repeated except
15 that the phosphor layer was formed in thickness of 200
μm, to prepare a radiation image storage panel consist-
ing of a support, a phosphor layer and a trans-
parent protective film.

Comparison Example 7

20 The procedure of Comparison Example 6 was repeated
except that the phosphor layer was formed in thickness
of 200 μm, to prepare a radiation image storage panel
consisting of a support, a phosphor layer and a
transparent protective film.

25 Each of the panel prepared in Example 6 and Com-
parison Example 7 was evaluated on the sharpness of

image and the adhesion strength of the phosphor layer to the support in the same manner described previously. The results are set forth in Table 6.

Table 6

	Ex. 6	Com. Ex. 7
Sharpness	0.50	0.44
Adhesion strength	170	75
Relative sensitivity	59	63

Example 7

5 The procedure of Example 5 was repeated except that the polyethylene terephthalate film containing carbon black was replaced with a polyethylene terephthalate film having the same thickness but containing titanium dioxide, to prepare a radiation image
10 storage panel consisting of a support, a phosphor layer and a transparent protective film.

Comparison Example 8

The procedure of Comparison Example 6 was repeated except that the polyethylene terephthalate film containing carbon black was replaced with a polyethylene terephthalate film having the same thickness but containing titanium dioxide, to prepare a radiation image storage panel consisting of a support, a phosphor layer and a transparent protective film.

20 Each of the panels prepared in Example 7 and Comparison Example 8 was evaluated on the sharpness of image and the adhesion strength of the phosphor layer to the support in the same manner described previously. The results are set forth in Table 7.

Table 7

	Ex. 7	Com. Ex. 8
Sharpness	0.33	0.29
Adhesion strength	170	75
Relative sensitivity	97	100

Example 8

The procedure of Example 5 was repeated except that the thickness of the phosphor layer was varied in the range of 200 - 300 μm , to prepare a radiation image storage panel consisting of a support, a phosphor layer and a transparent protective film.

Comparison Example 9

The procedure of Example 8 was repeated except that no sand blasting was applied to the surface of the support, to prepare a radiation image storage panel consisting of a support, a phosphor layer and a transparent film.

The sharpness of image was evaluated on a variety of the panels prepared in Example 8 and Comparison Example 9. The results are illustrated graphically in Figure 1.

In Figure 1, the relationship between the sharpness and the relative sensitivity observed in the panels prepared in Example 8 is given under the indication A, while the relationship therebetween observed in the panels prepared in Comparison Example 9 is given under the indication B.

From the results given in Figure 1, the radiation image storage panel of the invention shows prominently higher sharpness of image than the radiation image storage panel prepared according to the conventional method, under the conditions that the sensitivity is set at the same value.

CLAIMS:

1. A radiographic intensifying screen comprising a support and at least one phosphor layer comprising a binder and a phosphor dispersed therein, in which the support is provided on the surface facing the phosphor layer with a great number of pits having a mean depth of at least 1 μm , a maximum depth of more than 1 μm to 100 μm , and a mean diameter at the opening of at least 1 μm .
- 10 2. The radiographic intensifying screen as claimed in Claim 1, in which the pits have a mean depth of 1 - 10 μm , inclusive, a maximum depth of more than 1 μm to 50 μm , and a mean diameter at the opening of 1 - 100 μm , inclusive.
- 15 3. The radiographic intensifying screen as claimed in Claim 2, in which the pits have a mean depth of 1 - 5 μm , inclusive, a maximum depth of 2 - 20 μm , inclusive, and a mean diameter at the opening of 10 - 50 μm , inclusive.
- 20 4. The radiographic intensifying screen as claimed in any one of Claims 1 through 3, in which the support is made of a plastic film.
5. The radiographic intensifying screen as claimed in any one of Claims 1 through 3, in which the binder comprises a linear polyester as a principal component.
- 25 6. The radiographic intensifying screen as claimed in any one of Claims 1 through 3, in which the binder comprises nitrocellulose as a principal component.

7. The radiographic intensifying screen as claimed in any one of Claims 1 through 3, in which the binder comprises a mixture of a linear polyester and nitrocellulose as a principal component.

5 8. The radiographic intensifying screen as claimed in any one of Claims 1 through 3, in which the pits are those formed by applying hard solid particles onto the surface of support at high speed.

10 9. A process for the preparation of a radiographic intensifying screen comprising a support and at least one phosphor layer comprising a binder and a phosphor dispersed therein, in which the support is provided on the surface facing the phosphor layer with a great number of pits having a mean depth of at least 1 μm , a maximum depth of more than 1 μm to 100 μm , and a mean diameter at the opening of at least 1 μm , which comprises applying hard solid particles onto the surface of support at high speed to form the pits.

15 10. A process as claimed in Claim 9, in which the support is made of a plastic film.

20 11. A radiation image storage panel comprising a support and at least one phosphor layer comprising a binder and a stimulable phosphor dispersed therein, in which the support is provided on the surface facing the phosphor layer with a great number of pits having a mean depth of at least 1 μm , a maximum depth of more than 1 μm to 100 μm , and a mean diameter at the opening of at least 1 μm .

25 12. The radiation image storage panel as claimed in Claim 11, in which the pits have a mean depth of 1 - 10 μm , inclusive, a maximum depth of more than 1 μm

to 50 μm , and a mean diameter at the opening of 1 - 100 μm , inclusive.

13. The radiation image storage panel as claimed in Claim 12, in which the pits have a mean depth of 1 - 5 μm , inclusive, a maximum depth of 2 - 20 μm , inclusive, and a mean diameter at the opening of 10 - 50 μm , inclusive.

14. The radiation image storage panel as claimed in any one of Claims 11 through 13, in which the support 10 is made of a plastic film.

15. The radiation image storage panel as claimed in any one of Claims 11 through 13, in which the binder comprises a linear polyester as a principal component.

16. The radiation image storage panel as claimed in 15 any one of Claims 11 through 13, in which the binder comprises nitrocellulose as a principal component.

17. The radiation image storage panel as claimed in any one of Claims 11 through 13, in which the binder comprises a mixture of a linear polyester and nitro-cellulose as a principal component.

any one of/
18. The radiation image storage panel as claimed in Claims 11 through 13, in which the stimulable phosphor is a divalent europium activated alkaline earth metal fluorohalide.

25 19. The radiation image storage panel as claimed in any one of Claims 11 through 13, in which the pits are those formed by applying hard solid particles onto the surface of support at high speed.

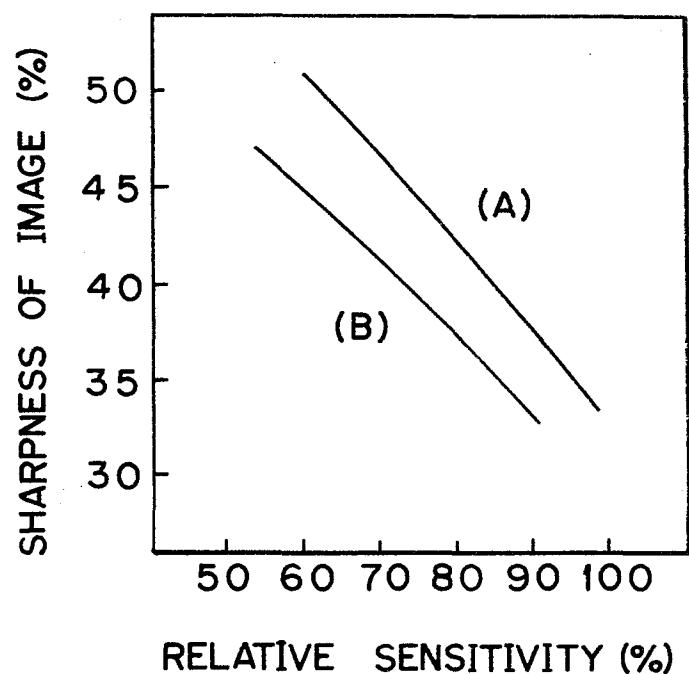
20. A process for the preparation of a radiation image storage panel comprising a support and at least one phosphor layer comprising a binder and a stimulable phosphor dispersed therein, in which the support is provided on 5 the surface facing the phosphor layer with a great number of pits having a mean depth of at least 1 μm , a maximum depth of more than 1 μm to 100 μm , and a mean diameter at the opening of at least 1 μm , which comprises applying hard solid particles onto the surface of support 10 at high speed to form the pits.

21. A process as claimed in Claim 20, in which the support is made of a plastic film.

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FIG. I





DOCUMENTS CONSIDERED TO BE RELEVANT		Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int. Cl. 3)
Category	Citation of document with indication, where appropriate, of relevant passages		
X, Y	FR-A- 735 923 (SIEMENS-REINIGER-VEIFA) * Whole document *	1-21	G 03 C 5/17
X, Y	DE-C- 743 340 (K. STAIGER) * Figure; whole document *	1-21	
Y	US-A-4 204 125 (CAROL L. FATUZZO) * Figure; abstract *	1-21	
Y	RESEARCH DISCLOSURE, no. 164, December 1977, pages 53-56, disclosure no. 16435, Homewell Havant, Hampshire, GB. Chen-I LU et al.: "Phosphorescent screens" * Whole article *	1-21	
A	GB-A- 926 086 (NEUGASS) * Figure 2 *	1	G 03 C 5/17 G 21 K 4/00
A	DE-C- 242 129 (REINIGER) * Page 1, line 24 *	6,16	

The present search report has been drawn up for all claims			
Place of search THE HAGUE	Date of completion of the search 27-06-1983	Examiner RASSCHAERT A.	
CATEGORY OF CITED DOCUMENTS		T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document	
X : particularly relevant if taken alone			
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