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(54) **INTRAOPERATIVE AND ENDOSCOPIC TUMOR DETECTION AND THERAPY**

INTRAOPERATIVE ERSTELLUNG DES BEFUNDES UND TUMOR-THERAPIE MITTELS
ENDOSKOP

DETECTION ET THERAPIE INTRA-OPERATOIRES ET ENDOSCOPIQUES DE TUMEURS

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(56) References cited:

US-A- 4 266 549	US-A- 4 348 376
US-A- 4 361 544	US-A- 4 431 626
US-A- 4 444 744	US-A- 4 460 559
US-A- 4 460 561	US-A- 4 595 014
US-A- 4 624 846	

• **Aitken et al 1984. Dis. of the Colon and Rectum**
27:279-282

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The file contains technical information submitted
after the application was filed and not included in this
specification

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Description

BACKGROUND OF THE INVENTION

The present invention is useful in improved methods for detecting tumors in the course of intraoperative and endoscopic examination using a small radiation detecting probe, whereby background radiation is reduced, or compensated for, and discrimination between tumor and non-tumor tissue is thereby enhanced.

Surgical resection remains the primary curative approach in the management of cancer. Radioimmuno-detection (RAID) is used to locate and stage tumors, and to monitor post-operative patients, typically using serum levels of markers (antigens) produced by and/or associated with tumors ("tumor markers"), e.g., carcinoembryonic antigen (CEA), as both a pre-operative diagnostic predicate and a post-operative diagnostic indicator of recurrence. Antibodies and/or antibody fragments which specifically bind tumor markers ("anti-cancer antibodies") are used as carriers for radiolabels in imaging and for in vitro assays. It will be appreciated that a tumor antigen can serve as a target for an antibody carrier even if it is not present in serum in a detectable amount.

Resolution is affected by several factors that can limit the size of a tumor, especially a metastasis, which can be imaged by RAID. Non-invasive RAID is inherently limited by the distance between the radiation detector and the tumor. In the case of small, deep-seated metastatic tumors, this becomes the limiting factor in their detection.

Second look surgery has been practiced where recurrence of a previously excised primary tumor was indicated by elevated levels of tumor marker, e.g., CEA. Recently, a small gamma detection probe has been developed which is capable of detecting gamma emission at short distances. Its intraoperative use in second look surgery has been reported to provide important information to the surgeon for determining safe margins for resection and for detecting small metastases, by Aitken et al., *Dis. Colon & Rectum*, 27, 279-282(1984).

Nevertheless, elevated background radiation levels can interfere with and vitiate the advantage of short measuring distances in this technique. In addition, non-specific immunoglobulin uptake by tumor tissue can complicate diagnosis. Moreover, background radiation due to non-specific uptake of labeled antibody often increases with time after injection thereof and clearance of non-specific background radioactivity can require several days for optimal detection of tumors. A need therefore continues to exist for methods for reducing background levels and compensating for non-specific immunoglobulin uptake so that enhanced resolution can be achieved for short-range intraoperative and endoscopic tumor detection and therapy.

OBJECTS OF THE INVENTION

The principal object of the present invention is to improve short-range intraoperative and endoscopic detection of tumors whereby discrimination between tumor and non-tumor tissue is enhanced so that smaller tumors can be detected and appropriate margins can be determined more accurately for surgical resection, intraoperative irradiation and/or endoscopic tumor removal.

Upon further study of the specification and appended claims, further objects and advantages of this invention will become apparent to those skilled in the art.

SUMMARY OF THE INVENTION

In one aspect, our invention provides the use of

(a) a marker specific primary antibody or antibody fragment specific against a marker produced by or associated with a tumor and labeled with a pharmacologically inert radioisotope capable of detection at close range with a radiation detection probe; and

a background compensation or reduction agent which is either of

(b) a dual isotope correction agent radiolabeled with a radioisotope emitting an energy which is separately detectable at close range from the primary antibody label using said radiation detection probe, said agent comprising irrelevant immunoglobulin from the same or different species as that used to prepare the primary antibody and not being an organ, blood pool or interstitial fluid non-tumor specific contrast agent, the irrelevant immunoglobulin being so labeled that the kinetics and distribution of the radiolabeled primary antibody and irrelevant immunoglobulin in the patient are substantially the same during the time required for scanning;

or

(b') unlabeled second antibody which specifically binds said primary antibody or the labeling moiety thereof,

in the preparation of an agent for use in a method for short-range intraoperative or endoscopic detection of a tumor, wherein a surgical or endoscopy patient is injected parenterally with a radiolabeled primary antibody which specifically binds a marker produced by or associated with a tumor, the surgically exposed or endoscopically accessed interior of a body cavity of said patient is scanned at close range with a radiation detection probe, and the sites of accretion of said labeled antibody are located by detecting elevated levels of radiation at said sites with said probe,

and wherein non-target background radiation is compensated for or reduced by injecting said patient parenterally, either concurrently or sequentially, with:

(a) a contrast or subtraction agent radiolabeled with a radioisotope emitting an energy which is separately detectable from the primary antibody label using a radiation detection probe; radiation detected from emission of the contrast or subtraction agent being used to better define the tumor, wherein said contrast or subtraction agent is a dual isotope correction agent comprising irrelevant immunoglobulin from the same or different species as that used to prepare the primary antibody and not being an organ, blood pool or interstitial fluid non-tumor specific contrast agent, the irrelevant immunoglobulin being so labeled that the kinetics and distribution of the radio-labeled primary antibody and irrelevant immunoglobulin in the patient are substantially the same during the time period required for scanning; and wherein the ratio of primary antibody label activity to irrelevant immunoglobulin label activity at a selected site is compared to said ratio at a known non-tumor site, whereby an elevated level of primary antibody label accretion due to antigen-antibody complex formation at said selected site can be discriminated;

or

(b) unlabeled second antibody which specifically binds the primary antibody or the labeling moiety thereof, the second antibody being injected at a time after the injection of the primary antibody sufficient to permit specific uptake of the primary antibody by a tumor in the body cavity, and in an amount sufficient to reduce the circulating level of the primary antibody label by at least about 10-85%, or to increase the localization ratio of the labeled primary antibody by at least about 20%, within about 2-72 hours following injection of the second antibody, whereby background levels of nonspecifically distributed primary antibody and/or label are reduced in the body cavity, and the sites of accretion of labeled primary antibody as well as the level of specific uptake thereof are more effectively discriminated.

Thus, the use of endoscopic detection, in combination with radiolabeled antibodies, to detect and define tumors and tumor margins represents a novel technique in its own right, even without the improved background correction and/or reduction methods described herein with respect to surgical techniques where the patient is operated upon to open and expose an area of possible tumor growth. The further combination of such endoscopic detection with background correction or reduction techniques and/or with means for coagulating and/or removing tumor tissue and immediately adjacent tumor margins through the endoscope represent embodiments which improve upon this basic technique.

The technique of injecting labeled specific antibody and separately detectably labeled irrelevant antibody for non-specific background correction is referred to herein,

interchangeably, as "subtraction" or "dual isotope correction".

Combinations of the foregoing methods can also be used to further enhance the resolution of the tumor detection process. For example, subtraction can be combined with second antibody clearance to produce even greater differentiation between specific uptake of labeled antibody and background due to circulating labeled antibody, free label and/or non-specific uptake of immunoglobulin and/or label. Hybrid antibodies which specifically bind both primary antibody and label can be used to clear background label regardless of whether the integrity of the antibody conjugate is maintained or whether the label has become detached from the antibody or antibody has metabolized, fragmented or has otherwise been degraded. In this context, the term "label" refers to whatever carrier for the label is used to bind the radionuclide to the antibody, e.g., a chelator for a radiometal ion, a metabolite and/or fragment of the antibody bearing the radionuclide, e.g., a tyrosine residue substituted with one or more atoms of a radioactive iodine isotope, whether as such or incorporated in a longer oligopeptide or further metabolized, or a radioiodide ion or other iodinated species, or the like.

DETAILED DISCUSSION

It must be recognized that the present method relates to intraoperative or endoscopic examination of tissues and/or organs with a radiation detector capable of close approach to suspected sites of tumor recurrence, metastasis or incomplete removal, rather than a non-invasive tumor imaging procedure. Subtraction methods, as hitherto practiced, rely on normalizing counts emitted from two different radionuclides having two different energy ranges. The counts are accumulated, generally over a time of less than one hour to several hours, by scanning a selected body region, using a gamma camera equipped with a suitable collimator. The counts are then normalized, pixel-by-pixel, after which the processor constructs an image by first subtracting the counts calculated to correspond to background from the specific label counts for each pixel, and then displays the result, e.g. as a graded color or black and white image.

In contrast to the foregoing techniques, the method of the present invention does not involve processing of images, both target specific and non-target specific. Rather, it enables a surgeon or clinician, through the use of an intraoperative probe or an endoscope, to scan areas of suspected tumor growth relatively quickly and use the level of counts, or the differences in counts in selected scan sites and the ratio of tumor to non-tumor counts, to more precisely discriminate tumor tissue from non-tumor tissue and thereby more precisely define tumor borders for surgical resection or diagnostic evaluation, or for external radiation therapy.

Earlier workers have indicated the desirability of reducing background counts in an intraoperative probe

method without suggesting how this can be achieved. The present method provides solutions to this problem. By reducing non-target radioactivity, either directly or by compensating for it so that it can be effectively factored out, and thereby increasing the ratio of counts due to specific uptake to those due to background, a better discrimination can be achieved, to permit improved demarcation of tumor sites and borders.

The invention also embraces embodiments wherein optimal times for surgery and intraoperative radiodetection and radiotherapy are indicated. Both subtraction methods and second antibody clearance for enhanced imaging can optimize images using repeated scans at different intervals following injection of primary antibody and/or second antibody. On the other hand, for a surgical procedure, it will be necessary to optimize the injections of primary and/or second antibody to coincide with the surgical schedule. By taking a blood sample at intervals after injection of second antibody, the concentration of radioactivity in the circulation can serve as an indicator of the best time for surgery and intraoperative radiation detection, and/or whether a repeated dose of second antibody is indicated.

Use of a radionuclide label with both therapeutic and diagnostic emissions permits further refinement in the foregoing techniques. For example, an antibody labeled with Cu-67, having both beta and gamma emission of appropriate energies, permits the surgeon to detect and excise foci of high activity, using primarily the gamma emission, and at the same time to permit areas of slightly elevated activity to benefit from the therapeutic, i.e., cytotoxic to tumor cells, radiation, primarily the beta emission, or to target these areas for external radiation treatment.

The short-range tumor detection method according to the invention uses a detector capable of detecting radiation emitted from a radiolabel bound to the primary antibody. The radiation can be alpha, gamma, beta, positron or any other detectable radiation which can be produced by a convenient label capable of attachment to an antibody. For example, a gamma detector suitable for such a function has been reported by Aitken et al., *Dis. Colon & Rectum*, 27, 279-282 (1984). These authors describe a hand-held gamma probe using a cadmium telluride scintillation crystal, a preamplifier and an amplifier with a digital readout displaying the radioactive counts (Radiation Monitoring Devices, Watertown, MA.). The scintillation crystal is housed in a 16-mm diameter lead collimator with a 4-mm aperture. This device has been shown to detect tumor with radiolabeled antibody injected intraperitoneally, and to distinguish tumor tissue from nearby non-tumor tissue. No subtraction or enhanced clearance was used or suggested by these authors, nor was any use outside other than in a surgical procedure suggested. Further, the method requires long delays between injection and probing, with unpredictable results obtained from patient to patient.

It will be apparent to the ordinary skilled artisan that other such detectors can be used and that the detector

is not limited to gamma radiation. It will also be apparent that the detector can be made to discriminate between different energies of incident radiation, e.g., between gamma radiation in different ranges within the broad 50 - 500 KeV range which is normally used for gamma scintillation counters and/or between alpha, gamma and beta radiation emitted by labels on the specific and the indifferent antibodies. Thus, the invention is not limited by the type of detector used, but is generally applicable to reducing background radiation levels regardless of the type of radiation used for detection or radionuclide(s) used to label the primary antibody and/or the irrelevant antibody, organ, blood pool or interstitial subtraction agent.

The detector(s) must be able to distinguish between the radiation emitted by the primary antibody label and that emitted by the subtraction agent, in those cases where dual antibody correction is used to enhance sensitivity. This can be effected by using two different probes or by using a single probe which is programmed to record counts of different energies in different channels, or to distinguish by other electronic means between radiation of different types or energies. One way in which this can be accomplished is to detect differences in brightness of a scintillation crystal response, which correlates with differences in photon energy of impinging gamma radiation, using a photomultiplier and a comparator circuit. The circuit is present to respond only to levels above a selected level corresponding to the desired gamma energy band for one of the two radioisotopes.

A scintillation crystal can be mounted on the end of a fiber optic cable and its optical response to incident gamma radiation can be transmitted to a photomultiplier and associated circuitry through the optical fiber. This can reduce the size of the detector to be compatible with use in conjunction with an endoscope (broadly defined). The endoscope can be shielded to serve as a collimator, where necessary, and/or fitted with a window at a known distance from its terminus, with the scintillation crystal housed therein. Various other modifications and adaptations of the foregoing will be readily apparent to the ordinary skilled artisan, in light of the particular needs of the situation. However, the method of the present invention is not limited by any specific type of radiation detector. Rather, any detector which is capable of detecting radiation emitted by an antibody label localized in tumor tissue can be used.

The probe can be used in the form of an endoscope, and inserted into a body cavity through an orifice, such as the mouth, nose, ear, anus or vagina. The term endoscope is herein used generically to refer to an anally introduced endoscope, an orally introduced bronchoscope, a urethrally introduced cystoscope, or the like. Certain of these may benefit greatly from further progress in miniaturization of components and their utility to practice the method of the present invention will be enhanced as a function of the development of suitably microminiaturized components for this type of instrumentation. Highly miniaturized probes which could be

introduced invasively, e.g., via catheters or the like, are also suitable for use in the method of the invention.

The radionuclide label used for detection agents according to the method of the present invention is preferably an isotope with a gamma radiation emission peak in the range of 50-500 Kev, primarily because the state of the art for radiation detectors currently favors such labels. Suitable such radionuclides include, e.g., Iodine-131, Iodine-123, Iodine-126, Iodine-133, Bromine-77, Indium-111, Indium-113m, Copper-67, Gallium-67, Gallium-68, Ruthenium-95, Ruthenium-97, Ruthenium-103, Ruthenium-105, Mercury-197, Mercury-203, Rhodium-99m, Rhodium-101, Rhodium-105, Tellurium-121m, Tellurium-122m, Tellurium-125m, Thulium-165, Thulium-167, Thulium-168, Rhenium-186, Technetium-99m and Fluorine-18. Preferred radionuclides are Iodine-131, Iodine-123, Technetium-99m, Indium-111 and Gallium-67. Preferred gamma emitters include Iodine-131, Iodine-123, Indium-111, Gallium-67 and Technetium-99m.

Where more than one isotope is used for a method involving dual isotope correction, the two labels should be of sufficiently different energies to be separately detectable with the probe. Suitable such pairs of radioisotopes include, e.g., Iodine-131/Iodine 123, Gallium-67/Indium-111, Iodine-131/Technetium-99m and the like. It will generally be preferable that paired radionuclides used for subtraction should not both have significant scatter into channels wherein the emission of the other nuclide is being detected. A one-way scatter can readily be corrected for with currently available probe software.

In one embodiment of the present invention, techniques useful for subtraction in imaging applications are adapted to intraoperative detection. Methods of localization and therapy of tumors and infectious lesions, and methods of organ imaging, using labeled antibodies and antibody fragments which specifically bind markers produced by or associated with tumors, infectious lesions and normal organs or tissues, have been disclosed, *inter alia*, in U.S. Patents 4,331,647, 4,348,376, 4,361,544, 4,444,744, 4,460,561 and 4,624,846, and in related pending applications U.S. Serial Nos. 609,607 and 751,877, (hereinafter, "the Goldenberg patents"). These references also disclose antibodies and antibody fragments for use in the foregoing methods, together with methods for obtaining them and for labeling them with appropriate radionuclides.

The antibody used as the primary imaging agent in the method of the present invention may be whole IgG, IgA, IgD, IgE, IgM and the like, or a fragment such as, e.g., F(ab')₂, F(ab)₂, Fab', Fab or the like, including isotypes and subtypes thereof. It can be a polyclonal antibody, preferably an affinity-purified antibody from a human or an appropriate animal, e.g., a primate, goat, rabbit, mouse or the like, or a monoclonal antibody prepared by conventional techniques, e.g., a murine antibody derived from a hybridoma produced by fusion of lymph or spleen cells from a mouse immunized against

a cancer antigen with myeloma cells from an appropriate immortal cell line. It will be appreciated that newer techniques for production of monoclonals can also be used, e.g., human monoclonals, interspecies monoclonals, chimeric (e.g., human/mouse) monoclonals, genetically engineered antibodies and the like.

It should be noted that mixtures of antibodies, isotypes, and immunoglobulin classes, including fragments, can be used, as can hybrid antibodies and/or antibody fragments. The hybrids can have two different antigen specificities, e.g., one arm binding to a tumor antigen such as CEA and another arm binding to another antigen, e.g., CSAP. Or one arm could bind to one epitope on, e.g., CEA and the other arm could bind to another CEA epitope. The foregoing are merely illustrative, and other combinations of specificities can be envisioned that also fall within the scope of the invention. Hybrid antibody fragments with dual specificities can be prepared analogously to the anti-tumor marker hybrids disclosed in U.S. Patent 4,361,544. Other techniques for preparing hybrid antibodies are disclosed in, e.g., U.S. Patents 4,474,893 and 4,479,895, and in Milstein et al., *Immunol. Today*, 5, 299(1984).

One method for compensating for background radiation due to non-specific uptake of antibody by tumor and other tissues is to use "normal"/"irrelevant" immunoglobulin, labeled with a separately detectable label, as a subtraction agent. By "irrelevant" immunoglobulin is meant immunoglobulin which does not bind to cancer antigens or other antigens associated with the pathological lesion, and which does not substantially bind to other tissues, serum components or other substances in the body, as a result of specific antigen-antibody binding to the hyper-variable/idiotypic region of the immunoglobulin. Thus, ideally, a specific antibody and an irrelevant immunoglobulin, preferably but not necessarily of the same isotype and similar secondary and tertiary structures, should have substantially comparable biodistribution except where the specific antibody forms a complex with its complementary antigen.

Suitable such irrelevant immunoglobulin subtraction agents for use with specific anti-cancer antibodies are disclosed in the Goldenberg patents, especially U.S. 4,348,376 and U.S. 4,444,744, as are suitable radionuclides that can be paired for use in this method, ways to bind such radionuclides to antibodies, and ways to introduce such agents for effective imaging. It should be understood that the present invention is not limited to particular irrelevant immunoglobulins or pairs of radionuclides. Rather, any pair of labeled specific antibody and irrelevant immunoglobulin having separately detectable labels can be used, provided that the radiolabeling is so effected that the kinetics and distribution of the radiolabeled primary antibody and indifferent immunoglobulin in the patient are substantially the same during the time period required for scanning.

Various techniques can be employed to use the differences in counts between the radionuclide label of the specific primary antibody at different sites and the rela-

tive differences in counts between the radionuclide label of the irrelevant immunoglobulin at those sites to compensate for non-specific antibody uptake. These techniques will involve elements of statistical analysis, starting with an ideal case and proceeding to the types of corrections necessary to compensate for deviations from ideality found in real intraoperative and/or endoscopy situations. It will be useful to set out an illustrative ideal case and examples of the types of correction factors which can be applied, but it should be recognized that other conventional statistical approaches can be used which are substantially equivalent.

The model case will use a specific antibody binding to a cancer antigen and labeled with I-131 (131-I-Ab), and irrelevant immunoglobulin labeled with I-123 (123-I-N). The following definitions and relationships will be used to relate the activity in normal/non-tumor tissue and the activity in tumor tissue for the ideal case:

- x = 131-I-Ab activity in non-tumor tissue;
- y = 123-I-N activity in non-tumor tissue;
- A = 131-I-Ab activity at putative tumor site;
- B = 123-I-N activity at putative tumor site.

Assuming that the amount of 131-I-Ab activity is equal to the amount of 123-I-N activity initially (or that the relative activities are normalized), and that their non-specific uptakes are the same but specific uptake of 131-I-Ab in tumor occurs, it follows that, in the ideal case:

$$x/y = 1;$$

$$A/B > 1 \text{ and } A/B > x/y \text{ at a tumor site};$$

and that, when A and B are determined at a tumor site:

$$A/x > 1; B/y \geq 1; \text{ and } A/x \geq B/y.$$

In an ideal intraoperative or endoscopic scanning procedure, a probe able to separately detect radiation in two channels corresponding to emission from the primary antibody label and the irrelevant antibody label, respectively (assuming no scatter for the moment), is first placed over an area, preferably several areas, of normal tissue, then moved to a site of suspected tumor. The following operations are effected:

1. Confirm $x/y = 1$ (deviations from ideality corrected infra);
2. Determine A/B from counts in the separate detector channels;
3. When $A/B > 1$ for the suspected site, it is likely that tumor tissue is present at that site.

This ideal model can easily be corrected/modified to take account of, e.g.:

- Biodistribution differences of Ab and N;
- Isotope scatter;
- Physical decay and isotope ratio variance.

To correct for biodistribution differences, i.e., the situation where x/y departs from unity, the value of x/y in a representative number of non-tumor areas is determined, and the average value, herein denoted " r ", is set as the correction factor by which A/B must be multiplied to correct for differing biodistribution of the labeled specific antibody and labeled irrelevant immunoglobulin.

To correct for isotope scatter, an empirical determination will be required, using separate samples of the individual labels. It will be difficult to correct for scatter if emissions from both labels cross over into the channel for the other label, and it is strongly preferred that substantially only one of the two radionuclides used to label the immunoglobulins, at most, crosses over into the channel for the other label. Assuming that such is the case, an empirical determination is made of the counts in each channel for a known amount of the radionuclide label that crosses over, and a correction factor, herein denoted " s ", is calculated. This factor must be applied to correct individual values for x and y at a particular site before x/y is determined, and must similarly be used to correct A and B before A/B is determined.

For example, if the label on Ab shows crossover to the channel for the label on N, an empirical determination is effected using the Ab label alone, and the proportion of counts in the N channel relative to the Ab channel, s , is measured. Later readings of counts in the N channel, in the presence of both the N and the Ab label, again assuming substantially no crossover of the N label to the Ab channel, must be reduced by $(s)(x)$ or $(s)(A)$ counts for determinations of y or B .

To correct for physical decay and isotope ratio variance, the initial isotope activity ratio, " p ", is determined, and then the rates of decay of the two labels are used to calculate the expected activity ratio at a later time, t , at which the readings are effected in normal and suspected tumor tissues. For example, if the activity of 123-I-N is 10 times the activity of 131-I-Ab at the time of injection, and a reading during surgery or endoscopic examination is made 24 hours after injection, the corrections are made as follows:

$$\text{At injection, } x/y = 1/10.$$

The 123-I half-life is 13 hours and the 131-I half-life is 8 days; so that after 24 hours, only about 1/16 of the activity of 131-I is lost, whereas about 3/4 of the 123-I activity is lost. The expected normal ratio, x/y , should therefore be:

$$(1/10)(0.918/0.25) = 0.367.$$

Suppose the crossover of counts from the Ab channel to the N channel is 35%, and that the actual readings for x and y in a region of normal tissue are

$$\text{Ab channel} = 1000 \text{ counts (131-I);}$$

$$\text{N channel} = 4000 \text{ counts (123-I).}$$

The reading in the N channel is corrected by subtracting for crossover, so that:

$$x = 1000 \text{ counts; and}$$

$$y = 4000 - [(1000)(0.35)] = 3650 \text{ counts.}$$

It is now seen that, at $t = 24$ hours,

$$x/y = 1000/3650 = 0.277.$$

Absent unequal biodistribution, we expected x/y to be 0.367: therefore,

$$r = 0.367/0.277 = 1.323.$$

The probe is then positioned over a site of suspected tumor tissue, and the process is repeated.

The readings in the Ab channel and the N channel are taken, and the 24 hour time is assumed invariant.

The reading in the N channel is corrected for crossover.

The ratio of the corrected readings in the Ab and N channels is calculated, and the biodistribution factor, r , is applied. The result, denoted A/B , is compared to x/y . If A/B is greater than x/y , then the site is considered to be a tumor tissue site.

Still more sophisticated corrections can be introduced into the model to account for other departures from ideality in actual detection situations. There will be some attenuation of signal for different thicknesses or compositions of normal and tumor tissue. Thus, several measurements of x/y for normal tissues may yield different corrected values because of unequal effects of these parameters on the two antibodies or radionuclide labels. It may be necessary to select a set of parameters from a library of such parameters determined in normal tissue, so that the various correction factors most closely approximate those for the type of tissue scanned. If the variation in the value of x/y in normal tissue is within a narrow range, it may suffice to take an average value thereof. Further minor corrections for departures from ideality of other sorts may be necessary in certain cases, but these will be readily apparent to the skilled clinician and/or nuclear medicine physician, and well within the ordinary skill of such a professional, and their inclusion is within the broad scope of the present invention.

The final processed readout from the dual channel probe can be provided to the surgeon or clinician in a variety of forms. For example, when the value for A/B at a suspected tumor site exceeds that for x/y , applying the necessary corrections as set forth above, the physician can select a level of difference which he considers significant, generally at least 15% of the normal value, preferably at least 30%, and set the probe to give an auditory or visual signal when that level is attained at any particular locus in the course of a scan.

The probe can be combined with surgical removal of detected tumor tissue, and this is the conventional

mode of operation in second look surgery. Another possibility for such surgery, and especially for endoscopic procedures, is to combine the probe with a laser device that could use the signal generated by the probe to indicate where laser irradiation should be directed to selectively destroy tumor tissue.

Suitable laser devices, combined with fiber optic transmission, are well known in the art. Representative examples thereof are described, inter alia, in, e.g., Dixon, Lasers in Surgery, in "Current Problems in Surgery", Pgs. 1-65 (Year Book Medical Pubs., Inc. 1984); Fleisher, Arch. Intern. Med., 144, 1225-1230 (1984); Wood et al., Am. J. Gastroent., 80, 715-718 (1985); and Hunter et al., Am. J. Surg., 148, 736-741 (1984). Three types of lasers are currently in fairly widespread use for medical therapy, namely the argon, carbon dioxide and neodymium-YAG (yttrium aluminum garnet) lasers. As noted by Fleischer, Nd-YAG and argon lasers have been used with fiber optic waveguides, although it is likely that further advances in CO₂ laser technology will permit its use with fiber optics in the near future.

The foregoing references show that lasers have been used for therapy, in conjunction with endoscopy, both in coagulative and in ablative modes, including their use for tumor therapy. The use of lasers and endoscopy has advantages where surgery is contraindicated. Used in conjunction with RAID in a combined endoscopic procedure according to the present invention, greater precision and mitigation of damage to normal tissue is achieved.

The use of second antibody clearance to enhance imaging of tumors and infectious lesions using an external radiation detector, e.g., a gamma camera, is disclosed in Goldenberg Patent U.S. 4,624,846. This reference provides ample disclosure of types of antibodies and sources thereof for use in clearance of primary antibodies and/or their labeling moieties from the circulation to reduce background radiation and to enhance imaging.

Second antibody clearance increases the localization ratio of the labeled primary antibody in tumor tissue. It is used in the present invention to reduce non-specific background radiation. As used herein, the term "localization ratio" means the ratio of target to non-target activity of the radionuclide used to label the primary antibody. In general, the method of the invention will increase the localization ratio by at least about 20%, preferably at least about 50%, and often by a considerably higher factor, within about 2-72 hours following injection of the second antibody. Generally this is accompanied by a reduction in the level of circulating labeled primary antibody by about 10-85%, preferably by at least about 50%, and often higher, within about 2-72 hours following injection of the second antibody.

It will be understood that the second antibody used for clearance of primary antibody and/or its labeling moiety can be whole immunoglobulin or an immunoglobulin fragment, as disclosed for the related clearance method in U.S. 4,624,846. The administration protocols and

other strategies for further enhancing localization and reducing background will be similar to those disclosed in the aforementioned reference for second antibody clearance in imaging procedures, and the skilled clinician will recognize those factors common to these two different procedures which would indicate an overlap in particular factors involved.

However, it normally will not be possible to optimize scanning in the same way for intraoperative or endoscopic examination as it is for external imaging. Rather, in the event that it is desired to optimize the timing of surgery or endoscopy, a blood sample can be taken at periodic intervals after injection of the second antibody and the level of activity of the primary antibody label in the blood is determined, so that the efficacy of clearance and the level of circulating label can be observed. This will indicate the best time for surgery or endoscopy, and/or the need for repeated injection of second antibody to further reduce the level of circulating label. For example, when the level of circulating primary antibody label is reduced by at least about 75%, preferably by at least about 85%, or even more, the interference of background radiation with the short-range tumor detection process will be minimized, and surgery will be optimal.

It is again emphasized that combinations of subtraction and second antibody clearance can be used to further enhance the efficacy of background reduction and correction for non-specific uptake of label provided by the herein disclosed aspects and embodiments of the invention, and that such combinations fall within the broad scope of the present invention.

Without further elaboration, it is believed that one skilled in the art can, using the preceding description, utilize the present invention to its fullest extent. The following preferred specific embodiments are, therefore, to be construed as merely illustrative, and not limitative of the remainder of the disclosure in any way whatsoever. In the following examples, all temperatures are set forth uncorrected in degrees Celsius; unless otherwise indicated, all parts and percentages are by weight.

EXAMPLE 1

Intraoperative Tumor Detection

A male patient with a sigmoid colon cancer, as diagnosed by sigmoidoscopy and biopsy, is injected intravenously with I-131-labeled murine monoclonal antibody to carcinoembryonic antigen (CEA) (3 mCi I-131; 1 mg antibody immunoglobulin-G F(ab')₂ and irrelevant murine IgG F(ab')₂ labeled with I-123 (8 mCi; 1 mg IgG fragment). The patient is scanned with a gamma camera and the site or sites of tumor are imaged according to the methods of Goldenberg Patent No. 4,331,647. At a time when the optimal differentiation of I-123 irrelevant activity from I-131 specific (tumor) activity is achieved, usually within about 24 hrs, the patient undergoes surgery for removal of the sigmoid colon cancer and any other sites in regional lymph nodes, in the liver, or elsewhere. This is

achieved by passing a sterile probe over the viscera. The probe has a cadmium telluride scintillation crystal, collimator, preamplifier and amplifier, similar to that reported by Aitken et al., *op. cit.*, but is modified to include a comparator circuit capable of selecting only the high energy I-131 band in one channel or a total gamma counts band on an alternating basis, and a derived difference readout, corrected for scatter as described hereinabove, corresponding to the I-123 counts in a second channel.

The probe signals are processed to produce a reading corresponding to the ratio of counts in the I-131 channel to those in the I-123 channel, corrected for the decay rates of the radionuclides, and normalized to unity at representative non-tumor sites. The processed readings are translated into a digital recording and an auditory signal, such that a significant increase in the ratio of gamma ray counts of specific antibody I-131 over background I-123 results in an increase in auditory pitch. An increase in counts ratio and signal of at least 15% relative to non-tumor areas is noted in this patient at the site of the sigmoid colon mass and extending to a distance of about 1.5 cm from the gross margins of the tumor. The tumor mass is surgically resected, together with a section of the sigmoid colon extending a distance of 1.5 cm from the gross margins of the tumor on all sides, at which distance the ratio of counts was not more than 5% higher than the normalized baseline ratio. Also, two mesenteric lymph nodes give at least 15% increased signals and are resected. For control purposes, six other regional lymph nodes without increased signals are also resected.

The resected tissues are fixed in formalin and are found by histopathology, except for the six lymph nodes without increased signals, to contain adenocarcinoma, classified as a Dukes' C lesion. The colon tumor borders are found to be free of cancer invasion, since these are determined by the drop of signal beyond the major tumor mass. No areas of increased signal (specific antibody radioactivity compared to control radioactivity) are found elsewhere in the abdominal cavity, including over the liver, which is the major distant site of colon cancer metastasis. Based upon follow-up of the patient up to one year after surgery, no evidence of local or distant recurrence of the cancer is found, despite repeated CT scans and laboratory tests for circulating CEA and liver function.

EXAMPLE 2

Endoscopic Tumor Detection and Therapy

(A) A man with a history of multiple polyps is admitted for colonoscopy because of a recent positive hemoccult test for the presence of blood in his stool. A dose of murine monoclonal antibody against colon cancer-associated antigen labeled with I-131, is injected i.v. (3 mCi I-131 with 0.5 mg IgG protein), and 6 hrs later, 12 mg of goat antibody against the murine monoclonal antibody (anti-antibody or second antibody) is injected to rapidly clear the nontar-

get (circulating and background nonspecific) radioactivity. On the next day, approximately 16 hrs after administration of second antibody, the patient undergoes colonoscopy, using a colonoscope equipped with a radiation detector capable of measuring gamma radiation emitted by the radiolabeled antibody deposition. The detector comprises a cadmium telluride scintillation crystal mounted on the tip of an optical fiber waveguide. The optical fiber is housed within a shielded tube which itself is inserted inside the colonoscope and extends to within about 4 mm of the open end thereof, the remaining length of tubing serving as a collimator. The other end of the optical fiber leads to a photomultiplier, a preamplifier and amplifier, and means to convert the resultant signal to a corresponding auditory signal.

The gastroenterologist examining the colon with the colonoscope finds six small pedunculated polyps within a distance of 30 cm from the anal verge, and two larger lesions measuring more than 1 cm in diameter. The radiation detector shows an enhanced signal only over one of the two larger polyps, this signal appearing at least five times higher than background signals or those over the other polyps. A total of 5 polyps are removed by means of loop inserted in the colonoscope, extracted through the colonoscope and processed for histopathology. It is found that all but the one having a high radioactivity signal are free of cancer cells. The affected polyp had a nodule of adenocarcinoma of about 0.3 cm diameter.

(B) In another case of colonoscopy similar to the above, a patient receives murine monoclonal antibody against colon cancer-associated antigen (labeled with I-131), followed by a single dose of rabbit antibody against the first murine anticancer antibody. A single small polyp of about 0.7 cm in diameter is found to have an increased I-131 signal. The colonoscope is equipped with a fiber optic laser used to deliver a laser dose that coagulates the entire polyp.

The preceding examples can be repeated with similar success by substituting the generically or specifically described reactants and/or operating conditions of this invention for those used in the preceding examples.

From the foregoing description, one skilled in the art can easily ascertain the essential characteristics of this invention and, without departing from the scope thereof, can make various changes and modifications of the invention to adapt it to various usages and conditions.

Claims

1. The use of

(a) a marker specific primary antibody or antibody fragment specific against a marker pro-

duced by or associated with a tumor and labeled with a pharmacologically inert radioisotope capable of detection at close range with a radiation detection probe; and

a background compensation or reduction agent which is either of

(b) a dual isotope correction agent radiolabeled with a radioisotope emitting an energy which is separately detectable at close range from the primary antibody label using said radiation detection probe, said agent comprising irrelevant immunoglobulin from the same or different species as that used to prepare the primary antibody and not being an organ, blood pool or interstitial fluid non-tumor specific contrast agent, the irrelevant immunoglobulin being so labeled that the kinetics and distribution of the radiolabeled primary antibody and irrelevant immunoglobulin in the patient are substantially the same during the time required for scanning;

or

(b') unlabeled second antibody which specifically binds said primary antibody or the labeling moiety thereof,

in the preparation of an agent for use in a method for short-range intraoperative or endoscopic detection of a tumor, wherein a surgical or endoscopy patient is injected parenterally with a radiolabeled primary antibody which specifically binds a marker produced by or associated with a tumor, the surgically exposed or endoscopically accessed interior of a body cavity of said patient is scanned at close range with a radiation detection probe, and the sites of accretion of said labeled antibody are located by detecting elevated levels of radiation at said sites with said probe,

and wherein non-target background radiation is compensated for or reduced by injecting said patient parenterally, either concurrently or sequentially, with:

(a) a contrast or subtraction agent radiolabeled with a radioisotope emitting an energy which is separately detectable from the primary antibody label using a radiation detection probe; radiation detected from emission of the contrast or subtraction agent being used to better define the tumor, wherein said contrast or subtraction agent is a dual isotope correction agent comprising irrelevant immunoglobulin from the same or different species as that used to prepare the primary antibody and not being an organ, blood pool or interstitial fluid non-tumor specific contrast agent, the irrelevant immunoglobulin being so labeled that the kinetics and distribution of the radio-labeled primary anti-

body and irrelevant immunoglobulin in the patient are substantially the same during the time period required for scanning; and wherein the ratio of primary antibody label activity to irrelevant immunoglobulin label activity at a selected site is compared to said ratio at a known non-tumor site, whereby an elevated level of primary antibody label accretion due to antigen-antibody complex formation at said selected site can be discriminated;

or

(b) unlabeled second antibody which specifically binds the primary antibody or the labeling moiety thereof, the second antibody being injected at a time after the injection of the primary antibody sufficient to permit specific uptake of the primary antibody by a tumor in the body cavity, and in an amount sufficient to reduce the circulating level of the primary antibody label by at least about 10-85%, or to increase the localization ratio of the labeled primary antibody by at least about 20%, within about 2-72 hours following injection of the second antibody, whereby background levels of nonspecifically distributed primary antibody and/or label are reduced in the body cavity, and the sites of accretion of labeled primary antibody as well as the level of specific uptake thereof are more effectively discriminated.

2. The use according to claim 1, wherein said background compensation or reduction agent is a dual isotope correction agent comprising irrelevant immunoglobulin from the same or different species as that used to prepare the primary antibody and radiolabeled with a radioisotope emitting at an energy which is separately detectable from the primary antibody label using said radiation detection probe, the irrelevant immunoglobulin being so labeled that the kinetics and distribution of the radiolabeled primary antibody and irrelevant immunoglobulin in the patient are substantially the same during the time required for scanning; and wherein in said method, non-target background radiation is compensated for by injecting said patient parenterally, either concurrently or sequentially, with said dual isotope correction agent, radiation detected from emission of the dual isotope correction agent being used to better define the tumor, in particular, the ratio of primary antibody label activity to irrelevant immunoglobulin label activity at a selected site is compared to said ratio at a known non-tumor site, whereby an elevated level of primary antibody label accretion due to antigen-antibody complex formation at said selected site can be discriminated.
3. The use according to claim 2, wherein each of said primary antibody and said irrelevant immunoglobulin is an antibody fragment.

4. The use according to claim 1, wherein said background compensation or reduction agent is unlabeled second antibody which specifically binds said primary antibody or the labeling moiety thereof; and wherein said method, non-target background radiation is reduced by injecting said patient parenterally with said unlabeled second antibody, the second antibody being injected at a time after the injection of the primary antibody sufficient to permit specific uptake of the primary antibody by a tumor in the body cavity, and in an amount sufficient to reduce the circulating level of the primary antibody label by at least about 10-85%, or to increase the localization ratio of the labeled primary antibody by at least about 20%, within about 2-72 hours following injection of the second antibody, whereby background levels of non-specifically distributed primary antibody and/or label are produced in the body cavity, and the sites of accretion of labeled primary antibody as well as the level of specific uptake thereof are more effectively discriminated.
5. The use according to claim 4, wherein said primary antibody is an antibody fragment.
6. The use according to claim 4 or claim 5, wherein said unlabeled second antibody is whole immunoglobulin.
7. The use according to claim 4 or claim 5, wherein said amount of second antibody is sufficient to reduce the circulating level of the primary antibody label by at least about 50% within about 2-72 hours following injection of the second antibody.
8. The use according to claim 4 or claim 5, wherein said amount of second antibody is sufficient to reduce the circulating level of the primary antibody label by at least about 75% within about 2-72 hours following injection of the second antibody.
9. The use according to claim 4 or claim 5, wherein said amount of second antibody is sufficient to reduce the circulating level of the primary antibody label by at least about 85% within 2-72 hours following injection of the second antibody.

Patentansprüche

1. Verwendung von

(a) einem markerspezifischen primären Antikörper oder Antikörperfragment, die spezifisch für einen von einem Tumor gebildeten oder mit diesem assoziierten Marker sind und mit einem pharmakologisch inerten Radioisotop, das im Nahbereich mit einer Strahlungsnachweissonde nachgewiesen werden kann, markiert sind; und

einem Hintergrund-Kompensations- oder -Verringerungsmittel, bei dem es sich um folgendes handelt:

entweder

- (b) ein duales Isotopenkorrekturmittel, das mit einem Radioisotop radioaktiv markiert ist, das eine Energie ausstrahlt, die im Nahbereich zur primären Antikörpermarkierung unter Verwendung der Strahlungsnachweissonde getrennt nachweisbar ist, wobei das Mittel ein irrelevantes Immunoglobulin aus der gleichen oder einer unterschiedlichen Spezies, wie sie zur Herstellung des primären Antikörpers eingesetzt worden ist, enthält, und bei dem es sich nicht um ein nicht-tumorspezifisches Organ-, Blutpool- und Interstitialflüssigkeit-Kontrastmittel handelt, wobei das irrelevante Immunoglobulin so markiert ist, daß die Kinetik und die Verteilung des radioaktiv markierten primären Antikörpers und des irrelevanten Immunoglobulins im Patienten während der für den Abtastvorgang erforderlichen Zeitspanne im wesentlichen gleich sind; oder
- (b') unmarkierten sekundären Antikörper, der spezifisch den primären Antikörper oder dessen Markierungsrest bindet,

bei der Herstellung eines Mittels zur Verwendung in einem Verfahren zum intraoperativen oder endoskopischen Nahbereich-Nachweis eines Tumors, wobei einem für die chirurgische oder endoskopische Behandlung vorgesehenen Patienten parenteral ein radioaktiv markierter primärer Antikörper injiziert wird, der spezifisch einen vom Tumor gebildeten oder mit diesem assoziierten Marker bindet, wobei der chirurgisch freigelegte oder endoskopisch zugänglich gemachte Innenraum einer Körperhöhle des Patienten aus der Nähe mit einer Strahlungsnachweissonde abgetastet wird und wobei die Ansammlungsstellen des markierten Antikörpers durch Nachweis von erhöhten Strahlungspegeln an diesen Stellen mit der Sonde geortet werden,

und wobei eine Nichtziel-Hintergrundstrahlung kompensiert oder verringert wird, indem man dem Patienten auf parenteralem Wege entweder gleichzeitig oder nacheinander folgendes injiziert:

- (a) ein Kontrast- oder Subtraktionsmittel, das radioaktiv mit einem Radioisotop markiert ist, das eine Energie ausstrahlt, die unter Verwendung einer Strahlungsnachweissonde getrennt von der primären Antikörpermarkierung nachweisbar ist; wobei die Strahlung aufgrund der Emission des Kontrast- oder Subtraktionsmittels zur besseren Eingrenzung des Tumors verwendet wird, wobei es sich beim Kontrast- oder Subtraktionsmittel um ein duales Isotopenkorrekturmittel handelt, das irrelevantes Immuno-

globulin aus der gleichen oder einer unterschiedlichen Spezies, wie sie zur Herstellung des primären Antikörpers eingesetzt worden ist, enthält und bei dem es sich nicht um ein nicht-tumorspezifisches Organ-, Blutpool- oder Interstitialflüssigkeit-Kontrastmittel handelt, wobei das irrelevante Immunoglobulin so markiert ist, daß die Kinetik und die Verteilung des radioaktiv markierten primären Antikörpers und des irrelevanten Immunoglobulins im Patienten während der für den Abtastvorgang erforderlichen Zeitspanne im wesentlichen gleich sind; und wobei das Verhältnis der Aktivität der primären Antikörpermarkierung zur Aktivität der irrelevanten Immunoglobulinmarkierung an einer ausgewählten Stelle mit diesem Verhältnis an einer bekannten Nichttumorstelle verglichen wird, wodurch ein erhöhtes Niveau einer primären Antikörpermarkierungsansammlung aufgrund von Antigen-Antikörper-Komplexbildung an der ausgewählten Stelle unterschieden werden kann;

oder

(b) unmarkierten sekundären Antikörper, der spezifisch den primären Antikörper oder dessen markierenden Rest bindet, wobei der sekundäre Antikörper nach einer Zeitspanne nach Injektion des primären Antikörpers injiziert wird, die ausreicht, um eine spezifische Aufnahme des primären Antikörpers durch einen Tumor in der Körperhöhle zu ermöglichen, und in einer Menge, die ausreicht, um den zirkulierenden Spiegel der primären Antikörpermarkierung um mindestens etwa 10-85% zu verringern, oder um das Lokalisierungsverhältnis des markierten primären Antikörpers um mindestens etwa 20% innerhalb von etwa 2-72 Stunden im Anschluß an die Injektion des zweiten Antikörpers zu erhöhen, wobei Hintergrundspiegel von nicht-spezifisch verteiltem primärem Antikörper und/oder Markierung in der Körperhöhle verringert werden und die Stellen der Ansammlung von markiertem primärem Antikörper sowie das Niveau von dessen spezifischer Aufnahme in wirksamerer Weise unterschieden werden.

2. Verwendung nach Anspruch 1, wobei es sich beim Mittel zur Kompensation oder Verringerung des Hintergrunds um ein duales Isotopenkorrekturmittel handelt, das irrelevantes Immunoglobulin aus der gleichen oder einer unterschiedlichen Spezies, wie sie zur Herstellung des primären Antikörpers eingesetzt worden ist, enthält, und mit einem Radioisotop radioaktiv markiert ist, das eine Energie emittiert, die getrennt von der primären Antikörpermarkierung unter Verwendung der Strahlungsnachweissonde erfaßt werden kann, wobei das irrelevante Immunoglobulin so markiert ist, daß die Kinetik und die Ver-

teilung des radioaktiv markierten primären Antikörpers und des irrelevanten Immunoglobulins im Patienten im wesentlichen während der für den Abtastvorgang erforderlichen Zeitspanne gleich sind; und wobei bei dem Verfahren die Nichtziel-Hintergrundstrahlung kompensiert wird, indem man dem Patienten entweder gleichzeitig oder sequentiell parenteral das duale Isotopen-Korrekturmittel injiziert, wobei die erfaßte Strahlung der Emission des dualen Isotopen-Korrekturmittels zur besseren Abgrenzung des Tumors verwendet wird, wobei insbesondere das Verhältnis der Aktivität der primären Antikörpermarkierung zur Aktivität der Markierung des irrelevanten Immunoglobulins an einer ausgewählten Stelle mit dem Verhältnis an einer bekannten Nichttumorstelle verglichen wird, wobei ein erhöhtes Ausmaß an Ansammlung von primärer Antikörpermarkierung aufgrund der Bildung eines Antigen-Antikörper-Komplexes an der ausgewählten Stelle unterschieden werden kann.

3. Verwendung nach Anspruch 2, wobei es sich beim primären Antikörper und beim irrelevanten Immunoglobulin jeweils um Antikörper-Fragmente handelt.

4. Verwendung nach Anspruch 1, wobei es sich beim Mittel zur Kompensation oder Verringerung des Hintergrunds um einen unmarkierten sekundären Antikörper handelt, der spezifisch den primären Antikörper oder dessen Markierungsrest bindet; und wobei in dem Verfahren die Nichtziel-Hintergrundstrahlung durch Verabreichung einer parenteralen Injektion des unmarkierten sekundären Antikörpers an den Patienten verringert wird, wobei der sekundäre Antikörper zu einem solchen Zeitpunkt nach der Injektion des primären Antikörpers verabreicht wird, der eine spezifische Aufnahme des primären Antikörpers durch einen Tumor in der Körperhöhle ermöglicht, und in einer solchen Menge, die ausreicht, daß der zirkulierende Spiegel der primären Antikörpermarkierung um mindestens etwa 10-85% verringert wird oder das Lokalisierungsverhältnis des markierten primären Antikörpers um mindestens etwa 20% innerhalb von etwa 2-72 Stunden im Anschluß an die Injektion des sekundären Antikörpers erhöht wird, wobei Hintergrundspiegel von nicht-spezifisch verteiltem primärem Antikörper und/oder Markierung in der Körperhöhle entstehen und die Ansammlungsstellen von markiertem primärem Antikörper sowie das Niveau von dessen spezifischer Aufnahme in wirkungsvollerer Weise unterschieden werden.

5. Verwendung nach Anspruch 4, wobei es sich beim primären Antikörper um ein Antikörperfragment handelt.

6. Verwendung nach Anspruch 4 oder 5, wobei es sich beim unmarkierten sekundären Antikörper um vollständiges Immunoglobulin handelt.

7. Verwendung nach Anspruch 4 oder 5, wobei die Menge des zweiten Antikörpers ausreicht, um den zirkulierenden Spiegel der primären Antikörpermarkierung um mindestens etwa 50% innerhalb von 2 - 72 Stunden im Anschluß an die Injektion des sekundären Antikörpers zu verringern.

8. Verwendung nach Anspruch 4 oder 5, wobei die Menge des sekundären Antikörpers ausreicht, um den zirkulierenden Spiegel der primären Antikörpermarkierung um mindestens etwa 75% innerhalb von etwa 2-72 Stunden im Anschluß an die Injektion des zweiten Antikörpers zu verringern.

9. Verwendung nach Anspruch 4 oder 5, wobei die Menge des sekundären Antikörpers ausreicht, um den zirkulierenden Spiegel der primären Antikörpermarkierung um mindestens etwa 85% innerhalb von 2 - 72 Stunden im Anschluß an die Injektion des zweiten Antikörpers zu verringern.

Revendications

1. Utilisation

(a) d'un anticorps ou fragment d'anticorps primaire spécifique de marqueur spécifique pour un marqueur produit par ou associé à une tumeur et marqué avec un radio-isotope pharmacologiquement inerte capable d'être détecté à courte portée avec une sonde de détection de rayonnement, et

un agent de compensation ou de réduction de bruit de fond qui est

(b) un agent de correction à double marquage isotopique radiomarké avec un radio-isotope émettant une énergie qui est détectable à courte portée séparément du marqueur de l'anticorps primaire à l'aide de ladite sonde de détection de rayonnement, ledit agent comprenant une immunoglobuline non pertinente provenant de la même espèce ou d'une espèce différente de celle utilisée pour préparer l'anticorps primaire et n'étant pas un agent de contraste non spécifique de tumeur d'organe, d'accumulation de sang ou de liquide interstitiel, l'immunoglobuline non pertinente étant marquée de manière que la cinétique et la distribution de l'anticorps primaire radiomarké et de l'immunoglobuline non pertinente dans le patient soient sensiblement les mêmes pendant la durée nécessaire pour le balayage; ou

(b') un second anticorps non marqué qui se lie spécifiquement audit anticorps primaire ou à sa fraction de marquage,

dans la préparation d'un agent destiné à être utilisé dans un procédé pour la détection intra-opératoire ou endoscopique à courte portée d'une tumeur dans lequel un patient soumis à une intervention chirurgicale ou à une endoscopie subit une injection parentérale d'un anticorps primaire radiomarké qui se lie spécifiquement à un marqueur produit par ou associé à une tumeur, l'intérieur exposé par voie chirurgicale ou atteint par endoscopie d'une cavité corporelle dudit patient est balayé à courte portée avec une sonde de détection de rayonnement, et les sites d'accrétion dudit anticorps marqué sont localisés par détection de niveaux élevés de rayonnement à ces sites avec ladite sonde,

et dans lequel le rayonnement de fond non-cible est compensé ou réduit par injection audit patient par voie parentérale, simultanément ou successivement, de :

(a) un agent de contraste ou de soustraction radiomarké avec un radio-isotope émettant une énergie qui est détectable séparément du marqueur de l'anticorps primaire à l'aide d'une sonde de détection de rayonnement, le rayonnement détecté provenant de l'émission de l'agent de contraste ou de soustraction étant utilisé pour mieux définir la tumeur, dans lequel ledit agent de contraste ou de soustraction est un agent de correction à double marquage isotopique comprenant une immunoglobuline non pertinente provenant de la même espèce ou d'une espèce différente de celle utilisée pour préparer l'anticorps primaire et n'étant pas un agent de contraste non spécifique de tumeur d'organe, d'accumulation de sang ou de liquide interstitiel, l'immunoglobuline non pertinente étant marquée de manière que la cinétique et la distribution de l'anticorps primaire radiomarké et de l'immunoglobuline non pertinente dans le patient soient sensiblement les mêmes pendant la durée nécessaire pour le balayage, et dans lequel le rapport de l'activité du marqueur de l'anticorps primaire à l'activité du marqueur de l'immunoglobuline non pertinente à un site choisi est comparé audit rapport à un site non tumoral connu de sorte qu'un niveau élevé d'accrétion de marqueur de l'anticorps primaire dû à la formation d'un complexe antigène-anticorps audit site choisi puisse être distingué; ou

(b) un second anticorps non marqué qui se lie spécifiquement à l'anticorps primaire ou à sa portion de marquage, le second anticorps étant injecté au bout d'une durée après l'injection de l'anticorps primaire suffisante pour permettre

une absorption spécifique de l'anticorps primaire par une tumeur dans la cavité corporelle et en une quantité suffisante pour réduire le niveau circulant du marqueur de l'anticorps primaire d'au moins environ 10 à 85% ou pour augmenter le rapport de localisation de l'anticorps primaire marqué d'au moins environ 20%, dans les 2 à 72 h environ qui suivent l'injection du second anticorps, de sorte que les niveaux de bruit de fond de l'anticorps primaire et/ou du marqueur distribués non spécifiquement sont réduits dans la cavité corporelle et que les sites d'accrétion de l'anticorps primaire marqué et le niveau d'absorption spécifique de celui-ci sont distingués plus efficacement.

2. Utilisation selon la revendication 1, dans laquelle ledit agent de compensation ou de réduction de bruit de fond est un agent de correction à double marquage isotopique comprenant une immunoglobuline non pertinente provenant de la même espèce ou d'une espèce différente de celle utilisée pour préparer l'anticorps primaire et radiomarkée avec un radio-isotope émettant à une énergie qui est détectable séparément du marqueur de l'anticorps primaire à l'aide de ladite sonde de détection de rayonnement, l'immunoglobuline non pertinente étant marquée de manière que la cinétique et la distribution de l'anticorps primaire radiomarké et de l'immunoglobuline non pertinente dans le patient soient sensiblement les mêmes pendant la durée nécessaire pour le balayage, et dans laquelle, dans ledit procédé, le rayonnement de fond non cible est compensé par injection audit patient par voie parentérale, simultanément ou successivement, dudit agent de correction à double marquage isotopique, le rayonnement détecté provenant de l'émission de l'agent de correction à double marquage isotopique étant utilisé pour mieux définir la tumeur, en particulier, le rapport de l'activité du marqueur de l'anticorps primaire à l'activité du marqueur de l'immunoglobuline non pertinente à un site choisi est comparé audit rapport à un site non tumoral connu, de sorte qu'il est possible de distinguer un niveau élevé d'accrétion du marqueur de l'anticorps primaire due à la formation d'un complexe antigène-anticorps audit site choisi.

3. Utilisation selon la revendication 2, dans laquelle ledit anticorps primaire et ladite immunoglobuline non pertinente sont chacun un fragment d'anticorps.

4. Utilisation selon la revendication 1, dans laquelle ledit agent de compensation ou de réduction de bruit de fond est un second anticorps non marqué qui se lie spécifiquement audit anticorps primaire ou à sa portion de marquage, et dans laquelle, dans ledit procédé, le rayonnement de fond non-cible est réduit par injection audit patient par voie parentérale dudit

second anticorps non marqué, le second anticorps étant injecté au bout d'une durée après l'injection de l'anticorps primaire suffisante pour permettre l'absorption spécifique de l'anticorps primaire par une tumeur dans la cavité corporelle, et en une quantité suffisante pour réduire le niveau circulant du marqueur de l'anticorps primaire d'au moins environ 10 à 85%, ou pour augmenter le rapport de localisation de l'anticorps primaire marqué d'au moins environ 20%, dans les 2 à 72 h environ qui suivent l'injection du second anticorps, de sorte que des niveaux de bruit de fond de l'anticorps primaire et/ou du marqueur distribués de manière non spécifique sont produits dans la cavité corporelle, et les sites d'accrétion de l'anticorps primaire marqué ainsi que le niveau d'absorption spécifique de celui-ci sont distingués plus efficacement.

5. Utilisation selon la revendication 4, dans laquelle ledit anticorps primaire est un fragment d'anticorps.
6. Utilisation selon la revendication 4 ou la revendication 5, dans laquelle ledit second anticorps non marqué est une immunoglobuline complète.
7. Utilisation selon la revendication 4 ou la revendication 5, dans laquelle ladite quantité du second anticorps est suffisante pour réduire le niveau circulant du marqueur de l'anticorps primaire d'au moins environ 50% dans les 2 à 72 h environ qui suivent l'injection du second anticorps.
8. Utilisation selon la revendication 4 ou la revendication 5 dans laquelle ladite quantité du second anticorps est suffisante pour réduire le niveau circulant du marqueur de l'anticorps primaire d'au moins environ 75% dans les 2 à 72 h environ qui suivent l'injection du second anticorps.
9. Utilisation selon la revendication 4 ou la revendication 5, dans laquelle ladite quantité du second anticorps est suffisante pour réduire le niveau circulant du marqueur de l'anticorps primaire d'au moins environ 85% dans les 2 à 72 h qui suivent l'injection du second anticorps.

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