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(54) **Artificial intervertebral disc having a captured ball and socket joint**

Künstliche Bandscheibe mit eingeschlossener Kugel und Muffenverbindung

Disque intervertébral artificiel doté d'une articulation à rotule sphérique capturée

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Description

FIELD OF THE INVENTION

[0001] This invention relates generally to a spinal implant assembly for implantation into the intervertebral space between adjacent vertebral bones to simultaneously provide stabilization and continued flexibility and proper anatomical motion, and more specifically to such a device that has a captured ball and socket joint. The document US-A-6 063 121 represents the closest prior art and discloses an intervertebral implant comprising a first baseplate, with an articulation member having a spherical outer surface mounted on the first baseplate, a housing mounted on the articulation member and a second base plate mounted on the housing, wherein the housing has an articulation surface for contact with the spherical outer surface of the articulation member.

BACKGROUND OF THE INVENTION

[0002] The bones and connective tissue of an adult human spinal column consists of more than twenty discrete bones coupled sequentially to one another by a tri-joint complex that consists of an anterior disc and the two posterior facet joints, the anterior discs of adjacent bones being cushioned by cartilage spacers referred to as intervertebral discs. These more than twenty bones are anatomically categorized as being members of one of four classifications: cervical, thoracic, lumbar, or sacral. The cervical portion of the spine, which comprises the top of the spine, up to the base of the skull, includes the first seven vertebrae. The intermediate twelve bones are the thoracic vertebrae, and connect to the lower spine comprising the five lumbar vertebrae. The base of the spine is the sacral bones (including the coccyx). The component bones of the cervical spine are generally smaller than those of the thoracic spine, which are in turn smaller than those of the lumbar region. The sacral region connects laterally to the pelvis. While the sacral region is an integral part of the spine, for the purposes of fusion surgeries and for this disclosure, the word spine shall refer only to the cervical, thoracic, and lumbar regions.

[0003] The spinal column is highly complex in that it includes these more than twenty bones coupled to one another, housing and protecting critical elements of the nervous system having innumerable peripheral nerves and circulatory bodies in close proximity. In spite of these complications, the spine is a highly flexible structure, capable of a high degree of curvature and twist in nearly every direction.

[0004] Genetic or developmental irregularities, trauma, chronic stress, tumors, and degenerative wear are a few of the causes that can result in spinal pathologies for which surgical intervention may be necessary. A variety of systems have been disclosed in the art that achieve immobilization and/or fusion of adjacent bones by implanting artificial assemblies in or on the spinal col-

umn. The region of the back that needs to be immobilized, as well as the individual variations in anatomy, determine the appropriate surgical protocol and implantation assembly. With respect to the failure of the intervertebral disc, the interbody fusion cage has generated substantial interest because it can be implanted laparoscopically into the anterior of the spine, thus reducing operating room time, patient recovery time, and scarification.

[0005] Referring now to Figs. 13-14, in which a side perspective view of an intervertebral body cage and an anterior perspective view of a post implantation spinal column are shown, respectively, a more complete description of these devices of the prior art is herein provided. These cages 1 generally comprise tubular metal body 2 having an external surface threading 3. They are inserted transverse to the axis of the spine 4, into pre-formed cylindrical holes at the junction of adjacent vertebral bodies (in Figure 14 the pair of cages 1 are inserted between the fifth lumbar vertebra (L5) and the top of the sacrum (S1)). Two cages 1 are generally inserted side by side with the external threading 4 tapping into the lower surface of the vertebral bone above (L5), and the upper surface of the vertebral bone (S1) below. The cages 1 include holes 5 through which the adjacent bones are to grow. Additional materials, for example autogenous bone graft materials, may be inserted into the hollow interior 6 of the cage 1 to incite or accelerate the growth of the bone into the cage. End caps (not shown) are often utilized to hold the bone graft material within the cage 1.

[0006] These cages of the prior art have enjoyed medical success in promoting fusion and grossly approximating proper disc height. It is, however, important to note that the fusion of the adjacent bones is an incomplete solution to the underlying pathology as it does not cure the ailment, but rather simply masks the pathology under a stabilizing bridge of bone. This bone fusion limits the overall flexibility of the spinal column and artificially constrains the normal motion of the patient. This constraint can cause collateral injury to the patient's spine as additional stresses of motion, normally borne by the now-fused joint, are transferred onto the nearby facet joints and intervertebral discs. It would therefore, be a considerable advance in the art to provide an implant assembly which does not promote fusion, but, rather, which mimics the biomechanical action of the natural disc cartilage, thereby permitting continued normal motion and stress distribution.

[0007] It is, therefore, an object of the invention to provide an intervertebral spacer that stabilizes the spine without promoting a bone fusion across the intervertebral space.

[0008] It is further an object of the invention to provide an implant device that stabilizes the spine while still permitting normal motion.

[0009] It is further an object of the invention to provide a device for implantation into the intervertebral space that does not promote the abnormal distribution of biomechanical stresses on the patient's spine.

[0010] It is further an object of the invention to provide an artificial disc that provides free rotation of the baseplates relative to one another.

[0011] It is further an object of the invention to provide an artificial disc that provides limited rotation of the baseplates relative to one another.

[0012] It is further an object of the invention to provide an artificial disc that supports compression loads.

[0013] It is further an object of the invention to provide an artificial disc that permits the baseplates to axially compress toward one another under a compressive load.

[0014] It is further an object of the invention to provide an artificial disc that permits the baseplates to axially compress toward one another under a compressive load and restore to their original uncompressed relative positions when the compressive load is relieved.

[0015] It is further an object of the invention to provide an artificial disc that supports tension loads.

[0016] It is further an object of the invention to provide an artificial disc that prevents lateral translation of the baseplates relative to one another.

[0017] It is further an object of the invention to provide an artificial disc that provides a centroid of motion centrally located within the intervertebral space.

[0018] Other objects of the invention not explicitly stated will be set forth and will be more clearly understood in conjunction with the descriptions of the preferred embodiments disclosed hereafter.

SUMMARY OF THE INVENTION

[0019] The preceding objects are achieved by the invention, which is an artificial intervertebral disc or intervertebral spacer device comprising a pair of support members (e.g., spaced apart baseplates), each with an outwardly facing surface. Because the artificial disc is to be positioned between the facing endplates of adjacent vertebral bodies, the baseplates are arranged in a substantially parallel planar alignment (or slightly offset relative to one another in accordance with proper lordotic angulation) with the outwardly facing surfaces facing away from one another. The baseplates are to mate with the vertebral bodies so as to not rotate relative thereto, but rather to permit the spinal segments to bend (and in some embodiments, axially compress) relative to one another in manners that mimic the natural motion of the spinal segment. This natural motion is permitted by the performance of a ball and socket joint disposed between the secured baseplates, and the securing of the baseplates to the vertebral bone is achieved through the use of a vertebral body contact element attached to the outwardly facing surface of each baseplate.

[0020] Preferable vertebral body contact elements include, but are not limited to, one or more of the following: a convex mesh, a convex solid dome, and one or more spikes. The convex mesh is preferably secured at its perimeter to the outwardly facing surface of the respective baseplate. This can be accomplished in any effective

manner, however, laser welding and plasma coating burying are two preferred methods when the mesh is comprised of metal. While domed in its initial undeflected conformation, the mesh deflects as necessary during insertion of the artificial disc between vertebral bodies, and, once the artificial disc is seated between the vertebral bodies, the mesh deforms as necessary under anatomical loads to reshape itself to the concave surface of the vertebral endplate. Thus, the mesh is deformably reshapeable under anatomical loads such that it conformably deflects against the concave surface to securably engage the vertebral body endplate. Stated alternatively, because the mesh is convexly shaped and is secured at its perimeter to the baseplate, the mesh is biased away from the baseplate but moveable toward the plate (under a load overcoming the bias; such a load is present, for example, as an anatomical load in the intervertebral space) so that it will securably engage the vertebral body endplate when disposed in the intervertebral space. This affords the baseplate having the mesh substantially superior gripping and holding strength upon initial implantation, as compared with other artificial disc products. The convex mesh further provides an osteoconductive surface through which the bone may ultimately grow. The mesh preferably is comprised of titanium, but can also be formed from other metals and/or non-metals. Inasmuch as the mesh is domed, it does not restrict the angle at which the artificial disc can be implanted. It should be understood that while the flexible dome is described herein preferably as a wire mesh, other meshed or solid flexible elements can also be used, including flexible elements comprised of non-metals and/or other metals. Further, the flexibility, deflectability and/or deformability need not be provided by a flexible material, but can additionally or alternatively be provided mechanically or by other means.

[0021] It should be understood that the convex mesh attachment devices and methods described herein can be used not only with the artificial discs and artificial disc baseplates described or referred to herein, but also with other artificial discs and artificial disc baseplates, including, but not limited to, those currently known in the art. Therefore, the description of the mesh attachment devices and methods being used with the artificial discs and artificial disc baseplates described or referred to herein should not be construed as limiting the application and/or usefulness of the mesh attachment device.

[0022] To enhance the securing of the baseplates to the vertebral bones, each baseplate further comprises a porous area, which at least extends in a ring around the lateral rim of each outwardly facing surface. The porous area may be, for example, a sprayed deposition layer, or an adhesive applied beaded metal layer, or another suitable porous coating known in the art. The porous ring permits the long-term ingrowth of vertebral bone into the baseplate, thus permanently securing the prosthesis within the intervertebral space. The porous layer may extend beneath the domed mesh as well, but is more

importantly applied to the lateral rim of the outwardly facing surface of the baseplate that seats directly against the vertebral body.

[0023] Some of the embodiments described herein uses two baseplates each having the above described convex mesh on its outwardly facing surface, while other embodiments use two baseplates each having a convex solid dome in combination with a plurality of spikes on the lateral rim of the outwardly facing surface of the baseplates. It should be understood, however, that the various attachments devices or methods described herein (as well as any other attachment devices or methods, such as, for example, keels) can be used individually or in combination in any permutation, without departing from the scope of the present invention.

[0024] The ball and socket joint disposed between the baseplates permits rotation and angulation of the two baseplates relative to one another about a centroid of motion centrally located between the baseplates. The housing (e.g., the second baseplate and/or the convex structure) has a protrusion (e.g., a hemispherical protrusion or a hemispherical head of a pin secured in a pin hole in the housing) that interferes with a recess on the ball.

[0025] Therefore, when assembled, the invention enables angulation and limited rotation of the baseplates relative to one another about a centroid of motion that remains centrally located between the baseplates (at the center of the sphere defined by the ball), similar to the centroid of motion in a healthy natural intervertebral disc that is limited in its rotation by surrounding body structures. A benefit of limiting the relative rotation of the baseplates is that relative rotation beyond a certain range in a healthy natural disc is neither needed nor desired, because, for example, excess strain can be placed on the facet joints or ligaments thereby. The construction also prevents translation and separation of the baseplates relative to one another during rotation and angulation.

BRIEF DESCRIPTION OF THE DRAWINGS

[0026] The invention is shown in Figs 10a-10t.

[0027] The rest of the figures are useful for understanding the invention.

[0028] Figs. 1a-c show top (Fig. 1a), side cutaway (Fig. 1b) and bottom (Fig. 1c) views of a first baseplate, the first baseplate having an inwardly directed radially compressible ball.

[0029] Figs. 1d-f show top (Fig. 1d), side cutaway (Fig. 1e) and bottom (Fig. 1f) views of a second baseplate, the second baseplate having a circular recess within which seats a flexible convex structure.

[0030] Figs. 1g-h show side cutaway (Fig. 1g) and top perspective (Fig. 1h) views of a flexible convex structure, the flexible convex structure having spiral slots and radially extending grooves.

[0031] Figs. 1i-j show exploded (Fig. 1i) and assembled (Fig. 1j) views of an exemplary intervertebral im-

plant.

[0032] Figs. 2a-c show top (Fig. 2a), side cutaway (Fig. 2b) and bottom (Fig. 2c) views of a first baseplate, the first baseplate having an inwardly directed radially compressible ball.

[0033] Figs. 2d-f show top (Fig. 2d), side cutaway (Fig. 2e) and bottom (Fig. 2f) views of a second baseplate, the second baseplate having a curvate socket within which the ball is capturable for free rotation and angulation therein.

[0034] Figs. 2g-h show exploded (Fig. 2g) and assembled (Fig. 2h) views of another exemplary intervertebral implant.

[0035] Figs. 3a-e show top (Fig. 3a), side (Fig. 3b), side cutaway (Fig. 3c), perspective cutaway (Fig. 3d) and perspective (Fig. 3e) views of a first baseplate.

[0036] Figs. 3f-j show top (Fig. 3f), side (Fig. 3g), side cutaway (Fig. 3h), perspective cutaway (Fig. 3i) and perspective (Fig. 3j) views of a first type of a second baseplate, the first type of second baseplate having a convex structure integrated therewith.

[0037] Figs. 3k-o show top (Fig. 3k), side (Fig. 3l), side cutaway (Fig. 3m), perspective cutaway (Fig. 3n) and perspective (Fig. 3o) views of a first type of a ball.

[0038] Figs. 3p-t show top (Fig. 3p), side (Fig. 3q), side cutaway (Fig. 3r), perspective cutaway (Fig. 3s) and perspective (Fig. 3t) views of a first type of a cap.

[0039] Figs. 3u-y show top (Fig. 3u), side (Fig. 3v), side cutaway (Fig. 3w), perspective cutaway (Fig. 3x) and perspective (Fig. 3y) views of an assembled exemplary intervertebral implant. Fig. 3z shows a side cutaway of an alternate assembled exemplary intervertebral implant, having a bifurcated cap housing a spring member.

[0040] Figs. 4a-e show top (Fig. 4a), side (Fig. 4b), side cutaway (Fig. 4c), perspective cutaway (Fig. 4d) and perspective (Fig. 4e) views of a second type of the second baseplate, the second type of the second baseplate having the convex structure integrated therewith and also having a curvate recess.

[0041] Figs. 4f-j show top (Fig. 4f), side (Fig. 4g), side cutaway (Fig. 4h), perspective cutaway (Fig. 4i) and perspective (Fig. 4j) views of a second type of the ball, the second type of the ball having a protrusion.

[0042] Figs. 4k-o show top (Fig. 4k), side (Fig. 4l), side cutaway (Fig. 4m), perspective cutaway (Fig. 4n) and perspective (Fig. 4o) views of a second type of a cap, the second type of cap having a curvate recess.

[0043] Figs. 4p-t show top (Fig. 4p), side (Fig. 4q), side cutaway (Fig. 4r), perspective cutaway (Fig. 4s) and perspective (Fig. 4t) views of an assembled exemplary intervertebral implant. Fig. 4u shows a side cutaway of an alternate assembled exemplary intervertebral implant, having a bifurcated cap housing a spring member.

[0044] Figs. 5a-e show top (Fig. 5a), side (Fig. 5b), side cutaway (Fig. 5c), perspective cutaway (Fig. 5d) and perspective (Fig. 5e) views of a third type of the second baseplate, the third type of the second baseplate having the convex structure integrated therewith and also having

a protrusion.

[00445] Figs. 5f-j show top (Fig. 5f), side (Fig. 5g), side cutaway (Fig. 5h), perspective cutaway (Fig. 5i) and perspective (Fig. 5j) views of a third type of the ball, the third type of the ball having a curvate recess.

[00446] Figs. 5k-o show top (Fig. 5k), side (Fig. 5l), side cutaway (Fig. 5m), perspective cutaway (Fig. 5n) and perspective (Fig. 5o) views of an assembled exemplary intervertebral implant. Fig. 5p shows a side cutaway of an alternate assembled intervertebral implant, having a bifurcated cap housing a spring member.

[00447] Figs. 6a-e show top (Fig. 6a), side (Fig. 6b), side cutaway (Fig. 6c), perspective cutaway (Fig. 6d) and perspective (Fig. 6e) views of a fourth type of the second baseplate, the fourth type of the second baseplate having the convex structure integrated therewith and also having a pin through hole for housing a pin.

[00448] Figs. 6f-j show top (Fig. 6f), side (Fig. 6g), side cutaway (Fig. 6h), perspective cutaway (Fig. 6i) and perspective (Fig. 6j) views of an assembled exemplary intervertebral implant. Fig. 6k shows a side cutaway of an alternate assembled exemplary intervertebral implant, having a bifurcated cap housing a spring member.

[00449] Figs. 7a-e show top (Fig. 7a), side (Fig. 7b), side cutaway (Fig. 7c), perspective cutaway (Fig. 7d) and perspective (Fig. 7e) views of a fifth type of the second baseplate, the fifth type of the second baseplate having the convex structure integrated therewith and also having a recess.

[00500] Figs. 7f-j show top (Fig. 7f), side (Fig. 7g), side cutaway (Fig. 7h), perspective cutaway (Fig. 7i) and perspective (Fig. 7j) views of an assembled exemplary intervertebral implant. Fig. 7k shows a side cutaway of an alternate assembled exemplary intervertebral implant, having a bifurcated cap housing a spring member.

[00511] Figs. 8a-e show top (Fig. 8a), side (Fig. 8b), side cutaway (Fig. 8c), perspective cutaway (Fig. 8d) and perspective (Fig. 8e) views of a first baseplate.

[00521] Figs. 8f-j show top (Fig. 8f), side (Fig. 8g), side cutaway (Fig. 8h), perspective cutaway (Fig. 8i) and perspective (Fig. 8j) views of a first type of second baseplate, the first type of the second baseplate having a central curvate pocket of the fourth embodiment family.

[00531] Figs. 8k-o show top (Fig. 8k), side (Fig. 8l), side cutaway (Fig. 8m), perspective cutaway (Fig. 8n) and perspective (Fig. 8o) views of a first type of a ball.

[00541] Figs. 8p-t show top (Fig. 8p), side (Fig. 8q), side cutaway (Fig. 8r), perspective cutaway (Fig. 8s) and perspective (Fig. 8t) views of a first type of a convex structure.

[00551] Figs. 8u-y show top (Fig. 8u), side (Fig. 8v), side cutaway (Fig. 8w), perspective cutaway (Fig. 8x) and perspective (Fig. 8y) views of an assembled exemplary intervertebral implant. Fig. 8z shows a side cutaway of an alternate assembled exemplary intervertebral implant, having a bifurcated second baseplate housing a spring member.

[00556] Figs. 8aa-8bb show top (Fig. 8aa) and side cut-

away (Fig. 8bb) views of an alternate first baseplate 9400.

[00571] Figs. 8cc-8dd show top (Fig. 8cc) and side cutaway (Fig. 8dd) views of an alternate second baseplate 9500.

5 **[00581]** Figs. 9a-e show top (Fig. 9a), side (Fig. 9b), side cutaway (Fig. 9c), perspective cutaway (Fig. 9d) and perspective (Fig. 9e) views of a second type of second baseplate, the second type of the second baseplate having the central curvate pocket and also having a curvate recess.

10 **[00591]** Figs. 9f-j show top (Fig. 9f), side (Fig. 9g), side cutaway (Fig. 9h), perspective cutaway (Fig. 9i) and perspective (Fig. 9j) views of a second type of the ball, the second type of the ball having a protrusion.

15 **[00601]** Figs. 9k-o show top (Fig. 9k), side (Fig. 9l), side cutaway (Fig. 9m), perspective cutaway (Fig. 9n) and perspective (Fig. 9o) views of a second type of the convex structure, the second type of the convex structure having a curvate recess.

20 **[00611]** Figs. 9p-t show top (Fig. 9p), side (Fig. 9q), side cutaway (Fig. 9r), perspective cutaway (Fig. 9s) and perspective (Fig. 9t) views of an assembled exemplary intervertebral implant. Fig. 9u shows a side cutaway of an alternate assembled exemplary intervertebral implant, having a bifurcated second baseplate housing a spring member.

25 **[00621]** Figs. 10a-e show top (Fig. 10a), side (Fig. 10b), side cutaway (Fig. 10c), perspective cutaway (Fig. 10d) and perspective (Fig. 10e) views of a third type of second baseplate according to the invention, the third type of the second baseplate having the central curvate pocket and also having a recess on a circumferential wall around the curvate pocket.

30 **[00631]** Figs. 10f-j show top (Fig. 10f), side (Fig. 10g), side cutaway (Fig. 10h), perspective cutaway (Fig. 10i) and perspective (Fig. 10j) views of a third type of the ball according to the invention, the third type of the ball having a curvate recess.

35 **[00641]** Figs. 10k-o show top (Fig. 10k), side (Fig. 10l), side cutaway (Fig. 10m), perspective cutaway (Fig. 10n) and perspective (Fig. 10o) views of a third type of the convex structure according to the invention, the third type of the convex structure having a protrusion.

40 **[00651]** Figs. 10p-t show top (Fig. 10p), side (Fig. 10q), side cutaway (Fig. 10r), perspective cutaway (Fig. 10s) and perspective (Fig. 10t) views of an assembled preferred embodiment. Fig. 10u shows a side cutaway of an alternate assembled preferred embodiment, having a bifurcated second baseplate housing a spring member.

45 **[00661]** Figs. 11a-e show top (Fig. 11 a), side (Fig. 11 b), side cutaway (Fig. 11c), perspective cutaway (Fig. 11 d) and perspective (Fig. 11e) views of a fourth type of the convex structure, the fourth type of the convex structure having a pin through hole for housing a pin.

50 **[00671]** Figs. 11f-j show top (Fig. 11f), side (Fig. 11g), side cutaway (Fig. 11h), perspective cutaway (Fig. 11i) and perspective (Fig. 11j) views of an assembled exemplary intervertebral implant. Fig. 11k shows a side cuta-

way of an alternate assembled exemplary intervertebral implant, having a bifurcated second baseplate housing a spring member.

[0068] Figs. 12a-e show top (Fig. 12a), side (Fig. 12b), side cutaway (Fig. 12c), perspective cutaway (Fig. 12d) and perspective (Fig. 12e) views of a fifth type of the convex structure, the fifth type of the convex structure having a recess adjacent a curvate taper.

[0069] Figs. 12f-j show top (Fig. 12f), side (Fig. 12g), side cutaway (Fig. 12h), perspective cutaway (Fig. 12i) and perspective (Fig. 12j) views of fourth type of ball, the fourth type of ball having a curvate recess.

[0070] Figs. 12k-o show top (Fig. 12k), side (Fig. 12l), side cutaway (Fig. 12m), perspective cutaway (Fig. 12n) and perspective (Fig. 12o) views of an assembled exemplary intervertebral implant. Fig. 12p shows a side cutaway of an alternate assembled intervertebral implant, having a bifurcated second baseplate housing a spring member.

[0071] Fig. 13 shows a side perspective view of a prior art interbody fusion device.

[0072] Fig. 14 shows a front view of the anterior portion of the lumbo-sacral region of a human spine, into which a pair of interbody fusion devices of Fig. 13 have been implanted.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

[0073] While the invention will be described more fully hereinafter with reference to the accompanying drawings, in which particular embodiments and methods of implantation are shown, it is to be understood at the outset that persons skilled in the art may modify the invention herein described while achieving the functions and results of the invention. Accordingly, the descriptions that follow are to be understood as illustrative and exemplary of specific structures, aspects and features within the broad scope of the invention and not as limiting of such broad scope. Like numbers refer to similar features of like elements throughout

[0074] Exemplary intervertebral implants will now be described.

[0075] Referring to Figs. 1a-c, a first baseplate 10 is shown in top (Fig. 1a), side cutaway (Fig. 1b) and bottom (Fig. 1c) views. Also referring to Figs. 1d-f, a second baseplate 30 is shown in top (Fig. 1d), side cutaway (Fig. 1e) and bottom (Fig. 1f) views.

[0076] More specifically, each baseplate 10,30 has an outwardly facing surface 12,32. Because the artificial disc of the invention is to be positioned between the facing surfaces of adjacent vertebral bodies, the two baseplates 10,30 used in the artificial disc are disposed such that the outwardly facing surfaces 12,32 face away from one another (as best seen in exploded view in Fig. 1g and in assembly view in Fig. 1h). The two baseplates 10,30 are to mate with the vertebral bodies so as to not rotate relative thereto, but rather to permit the spinal segments to

bend relative to one another in manners that mimic the natural motion of the spinal segment. This motion is permitted by the performance of a ball and socket joint disposed between the secured baseplates 10,30. The mating of the baseplates 10,30 to the vertebral bodies and the construction of the ball and socket joint are described below.

[0077] More particularly, each baseplate 10,30 is a flat plate preferably made of a metal such as, for example, cobalt-chromium or titanium) having an overall shape that conforms to the overall shape of the respective endplate of the vertebral body with which it is to mate. Further, each baseplate 10,30 comprises a vertebral body contact element (e.g., a convex mesh 14,34, preferably oval in shape) that is attached to the outwardly facing surface 12,32 of the baseplate 10,30 to provide a vertebral body contact surface. The mesh 14,34 is secured at its perimeter to the outwardly facing surface 12,32 of the baseplate 10,30. The mesh 14,34 is domed in its initial undeflected conformation, but deflects as necessary during insertion of the artificial disc between vertebral bodies, and, once the artificial disc is seated between the vertebral bodies, deforms as necessary under anatomical loads to reshape itself to the concave surface of the vertebral endplate. This affords the baseplate 10,30 having the mesh 14,34 substantially superior gripping and holding strength upon initial implantation as compared with other artificial disc products. The mesh 14,34 further provides an osteoconductive surface through which the bone may ultimately grow. The mesh 14,34 is preferably comprised of titanium, but can also be formed from other metals and/or non-metals without departing from the scope of the invention.

[0078] Each baseplate 10,30 further comprises at least a lateral ring 16,36 that is osteoconductive, which may be, for example, a sprayed deposition layer, or an adhesive applied beaded metal layer, or another suitable porous coating. This porous ring 16,36 permits the long-term ingrowth of vertebral bone into the baseplate 10,30, thus permanently securing the prosthesis within the intervertebral space. It shall be understood that this porous layer 16,36 may extend beneath the domed mesh 14,34 as well, but is more importantly applied to the lateral rim of the outwardly facing surface 12,32 of the baseplate 10,30 that seats directly against the vertebral body.

[0079] The convex structure is configured as a flexible element and functions as a spring element that provides axial cushioning to the device. The convex structure has the socket of the ball and socket joint at its peak. In order to permit the flexible convex structure to flex under compressive loads applied to the device, it is a separate element from the second baseplate. In the preferred embodiment, the flexible convex structure is a bellville washer that has a frusto-conical shape. Other flexible convex structures are also contemplated as being suitable, such as, for example, convex structures that flex because of the resilience of the material from which they are made, because of the shape into which they are

formed, and/or or because of the mechanical interaction between sub-elements of an assembly forming the convex structure. Although the convex structure is a separate element from the second baseplate in this embodiment family (so that it is able to flex), it is preferably maintained near the second baseplate so that the device does not separate in tension. Therefore, an extension of the second baseplate is provided (in the form of a shield element) to cover enough of the convex structure to so maintain it. Stated alternatively, the shield is a separate element from the second baseplate to ease manufacturing (during assembly, the flexible convex structure is first placed against the second baseplate, and then the shield is placed over the convex structure and secured to the second baseplate so that the convex structure is maintained between the second baseplate and the shield), but once the device is assembled, the second baseplate and the shield are effectively one element. That is, the second baseplate and shield can be considered to be a single integral housing within which the separate flexible convex structure flexes, because but for the sake of achieving desirable manufacturing efficiencies, the second baseplate and shield would be one piece.

[0080] The manner of capturing the ball in the socket is effected by the ball being selectively radially compressible. That is, the ball is radially compressed to fit into the socket and thereafter receives a deflection preventing element to prevent subsequent radial compression, so that the ball remains captured in the socket. A more detailed description of the preferred manner in which this is accomplished is described below. Because the socket is formed at the peak of the flexible convex structure discussed immediately above, the capturing of the ball in the socket in this manner allows the ball to remain securely held for rotation and angulation even though the socket moves upward and downward with the flexing of the convex structure. The second baseplate preferably includes an access hole that accommodates placement of the deflection preventing element, so that the same can be applied to the ball after the ball is fitted into the socket. Accordingly, the ball is maintained in the socket.

[0081] More specifically, with regard to joining the two baseplates 10,30 with a ball and socket joint, each of the baseplates 10,30 comprises features that, in conjunction with other components described below, form the ball and socket joint. More specifically, the first baseplate 10 includes an inwardly facing surface 18 that includes a perimeter region 20 and a ball 22 mounted to protrude from the inwardly facing surface 18. The ball 22 preferably has a semispherical shape defining a spherical contour. The ball 22 includes a series of slots 24 that render the ball 22 radially compressible and expandable in correspondence with a radial pressure (or a radial component of a pressure applied thereto and released therefrom). The ball 22 further includes an axial bore 26 that accepts a deflection preventing element (e.g., rivet, plug, dowel, or screw; a rivet 28 is used herein as an example) (shown in Figs. 1i-j). (Alternatively, the axial bore can be

threaded to accept a screw.) Prior to the insertion of the rivet 28, the ball 22 can deflect radially inward because the slots 24 will narrow under a radial pressure. The insertion of the rivet 28 eliminates the capacity for this deflection. Therefore, the ball 22, before receiving the rivet 28, can be compressed to pass into, and thereafter seat in, a central curvate socket of a convex structure (described below). Once the ball 22 has been seated in the curvate socket, the rivet 28 can be inserted into the axial bore 26 to ensure that the ball 22 remains held in the curvate socket. As described below, an access hole is preferably provided in the second baseplate 30 so that the interior of the device may be readily accessed for inserting the rivet 28 into the axial bore 26, or for other purposes.

[0082] The second baseplate 30 includes an inwardly facing surface 38 that includes a perimeter region 40 and a central circular recess 42 within which the wide end of the convex structure resides, and a pair of holes 44 through which rivets 46 (shown in Figs. 1g-h) may be provided for securing a shield element 48 that is placed over the convex structure, which shield 48 thus serves as an extension of the second baseplate 30 (the shield 48 is more fully set forth below with and shown on Figs. 1i-j).

[0083] Referring now to Figs. 1g-h, the convex structure 31 that resides in the circular recess 42 is shown in side cutaway (Fig. 1g) and top perspective (Fig. 1h) views. The convex structure 31 is frusto-conical and is flexible. Because the convex structure 31 is flexible, it functions as a force restoring element (e.g., a spring) that provides axial cushioning to the device, by deflecting under a compressive load and restoring when the load is relieved. The flexible convex structure 31 is preferably, as shown, a belleville washer that has a frusto-conical shape. The belleville washer 31 preferably, as shown, has spiral slots and radially extending grooves. The restoring force of the belleville washer 31 is proportional to the elastic properties of the material or materials from which it is made. It should be understood that belleville washers having the configuration shown can be used, but that belleville washers having other conformations, that is, without or without slots and/or grooves, and/or with other groove and slots configurations, including the same or different numbers of grooves and/or slots, can also be used with and are encompassed by the present invention.

[0084] The belleville washer 31 comprises a series of spiral slots 33 formed therein. The slots 33 extend from the outer edge of the belleville washer 31, inward along arcs generally directed toward the center of the element. The slots 33 do not extend fully to the center of the element. Preferably, the slots 33 extend anywhere from a quarter to three quarters of the overall radius of the washer 31, depending upon the requirements of the patient, and the anatomical requirements of the device.

[0085] The belleville washer 31 further comprises a series of grooves 35 formed therein. The grooves 35 extend

radially from the outer edge of the belleville washer 31 toward the center of the element. Preferably, the width and depth of each groove 35 decreases along the length of the groove 35 from the outer edge of the washer 31 toward the center of the washer 31, such that the center of the washer 31 is flat, while the outer edge of the washer 31 has grooves of a maximum groove depth. It should be understood that, one or both of the depth and the width of each groove can be (1) increasing along the length of the groove from the outer edge of the washer toward the center of the washer, (2) uniform along the length of the groove from the outer edge of the washer toward the center of the washer, or (3) varied along the length of each groove from the outer edge of the washer toward the center of the washer, either randomly or according to a pattern. Moreover, it can be the case that each groove is not formed similarly to one or more other grooves, but rather one or more grooves are formed in any of the above-mentioned fashions, while one or more other grooves are formed in another of the above-mentioned fashions or other fashions. It should be clear that any groove pattern can be implemented, including, but not limited to, at least one radially spaced concentric groove, including, but not limited to, at least one such groove having at least one dimension that varies along the length of the groove. Belleville washers having circumferential extents that radially vary in at least one dimension, are also contemplated by the present invention.

[0086] As a compressive load is applied to the belleville washer 31, the forces are directed into a hoop stress which tends to radially expand the washer 31. This hoop stress is counterbalanced by the material strength of the washer 31, and the force necessary to widen the spiral slots 33 and the radial grooves 35 along with the strain of the material causes a deflection in the height of the washer 31. Stated equivalently, the belleville washer 31 responds to a compressive load by deflecting compressively; the spiral slots and/or radial grooves cause the washer to further respond to the load by spreading as the slots and/or the grooves in the washer expand under the load. The spring, therefore, provides a restoring force which is proportional to the elastic modulus of the material in a hoop stressed condition.

[0087] With regard to the above discussion regarding the curvate socket that receives the ball 22 of the first baseplate 10, the curvate socket is formed at the peak of the convex structure 31. The curvate socket 37 is provided inasmuch as the central opening of the belleville washer 31 is enlarged. This central opening includes a curvate volume 37 for receiving therein the ball 22 of the first baseplate 10. More particularly, the curvate volume 37 has a substantially constant radius of curvature that is also substantially equivalent to the radius of the ball 22. In this embodiment, the spiral slots 33 of the washer 31 do not extend all the way to the central opening, and approach the opening only as far as the material strength of the washer 31 can handle without plastically deforming under the expected anatomical loading. Further, the

depth of each groove 35 of the washer 31 decreases along the length of the groove 35 from the outer edge of the washer 31 toward the center of the washer 31, such that the center of the washer 31 is flat, while the outer edge of the washer 31 has grooves of a maximum groove depth. Therefore, the central opening can be formed from flat edges. It should be understood that this is not required, but rather is preferred.

[0088] The curvate socket 37 has an opening diameter that accommodates passage therethrough of the ball 22 in a radially compressed state (but not in an uncompressed state), and a larger inner diameter that accommodates the ball 22 in the uncompressed state. Therefore, the ball 22 can be radially compressed to pass into the curvate socket 37 under force, and then will radially expand to the uncompressed state once in the curvate socket 37. Once the rivet 28 is then secured into the axial bore 26, the rivet 28 prevents the ball 22 from radially compressing, and therefore the ball 22 cannot back out through the opening. An access hole 39 in the second baseplate 30 below the curvate socket 37 has a diameter that accommodates the diameter of the rivet 28 and thereby provides easy access to insert the rivet 28 in the axial bore 26 after the ball 22 has been seated in the curvate socket 37. To prevent the ball 22 from escaping the curvate socket 37 through the second baseplate 30, the diameter of the access hole 39 is smaller than the inner diameter of the curvate socket 37.

[0089] The curvate socket 37 defines a spherical contour that closely accommodates the ball 22 for free rotation and angulation in its uncompressed state. Therefore, when seated in the curvate socket 37, the ball 22 can rotate and angulate freely relative to the curvate socket 37 through a range of angles, thus permitting the opposing baseplates 10,30 to rotate and angulate freely relative to one another through a corresponding range of angles equivalent to the fraction of normal human spine rotation and angulation (to mimic normal disc rotation and angulation). Further preferably, the perimeter regions 20,40 have corresponding contours, so that the meeting of the perimeter regions 20,40 as a result of the angulation of the baseplates 10,30 reduces any surface wearing.

[0090] Referring to Figs. 1i-j, exploded (Fig. 1i) and assembled (Fig. 1j) views of an exemplary intervertebral implant. Included in these views are the shield 48 and the corresponding rivets 46. More particularly, assembly of the disc is preferably as follows. The first and second baseplates 10,30 are disposed so that their outwardly facing surfaces 12,32 face away from one another and their inwardly facing surfaces 18,38 are directed toward one another. The convex structure 31 is then positioned with its wide end in the circular recess 42 of the second baseplate, so that the curvate socket 37 of the convex structure 31 is aligned with the ball 22 of the first baseplate 10. Then, the shield 48 is secured over the belleville washer 31 (the shield 48 is preferably frusto-conical to follow the shape of the belleville washer 31, although other shield shapes are suitable and contemplated) by

passing the central hole 41 of the shield 48 over the curvate socket 37 and applying the rivets 46 through rivet holes 43 in the shield 48 and into the rivet holes 44 in the second baseplate 30. Then, the ball 22 is pressed into the curvate socket 37 under a force sufficient to narrow the slots 24 and thereby radially compress the ball 22 until the ball 22 fits through and passes through the opening of the curvate socket 37. Once the ball 22 is inside the curvate socket 37, the ball 22 will radially expand as the slots 24 widen until it has returned to its uncompressed state and the spherical contour defined by the ball 22 is closely accommodated by the spherical contour defined by the curvate socket 37 and the ball 22 can rotate and angulate freely relative to the curvate socket 37. Thereafter, the rivet 28 is passed through the access hole 39 and pressed into the axial bore 26 of the ball 22 to prevent any subsequent radially compression of the ball 22 and therefore any escape from the curvate socket 37 thereby. Because the diameter of the circular recess 42 is greater than the diameter of the wide end of the belleville washer 31, compressive loading of the device (and therefore the belleville washer) can result in an unrestrained radial deflection of the belleville washer 31. The spiral slots 33 and radial grooves 35 of the belleville washer 31 enhance this deflection. When the load is removed, the belleville washer 31 springs back to its original shape.

[0091] Accordingly, when the device is assembled, the baseplates 10,30 are rotatable relative to one another because the ball 22 rotates freely within the curvate socket 37, and angulatable relative to one another because the ball 22 angulates freely within the socket 37. Because the convex structure 31 is flexible (and is housed in the second baseplate 30 in a manner that permits it to flex), the baseplates 10,30 are also axially compressible relative to one another. Because the ball 22 is held within the curvate socket 37 by a rivet 28 in the axial bore 26 preventing radial compression of the ball 22, the artificial disc can withstand tension loading of the baseplates 10,30. More particularly, when a tension load is applied to the baseplates 10,30, the ball 22 in the curvate socket 37 seeks to radially compress to fit through the opening of the curvate socket 37. However, the rivet 28 in the axial bore 26 of the ball 22 prevents the radial compression, thereby preventing the ball 22 from exiting the curvate socket 37. Therefore, the assembly does not come apart under normally experienced tension loads. This ensures that no individual parts of the assembly will pop out or slip out from between the vertebral bodies when, e.g., the patient stretches or hangs while exercising or performing other activities. Thus, in combination with the securing of the baseplates 10,30 to the adjacent vertebral bones via the mesh domes 14,34, the disc assembly has an integrity similar to the tension-bearing integrity of a healthy natural intervertebral disc. Also, because the ball 22 is laterally captured in the curvate socket 37, lateral translation of the baseplates 10,30 relative to one another is prevented during rotation and angulation, similar to the

performance of healthy natural intervertebral disc. Because the baseplates 10,30 are made angulatable relative to one another by the ball 22 being rotatably and angulatably coupled in the curvate socket 37, the disc assembly provides a centroid of motion within the ball 22. Accordingly, the centroid of motion of the disc assembly remains centrally located between the vertebral bodies, similar to the centroid of motion in a healthy natural intervertebral disc.

[0092] Referring to Figs. 2a-c, a first baseplate 50 is shown in top (Fig. 2a), side cutaway (Fig. 2b) and bottom (Fig. 2c) views. Also referring to Figs. 2d-f, a second baseplate 70 is shown in top (Fig. 2d), side cutaway (Fig. 2e) and bottom (Fig. 2f) views.

[0093] With regard to the configuration of the convex structure, and the manner in which the ball is captured in the socket, the convex structure is configured as a non-flexible element that is integral with the second baseplate, and has the socket of the ball and socket joint at its peak. More clearly stated, the devices of this second embodiment family do not feature a flexible convex structure, and therefore (and also because of the manner in which the ball is captured in this second embodiment family, discussed immediately below) there is no need for the convex structure to be a separate element from the second baseplate. (By contrast, in the first embodiment family, as discussed above, because the convex structure is flexible, it is separated from the second baseplate so that it is able to flex.) In the preferred embodiment, the convex structure has a frusto-conical shape. The manner of capturing the ball in the socket is identical to that shown in Figs. 1a-1j.

[0094] More specifically, the first and second baseplates 50,70 are similar to the first and second baseplates 10,30 of the first embodiment family described above with regard to each outwardly facing surface 52,12 having a vertebral body contact element 54,74 and an adjacent osteoconductive ring 56,76, and each inwardly facing surface 58,78 having a perimeter region 60,80.

[0095] Further, the two baseplates 50,70 are joined with a ball and socket joint, and therefore each of the baseplates 50,70 comprises features that, in conjunction with other components described below, form the ball and socket joint. More specifically, the first baseplate 50 is formed similarly to the first baseplate 10 of the first embodiment family, having a ball 62 mounted to protrude from the inwardly facing surface 58. The ball 62 preferably has a semispherical shape defining a spherical contour. The ball 62 is structurally and functionally identical to the ball 22, and as such is selectively radially compressible in the same manner as the ball 22 of the first embodiment family. As with the ball 22, the ball 62 is capturable in a curvate socket 77 formed at the peak of a convex structure 71 protruding from the second baseplate 70. The curvate socket 77 is functionally and structurally identical to the curvate socket 37. However, the convex structure 77 of the device, rather than being a flexible separate element from the second baseplate as

in the first embodiment family, is integral with the second baseplate 70. The convex structure 77 is frusto-conical, but is not flexible, and therefore does not function as a force restoring element as does the flexible convex structure 37. Access to the convex structure 77 for providing easy access to insert the rivet 68 in the axial bore 66 of the ball 62 after the ball 62 has been seated in the curvate socket 77 is provided by an access hole 79 in the second baseplate 70 below and leading to the curvate socket 77. The access hole 79 is otherwise structurally identical to the access hole 39 in the second baseplate 30.

[0096] Referring to Figs. 2g-h, an assembled exemplary intervertebral implant is shown in exploded (Fig. 2g) and assembled (Fig. 2h) views. More particularly, assembly of the disc is preferably as follows. The first and second baseplates 50,70 are disposed so that their outwardly facing surfaces 52,72 face away from one another and their inwardly facing surfaces 58,78 are directed toward one another, and so that the ball 62 of the first baseplate 50 is aligned with the curvate socket 77 of the convex structure 71 of the second baseplate 70. Then, the ball 62 is pressed into the curvate socket 77 under a force sufficient to narrow the slots 64 and thereby radially compress the ball 62 until the ball 62 fits through and passes through the opening of the curvate socket 77. Once the ball 62 is inside the curvate socket 77, the ball 62 will radially expand as the slots 64 widen until it has returned to its uncompressed state and the spherical contour defined by the ball 62 is closely accommodated by the spherical contour defined by the curvate socket 77 and the ball 62 can rotate and angulate freely relative to the curvate socket 77. Thereafter, the rivet 68 is passed through the access hole 79 and pressed into the axial bore 66 of the ball 62 to prevent any subsequent radially compression of the ball 62 and therefore any escape from the curvate socket 77 thereby.

[0097] Accordingly, when the device is assembled, the baseplates 50,70 are rotatable relative to one another because the ball 62 rotates freely within the curvate socket 77, and angulatable relative to one another because the ball 62 angulates freely within the socket 77. Because the ball 62 is held within the curvate socket 77 by a rivet 68 in the axial bore 66 preventing radial compression of the ball 62, the artificial disc can withstand tension loading of the baseplates 50,70. More particularly, when a tension load is applied to the baseplates 50,70, the ball 62 in the curvate socket 77 seeks to radially compress to fit through the opening of the curvate socket 77. However, the rivet 68 in the axial bore 66 of the ball 62 prevents the radial compression, thereby preventing the ball 62 from exiting the curvate socket 77. Therefore, the assembly does not come apart under normally experienced tension loads. This ensures that no individual parts of the assembly will pop out or slip out from between the vertebral bodies when, e.g., the patient stretches or hangs while exercising or performing other activities. Thus, in combination with the securing of the baseplates 50,70 to the adjacent vertebral bones via the mesh domes 54,74,

the disc assembly has an integrity similar to the tension-bearing integrity of a healthy natural intervertebral disc. Also because the ball 62 is laterally captured in the curvate socket 77, lateral translation of the baseplates 50,70 relative to one another is prevented during rotation and angulation, similar to the performance of healthy natural intervertebral disc. Because the baseplates 50,70 are made angulatable relative to one another by the ball 62 being rotatably and angulatably coupled in the curvate socket 77, the disc assembly provides a centroid of motion within the ball 62. Accordingly, the centroid of motion of the disc assembly remains centrally located between the vertebral bodies, similar to the centroid of motion in a healthy natural intervertebral disc.

[0098] With regard to the configuration of the convex structure, the convex structure is configured as a non-flexible element that is integral with the second baseplate, and has the socket of the ball and socket joint at its peak, similar to the configuration of the convex structure above. The convex structure is shaped to have a curved taper.

[0099] With regard to the manner in which the ball is captured in the socket, the capturing is effected through the use of a solid ball. In order to permit the seating of the ball into the socket formed at the peak of the: convex structure, the access hole in the second baseplate has a diameter that accommodates the diameter of the ball, and leads to the interior of the peak, which interior is formed as a concavity having an opening diameter that accommodates the diameter of the ball. (Preferably, the concavity has a curvature closely accommodating the contour of the ball, and the concavity is either hemispherical or less-than-hemispherical so that the ball can easily be placed into it.) Further, in order to maintain the ball in the socket, an extension of the second baseplate (in the form of a cap element) is provided for sealing the access hole in the second baseplate (or reducing the opening diameter of the hole to a size that does not accommodate the diameter of the ball). The cap has an interior face that preferably has a concavity (that has a curvature that closely accommodates the contour of the ball) to complete the socket. The peak of the convex structure has a bore that accommodates a post to which the ball and the first baseplate are attached (one to each end of the post), but does not accommodate the ball for passage through the bore. Accordingly, the ball is maintained in the socket.

[0100] Referring to Figs. 3a-e, a first baseplate 100 is shown in top (Fig. 3a), side (Fig. 3b), side cutaway (Fig. 3c), perspective cutaway (Fig. 3d) and perspective (Fig. 3e) views. Also referring to Figs. 3f-j, a first type 200 of a second baseplate is shown in top (Fig. 3f), side (Fig. 3g), side cutaway (Fig. 3h), perspective cutaway (Fig. 3i) and perspective (Fig. 3j) views.

[0101] More specifically, the first and second baseplates 100,200 are similar to the first and second baseplates 50,70 described above with regard to each having an outwardly facing surface 102,202, and each inwardly facing surface 108,208 having a perimeter region

110,210, all of which elements are, for example, identical to the corresponding elements as described above. However, each of the first and second baseplates 100,200 instead of having a convex mesh as a vertebral body contact element, have a convex solid dome 103,203 and a plurality of spikes 105,205 as vertebral body contact element. Preferably, the dome 103,203 is covered with an osteoconductive layer of a type known in the art. It should be noted that the convex solid dome 203 of the second baseplate 200 is provided by the cap element (described below) that serves as an extension of the second baseplate 200 to capture the ball (described below), as best shown in Figs. 3u-y. It should also be noted that the convex mesh is suitable for use with these other vertebral body contact elements, and can be attached over the convex dome 103,203 by laser welding, or more preferably, by plasma burying (where the perimeter region of the convex mesh is buried under a plasma coating, which coating secures to the outwardly facing surface of the baseplate to which it is applied, and thus secures the convex mesh to the outwardly facing surface).

[0102] Further, the two baseplates 100,200, are joined with a ball and socket joint, and therefore each of the baseplates 100,200 comprises features that, in conjunction with other components described below, form the ball and socket joint. The ball and socket joint includes a solid ball (described below) mounted to protrude from the inwardly facing surface 108 of the first baseplate 100, and a curvate socket formed at a peak of a non-flexible convex structure (described below) that is integral with the second baseplate 200, within which curvate socket the ball is capturable for free rotation and angulation therein. As shown in Figs. 3a-e, the mounting for the ball includes a central hole 112 on the inwardly facing surface 108 of the first baseplate 100, which hole 112 accepts a tail end of a post (described below) that has the ball at a head end of the post. Preferably, the tail end compression locks into the hole 112. As shown in Figs. 3f-j, the convex structure 201 is integral with the second baseplate 200 and includes a curvate pocket 212 formed by a central portion of the inwardly facing surface 209 of the convex structure 201 convexing inwardly and by a central portion of an outwardly facing surface 213 of the convex structure 201 concaving inwardly. The pocket 212 has a semispherical contour on the central portion of the outwardly facing surface 213 and an apex at the center of the semispherical contour. Further, the convex structure 201 has a bore 214 through the apex of the pocket 212, to accommodate the post. Further, the second baseplate 200 has on its outwardly facing surface 202 an access hole 209 surrounded by a circular recess 216 leading to the pocket 212, which recess 216 accepts the cap (described below) that serves as an extension of the second baseplate 200.

[0103] Referring now to Figs. 3k-o, a first type 300 of the ball is shown in top (Fig. 3k), side (Fig. 3l), side cutaway (Fig. 3m), perspective cutaway (Fig. 3n) and perspective (Fig. 3o) views. The ball 300 is mounted at a

head end 306 of a post 302 that also has a tail end 304. The ball 300 defines a spherical contour that is interrupted by the shaft of the post 302.

[0104] Referring now to Figs. 3p-t, a first type 400 of the cap is shown in top (Fig. 3p), side (Fig. 3q), side cutaway (Fig. 3r), perspective cutaway (Fig. 3s) and perspective (Fig. 3t) views. The cap 400 includes an outwardly facing surface 402 that complements the outwardly facing surface 202 of the second baseplate 200 when the cap 400 is secured in the circular recess 216 of the second baseplate 200 (preferably, as shown, the outwardly facing surface 402 of the cap 400 provides the second baseplate 200 with the convex dome 203, as best shown in Figs. 3u-y). The cap 400 further includes an inwardly facing surface 404, and a curvate pocket 406 formed by a central portion of the inwardly facing surface 404 of the cap 400 concaving outwardly. The pocket 406 has a semispherical contour that closely accommodates the spherical contour defined by the ball 300. The semispherical contour of the pocket 406 of the cap 400 opposes the semispherical contour of the pocket 212 of the convex structure 201 such that when the cap 400 is secured in the circular recess 216 of the second baseplate 200, the semispherical contours together define a socket 207 defining a spherical contour that closely accommodates the spherical contour defined by the ball 300 for free rotation and angulation of the ball 300 in the pockets 406,212. Each of the semispherical contour of the pocket 406 and the semispherical contour of the pocket 212 are preferably no greater than hemispherical, to make easier the assembly of the device.

[0105] Referring now to Figs. 3u-y, an assembled first preferred embodiment is shown in top (Fig. 3u), side (Fig. 3v), side cutaway (Fig. 3w), perspective cutaway (Fig. 3x) and perspective (Fig. 3y) views. More particularly, assembly of the disc is preferably as follows. The tail end 304 of the post 302 is passed through the access hole 209 in the second baseplate 200 and through the bore 214 at the apex of the curvate pocket 212 of the convex structure 201, and the tail end 304 is thereafter secured to the central hole 112 in the first baseplate 100. (The access hole 209 has a diameter that accommodates the diameter of the ball 300 at the head 306 of the post 302, and the curvate pocket 212 on the outwardly facing surface 213 of the convex structure 201 has an opening diameter that accommodates the ball 300 for seating in the pocket 212 when the tail end 304 is fully passed through the bore 214. Thus, the ball 300 can be placed through the access hole 209 and into the curvate pocket 212 during this step.) The bore 214 at the apex of the curvate pocket 212 has a diameter greater than the diameter of the post 302 but smaller than the diameter of the ball 300 at the head 306 of the post 302. Therefore, as the ball 300 is being placed into the curvate pocket 212, the post 302 fits through the bore 214, but the ball 300 does not, and the convex structure 201 (and the second baseplate 200) cannot be freed from the ball 300 once the tail end 304 of the post 302 is secured to the first baseplate 100.

The attachment of the tail end 304 of the post 302 is preferably accomplished by compression locking (if accomplished alternatively or additionally by laser welding, the laser weld can, e.g., be applied from the outwardly facing surface 102 of the first baseplate 100 if the hole 112 passes completely through the first baseplate 100). The tail end 304 can also alternatively or additionally be threaded into the central hole 112 for increased stability of the attachment.

[0106] The semispherical contour of the pocket 212 closely accommodates the spherical contour defined by the ball 300, so that the ball 300 can freely rotate in the pocket 212 about the longitudinal axis of the post 302, and can freely angulate in the pocket 212 about a centroid of motion located at the center of the ball 300. Further, the bore 214 is tapered to a larger diameter toward the first baseplate 100, to permit the post 302 to angulate (about the centroid of motion at the center of the ball 300) with respect to the bore 214 as the ball 300 angulates in the pocket 212. Preferably, the conformation of the taper accommodates angulation of the post 302 at least until the perimeter regions 110,210 of the inwardly facing surfaces 108,208/211 meet.

[0107] Finally, the cap 400 is secured in the circular recess 216 of the second baseplate 200, so that the curvate pocket 406 of the cap 400 and the opposing curvate pocket 212 of the convex structure 201 together form the socket 207 defining the spherical contour within which the ball 300 at the head 306 of the post 302 freely rotates and angulates as described above. The application of the cap 400 also seals the access hole 209 in the second baseplate (or, if the cap 400 has a bore, it preferably reduces the diameter of the access hole 209 to a size that does not accommodate the diameter of the ball 300). The cap 400 preferably is secured in the circular recess 216 by compression locking (a laser weld can alternatively or additionally be used, or other suitable attachment means). As stated above, the cap 400 preferably has an outwardly facing surface 402 that complements the outwardly facing surface 202 of the second baseplate 200 for surface uniformity once the cap 400 is secured. The cap 400 may also additionally or alternatively be threaded into the circular recess 216 for increased stability of the attachment.

[0108] Referring now to Fig. 3z, an assembled alternate intervertebral implant is shown in side cutaway view. This one incorporates a multi-part cap (with first part 4000a and second part 4000b) housing a spring member 4100 that provides axial compressibility, such that a compressive load applied to the baseplates is borne by the spring member 4100. Elements of this implant that are also elements found in the above described implants are like numbered, and the assembly is identical to that above, with some differences due to the incorporation of the spring member 4100. (For example, the cap features are numbered in the 4000's rather than the 400's.) More particularly, assembly of the disc is preferably as follows. The tail end 304 of the post 302 is passed through the

access hole 209 in the second baseplate 200 and through the bore 214 at the apex of the curvate pocket 212 of the convex structure 201, and the tail end 304 is thereafter secured to the central hole 112 in the first baseplate 100. (The access hole 209 has a diameter that accommodates the diameter of the ball 300 at the head 306 of the post 302, and the curvate pocket 212 on the outwardly facing surface 213 of the convex structure 201 has an opening diameter that accommodates the ball 300 for seating in the pocket 212 when the tail end 304 is fully passed through the bore 214. Thus, the ball 300 can be placed through the access hole 209 and into the curvate pocket 212 during this step.) The bore 214 at the apex of the curvate pocket 212 has a diameter greater than the diameter of the post 302 but smaller than the diameter of the ball 300 at the head 306 of the post 302. Therefore, as the ball 300 is being placed into the curvate pocket 212, the post 302 fits through the bore 214, but the ball 300 does not, and the convex structure 201 (and the second baseplate 200) cannot be freed from the ball 300 once the tail end 304 of the post 302 is secured to the first baseplate 100. The attachment of the tail end 304 of the post 302 is preferably accomplished by compression locking (if accomplished alternatively or additionally by laser welding, the laser weld can, e.g., be applied from the outwardly facing surface 102 of the first baseplate 100 if the hole 112 passes completely through the first baseplate 100). The tail end 304 can also alternatively or additionally be threaded into the central hole 112 for increased stability of the attachment.

[0109] The semispherical contour of the pocket 212 closely accommodates the spherical contour defined by the ball 300, so that the ball 300 can freely rotate in the pocket 212 about the longitudinal axis of the post 302, and can freely angulate in the pocket 212 about a centroid of motion located at the center of the ball 300. Further, the bore 214 is tapered to a larger diameter toward the first baseplate 100, to permit the post 302 to angulate (about the centroid of motion at the center of the ball 300) with respect to the bore 214 as the ball 300 angulates in the pocket 212. Preferably, the conformation of the taper accommodates angulation of the post 302 at least until the perimeter regions 110,210 of the inwardly facing surfaces 108,208/211 meet.

[0110] The second part 4000b of the multi-part cap is secured in the circular recess 216 of the second baseplate 200, so that the curvate pocket 406 of the inwardly facing surface 4040b of the cap second part 4000b and the opposing curvate pocket 212 of the convex structure 201 together form the socket 207 defining the spherical contour within which the ball 300 at the head 306 of the post 302 freely rotates and angulates as described above. The application of the cap second part 4000b (and the cap first part 4000a) also seals the access hole 209 in the second baseplate (or, if the cap second and first parts 4000b, 4000a have bores, it preferably reduces the diameter of the access hole 209 to a size that does not accommodate the diameter of the ball 300). The cap sec-

ond part 4000b is preferably not compressed into, but rather fits loosely within the boundaries of, the circular recess 216, so that when the first baseplate 100 is compressed toward the second baseplate 200, the cap second part 4000b may travel toward the cap first part 4000a as the spring member 4100 compresses (due to the cap first part 4000a being secured in the circular recess 216 to the second baseplate 200). The spring member 4100 is then disposed on the outwardly facing surface 4020b of the cap second part 4000b. While not limited to any particular structure, assembly, or material, a spring member providing shock absorption preferably includes an elastomeric material, such as, for example, polyurethane or silicon, and a spring member providing shock dampening preferably includes a plastic material, such as, for example, polyethylene. It should be understood that metal springs may alternatively or additionally be used. The illustrated spring member 4100 is formed of an elastomeric material, for example. The illustrated spring member 4100 is ring-shaped, for example, such that it fits just inside the circumferential edge of the outwardly facing surface 4020b of the cap second part 4000b as shown.

[0111] Finally, the cap first part 4000a is secured in the circular recess 216 of the second baseplate 200 to incarcerate the cap second part 4000b, and the spring member 4100 between the outwardly facing surface 4020b of the cap second part 4000b and the inwardly facing surface 4040a of the cap first part 4000a.

The cap first part 4000a preferably is secured in the circular recess 216 by compression locking (a laser weld can alternatively or additionally be used, or other suitable attachment means). The cap second part 4000b should be dimensioned such that, and the spring member 4100 should have an uncompressed height such that, a gap is present between the outwardly facing surface 4020b of the cap second part 4000b and the inwardly facing surface 4040a of the cap first part 4000a when the disc is assembled. The gap preferably has a height equivalent to the anticipated distance that the spring member 4100 will compress under an anticipated load. The cap first part 4000a preferably has an outwardly facing surface 4020a that complements the outwardly facing surface 202 of the second baseplate 200 for surface uniformity once the cap first part 4000a is secured. The cap first part 4000a may also additionally or alternatively be threaded into the circular recess 216 for increased stability of the attachment. Accordingly, part or all of a compressive load applied to the baseplates will be borne by the spring member 4100, which will dampen the load and/or absorb the load and preferably help return the baseplates to their original uncompressed relative positions.

[0112] Accordingly, when a device is assembled, the baseplates are rotatable relative to one another because the ball 300 rotates freely within the socket 207, and angulatable relative to one another because the ball 300 angulates freely within the socket 207. Because the ball 300 is held within the socket 207 by the securing of the

tail end 304 of the post 302 to the first baseplate 100 and the securing of the cap 400 (or cap first part 4000a) to the second baseplate 200, the artificial disc can withstand tension loading of the baseplates 100,200. More particularly, when a tension load is applied to the baseplates 100,200 the ball 300 seeks to pass through the bore 214 at the apex of the curvate pocket 212. However, the smaller diameter of the bore 214 relative to the diameter of the ball 300 prevents the ball 300 from exiting the socket 207. Therefore, the assembly does not come apart under normally experienced tension loads. This ensures that no individual parts of the assembly will pop out or slip out from between the vertebral bodies when, e.g., the patient stretches or hangs while exercising or performing other activities. Thus, in combination with the securing of the baseplates 100,200 to the adjacent vertebral bones via the domes 103,203 and spikes 105,205, the disc assembly has an integrity similar to the tension-bearing integrity of a healthy natural intervertebral disc. Also because the ball 300 is laterally captured in the socket 207, lateral translation of the baseplates 100,200 relative to one another is prevented during rotation and angulation, similar to the performance of healthy natural intervertebral disc. Because the baseplates 100,200 are made angulatable relative to one another by the ball 300 being rotatably and angulatably coupled in the socket 207, the disc assembly provides a centroid of motion within the ball 300. Accordingly, the centroid of motion of the disc assembly remains centrally located between the vertebral bodies, similar to the centroid of motion in a healthy natural intervertebral disc.

[0113] The remaining implants limit the rotation (but preferably not the angulation) of the ball in the socket defined by the pocket of the convex structure and the pocket of the cap. Each implant accomplishes this in a different manner, but each one utilizes interference between a protrusion and a recess to limit the rotation. In some, the protrusion is preferably hemispherical, and the recess preferably has a semicylindrical contour within which the protrusion fits. In other, the protrusion is preferably hemispherical, and the recess preferably has a curvate contour that is not semicylindrical. (It should be understood that the described formations of the recess and the protrusion are merely preferred, and that alternate formations, curvate or otherwise, for each are contemplated; a particular shape or location of recess or a particular shape or location of protrusion is not required; any shape can be used so long as the recess and protrusion interact as desired. For example, the recess has a curvate contour that is not semicylindrical so that it optimally interacts with the protrusion in that embodiment.) The boundaries of the recess define the limits of rotation of the ball within the socket, by allowing movement of the protrusion relative to the recess as the ball rotates through a certain range in the socket, but providing interference with the protrusion to prevent rotation of the ball beyond that range in the socket. Preferably, for example, the recess has a depth equivalent to the radius

of the protrusion, but a radius of curvature greater than that of the protrusion. At the same time, the boundaries of the recess preferably do not limit the angulation of the ball within the socket, at least until the perimeter regions of the inwardly facing surfaces meet. Preferably for example, the recess has a length greater than the range of movement of the protrusion relative to the recess as the ball angulates in the socket

[0114] Therefore, when assembled, the discs enable angulation and limited rotation of the baseplates relative to one another about a centroid of motion that remains centrally located between the baseplates (at the center of the sphere defined by the ball), similar to the centroid of motion in a healthy natural intervertebral disc that is limited in its rotation by surrounding body structures. A benefit of limiting the relative rotation of the baseplates is that relative rotation beyond a certain range in a healthy natural disc is neither needed nor desired, because, for example, excess strain can be placed on the facet joints or ligaments thereby. As described above, the construction also prevents translation and separation of the baseplates relative to one another during rotation and angulation.

[0115] As noted above, each of the remaining implants forms the protrusion and corresponding recess in a different manner, utilizing components that are either identical or similar to the components above, and some embodiments utilize additional components. Other implants will now be described in greater detail.

[0116] A hemispherical protrusion is formed on the ball itself, and interacts in the above-described manner with a curvate recess formed adjacent the socket defined by the pocket of the convex structure and the pocket of the cap. More particularly, this implant uses the same first baseplate 100 as described above. Referring to Figs. 4a-e, a second type 500 of second baseplate is shown in top (Fig. 4a), side (Fig. 4b), side cutaway (Fig. 4c), perspective cutaway (Fig. 4d) and perspective (Fig. 4e) views. This second type 500 of second baseplate is identical to the first type 200 of second baseplate described above (and thus similar features are reference numbered similar to those of the first type 200 of second baseplate, but in the 500s rather than the 200s), except that this second type 500 of second baseplate has a curvate recess 518 adjacent the curvate pocket 512 in the convex structure 501.

[0117] Referring now to Figs. 4f-j, a second type 600 of ball is shown in top (Fig. 4f), side (Fig. 4g), side cutaway (Fig. 4h), perspective cutaway (Fig. 4i) and perspective (Fig. 4j) views. The ball 600 is identical to the first type 300 of ball described above (and thus similar features are reference numbered similar to those of the first type 300 of ball, but in the 600s rather than the 300s), except that the spherical contour defined by this second type 600 of ball is also interrupted by a hemispherical protrusion 608.

[0118] Referring now to Figs. 4k-o, a second type 700 of cap is shown in top (Fig. 4k), side (Fig. 4l), side cutaway

(Fig. 4m), perspective cutaway (Fig. 4n) and perspective (Fig. 4o) views. This second type 700 of cap is identical to the first type 400 of cap described above (and thus similar features are reference numbered similar to those of the first type 400 of cap, but in the 700s rather than the 400s), except that this second type 700 of cap has a curvate recess 708 adjacent the curvate pocket 706.

[0119] Referring now to Figs. 4p-t, an assembled implant is shown in top (Fig. 4p), side (Fig. 4q), side cutaway (Fig. 4r), perspective cutaway (Fig. 4s) and perspective (Fig. 4t) views. It can be seen that the curvate recesses 518,708 together form the recess described above in the discussion of the manner in which these remaining implants limit rotation of the ball in the socket, and that the protrusion 608 serves as the protrusion described above in the same discussion. Thus, the protrusion 608 and recesses 518,708 interact in the above described manner to limit the rotation of the ball 600 in the socket 507 defined by the curvate pockets 512,706. Assembly of the disc is identical to that described above, except that the protrusion 608 is longitudinally aligned with the recess 518, and the recess 708 is similarly aligned, so that when the cap 700 is secured to the second baseplate 500, the protrusion 608 is fitted within the recesses 518,708 for interaction as described above as the ball 600 rotates and angulates in the socket 507.

[0120] Referring now to Fig. 4u, an assembled alternate implant is shown in side cutaway view. This alternate implant incorporates a multi-part cap (with first part 7000a and second part 7000b) housing a spring member 7100 that provides axial compressibility, such that a compressive load applied to the baseplates is borne by the spring member 7100. Elements of this implant that are also elements found in the implants above are like numbered. (The cap features are numbered in the 7000's rather than the 700's.) The curvate recesses 518,7080 together form the recess described above, and the protrusion 608 serves as the protrusion described above, and thus the protrusion 608 and the recesses 518,7080 interact in the above described manner to limit the rotation of the ball 600 in the socket 507 defined by the curvate pockets 512,7060.

[0121] Assembly of this alternate implant is identical to that above, except that the protrusion 608 is longitudinally aligned with the recess 518, and the recess 7080 is similarly aligned, so that when the cap second part 7000b is disposed in the circular recess 516 of the second baseplate 500, the protrusion 608 is fitted within the recesses 518,7080 for interaction as described above as the ball 600 rotates and angulates in the socket 507. The cap second part 7000b is preferably not compressed into, but rather fits loosely within, the circular recess 516, so that when the first baseplate 100 is compressed toward the second baseplate 500, the cap second part 7000b may travel toward the cap first part 7000a as the spring member 7100 compresses (due to the cap first part 7000a being secured in the circular recess 516 to the second baseplate 500). The spring member 7100 is then

disposed on the outwardly facing surface 7020b of the cap second part 7000b. While not limited to any particular structure, assembly, or material, a spring member providing shock absorption preferably includes an elastomeric material, such as, for example, polyurethane or silicon, and a spring member providing shock dampening preferably includes a plastic material, such as, for example, polyethylene. It should be understood that metal springs may alternatively or additionally be used. The illustrated spring member 7100 is formed of an elastomeric material, for example. The illustrated spring member 7100 is ring-shaped, for example, such that it fits just inside the circumferential edge of the outwardly facing surface 7020b of the cap second part 7000b as shown.

[0122] Finally, the cap first part 7000a is secured in the circular recess 516 of the second baseplate 500 to incarcerate the cap second part 7000b, and the spring member 7100 between the outwardly facing surface 7020b of the cap second part 7000b and the inwardly facing surface 7040a of the cap first part 7000a. The cap first part 7000a preferably is secured in the circular recess 516 by compression locking (a laser weld can alternatively or additionally be used, or other suitable attachment means). The cap second part 7000b should be dimensioned such that, and the spring member 7100 should have an uncompressed height such that, a gap is present between the outwardly facing surface 7020b of the cap second part 7000b and the inwardly facing surface 7040a of the cap first part 7000a when the disc is assembled. The gap preferably has a height equivalent to the anticipated distance that the spring member 7100 will compress under an anticipated load. The cap first part 7000a preferably has an outwardly facing surface 7020a that complements the outwardly facing surface 502 of the second baseplate 500 for surface uniformity once the cap first part 7000a is secured. The cap first part 7000a may also additionally or alternatively be threaded into the circular recess 516 for increased stability of the attachment. Accordingly, part or all of a compressive load applied to the baseplates will be borne by the spring member 7100, which will dampen the load and/or absorb the load and preferably help return the baseplates to their original uncompressed relative positions.

[0123] A hemispherical protrusion is formed to protrude into the socket defined by the pocket of the convex structure and the pocket of the cap, and interacts in the above-described manner with a semicylindrical recess formed on the ball. More particularly, this implant uses the same first baseplate 100 and the same cap 400. Referring to Figs. 5a-e, a third type 800 of second baseplate is shown in top (Fig. 5a), side (Fig. 5b), side cutaway (Fig. 5c), perspective cutaway (Fig. 5d) and perspective (Fig. 5e) views. This third type 800 of second baseplate is identical to the first type 200 of second baseplate described above (and thus similar features are reference numbered similar to those of the first type 200 of second baseplate, but in the 800s rather than the 200s), except that this third type 800 of second baseplate has a protrusion 818 jutting out from the wall of the pocket 812 in the

convex structure 801.

[0124] Referring now to Figs. 5f-j, a third type 900 of ball is shown in top (Fig. 5f), side (Fig. 5g), side cutaway (Fig. 5h), perspective cutaway (Fig. 5i) and perspective (Fig. 5j) views. The ball 900 is identical to the first type 300 of ball described above (and thus similar features are reference numbered similar to those of the first type 300 of ball, but in the 900s rather than the 300s), except that the spherical contour of this third type 900 of ball is also interrupted by a curvate recess 908.

[0125] Referring now to Figs. 5k-o, an assembled implant is shown in top (Fig. 5k), side (Fig. 5l), side cutaway (Fig. 5m), perspective cutaway (Fig. 5n) and perspective (Fig. 5o) views. It can be seen that the curvate recess 908 forms the recess described above in the discussion of the manner in which these limit rotation of the ball in the socket, and that the protrusion 818 serves as the protrusion described above in the same discussion. Thus, the protrusion 818 and recess 908 interact in the above described manner to limit the rotation of the ball 900 in the socket 807 defined by the curvate pockets 812,406. Assembly of the disc is identical to that of the first preferred embodiment of the third embodiment family, except that the protrusion 818 is longitudinally aligned with the recess 908 during assembly so that the protrusion 818 is fitted within the recess 908 for interaction as described above as the ball 900 rotates and angulates in the socket 807.

[0126] Referring now to Fig. 5p, an assembled alternate implant is shown in side cutaway view. This incorporates a multi-part cap (with first part 4000a and second part 4000b) housing a spring member 4100 that provides axial compressibility, such that a compressive load applied to the baseplates is borne by the spring member 4100. Elements of this alternate implant that are also elements found above are like numbered. (The cap features are numbered in the 4000's rather than the 400's.) The curvate recess 908 forms the recess described above, and the protrusion 818 serves as the protrusion described above, and thus the protrusion 818 and the recess 908 interact in the above described manner to limit the rotation of the ball 900 in the socket 807 defined by the curvate pockets 812,4060.

[0127] Assembly of this alternate implant is identical to that as described above, except that the protrusion 818 is longitudinally aligned with the recess 908 during assembly so that the protrusion 818 is fitted within the recess 908 for interaction as described above as the ball 900 rotates and angulates in the socket 807. The cap second part 4000b is preferably not compressed into, but rather fits loosely within, the circular recess 816, so that when the first baseplate 100 is compressed toward the second baseplate 800, the cap second part 4000b may travel toward the cap first part 4000a as the spring member 4100 compresses (due to the cap first part 4000a being secured in the circular recess 816 to the second baseplate 800). The spring member 4100 is then dis-

posed on the outwardly facing surface 4020b of the cap second part 4000b. While not limited to any particular structure, assembly, or material, a spring member providing shock absorption preferably includes an elastomeric material, such as, for example, polyurethane or silicon, and a spring member providing shock dampening preferably includes a plastic material, such as, for example, polyethylene. It should be understood that metal springs may alternatively or additionally be used. The illustrated spring member 4100 is formed of an elastomeric material, for example. The illustrated spring member 4100 is ring-shaped, for example, such that it fits just inside the circumferential edge of the outwardly facing surface 4020b of the cap second part 4000b as shown.

[0128] Finally, the cap first part 4000a is secured in the circular recess 816 of the second baseplate 800 to incarcerate the cap second part 4000b, and the spring member 4100 between the outwardly facing surface 4020b of the cap second part 4000b and the inwardly facing surface 4040a of the cap first part 4000a. The cap first part 4000a preferably is secured in the circular recess 816 by compression locking (a laser weld can alternatively or additionally be used, or other suitable attachment means). The cap second part 4000b should be dimensioned such that, and the spring member 4100 should have an uncompressed height such that, a gap is present between the outwardly facing surface 4020b of the cap second part 4000b and the inwardly facing surface 4040a of the cap first part 4000a when the disc is assembled. The gap preferably has a height equivalent to the anticipated distance that the spring member 4100 will compress under an anticipated load. The cap first part 4000a preferably has an outwardly facing surface 4020a that complements the outwardly facing surface 802 of the second baseplate 800 for surface uniformity once the cap first part 4000a is secured. The cap first part 4000a may also additionally or alternatively be threaded into the circular recess 816 for increased stability of the attachment. Accordingly, part or all of a compressive load applied to the baseplates will be borne by the spring member 4100, which will dampen the load and/or absorb the load and preferably help return the baseplates to their original uncompressed relative positions.

[0129] A pin is secured in a pin hole so that the hemispherical head of the pin protrudes into the socket defined by the pocket of the convex structure and the pocket of the cap, and interacts in the above-described manner with a semicylindrical recess formed on the ball. More particularly, this implant uses the same first baseplate 100 and cap 400 and the same ball 900, but utilizes a fourth type of second baseplate. Referring to Figs. 6a-e, the fourth type 1000 of second baseplate is shown in top (Fig. 6a), side (Fig. 6b), side cutaway (Fig. 6c), perspective cutaway (Fig. 6d) and perspective (Fig. 6e) views. This fourth type 1000 of second baseplate is identical to the first type 200 of second baseplate described above (and thus similar features are reference numbered similar to those of the first type 200 of second baseplate, but in

the 1000s rather than the 200s), except that this fourth type 1000 of second baseplate has a lateral through hole (e.g., a pin hole 1020) and a protrusion (e.g., a pin 1018) secured in the pin hole 1020 (as shown in Figs. 6f-j) with the hemispherical head of the pin 1018 jutting out from the wall of the pocket 1012 toward the center of the pocket 1012 in the convex structure 1001.

[0130] Referring now to Figs. 6f-j, an assembled implant is shown in top (Fig. 6f), side (Fig. 6g), side cutaway (Fig. 6h), perspective cutaway (Fig. 6i) and perspective (Fig. 6j) views. It can be seen that the curvate recess 908 of the ball 900 forms the recess described above in the discussion of the manner in which these remaining implants limit rotation of the ball in the socket, and that the head of the pin 1018 serves as the protrusion described above in the same discussion. Thus, the head of the pin 1018 and the recess 908 interact in the above described manner to limit the rotation of the ball 900 in the socket 1007 defined by the curvate pockets 1012, 406. Assembly of the disc is identical to that described above, except that the head of the pin 1018 is longitudinally aligned with the recess 908 during assembly so that the head of the pin 1018 is fitted within the recess 908 for interaction as described above as the ball 900 rotates and angulates in the socket 1007.

[0131] Referring now to Fig. 6k, an assembled alternate implant is shown in side cutaway view. This incorporates a multi-part cap (with first part 4000a and second part 4000b) housing a spring member 4100 that provides axial compressibility, such that a compressive load applied to the baseplates is borne by the spring member 4100. Elements of this alternate implant that are also elements found above are like numbered. (The cap features are numbered in the 4000's rather than the 400's.) The curvate recess 908 of the ball 900 forms the recess described above, and the head of the pin 1018 serves as the protrusion described above, and thus the head of the pin 1018 and the recess 908 interact in the above described manner to limit the rotation of the ball 900 in the socket 1007 defined by the curvate pockets 1012, 406.

[0132] Assembly of this implant is identical to that above, except that the head of the pin 1018 is longitudinally aligned with the recess 908 during assembly so that the head of the pin 1018 is fitted within the recess 908 for interaction as described above as the ball 900 rotates and angulates in the socket 1007. The cap second part 4000b is preferably not compressed into, but rather fits loosely within, the circular recess 1016, so that when the first baseplate 100 is compressed toward the second baseplate 1000, the cap second part 4000b may travel toward the cap first part 4000a as the spring member 4100 compresses (due to the cap first part 4000a being secured in the circular recess 1016 to the second baseplate 1000). The spring member 4100 is then disposed on the outwardly facing surface 4020b of the cap second part 4000b. While not limited to any particular structure, assembly, or material, a spring member providing shock

absorption preferably includes an elastomeric material, such as, for example, polyurethane or silicon, and a spring member providing shock dampening preferably includes a plastic material, such as, for example, polyethylene. It should be understood that metal springs may alternatively or additionally be used. The illustrated spring member 4100 is formed of an elastomeric material, for example. The illustrated spring member 4100 is ring-shaped, for example, such that it fits just inside the circumferential edge of the outwardly facing surface 4020b of the cap second part 4000b as shown.

[0133] Finally, the cap first part 4000a is secured in the circular recess 1016 of the second baseplate 1000 to incarcerate the cap second part 4000b, and the spring member 4100 between the outwardly facing surface 4020b of the cap second part 4000b and the inwardly facing surface 4040a of the cap first part 4000a.

The cap first part 4000a preferably is secured in the circular recess 1016 by compression locking (a laser weld can alternatively or additionally be used, or other suitable attachment means). The cap second part 4000b should be dimensioned such that, and the spring member 4100 should have an uncompressed height such that, a gap is present between the outwardly facing surface 4020b of the cap second part 4000b and the inwardly facing surface 4040a of the cap first part 4000a when the disc is assembled. The gap preferably has a height equivalent to the anticipated distance that the spring member 4100 will compress under an anticipated load. The cap first part 4000a preferably has an outwardly facing surface 4020a that complements the outwardly facing surface 1002 of the second baseplate 1000 for surface uniformity once the cap first part 4000a is secured. The cap first part 4000a may also additionally or alternatively be threaded into the circular recess 1016 for increased stability of the attachment. Accordingly, part or all of a compressive load applied to the baseplates will be borne by the spring member 4100, which will dampen the load and/or absorb the load and preferably help return the baseplates to their original uncompressed relative positions.

[0134] A ball bearing protrudes into the socket defined by the pocket of the convex structure and the pocket of the cap, and interacts in the above-described manner with a semicylindrical recess formed on the ball. More particularly, this implant uses the same first baseplate 100 and cap 400 and the same ball 900, but utilizes a fifth type of second baseplate. Referring to Figs. 7a-e, the fifth type 1200 of second baseplate is shown in top (Fig. 7a), side (Fig. 7b), side cutaway (Fig. 7c), perspective cutaway (Fig. 7d) and perspective (Fig. 7e) views. This fifth type 1200 of second baseplate is identical to the first type 200 of second baseplate described above (and thus similar features are reference numbered similar to those of the first type 200 of second baseplate, but in the 1200s rather than the 200s), except that this fifth type 1200 of second baseplate has a recess 1218 adjacent the curvate pocket 1212 in the convex structure 1201,

the recess 1218 preferably being semicylindrical as shown.

[0135] Referring now to Figs. 7f-j, an assembled implant is shown in top (Fig. 7f), side (Fig. 7g), side cutaway (Fig. 7h), perspective cutaway (Fig. 7i) and perspective (Fig. 7j) views. A ball bearing 1300 is captured for free rotation and angulation with one part closely accommodated in the semicylindrical recess 1218 and one part protruding into the curvate pocket 1212 to interact with the curvate recess 908 of the ball 900. It can be seen that the curvate recess 908 of the ball 900 forms the recess described above in the discussion of the manner in which these remaining implants limit rotation of the ball in the socket, and that the ball bearing 1300 serves as the protrusion described above in the same discussion. Thus, the ball bearing 1300 and the recess 908 interact in the above described manner to limit the rotation of the ball 900 in the socket 1207 defined by the curvate pockets 1212,406. Assembly of the disc is identical to that described above, except that the semicylindrical recess 1218 is longitudinally aligned with the curvate recess 908 during assembly so that the ball bearing 1300 can be and is then placed into the recesses 1218,908 for interaction as described above as the ball 900 rotates and angulates in the socket 1207.

[0136] Referring now to Fig. 7k, an assembled implant is shown in side cutaway view. This incorporates a multi-part cap (with first part 4000a and second part 4000b) housing a spring member 4100 that provides axial compressibility, such that a compressive load applied to the baseplates is borne by the spring member 4100. Elements of this alternate implant that are also elements found above are like numbered. (The cap features are numbered in the 4000's rather than the 400's.) The curvate recess 908 of the ball 900 forms the recess described above, and the ball bearing 1300 serves as the protrusion described above, and thus the ball bearing 1300 and the recess 908 interact in the above described manner to limit the rotation of the ball 900 in the socket 1207 defined by the curvate pockets 1212,4060.

[0137] Assembly of this alternate implant is identical to that described above, except that the semicylindrical recess 1218 is longitudinally aligned with the curvate recess 908 during assembly so that the ball bearing 1300 can be and is then placed into the recesses 1218,908 for interaction as described above as the ball 900 rotates and angulates in the socket 1207. The cap second part 4000b is preferably not compressed into, but rather fits loosely within, the circular recess 1216, so that when the first baseplate 100 is compressed toward the second baseplate 1200, the cap second part 4000b may travel toward the cap first part 4000a as the spring member 4100 compresses (due to the cap first part 4000a being secured in the circular recess 1216 to the second baseplate 1200). The spring member 4100 is then disposed on the outwardly facing surface 4020b of the cap second part 4000b. While not limited to any particular structure, assembly, or material, a spring member providing shock

absorption preferably includes an elastomeric material, such as, for example, polyurethane or silicon, and a spring member providing shock dampening preferably includes a plastic material, such as, for example, polyethylene. It should be understood that metal springs may alternatively or additionally be used. The illustrated spring member 4100 is formed of an elastomeric material, for example. The illustrated spring member 4100 is ring-shaped, for example, such that it fits just inside the circumferential edge of the outwardly facing surface 4020b of the cap second part 4000b as shown.

[0138] Finally, the cap first part 4000a is secured in the circular recess 1216 of the second baseplate 1200 to incarcerate the cap second part 4000b, and the spring member 4100 between the outwardly facing surface 4020b of the cap second part 4000b and the inwardly facing surface 4040a of the cap first part 4000a.

The cap first part 4000a preferably is secured in the circular recess 1216 by compression locking (a laser weld can alternatively or additionally be used, or other suitable attachment means). The cap second part 4000b should be dimensioned such that, and the spring member 4100 should have an uncompressed height such that, a gap is present between the outwardly facing surface 4020b of the cap second part 4000b and the inwardly facing surface 4040a of the cap first part 4000a when the disc is assembled. The gap preferably has a height equivalent to the anticipated distance that the spring member 4100 will compress under an anticipated load. The cap first part 4000a preferably has an outwardly facing surface 4020a that complements the outwardly facing surface 1202 of the second baseplate 1200 for surface uniformity once the cap first part 4000a is secured. The cap first part 4000a may also additionally or alternatively be threaded into the circular recess 1216 for increased stability of the attachment. Accordingly, part or all of a compressive load applied to the baseplates will be borne by the spring member 4100, which will dampen the load and/or absorb the load and preferably help return the baseplates to their original uncompressed relative positions.

[0139] With regard to the configuration of the convex structure, the convex structure is configured as a non-flexible element that has the socket of the ball and socket joint at its peak. The convex structure is shaped to have a curved taper, similar to the configuration of the convex structure described above. The convex structure is separated from the second baseplate during assembly of the device, for reasons related to the manner in which the ball is captured in the socket, but is attached to the second baseplate by the time assembly is complete.

[0140] With regard to the manner in which the ball is captured in the socket, the capturing is effected through the use of a solid ball. In order to permit the seating of the ball into the socket formed at the peak of the convex structure, the convex structure is a separate element from the second baseplate. The ball is first seated against the central portion of the second baseplate (which central

portion preferably has a concavity that has a curvature that closely accommodates the contour of the ball), and then the convex structure is placed over the ball to seat the ball in the socket formed in the interior of the peak of the convex structure (the interior is preferably formed as a concavity that is either hemispherical or less-than-hemispherical so that the ball can easily fit into it). After the convex structure is placed over the ball, the convex structure is attached to the second baseplate to secure the ball in the socket. The peak of the convex structure has a bore that accommodates a post to which the ball and the first baseplate are attached (one to each end of the post), but does not accommodate the ball for passage through the bore. Accordingly, the ball is maintained in the socket.

[0141] Referring to Figs. 8a-e, a first baseplate 1400 is shown in top (Fig. 8a), side (Fig. 8b), side cutaway (Fig. 8c), perspective cutaway (Fig. 8d) and perspective (Fig. 8e) views. Also referring to Figs. 8f-j, a first type 1500 of a second baseplate is shown in top (Fig. 8f), side (Fig. 8g), side cutaway (Fig. 8h), perspective cutaway (Fig. 8i) and perspective (Fig. 8j) views.

[0142] More specifically, the first and second baseplates 1400, 1500 are similar to the first and second baseplates described above with regard to their outwardly facing surfaces 1402, 1502 having a convex dome 1403, 1503 and a plurality of spikes 1405, 1505 as vertebral body contact elements, and the inwardly facing surface 1408 of the first baseplate having a perimeter region 1410, all of which elements are, for example, identical to the corresponding elements described above. Preferably, the dome 1403, 1503 is covered with an osteoconductive layer of a type known in the art. It should be noted that the convex mesh used in other implants is suitable for use with these other vertebral body contact elements, and can be attached over the convex dome 1403, 1503 by laser welding, or more preferably, by plasma burying (where the perimeter region of the convex mesh is buried under a plasma coating, which coating secures to the outwardly facing surface of the baseplate to which it is applied, and thus secures the convex mesh to the outwardly facing surface).

[0143] For example, and referring now to Figs. 8aa-8dd, an alternate first baseplate 9400 is shown in top (Fig. 8aa) and side cutaway (Fig. 8bb) views, respectively, and an alternate second baseplate 9500 is shown in top (Fig. 8cc) and side cutaway (Fig. 8dd) views, respectively. The alternate first and second baseplates 9400, 9500 are similar to the first and second baseplates described above, having identical features numbered in the 9400's and 9500's rather than the 1400's and 1500's, respectively. However, the alternate baseplates are different in that each has a convex mesh 9450, 9550 attached to the outwardly facing surface 9402, 9502 by burying the perimeter of the mesh 9450, 9550 in a plasma coating (or other suitable material, preferably having an osteoconductive surface) 9452, 9552 that is secured to both the outwardly facing surface 9402, 9502 and the

mesh 9450,9550. The plasma coating 9452,9552 serves not only to secure the mesh 9450,9550, but also to facilitate securing of the baseplates to the adjacent vertebral endplates. It should be understood that these alternate baseplates can be used in place of the other baseplates discussed herein, to construct artificial discs contemplated by the present invention.

[0144] Further, the two baseplates 1400,1500 are joined with a ball and socket joint, and therefore each of the baseplates 1400,1500 comprises features that, in conjunction with other components described below, form the ball and socket joint. The ball and socket joint includes a solid ball (described below) mounted to protrude from the inwardly facing surface 1408 of the first baseplate 1400, and a curvate socket formed at a peak of a non-flexible convex structure (described below) that is attached to the inwardly facing surface 1508 of the second baseplate 1500, within which curvate socket the ball is capturable for free rotation and angulation therein. As shown in Figs. 8a-d, the mounting for the ball includes a central inwardly directed post 1412 that extends from the inwardly facing surface 1408 of the first baseplate 1400, which post's head end compression locks into a central bore in the ball (described below). As shown in Figs. 8e-h, the second baseplate 1500 includes an inwardly facing surface 1508 and a curvate pocket 1512 formed by a central portion of the inwardly facing surface 1508 concaving outwardly with a semispherical contour (preferably a hemispherical contour). Preferably, as shown, the curvate pocket 1512 is surrounded by a circumferential wall 1514 and a circumferential recess 1516 that cooperate with the convex structure to attach the convex structure to the second baseplate 1500.

[0145] Referring now to Figs. 8k-o, a first type 1600 of a ball is shown in top (Fig. 8k), side (Fig. 8l), side cutaway (Fig. 8m), perspective cutaway (Fig. 8n) and perspective (Fig. 8o) views. The ball 1600 is semispherical (preferably greater than hemispherical as shown) and therefore defines a spherical contour, and has a central bore 1610 within which the first baseplate's post's head end is securable. The ball 1600 seats in the curvate pocket 1512 of the second baseplate 1500 with the spherical contour defined by the ball 1600 closely accommodated by the hemispherical contour of the curvate pocket 1512 for free rotation and free angulation of the ball 1600 in the curvate pocket 1512.

[0146] Referring now to Figs. 8p-t, a first type 1700 of a convex structure is shown in top (Fig. 8p), side (Fig. 8q), side cutaway (Fig. 8r), perspective cutaway (Fig. 8s) and perspective (Fig. 8t) views. The convex structure 1700 is shaped to have a curved taper on its inwardly facing surface 1706 (as opposed to the frusto-conical shape of the convex structure described above) and includes a central bore 1702 extending from an outwardly facing surface 1704 of the convex structure 1700 to an inwardly facing surface 1706 of the convex structure 1700, the bore 1702 being surrounded by a curvate taper 1708 on the outwardly facing surface 1704, and the cur-

vate taper 1708 being surrounded by a circumferential recess 1710 and a circumferential wall 1712. The convex structure 1700 is securable to the second baseplate 1500 with the circumferential recess 1710 of the convex structure 1700 mating with the circumferential wall 1514 of the second baseplate 1600 and the circumferential wall 1712 of the convex structure 1700 mating with the circumferential recess 1516 of the second baseplate 1500, so that when the convex structure 1700 is so secured, the curvate taper 1708 of the convex structure 1700 serves as a curvate pocket opposite the curvate pocket 1512 of the second baseplate 1500. That is, the curvate pocket 1708 complements the hemispherical contour of the curvate pocket 1512 of the second baseplate 1500 to form a semispherical (and preferably greater than hemispherical as shown) socket 1707 defining a spherical contour that closely accommodates the spherical contour defined by the ball 1600 so that the ball 1600 is captured in the socket 1707 for free rotation and free angulation of the ball 1600 therein. (When the formed socket 1707 is greater than hemispherical, and the shape of the ball 1600 is greater than hemispherical, the ball 1600 cannot escape the formed socket 1707.) Further, the inwardly facing surface 1706 of the convex structure 1700 has a perimeter region 1714 that faces the perimeter region 1410 of the first baseplate 1400 when the convex structure 1700 is secured to the second baseplate 1500.

[0147] Referring now to Figs. 8u-y, an assembled implant is shown in top (Fig. 8u), side (Fig. 8v), side cutaway (Fig. 8w), perspective cutaway (Fig. 8x) and perspective (Fig. 8y) views. More particularly, assembly of the disc is preferably as follows. The ball 1600 is seated within the curvate pocket 1512 of the second baseplate 1500 (the curvate pocket 1512 has an opening diameter that accommodates the ball 1600) so that the spherical contour defined by the ball 1600 is closely accommodated by the hemispherical contour of the curvate pocket 1512. Thereafter, the convex structure 1700 is secured to the second baseplate 1500 as described above with the convex structure's curvate pocket 1708 (the curvate tapered lip 1708 of the convex structure's central bore 1702) fitting against the ball 1600 so that the ball 1600 is captured in the socket 1707 (formed by the curvate taper 1708 and the curvate pocket 1512) for free rotation and free angulation of the ball 1600 therein. Thereafter, the first baseplate's post's head end is secured into the bore 1602 of the ball 1600. The central bore 1702 of the convex structure 1700 has a diameter that accommodates the diameter of the post 1412, but not the diameter of the ball 1600. Therefore, after the ball 1600 is secured in the socket 1707, the post 1412 fits through the bore 1702 so that the head end of the post 1412 can be compression locked to the ball 1600, but the ball 1600 is prevented from escaping the socket 1707 through the central bore 1702 of the convex structure 1700.

[0148] Accordingly, the ball 1600 is captured in the socket 1707 (so that the device will not separate in ten-

sion), can freely rotate in the socket 1707 about the longitudinal axis of the post 1412, and can freely angulate in the socket 1707 about a centroid of motion located at the center of the sphere defined by the ball 1600. Further, the opening of the bore 1702 of the cap 1700 on the inwardly facing surface 1706 of the convex structure 1700 is large enough to permit the post 1412 to angulate (about the centroid of motion at the center of the sphere defined by the ball 1600) with respect to the bore 1702 as the ball 1600 angulates in the socket 1707. Preferably, the conformation of the bore 1702 accommodates angulation of the post 1412 at least until the perimeter regions 1410, 1714 of the inwardly facing surfaces 1408, 1508/1706 meet. Further preferably, the perimeter regions 1410, 1714 have corresponding contours, so that the meeting of the perimeter regions reduces any surface wearing.

[0149] Referring now to Fig. 8z, an assembled alternate implant is shown in side cutaway view. This alternate first preferred embodiment incorporates a multi-part second baseplate (with first part 15000a and second part 15000b) housing a spring member 15100 that provides axial compressibility, such that a compressive load applied to the baseplates is borne by the spring member 15100. Elements of this alternate implant that are also elements found above are like numbered, and the assembly of this alternate implant is identical to that described above, with some differences due to the incorporation of the spring member 15100. (For example, the second baseplate features are numbered in the 15000's rather than the 1500's.) More particularly, assembly of the disc is preferably as follows. The ball 1600 is seated within the curvate pocket 15120 of the inwardly facing surface 15090b to the second baseplate second part 15000b (the curvate pocket 15120 has an opening diameter that accommodates the ball 1600) so that the spherical contour defined by the ball 1600 is closely accommodated by the hemispherical contour of the curvate pocket 15120. The spring member 15100 is then disposed on the outwardly facing surface 15020b of the second baseplate second part 15000b. While not limited to any particular structure, assembly, or material, a spring member providing shock absorption preferably includes an elastomeric material, such as, for example, polyurethane or silicon, and a spring member providing shock dampening preferably includes a plastic material, such as, for example, polyethylene. It should be understood that metal springs may alternatively or additionally be used. The illustrated spring member 15100 is formed of an elastomeric material, for example. The illustrated spring member 15100 is ring-shaped, for example, such that it fits just inside the circumferential edge of the outwardly facing surface 15020b of the second baseplate second part 15000b as shown.

[0150] The ball 1600, second baseplate second part 15000b, and spring member 15100 are then disposed on the inwardly facing surface 15090a of the second baseplate first part 15000a, such that the spring member

15100 is incarcerated between the inwardly facing surface 15090a of the second baseplate first part 15000a and the outwardly facing surface 15020b of the second baseplate second part 15000b. The second baseplate second part 15000b should be dimensioned such that, and the spring member 15100 should have an uncompressed height such that, a gap is present between the outwardly facing surface 15020b of the second baseplate second part 15000b and the inwardly facing surface 15090a of the second baseplate first part 15000a when the disc is assembled. The gap preferably has a height equivalent to the anticipated distance that the spring member 15100 will compress under an anticipated load. Thereafter, the convex structure 1700 is secured to the second baseplate first part 15000a, with the convex structure's curvate pocket 1708 (the curvate tapered lip 1708 of the convex structure's central bore 1702) fitting against the ball 1600 so that the ball 1600 is captured in the socket 1707 (formed by the curvate taper 1708 and the curvate pocket 15120) for free rotation and free angulation of the ball 1600 therein. The convex structure 1700 preferably is secured by compression locking (a laser weld can alternatively or additionally be used, or other suitable attachment means). The second baseplate first part 15000a may also additionally or alternatively be threaded to the convex structure 1700 for increased stability of the attachment. It should be understood that the second baseplate second part 15000b preferably fits loosely within the convex structure 1700 and the second baseplate first part 15000a, so that when the first baseplate 1400 is compressed toward the second baseplate first part 15000a, the second baseplate second part 15000b may travel toward the second baseplate first part 15000a as the spring member 15100 compresses. Thereafter, the first baseplate's post's head end is secured into the bore 1602 of the ball 1600. The central bore 1702 of the convex structure 1700 has a diameter that accommodates the diameter of the post 1412, but not the diameter of the ball 1600. Therefore, after the ball 1600 is secured in the socket 1707, the post 1412 fits through the bore 1702 so that the head end of the post 1412 can be compression locked to the ball 1600, but the ball 1600 is prevented from escaping the socket 1707 through the central bore 1702 of the convex structure 1700.

[0151] Accordingly, the ball 1600 is captured in the socket 1707 (so that the device will not separate in tension), can freely rotate in the socket 1707 about the longitudinal axis of the post 1412, and can freely angulate in the socket 1707 about a centroid of motion located at the center of the sphere defined by the ball 1600. Further, the opening of the bore 1702 of the convex structure 1700 on the inwardly facing surface 1706 of the convex structure 1700 is large enough to permit the post 1412 to angulate (about the centroid of motion at the center of the sphere defined by the ball 1600) with respect to the bore 1702 as the ball 1600 angulates in the socket 1707. Preferably, the conformation of the bore 1702 accommodates

angulation of the post 1412 at least until the perimeter regions 1410,1714 of the inwardly facing surfaces 1408,15080/1706 meet. Further preferably, the perimeter regions 1410,1714 have corresponding contours, so that the meeting of the perimeter regions reduces any surface wearing. Further accordingly, in this alternate implant, part or all of a compressive load applied to the baseplates will be borne by the spring member 15100, which will dampen the load and/or absorb the load and preferably help return the baseplates to their original uncompressed relative positions.

[0152] Accordingly, when a device is assembled, the baseplates 1400,1500 (or 1400,15000a) are rotatable relative to one another because the ball 1600 rotates freely within the socket 1707, and angulatable relative to one another because the ball 1600 angulates freely within the socket 1707. Because the ball 1600 is held within the socket 1707 by the securing of the tail end of the central post 1412 of the first baseplate 1400 to the ball 1600 and the securing of the convex structure 1700 to the second baseplate 1500 (or second baseplate first part 15000a), the artificial disc can withstand tension loading of the baseplates 1400,1500 (or 1400,15000a). More particularly, when a tension load is applied to the baseplates 1400,1500 (or 1400,15000a) the ball 1600 seeks to pass through the bore 1702 in the convex structure 1700. However, the curvate taper 1708 of the bore 1702 prevents the ball 1600 from exiting the socket 1707. Therefore, the assembly does not come apart under normally experienced tension loads. This ensures that no individual parts of the assembly will pop out or slip out from between the vertebral bodies when, e.g., the patient stretches or hangs while exercising or performing other activities. Thus, in combination with the securing of the baseplates 1400,1500 (or 1400,15000a) to the adjacent vertebral bones via the domes 1403,1503 (or 1403,15030) and spikes 1405,1505 (or 1405,15050), the disc assembly has an integrity similar to the tension-bearing integrity of a healthy natural intervertebral disc. Also, because the ball 1600 is laterally captured in the socket 1707, lateral translation of the baseplates 1400,1500 (or 1400,15000a) relative to one another is prevented during rotation and angulation, similar to the performance of healthy natural intervertebral disc. Because the baseplates 1400,1500 (or 1400,15000a) are made angulatable relative to one another by the ball 1600 being rotatably and angulatably coupled in the socket 1707, the disc assembly provides a centroid of motion within the sphere defined by the ball 1600. Accordingly, the centroid of motion of the disc assembly remains centrally located between the vertebral bodies, similar to the centroid of motion in a healthy natural intervertebral disc.

[0153] The remaining implants limit the rotation (but preferably not the angulation) of the ball in the socket formed by the curvate taper of the convex structure and the hemispherical contour of the curvate pocket of the second baseplate. Each implant accomplishes this in a different manner, but each one utilizes interference be-

tween a protrusion and a recess to limit the rotation, similar to the manner in which such interference is utilized above. In some implants, the protrusion is preferably hemispherical, and the recess preferably has a semicylindrical contour within which the protrusion fits. In other implants, the protrusion is preferably hemispherical, and the recess preferably has a curvate contour that is not semicylindrical. (It should be understood that the described formations of the recess and the protrusion are merely preferred, and that alternate formations, curvate or otherwise, for each are possible; a particular shape or location of recess or a particular shape or location of protrusion is not required; any shape can be used so long as the recess and protrusion interact as desired. For example, the recess has a curvate contour that is not semicylindrical, and other recess has a different curvate contour that is not semicylindrical, each being formed so that it optimally interacts with the protrusion in its respective implant.) The boundaries of the recess define the limits of rotation of the ball within the socket, by allowing movement of the protrusion relative to the recess as the ball rotates through a certain range in the socket, but providing interference with the protrusion to prevent rotation of the ball beyond that range in the socket. Preferably, for example, the recess has a depth equivalent to the radius of the hemispherical protrusion, but a radius of curvature greater than that of the protrusion. At the same time, the boundaries of the recess preferably do not limit the angulation of the ball within the socket, at least until the perimeter regions of the inwardly facing surface of the convex structure and the inwardly facing surface of the first baseplate meet. Preferably, for example, the recess has a length greater than the range of movement of the protrusion relative to the recess as the ball angulates in the socket.

[0154] Therefore, when assembled, the discs of the remaining implants enable angulation and limited rotation of the baseplates relative to one another about a centroid of motion that remains centrally located between the baseplates (at the center of the sphere defined by the ball), similar to the centroid of motion in a healthy natural intervertebral disc that is limited in its rotation by surrounding body structures. A benefit of limiting the relative rotation of the baseplates is that relative rotation beyond a certain range in a healthy natural disc is neither needed nor desired, because, for example, excess strain can be placed on the facet joints or ligaments thereby. As described above, the construction also prevents translation and separation of the baseplates relative to one another during rotation and angulation.

[0155] As noted above, each of the remaining implants forms the protrusion and corresponding recess in a different manner, utilizing components that are either identical or similar to the components described above, and some implants utilize additional components. Each of the remaining implants will now be described in greater detail.

[0156] A hemispherical protrusion is formed on the ball,

and interacts in the above-described manner with a recess formed adjacent the socket formed by the curvate taper of the convex structure and the hemispherical contour of the curvate pocket of the second baseplate. More particularly, it uses the same first baseplate 1400 as described above. Referring to Figs. 9a-e, a second type 1800 of second baseplate is shown in top (Fig. 9a), side (Fig. 9b), side cutaway (Fig. 9c), perspective cutaway (Fig. 9d) and perspective (Fig. 9e) views. This second type 1800 of second baseplate is identical to the first type 1500 of second baseplate described above (and thus similar features are reference numbered similar to those of the first type 1500 of second baseplate, but in the 1800s rather than the 1500s), except that this second type 1800 of second baseplate has a curvate recess 1818 adjacent the curvate pocket 1812, and preferably in the circumferential wall 1814.

[0157] Referring now to Figs. 9f-j, a second type 1900 of ball is shown in top (Fig. 9f), side (Fig. 9g), side cutaway (Fig. 9h), perspective cutaway (Fig. 9i) and perspective (Fig. 9j) views. The ball 1900 is identical to the first type 1600 of ball described above (and thus similar features are reference numbered similar to those of the first type 1600 of ball, but in the 1900s rather than the 1600s), except that the semispherical contour of this second type 1900 of ball is also interrupted by a hemispherical protrusion 1904.

[0158] Referring now to Figs. 9k-o, a second type 2000 of convex structure is shown in top (Fig. 9k), side (Fig. 9l), side cutaway (Fig. 9m), perspective cutaway (Fig. 9n) and perspective (Fig. 9o) views. This second type 2000 of convex structure is identical to the first type 1700 of convex structure described above (and thus similar features are reference numbered similar to those of the first type 1700 of convex structure, but in the 2000s rather than the 1700s), except that this second type 2000 of convex structure has a curvate recess 2016 adjacent the curvate taper 2008.

[0159] Referring now to Figs. 9p-t, an assembled implant is shown in top (Fig. 9p), side (Fig. 9q), side cutaway (Fig. 9r), perspective cutaway (Fig. 9s) and perspective (Fig. 9t) views. It can be seen that the curvate recesses 1818,2016 together form the recess described above in the discussion of the manner in which these remaining implants limit rotation of the ball in the socket formed by the curvate taper of the convex structure and the hemispherical contour of the curvate pocket of the second baseplate, and that the protrusion 1904 serves as the protrusion described above in the same discussion. Thus, the protrusion 1904 and recesses 1818,2016 interact in the above described manner to limit the rotation of the ball 1900 in the socket 2007. Assembly of the disc is identical to that above, except that the protrusion 1904 is longitudinally aligned with the recess 1818, and the recess 2016 is similarly aligned, so that when the convex structure 2000 is secured to the second baseplate 1800, the protrusion 1904 is fitted within the recesses 1818,2016 for interaction as described above as the ball

1900 rotates and angulates in the socket 2007.

[0160] Referring now to Fig. 9u, an assembled alternate implant is shown in side cutaway view. This implant incorporates a multi-part second baseplate (with first part 18000a and second part 18000b) housing a spring member 18100 that provides axial compressibility, such that a compressive load applied to the baseplates is borne by the spring member 18100. Elements of this alternate implant that are also elements found above are like numbered. (The second baseplate features are numbered in the 18000's rather than the 1800's.) The curvate recesses 18180,2016 together form the recess described above, and the protrusion 1904 serves as the protrusion described above, and thus the protrusion 1904 and recesses 18180,2016 interact in the above described manner to limit the rotation of the ball 1900 in the socket 2007.

[0161] Assembly is identical to that described above, except that the protrusion 1904 is longitudinally aligned with the recess 18180, and the recess 2016 is similarly aligned, so that when the convex structure 2000 is secured to the second baseplate first part 18000a, the protrusion 1904 is fitted within the recesses 18180,2016 for interaction as described above as the ball 1900 rotates and angulates in the socket 2007. It should be understood that the second baseplate second part 18000b preferably fits loosely within the convex structure 2000 and the second baseplate first part 18000a, so that when the first baseplate 1400 is compressed toward the second baseplate first part 18000a, the second baseplate second part 18000b may travel toward the second baseplate first part 18000a as the spring member 18100 compresses. While not limited to any particular structure, assembly, or material, a spring member providing shock absorption preferably includes an elastomeric material, such as, for example, polyurethane or silicon, and a spring member providing shock dampening preferably includes a plastic material, such as, for example, polyethylene. It should be understood that metal springs may alternatively or additionally be used. The illustrated spring member 18100 is formed of an elastomeric material, for example. The illustrated spring member 18100 is ring-shaped, for example, such that it fits just inside the circumferential edge of the outwardly facing surface 18020b of the second baseplate second part 18000b as shown. The second baseplate second part 18000b should be dimensioned such that, and the spring member 18100 should have an uncompressed height such that, a gap is present between the outwardly facing surface 18020b of the second baseplate second part 18000b and the inwardly facing surface 18090a of the second baseplate first part 18000a when the disc is assembled. The gap preferably has a height equivalent to the anticipated distance that the spring member 18100 will compress under an anticipated load. Accordingly, part or all of a compressive load applied to the baseplates will be borne by the spring member 18100, which will dampen the load and/or absorb the load and preferably help return the baseplates to their original uncompressed relative positions.

[0162] In the present invention, a hemispherical protrusion is formed to protrude into the socket formed by the curvate taper of the convex structure and the hemispherical contour of the curvate pocket of the second baseplate, and interacts in the above-described manner with a semicylindrical recess formed on the ball. More particularly, the invention uses the same first baseplate 1400 as described above. Referring to Figs. 10a-e, a third type 2100 of second baseplate is shown in top (Fig. 10a), side (Fig. 10b), side cutaway (Fig. 10c), perspective cutaway (Fig. 10d) and perspective (Fig. 10e) views. This third type 2100 of second baseplate is identical to the first type 1500 of second baseplate described above (and thus similar features are reference numbered similar to those of the first type 1500 of second baseplate, but in the 2100s rather than the 1500s), except that this third type 2100 of second baseplate has a recess 2118 adjacent the curvate pocket 2112, and preferably in the circumferential wall 2114 as shown.

[0163] Referring now to Figs. 10f-j, a third type 2200 of ball is shown in top (Fig. 10f), side (Fig. 10g), side cutaway (Fig. 10h), perspective cutaway (Fig. 10i) and perspective (Fig. 10j) views. The ball 2200 is identical to the first type 1600 of ball described above (and thus similar features are reference numbered similar to those of the first type 1600 of ball, but in the 2200s rather than the 1600s), except that the semispherical contour of this third type 2200 of ball is also interrupted by a curvate recess 2204.

[0164] Referring now to Figs. 10k-o, a third type 2300 of convex structure is shown in top (Fig. 10k), side (Fig. 10l), side cutaway (Fig. 10m), perspective cutaway (Fig. 10n) and perspective (Fig. 10o) views. This third type 2300 of convex structure is identical to the first type 1700 of convex structure described above (and thus similar features are reference numbered similar to those of the first type 1700 of convex structure, but in the 2300s rather than the 1700s), except that this third type 2300 of convex structure has a protrusion 2316 adjacent the curvate taper 2008.

[0165] Referring now to Figs. 10p-t, an assembled implant according to the invention is shown in top (Fig. 10p), side (Fig. 10q), side cutaway (Fig. 10r), perspective cutaway (Fig. 10s) and perspective (Fig. 10t) views. It can be seen that the curvate recess 2204 of the ball 2200 forms the recess described above in the discussion of the manner in which these remaining embodiments limit rotation of the ball in the socket formed by the curvate taper of the convex structure and the hemispherical contour of the curvate pocket of the second baseplate, and that the protrusion 2316 fits into the recess 2118 to serve as the protrusion described above in the same discussion. Thus, the protrusion 2316 and the recess 2204 interact in the above described manner to limit the rotation of the ball 2200 in the socket 2307. Assembly of the disc is identical to that above, except that the protrusion 2316 is longitudinally aligned with the recess 2204 and the recess 2118 during assembly so that the protrusion 2316

fits into the recess 2118 to extend into the recess 2204 for interaction as described above as the ball 2200 rotates and angulates in the socket 2307.

[0166] Referring now to Fig. 10u, an assembled alternate implant according to the invention is shown in side cutaway view. This alternate embodiment incorporates a multi-part second baseplate (with first part 21000a and second part 21000b) housing a spring member 21100 that provides axial compressibility, such that a compressive load applied to the baseplates is borne by the spring member 21100. Elements of this alternate embodiment that are also elements found

above are like numbered. (The second baseplate features are numbered in the 21000's rather than the 2100's.) The curvate recess 2204 of the ball 2200 forms the recess described above, and the protrusion 2316 fits into the recess 2118 to serve as the protrusion described above, and thus, the protrusion 2316 and the recess 2204 interact in the above described manner to limit the rotation of the ball 2200 in the socket 2307.

[0167] Assembly is identical to that described above, except that the protrusion 2316 is longitudinally aligned with the recess 2204 and the recess 2118 during assembly so that the protrusion 2316 fits into the recess 2118 to extend into the recess 2204 for interaction as described above as the ball 2200 rotates and angulates in the socket 2307. It should be understood that the second baseplate second part 21000b preferably fits loosely within the convex structure 2300 and the second baseplate first part 21000a, so that when the first baseplate 1400 is compressed toward the second baseplate first part 21000a, the second baseplate second part 21000b may travel toward the second baseplate first part 21000a as the spring member 21100 compresses. While not limited to any particular structure, assembly, or material, a spring member providing shock absorption preferably includes an elastomeric material, such as, for example, polyurethane or silicon, and a spring member providing shock dampening preferably includes a plastic material, such as, for example, polyethylene. It should be understood that metal springs may alternatively or additionally be used. The illustrated spring member 21100 is formed of an elastomeric material, for example. The illustrated spring member 21100 is ring-shaped, for example, such that it fits just inside the circumferential edge of the outwardly facing surface 21020b of the second baseplate second part 21000b as shown. The second baseplate second part 21000b should be dimensioned such that, and the spring member 21100 should have an uncompressed height such that, a gap is present between the outwardly facing surface 21020b of the second baseplate second part 21000b and the inwardly facing surface 21090a of the second baseplate first part 21000a when the disc is assembled. The gap preferably has a height equivalent to the anticipated distance that the spring member 21100 will compress under an anticipated load. Accordingly, in this alternate preferred embodiment, part or all of a compressive load applied to the baseplates will

be borne by the spring member 21100, which will dampen the load and/or absorb the load and preferably help return the baseplates to their original uncompressed relative positions.

[0168] A pin is secured in a pin hole so that the hemispherical head of the pin protrudes into the socket formed by the curvate taper of the convex structure and the hemispherical contour of the curvate pocket of the second baseplate, and interacts in the above-described manner with a semicylindrical recess formed on the ball. More particularly, this implant uses the same first baseplate 1400, and the same ball 2200 and second baseplate 2100. Referring to Figs. 11a-e, a fourth type 2400 of convex structure is shown in top (Fig. 11 a), side (Fig. 11 b), side cutaway (Fig. 11 c), perspective cutaway (Fig. 11 d) and perspective (Fig. 11e) views. This fourth type 2400 of convex structure is identical to the first type 1700 of convex structure described above (and thus similar features are reference numbered similar to those of the first type 1700 of convex structure, but in the 2400s rather than the 1700s), except that this fourth type 2400 of convex structure has a lateral through hole (e.g., a pin hole 2416) and a protrusion (e.g., a pin 2418) secured in the pin hole 2416 (as shown in Figs. 11f-j) and jutting into the socket 2407.

[0169] Referring now to Figs. 11f-j, an assembled implant is shown in top (Fig. 11f), side (Fig. 11g), side cutaway (Fig. 11h), perspective cutaway (Fig. 11i) and perspective (Fig. 11j) views. It can be seen that the curvate recess 2204 of the ball 2200 forms the recess described above in the discussion of the manner in which these remaining implants limit rotation of the ball in the socket formed by the curvate taper of the convex structure and the hemispherical contour of the curvate pocket of the second baseplate, and that the head of the pin 2418 serves as the protrusion described above in the same discussion. Thus, the head of the pin 2418 and the recess 2204 interact in the above described manner to limit the rotation of the ball 2200 in the socket 2407. Assembly of the disc is identical to that above, except that the head

of the pin 2418 is longitudinally aligned with the recess 2204 and the recess 2118 during assembly so that the head of the pin 2418 fits into the recess 2118 to extend into the recess 2204 for interaction as described above as the ball 2200 rotates and angulates in the socket 2407.

[0170] Referring now to Fig. 11k, an assembled alternate implant is shown in side cutaway view. This alternate implant incorporates a multi-part second baseplate (with first part 21000a and second part 21000b) housing a spring member 21100 that provides axial compressibility, such that a compressive load applied to the baseplates is borne by the spring member 21100. Elements of this alternate implant that are also elements found above are like numbered. (The second baseplate features are numbered in the 21000's rather than the 2100's.) The curvate recess 2204 of the ball 2200 forms the recess described above, and the head of the pin 2418 serves as the protrusion described above, and thus, the head of the pin

2418 and the recess 2204 interact in the above described manner to limit the rotation of the ball 2200 in the socket 2407.

[0171] Assembly is identical to that above, except that the head of the pin 2418 is longitudinally aligned with the recess 2204 and the recess 21180 during assembly so that the head of the pin 2418 fits into the recess 21180 to extend into the recess 2204 for interaction as described above as the ball 2200 rotates and angulates in the socket 2407. It should be understood that the second baseplate second part 21000b preferably fits loosely within the convex structure 2400 and the second baseplate first part 21000a, so that when the first baseplate 1400 is compressed toward the second baseplate first part 21000a, the second baseplate second part 21000b may travel toward the second baseplate first part 21000a as the spring member 21100 compresses. While not limited to any particular structure, assembly, or material, a spring member providing shock absorption preferably includes an elastomeric material, such as, for example, polyurethane or silicon, and a spring member providing shock dampening preferably includes a plastic material, such as, for example, polyethylene. It should be understood that metal springs may alternatively or additionally be used. The illustrated spring member 21100 is formed of an elastomeric material, for example. The illustrated spring member 21100 is ring-shaped, for example, such that it fits just inside the circumferential edge of the outwardly facing surface 21020b of the second baseplate second part 21000b as shown. The second baseplate second part 21000b should be dimensioned such that, and the spring member 21100 should have an uncompressed height such that, a gap is present between the outwardly facing surface 21020b of the second baseplate second part 21000b and the inwardly facing surface 21090a of the second baseplate first part 21000a when the disc is assembled. The gap preferably has a height equivalent to the anticipated distance that the spring member 21100 will compress under an anticipated load. Accordingly, in this alternate implant, part or all of a compressive load applied to the baseplates will be borne by the spring member 21100, which will dampen the load and/or absorb the load and preferably help return the baseplates to their original uncompressed relative positions.

[0172] A ball bearing protrudes into the socket formed by the curvate taper of the convex structure and the hemispherical contour of the curvate pocket of the second baseplate, and interacts in the above-described manner with a recess formed on the ball. More particularly, it uses the same first baseplate 1400 and the same second baseplate 2100. Referring to Figs. 12a-e, a fifth type 2500 of convex structure of the fourth embodiment family is shown in top (Fig. 12a), side (Fig. 12b), side cutaway (Fig. 12c), perspective cutaway (Fig. 12d) and perspective (Fig. 12e) views. This fifth type 2500 of convex structure is identical to the first type 1700 of convex structure described above (and thus similar features are reference

numbered similar to those of the first type 1700 of convex structure, but in the 2500s rather than the 1700s), except that this fifth type 2500 of convex structure has a recess 2516 adjacent the curvate taper 2508.

[0173] Referring to Figs. 12f-j, a fourth type of ball 2700 is shown in top (Fig. 12f), side (Fig. 12g), side cutaway (Fig. 12h), perspective cutaway (Fig. 12i) and perspective (Fig. 12j) views. The ball 2700 is identical to the first type 1600 of ball described above (and thus similar features are reference numbered similar to those of the first type 1600 of ball, but in the 2700s rather than the 1600s), except that the semispherical contour of this third type 2700 of ball is also interrupted by a curvate recess 2704.

[0174] Referring now to Figs. 12k-o, an assembled implant is shown in top (Fig. 12k), side (Fig. 12l), side cutaway (Fig. 12m), perspective cutaway (Fig. 12n) and perspective (Fig. 12o) views. A ball bearing 2600 is captured for free rotation and angulation, with one part of the ball bearing 2600 closely accommodated in the recesses 2118, 2516, and another part of the ball bearing 2600 protruding into the socket to interact with the curvate recess 2704 of the ball 2700. It can be seen that the curvate recess 2704 of the ball 2700 forms the recess described above in the discussion of the manner in which these remaining embodiments limit rotation of the ball in the socket, and that the ball bearing 2600 serves as the protrusion described above in the same discussion. Thus, the ball bearing 2600 and the recess 2704 interact in the above described manner to limit the rotation of the ball 2700 in the socket 2507. Assembly of the disc is identical to that above, except that the recess 2704 is aligned with the curvate recess 2118 during assembly so that the ball bearing 2600 can be and is then placed into the recesses 2118, 2704 (and then captured in the recess 2118 by the recess 2516 of the convex structure 2500) for interaction as described above as the ball 2700 rotates and angulates in the socket 2507.

[0175] Referring now to Fig. 12p, an assembled alternate implant is shown in side cutaway view. This alternate implant incorporates a multi-part second baseplate (with first part 21000a and second part 21000b) housing a spring member 21100 that provides axial compressibility, such that a compressive load applied to the baseplates is borne by the spring member 21100. Elements of this implant that are also elements found above are like numbered. (The second baseplate features are numbered in the 21000's rather than the 2100's.) The curvate recess 2704 of the ball 2700 forms the recess described above, and the ball bearing 2600 serves as the protrusion described above, and thus, the ball bearing 2600 and the recess 2704 interact in the above described manner to limit the rotation of the ball 2700 in the socket 2507.

[0176] Assembly is identical to that above, except that the recess 2704 is aligned with the curvate recess 2118 during assembly so that the ball bearing 2600 can be and is then placed into the recesses 2118, 2704 (and then captured in the recess 2118 by the recess 2516 of the convex structure 2500) for interaction as described

above as the ball 2700 rotates and angulates in the socket 2507. It should be understood that the second baseplate second part 21000b preferably fits loosely within the convex structure 2500 and the second baseplate first part 21000a, so that when the first baseplate 1400 is compressed toward the second baseplate first part 21000a, the second baseplate second part 21000b may travel toward the second baseplate first part 21000a as the spring member 21100 compresses. While not limited to any particular structure, assembly, or material, a spring member providing shock absorption preferably includes an elastomeric material, such as, for example, polyurethane or silicon, and a spring member providing shock dampening preferably includes a plastic material, such as, for example, polyethylene. It should be understood that metal springs may alternatively or additionally be used. The illustrated spring member 21100 is formed of an elastomeric material, for example. The illustrated spring member 21100 is ring-shaped, for example, such that it fits just inside the circumferential edge of the outwardly facing surface 21020b of the second baseplate second part 21000b as shown. The second baseplate second part 21000b should be dimensioned such that, and the spring member 21100 should have an uncompressed height such that, a gap is present between the outwardly facing surface 21020b of the second baseplate second part 21000b and the inwardly facing surface 21090a of the second baseplate first part 21000a when the disc is assembled. The gap preferably has a height equivalent to the anticipated distance that the spring member 21100 will compress under an anticipated load. Accordingly, part or all of a compressive load applied to the baseplates will be borne by the spring member 21100, which will dampen the load and/or absorb the load and preferably help return the baseplates to their original uncompressed relative positions.

[0177] While there has been described and illustrated specific embodiments of an artificial disc, it will be apparent to those skilled in the art that variations and modifications are possible without deviating from the scope of the invention. The invention, therefore, shall not be limited to the specific embodiments discussed herein.

Claims

1. An intervertebral implant comprising:

- a first baseplate (1400) having an outer vertebral body contact surface (1402) and an inner surface (1408);
- an articulation member (2200) mounted on the first baseplate, the articulation member having a spherical outer surface with a recess (2204) therein, the recess having a stop surface;
- a housing mounted (2300) on the articulation member (2200), the housing having an articulation surface (2308) for contact with the spherical

- outer surface of the articulation member, the articulation surface (2308) of the housing having a protrusion (2316) extending therefrom into the recess in the articulation member (2200); a second baseplate (2100) mounted on the housing, the second baseplate having an outer vertebral body contact surface (2102) and an inner surface having a spherical portion (2112) for contact with the spherical outer surface of the articulation member (2200); and wherein when the spherical outer surface of the articulation member (2200) is in contact with both the articulation surface (2308) of the housing (2300) and the spherical portion (2112) of the inner surface of the second baseplate (2100), articulation of the first and second baseplates with respect to one another is limited when the protrusion (2316) of the articulation surface (2308) of the housing (2300) contacts the stop surface of the recess (2204) of the articulation member.
2. The intervertebral implant of claim 1, wherein the inner surface of the first baseplate includes a circumferential concave recess.
 3. The intervertebral implant of claim 1, wherein the inner surface of the first baseplate has a central post (1412) extending outwardly therefrom, the central post surrounded by the circumferential concave recess of the inner surface of the first baseplate.
 4. The intervertebral implant of claim 3, wherein the central post includes a longitudinal axis and a head end.
 5. The intervertebral implant of claim 4, wherein the articulation member includes a flat surface having a bore (2202) therein, the bore adapted to house the central post of the first baseplate.
 6. The intervertebral implant of claim 1, wherein the articulation surface of the housing is a circumferential concave surface configured to matingly engage the spherical outer surface of the articulation member.
 7. The intervertebral implant of claim 2, wherein the housing includes a top surface having a circumferential convex portion (2306) configured to at least partially enter the circumferential concave recess of the first baseplate as the first and second baseplate articulate with respect to one another.
 8. The intervertebral implant of claim 7, wherein the articulation of the first and second baseplates with respect to one another is limited when the circumferential concave recess of the first baseplate con-
- tacts the circumferential convex portion of the second baseplate.
9. The intervertebral implant of claim 1, wherein at least one of the outer vertebral body contact surfaces of the first and second baseplates is osteoinductive.
 10. The intervertebral implant of claim 5, wherein the head end of the post is compression lockable into the bore of the articulation member.
 11. The intervertebral implant of claim 1, wherein at least one of the outer vertebral body contact surfaces of the first and second baseplates is dome shaped (1403, 2103).
 12. The intervertebral implant of claim 1, wherein the spherical portion of the inner surface of the second baseplate is surrounded by a circumferential wall (2114) and a circumferential recess (2116) on the inner surface of the second baseplate.
 13. The intervertebral implant of claim 1, wherein the housing further includes a bottom surface having a circumferential recess (2310) and a circumferential wall (2312).
 14. The intervertebral implant of claim 13, wherein the bottom surface of the housing is secured to the inner surface of the second baseplate by engaging the circumferential wall (2312) of the bottom surface of the housing with the circumferential recess (2116) of the inner surface of the second baseplate and engaging the circumferential recess (2310) of the bottom surface of the housing with the circumferential wall (2114) of the inner surface of the second baseplate.
 15. The intervertebral implant of claim 13, wherein the stop surface of the recess of the articulation member is concave, and wherein the protrusion of the articulation surface of the housing has a convex stop surface, and articulation of the first and second baseplates with respect to one another is limited when the convex stop surface of the protrusion of the articulation surface of the housing contacts the concave stop surface of the recess of the articulation member.

Patentansprüche

1. Intervertebrales Implantat, aufweisend:
 - eine erste Basisplatte (1400), die eine Vertebraelementberührungsaußenfläche (1402) und eine Innenfläche (1408) hat;
 - ein Gelenkelement (2200), das an der ersten Basisplatte angebracht ist, wobei das Gelen-

- kelement eine kugelförmige Außenfläche mit einer Aussparung (2204) umfasst, wobei die Aussparung eine Anschlagfläche hat;
- ein Gehäuse (2300), das an dem Gelenkelement (2200) angebracht ist, wobei das Gehäuse eine Gelenkfläche (2308) zur Berührung mit der kugelförmigen Außenfläche des Gelenkelements hat, wobei die Gelenkfläche (2308) des Gehäuses einen Vorsprung (2316) hat, der sich von dieser in die Aussparung in dem Gelenkelement (2200) erstreckt;
 - eine zweite Basisplatte (2100), die an dem Gehäuse angebracht ist, wobei die zweite Basisplatte eine Vertebralementberührungsaußenfläche (2102) und eine Innenfläche hat, die einen kugelförmigen Abschnitt (2112) zur Berührung mit der kugelförmigen Außenfläche des Gelenkelements (2200) hat; und
 - wobei im Falle der Berührung der kugelförmigen Außenfläche des Gelenkelements (2200) mit sowohl der Gelenkfläche (2308) des Gehäuses (2300) als auch dem kugelförmigen Abschnitt (2112) der Innenfläche der zweiten Basisplatte (2100) die Beweglichkeit der ersten und zweiten Basisplatte in Bezug zueinander begrenzt ist, wenn der Vorsprung (2316) der Gelenkfläche (2308) des Gehäuses (2300) die Anschlagfläche der Aussparung (2204) des Gelenkelements berührt.
2. Intervertebrales Implantat gemäß Anspruch 1, wobei die Innenfläche der ersten Basisplatte eine konkave, umlaufende Aussparung umfasst.
 3. Intervertebrales Implantat gemäß Anspruch 1, wobei die Innenfläche der ersten Basisplatte eine zentrale Säule (1412) hat, die sich von dieser nach außen erstreckt, wobei die zentrale Säule von der konkaven, umlaufenden Aussparung der Innenfläche der ersten Basisplatte umgeben ist.
 4. Intervertebrales Implantat gemäß Anspruch 3, wobei die zentrale Säule eine Längsachse und ein Kopfende umfasst.
 5. Intervertebrales Implantat gemäß Anspruch 4, wobei das Gelenkelement eine flache Fläche mit einer Bohrung (2202) umfasst, wobei die Bohrung angepasst ist, die zentrale Säule der ersten Basisplatte aufzunehmen.
 6. Intervertebrales Implantat gemäß Anspruch 1, wobei die Gelenkfläche des Gehäuses eine konkave Umfangsfläche ist, die ausgestaltet ist, zusammenpassend mit der kugelförmigen Außenfläche des Gelenkelements im Eingriff zu stehen.
 7. Intervertebrales Implantat gemäß Anspruch 2, wobei das Gehäuse eine obere Fläche umfasst, die einen konvexen Umfangsabschnitt (2306) umfasst, der ausgestaltet ist, zumindest teilweise in die konkave umlaufende Aussparung der ersten Basisplatte einzutreten, wenn sich die erste und zweite Basisplatte gegeneinander bewegen.
 8. Intervertebrales Implantat gemäß Anspruch 7, wobei die Beweglichkeit der ersten und zweiten Basisplatte in Bezug zueinander begrenzt ist, wenn die konkave, umlaufende Aussparung der ersten Basisplatte mit dem konvexen Umfangsabschnitt der zweiten Basisplatte in Berührung steht.
 9. Intervertebrales Implantat gemäß Anspruch 1, wobei zumindest ein Element aus den Vertebralementberührungsaußenflächen der ersten und zweiten Basisplatten osteoinduktiv ist.
 10. Intervertebrales Implantat gemäß Anspruch 5, wobei das Kopfende der Säule mittels Kompression an der Bohrung des Gelenkelements arretierbar ist.
 11. Intervertebrales Implantat gemäß Anspruch 1, wobei zumindest ein Element aus den Vertebralementberührungsaußenflächen (1403, 2103) der ersten und zweiten Basisplatte kuppelförmig ist.
 12. Intervertebrales Implantat gemäß Anspruch 1, wobei der kugelförmige Abschnitt der Innenfläche der zweiten Basisplatte von einer Umfangswand (2114) und einer umlaufenden Aussparung (2116) an der Innenfläche der zweiten Basisplatte umgeben ist.
 13. Intervertebrales Implantat gemäß Anspruch 1, wobei das Gehäuse weiterhin eine Bodenfläche mit einer umlaufenden Aussparung (2310) und eine Umfangswand (2312) umfasst.
 14. Intervertebrales Implantat gemäß Anspruch 13, wobei die Bodenfläche des Gehäuses an der Innenfläche der zweiten Basisplatte durch In-Eingriff-Bringen der Umfangswand (2313) der Bodenfläche des Gehäuses mit der umlaufenden Aussparung (2116) der Innenfläche der zweiten Basisplatte und durch In-Eingriff-Bringen der umlaufenden Aussparung (2310) der Bodenfläche des Gehäuses mit der Umfangswand (2114) der Innenfläche der zweiten Basisplatte befestigt ist.
 15. Intervertebrales Implantat gemäß Anspruch 13, wobei die Anschlagfläche der Aussparung des Gelenkelements konkav ist, wobei der Vorsprung der Gelenkfläche des Gehäuses eine konvexe Anschlagfläche hat, wobei die Beweglichkeit der ersten und zweiten Basisplatte in Bezug zueinander begrenzt ist, wenn die konvexe Anschlagfläche des Vorsprungs der Gelenkfläche des Gehäuses mit der

konkaven Anschlagfläche der Aussparung des Gelenkelements in Berührung steht.

Revendications

1. Implant intervertébral comprenant :

- une première plaque de base (1400) ayant une surface de contact externe de corps vertébral (1402) et une surface interne (1408) ; 10
- un élément d'articulation (2200) monté sur la première plaque de base, l'élément d'articulation ayant une surface externe sphérique dotée d'une cavité (2204) dans celle-ci, la cavité ayant une surface d'arrêt ; 15
- un logement monté (2300) sur l'élément d'articulation (2200), le logement ayant une surface d'articulation (2308) pour un contact avec la surface externe sphérique de l'élément d'articulation, la surface d'articulation (2308) du logement ayant une proéminence (2316) s'étendant à partir de celle-ci dans la cavité dans l'élément d'articulation (2200) ; 20
- une deuxième plaque de base (2100) montée sur le logement, la deuxième plaque de base ayant une surface de contact du corps vertébral (2102) et une surface interne ayant une partie sphérique (2112) pour un contact avec la surface externe sphérique de l'élément d'articulation (2200) ; et 25

dans lequel la surface externe sphérique de l'élément d'articulation (2200) est en contact avec à la fois la surface d'articulation (2308) du logement (2300) et la partie sphérique (2112) de la surface interne de la deuxième plaque de base (2100), l'articulation des première et deuxième plaques de base l'une par rapport à l'autre étant limitée lorsque la proéminence (2316) de la surface d'articulation (2308) du logement (2300) est en contact avec la surface d'arrêt de la cavité (2204) de l'élément d'articulation. 30

2. Implant intervertébral selon la revendication 1, dans lequel la surface interne de la première plaque de base a une cavité concave circonférentielle. 35

3. Implant intervertébral selon la revendication 1, dans lequel la surface interne de la première plaque de base a un montant central (1412) s'étendant vers l'extérieur de celle-ci, le montant central étant entouré par la cavité concave circonférentielle de la surface interne de la première plaque de base. 40

4. Implant intervertébral selon la revendication 3, dans lequel le montant central comprend un axe longitudinal et une tête d'extrémité. 45

5. Implant intervertébral selon la revendication 4, dans lequel l'élément d'articulation comprend une surface plane ayant un alésage (2202) dans celle-ci, l'alésage étant adapté pour recevoir le montant central de la première plaque de base. 5

6. Implant intervertébral selon la revendication 1, dans lequel la surface d'articulation du logement est une surface concave circonférentielle configurée pour être en prise de façon appariée avec la surface externe sphérique de l'élément d'articulation. 10

7. Implant intervertébral selon la revendication 2, dans lequel le logement comprend une surface supérieure ayant une partie convexe circonférentielle (2306) configurée pour entrer au moins partiellement dans la cavité concave circonférentielle de la première plaque de base lorsque les première et deuxième plaques de base s'articulent l'une par rapport à l'autre. 15

8. Implant intervertébral selon la revendication 7, dans lequel l'articulation des première et deuxième plaques de base l'une par rapport à l'autre est limité lorsque la cavité concave circonférentielle de la première plaque de base est en contact avec la partie convexe circonférentielle de la deuxième plaque de base. 20

9. Implant intervertébral selon la revendication 1, dans lequel au moins l'une des surfaces de contact du corps vertébral externe des première et deuxième plaques de base est ostéo-inductrice. 25

10. Implant intervertébral selon la revendication 5, dans lequel la tête d'extrémité du montant peut être bloquée par compression dans l'alésage de l'élément d'articulation. 30

11. Implant intervertébral selon la revendication 1, dans lequel au moins l'une des surfaces de contact du corps vertébral externe des première et deuxième plaques de base est en forme de dôme (1403, 2103). 35

12. Implant intervertébral selon la revendication 1, dans lequel la partie sphérique de la surface interne de la deuxième plaque de base est entourée d'une paroi circonférentielle (2114) et une cavité circonférentielle (2116) sur la surface interne de la deuxième plaque de base. 40

13. Implant intervertébral selon la revendication 1, dans lequel le logement comprend en outre une surface de fond ayant une cavité circonférentielle (2310) et une paroi circonférentielle (2312). 45

14. Implant intervertébral selon la revendication 13, dans lequel la surface de fond du logement est fixée 50

à la surface interne de la deuxième plaque de base en mettant en prise la paroi circonférentielle (2312) de la surface de fond du logement avec la cavité circonférentielle (2116) de la surface interne de la deuxième plaque de base et mettant en prise la cavité circonférentielle (2310) de la surface de fond du logement avec la paroi circonférentielle (2114) de la surface interne de la deuxième plaque de base.

15. Implant intervertébral selon la revendication 13, dans lequel la surface d'arrêt de la cavité de l'élément d'articulation est concave et dans lequel la proéminence de la surface d'articulation du logement a une surface d'arrêt convexe et l'articulation des première et deuxième plaques de base l'une par rapport à l'autre est limitée lorsque la surface d'arrêt convexe de la proéminence de la surface d'articulation du logement est en contact avec la surface d'arrêt concave de l'élément d'articulation.

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FIG. 1A

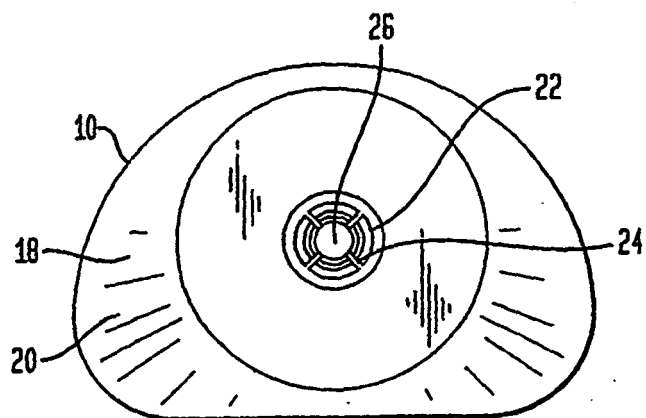


FIG. 1B

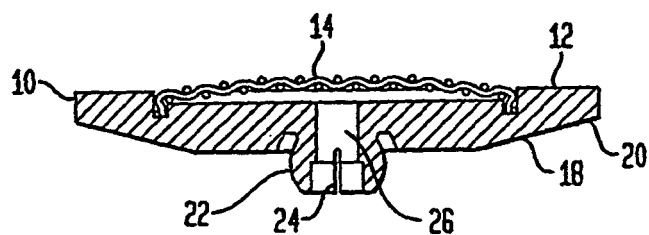


FIG. 1C

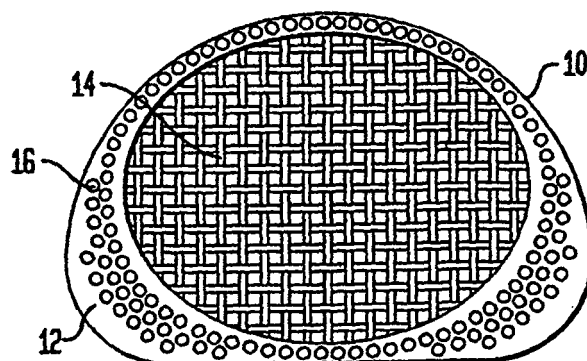


FIG. 1D

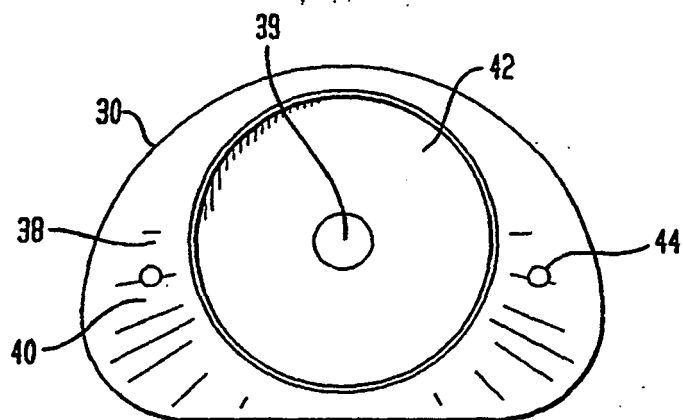


FIG. 1E

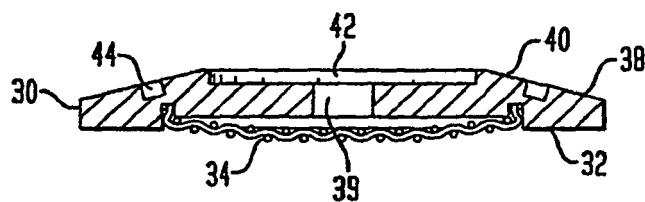


FIG. 1F

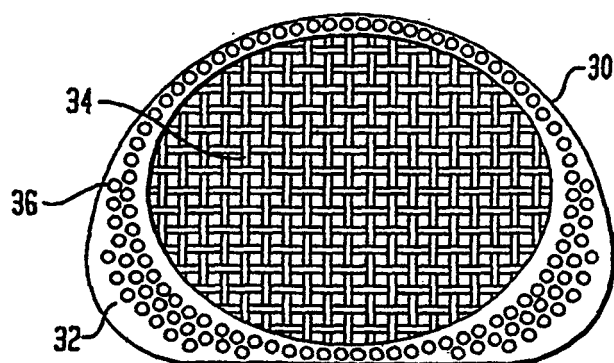


FIG. 1G

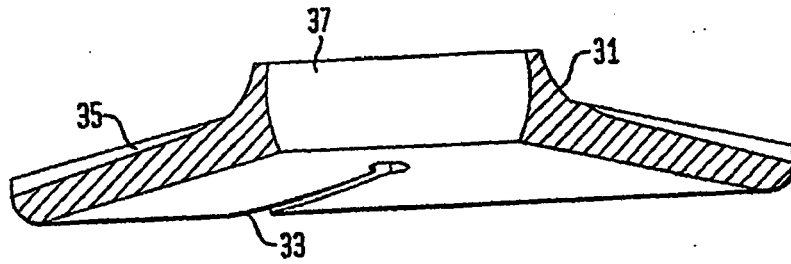


FIG. 1H

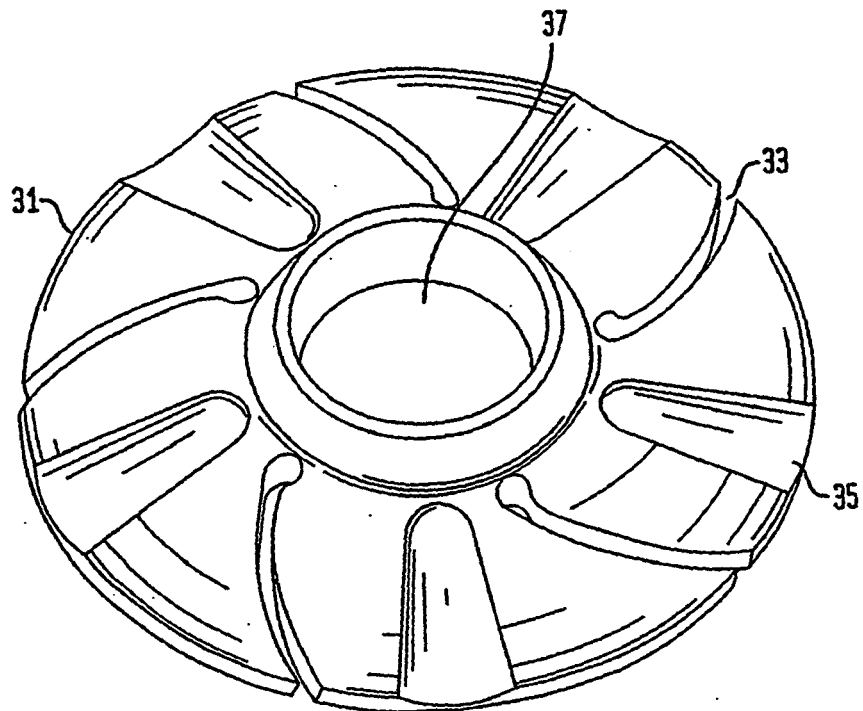


FIG. 1I

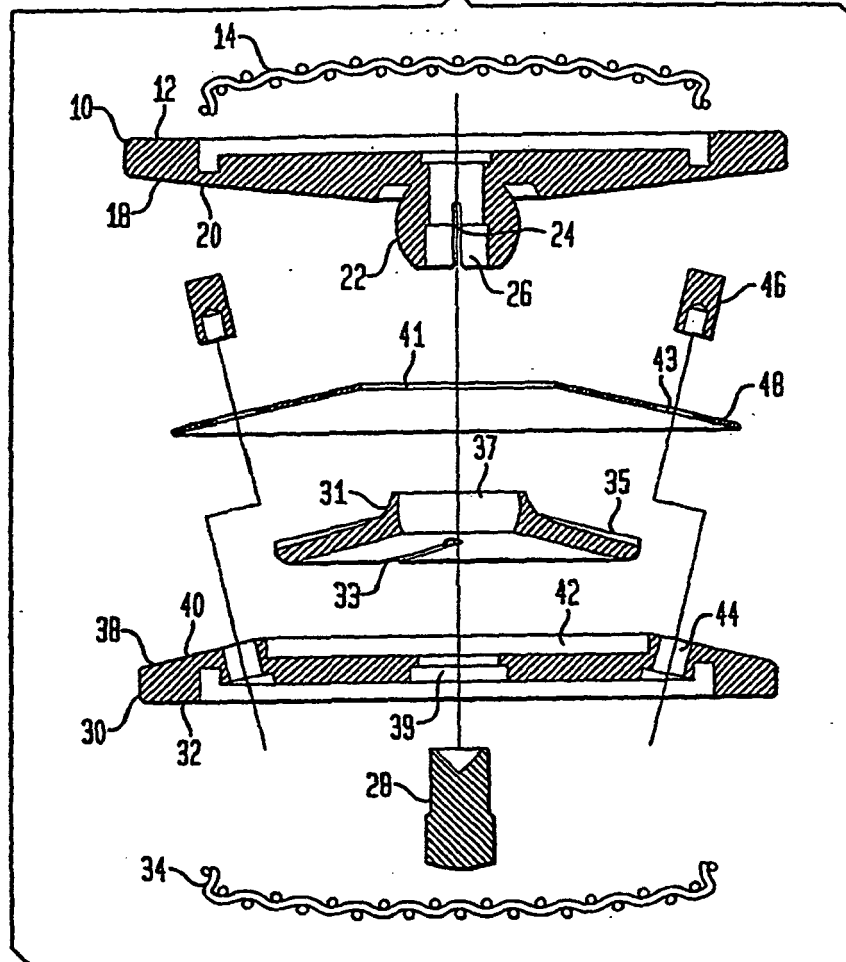


FIG. 1J

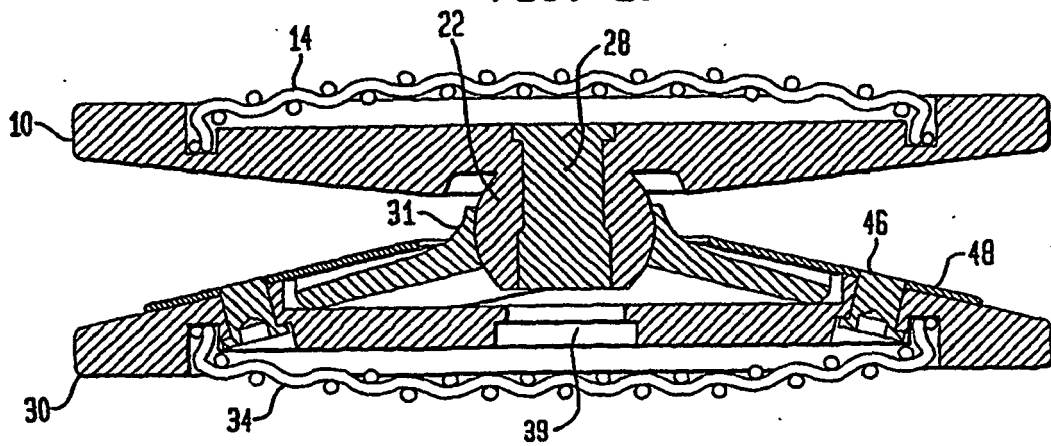


FIG. 2A

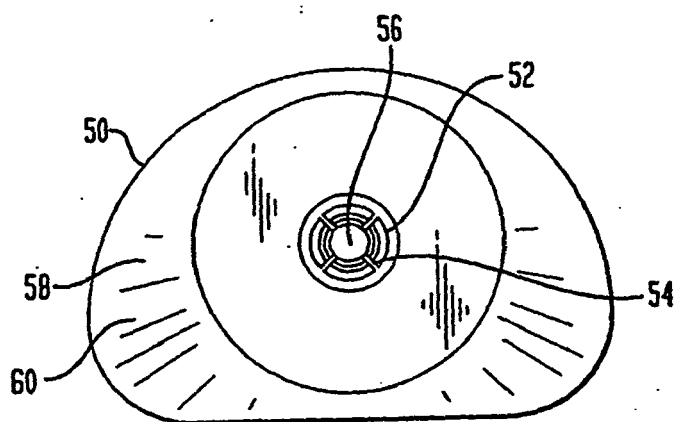


FIG. 2B

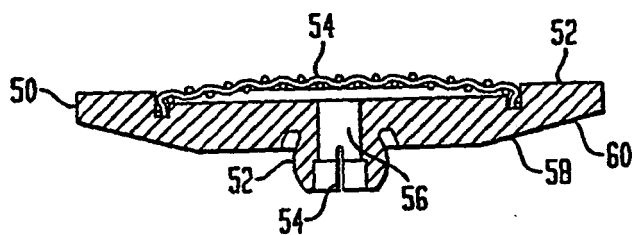


FIG. 2C

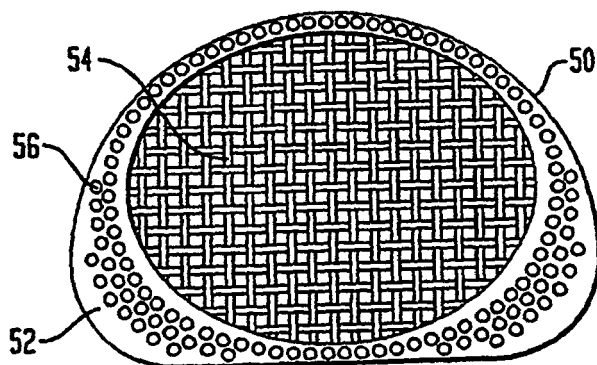


FIG. 2D

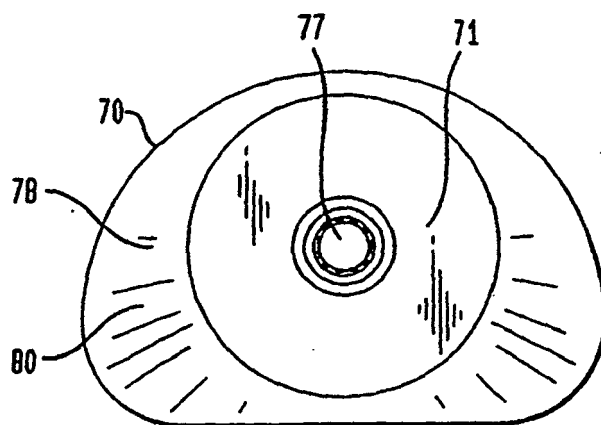


FIG. 2E

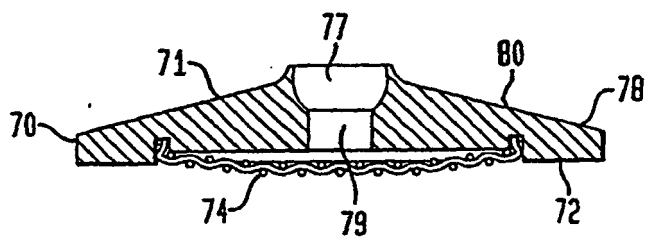


FIG. 2F

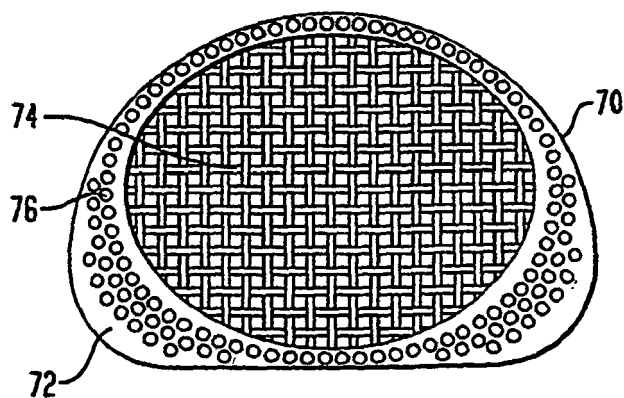


FIG. 2G

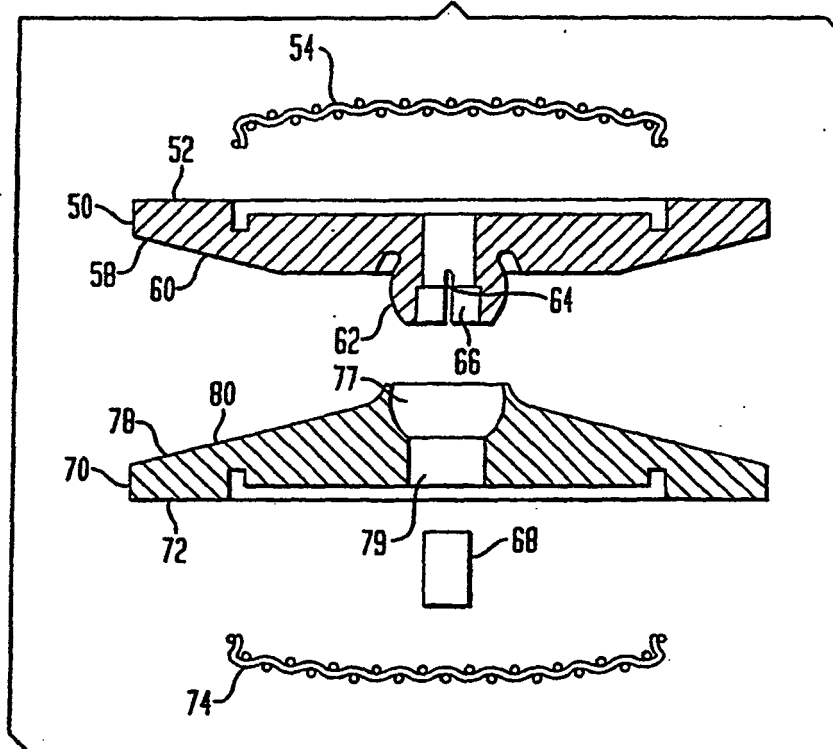


FIG. 2H

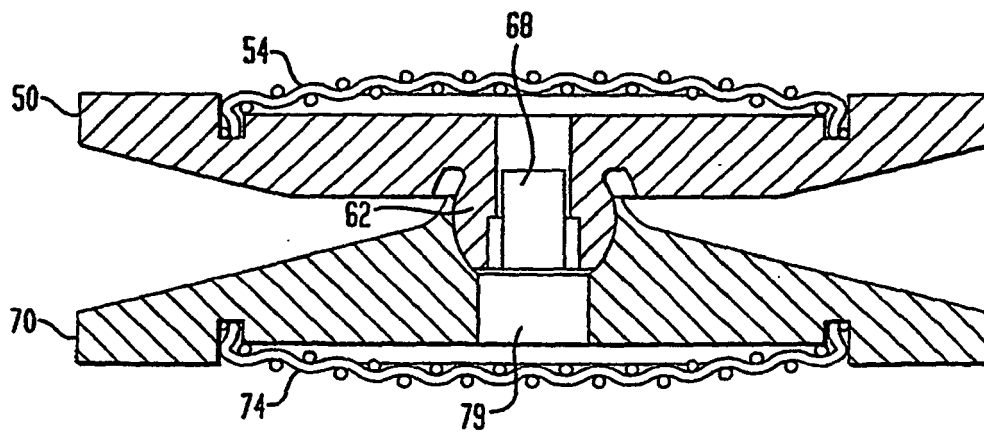


FIG. 3A

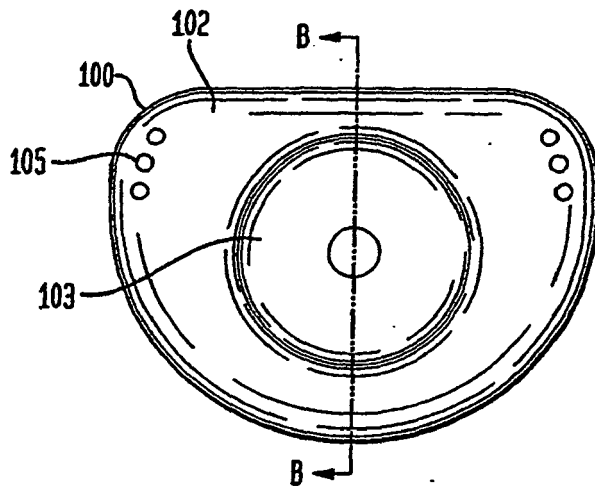


FIG. 3C

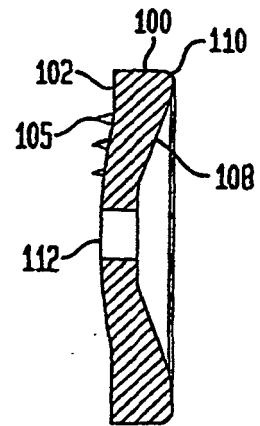


FIG. 3B

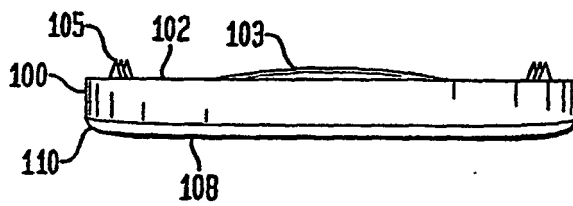


FIG. 3D

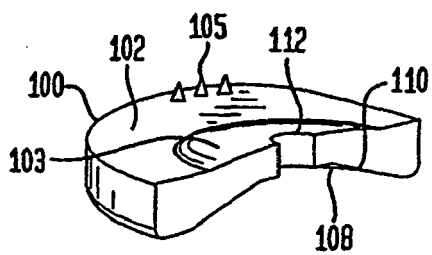


FIG. 3E

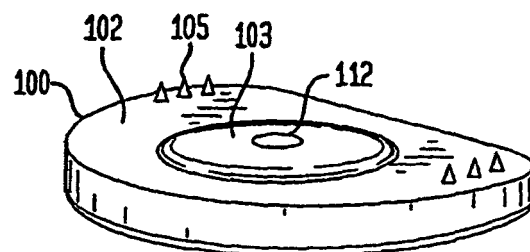


FIG. 3F

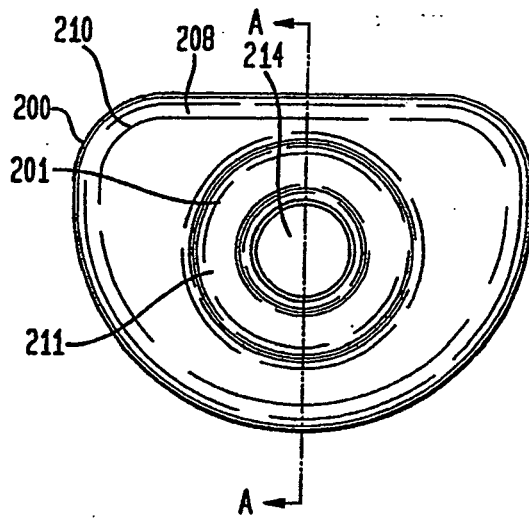


FIG. 3H

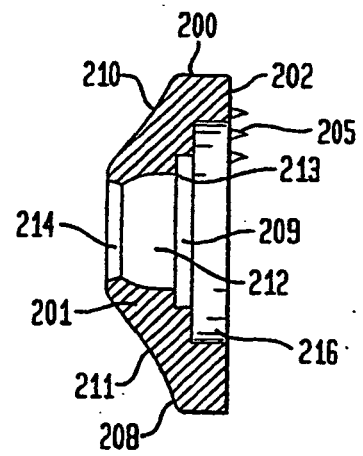


FIG. 3G

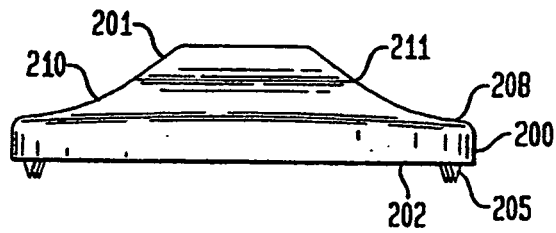


FIG. 3I

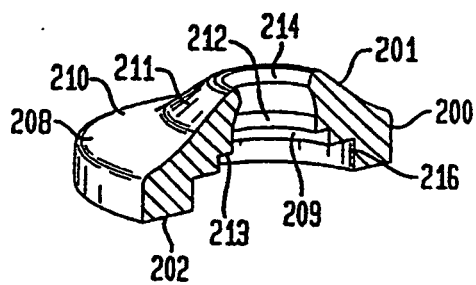


FIG. 3J

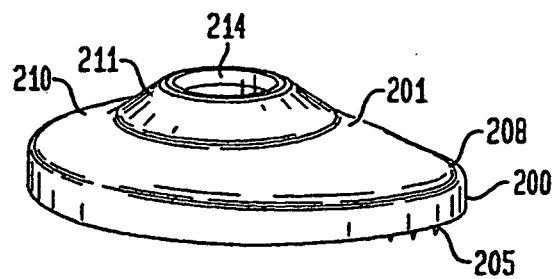


FIG. 3K

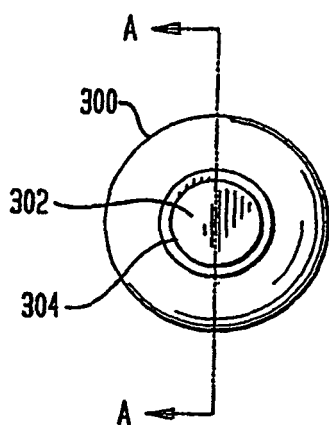


FIG. 3M

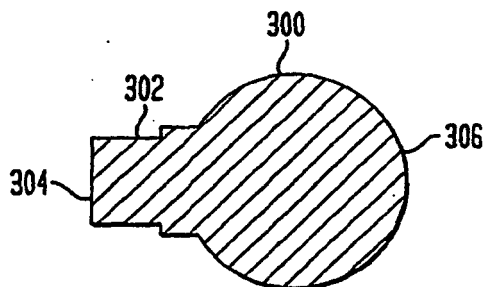


FIG. 3L

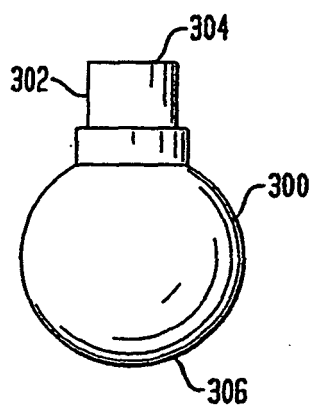


FIG. 3N

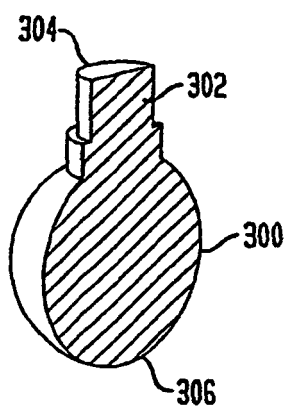


FIG. 3O

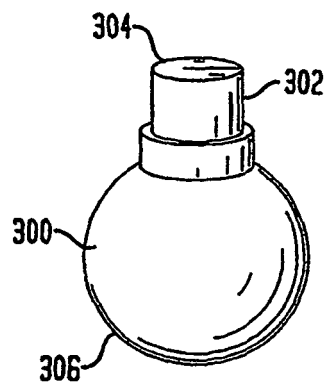


FIG. 3P

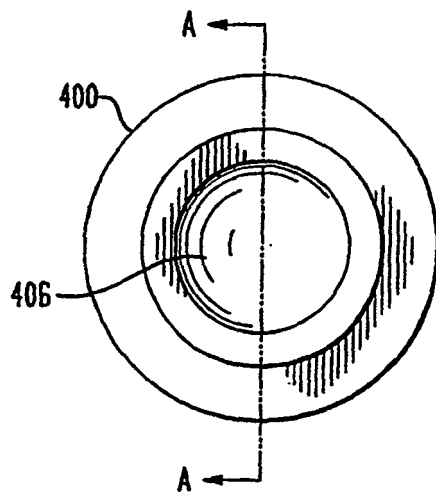


FIG. 3R

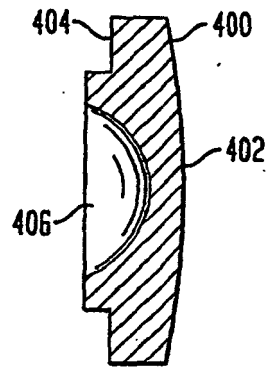


FIG. 3Q

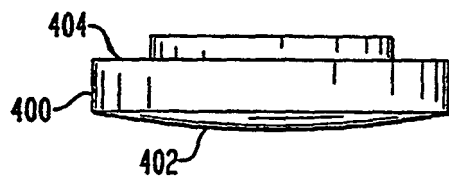


FIG. 3S

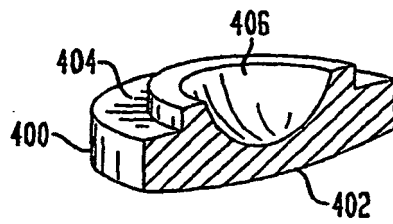


FIG. 3T

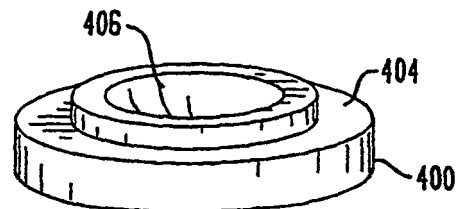


FIG. 3U

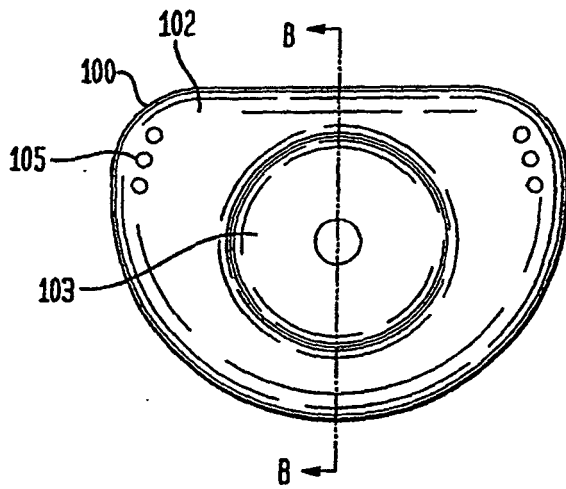


FIG. 3W

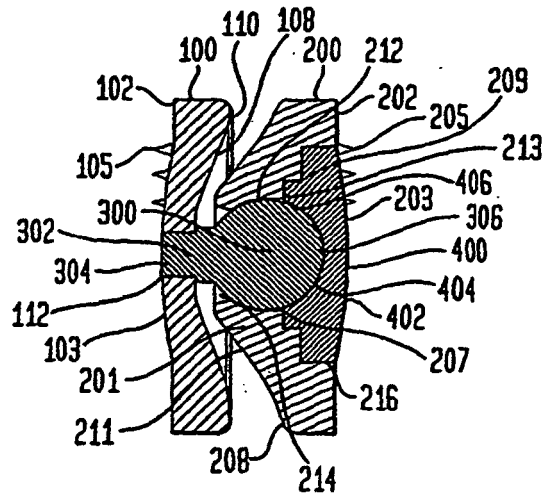


FIG. 3V

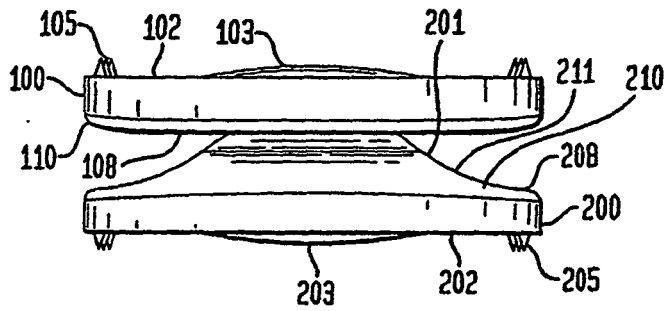


FIG. 3X

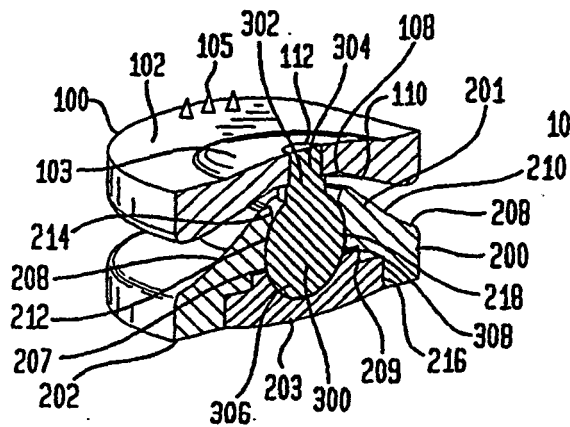


FIG. 3Y

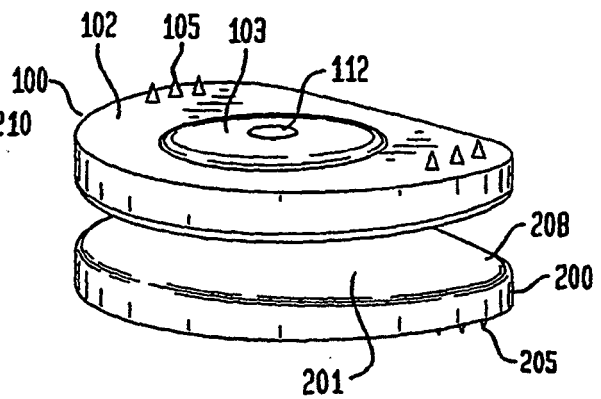


FIG. 4A

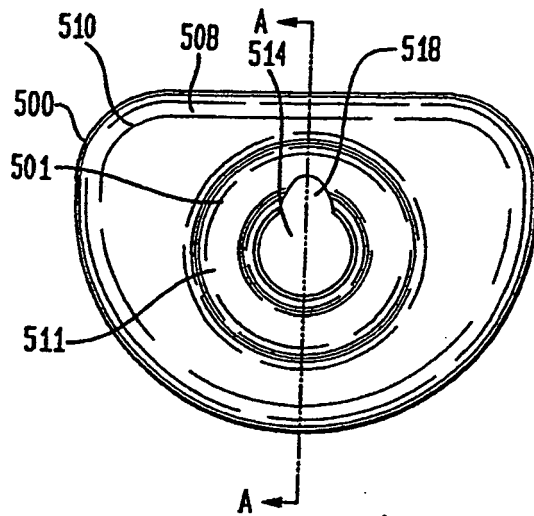


FIG. 4C

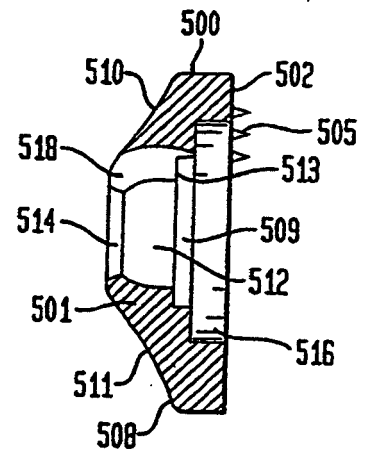


FIG. 4B

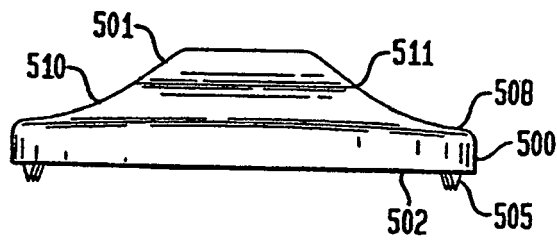


FIG. 4D

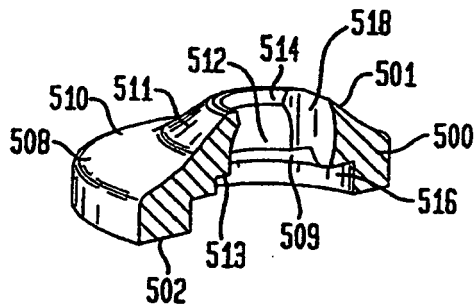


FIG. 4E

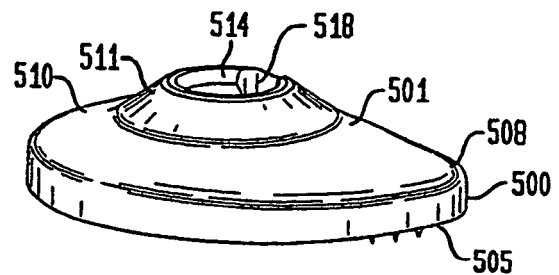


FIG. 4F

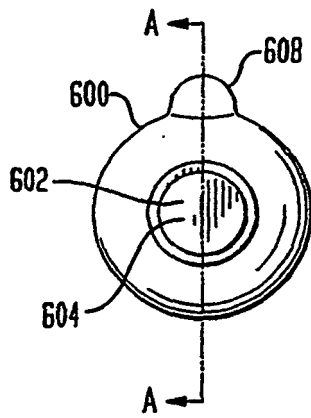


FIG. 4H

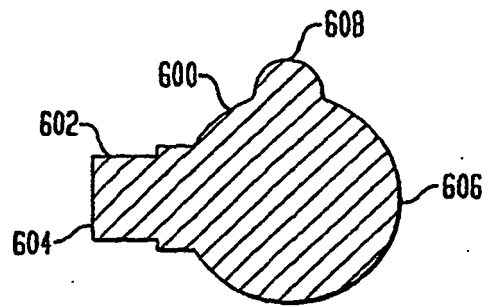


FIG. 4G

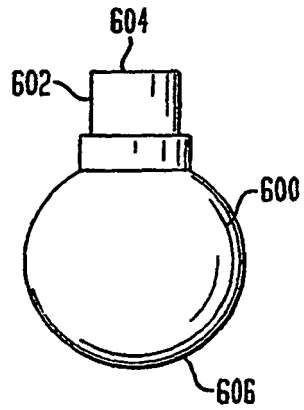


FIG. 4I

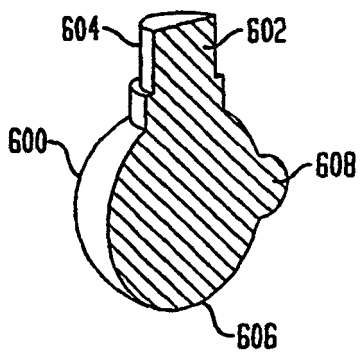


FIG. 4J

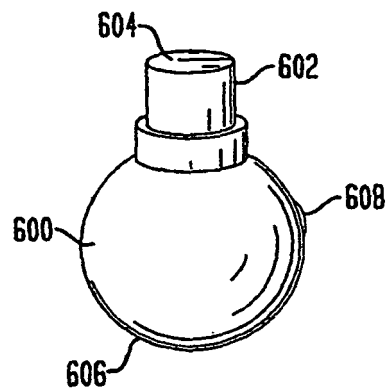


FIG. 4K

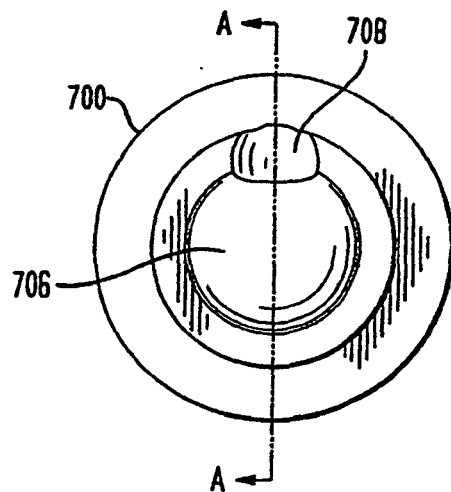


FIG. 4M

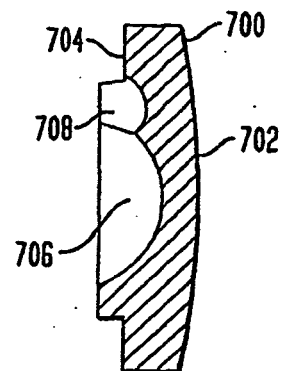


FIG. 4L

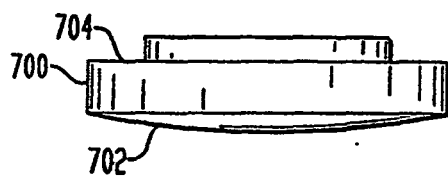


FIG. 4N

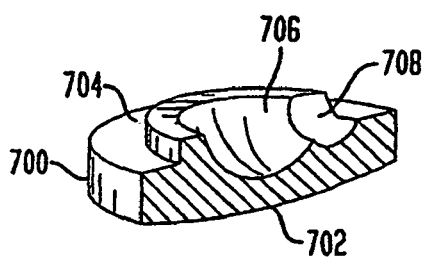


FIG. 4O

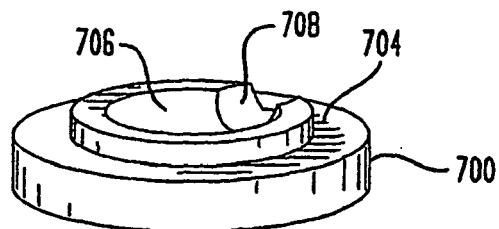


FIG. 4P

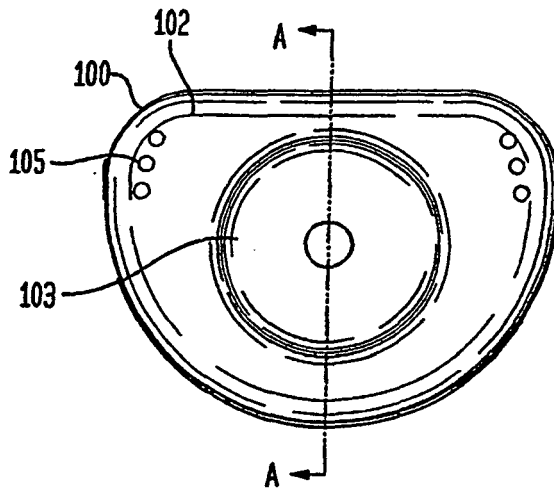


FIG. 4R

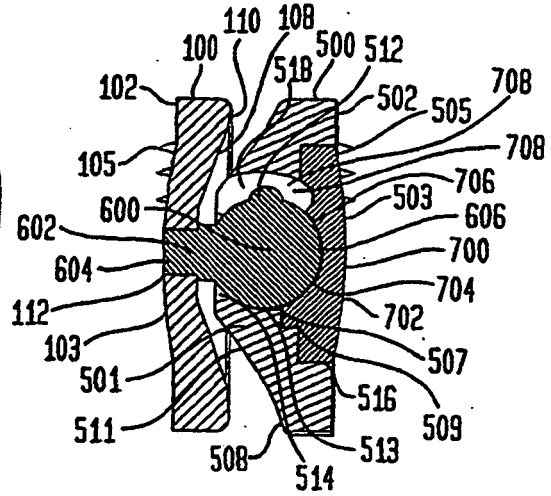


FIG. 4Q

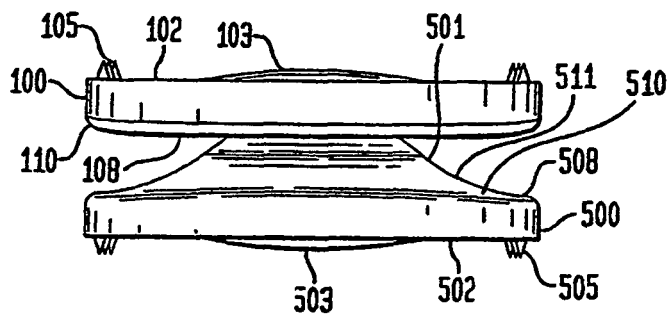


FIG. 4S

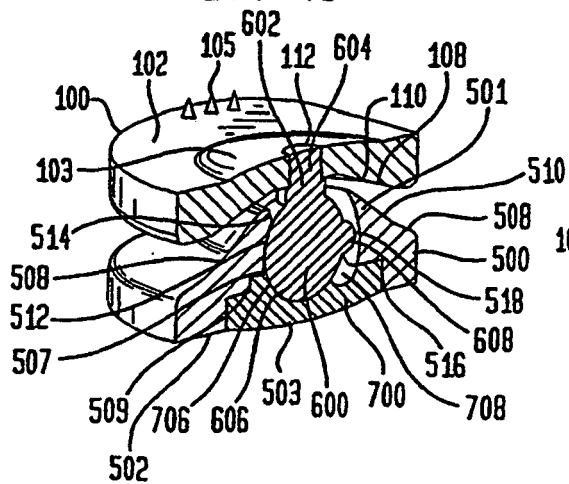


FIG. 4T

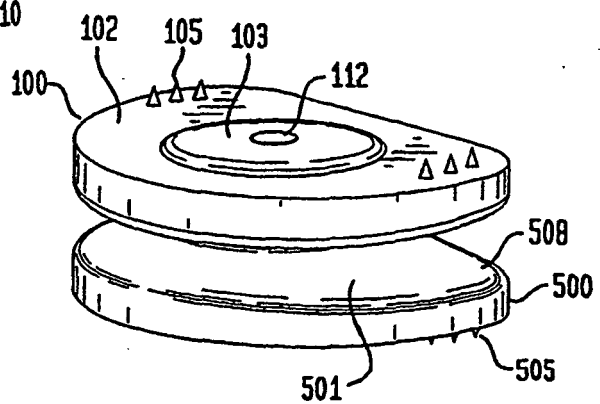


FIG. 5A

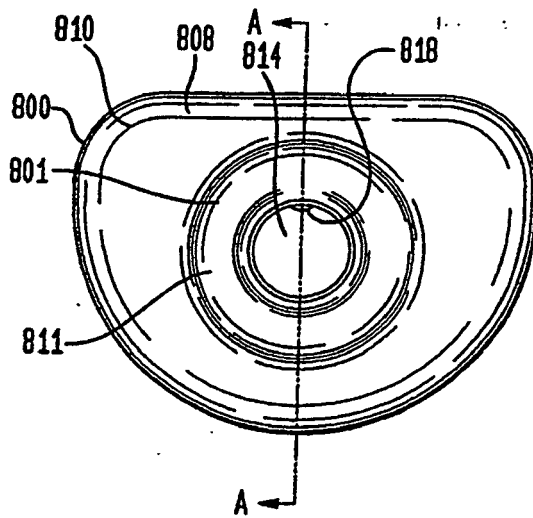


FIG. 5C

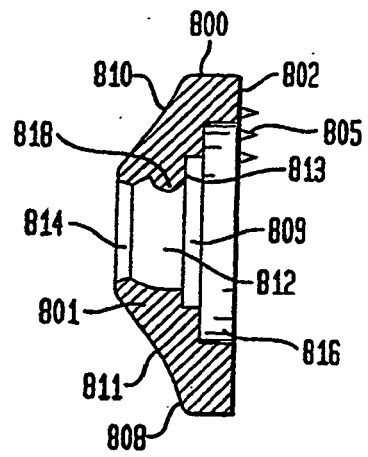


FIG. 5B

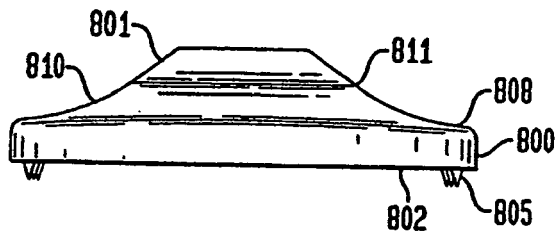


FIG. 5D

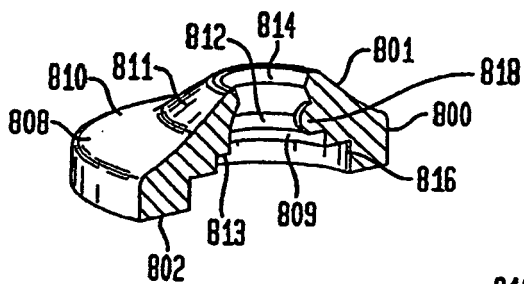


FIG. 5E

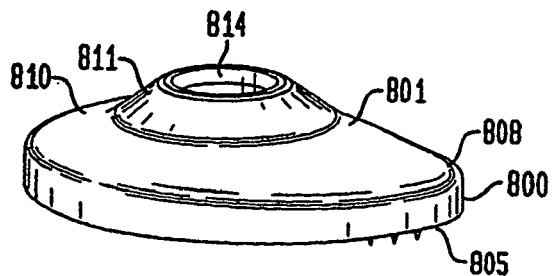


FIG. 5F

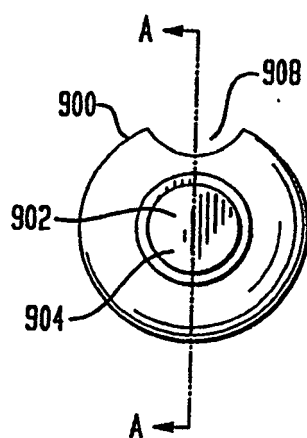


FIG. 5H

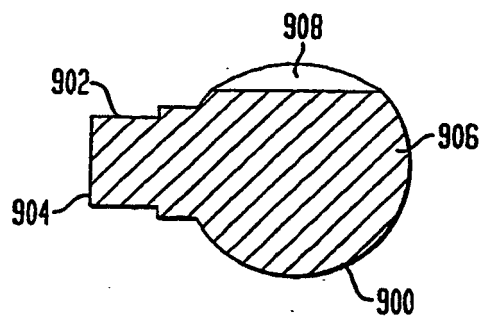


FIG. 5G

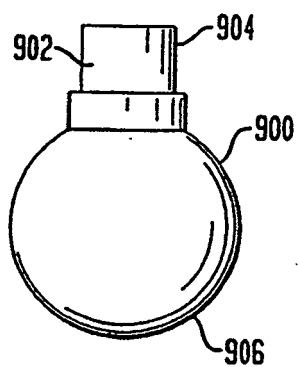


FIG. 5I

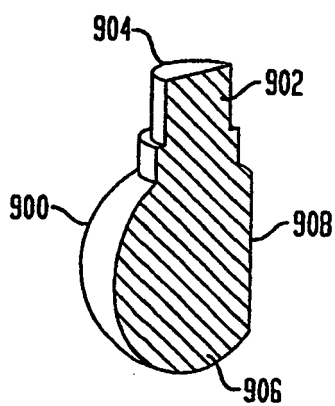


FIG. 5J

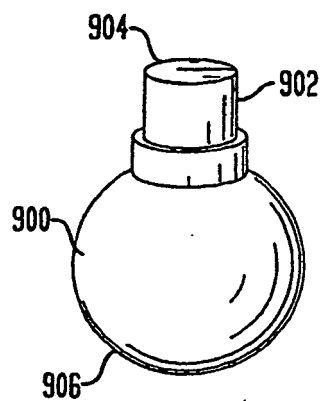


FIG. 5K

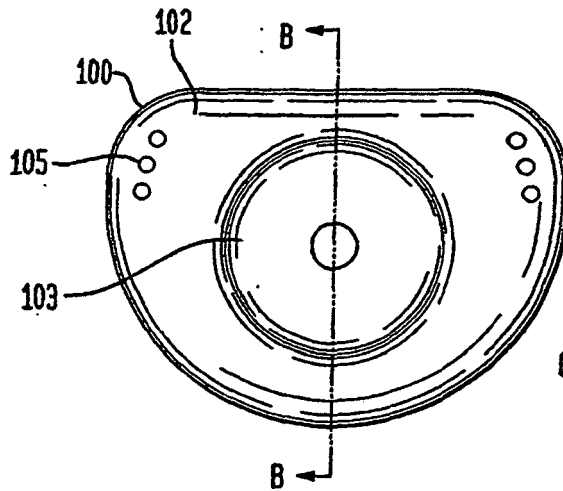


FIG. 5M

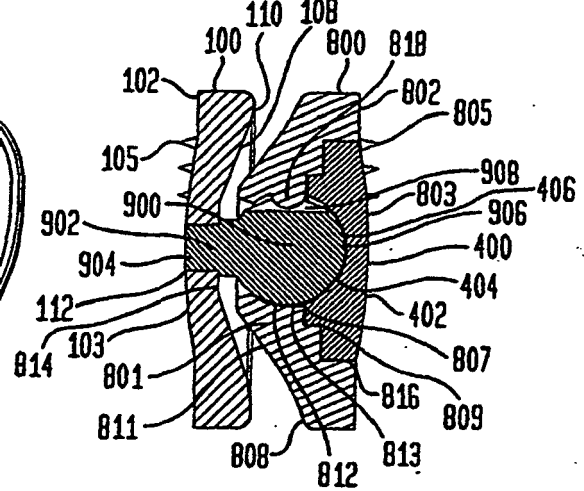


FIG. 5L

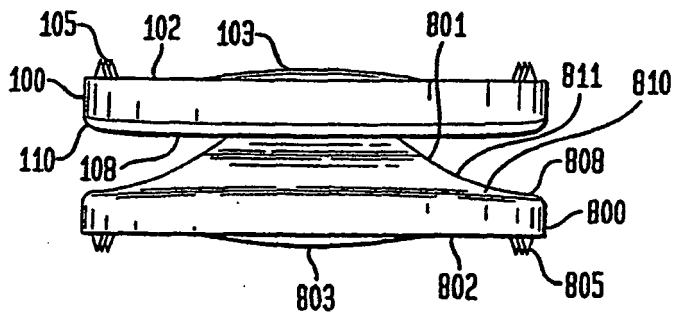


FIG. 5N

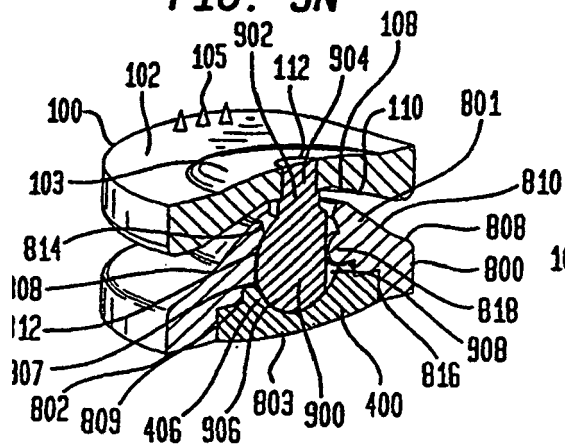


FIG. 50

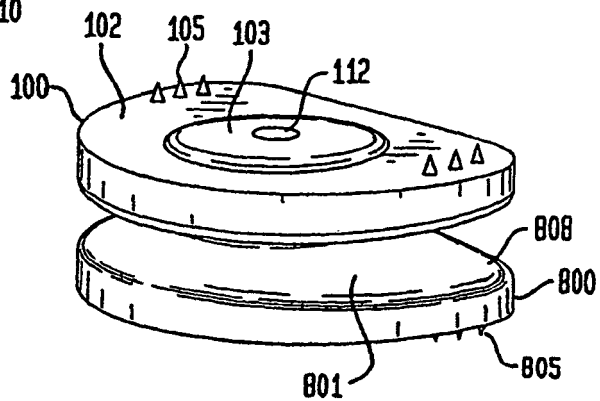


FIG. 6A

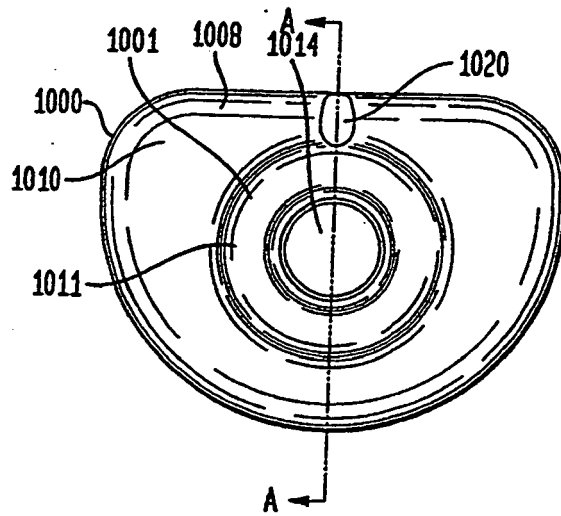


FIG. 6C

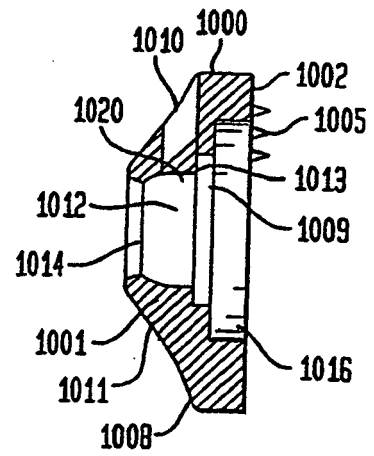


FIG. 6B

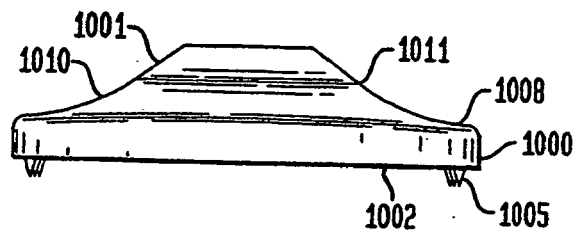


FIG. 6D

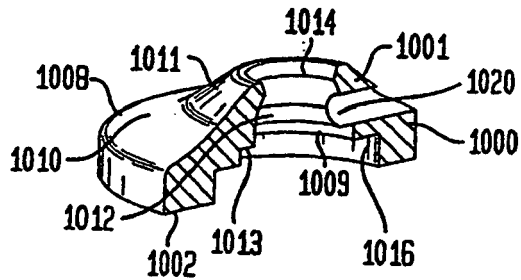


FIG. 6E

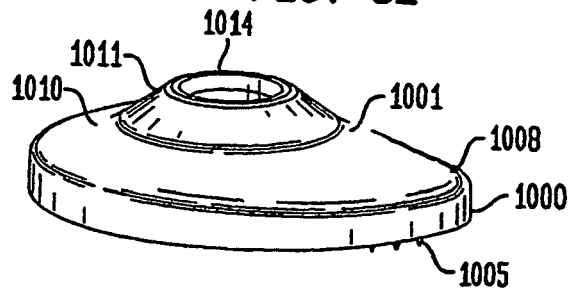


FIG. 6F

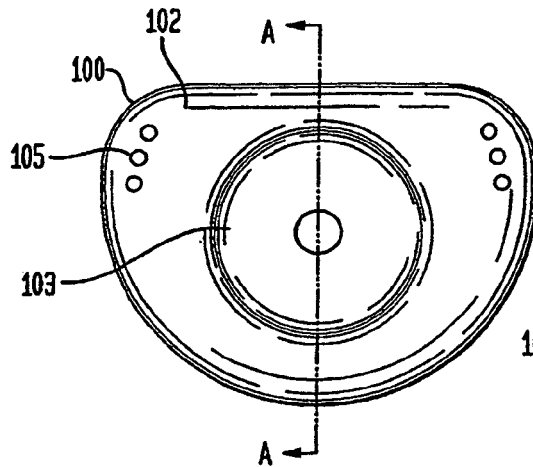


FIG. 6H

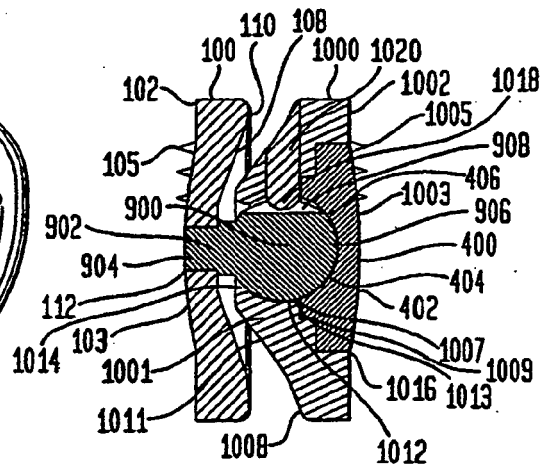


FIG. 6G

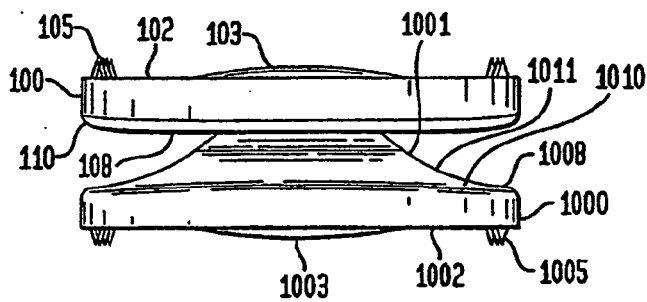


FIG. 6I

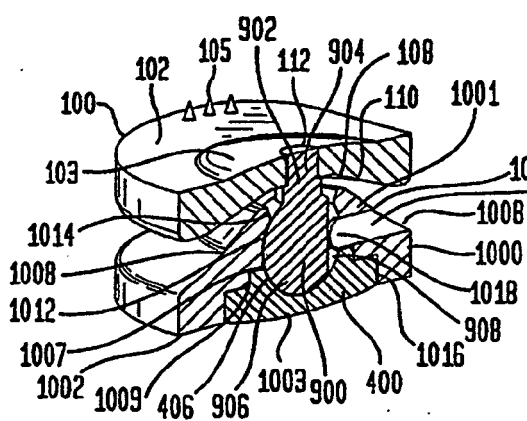


FIG. 6J

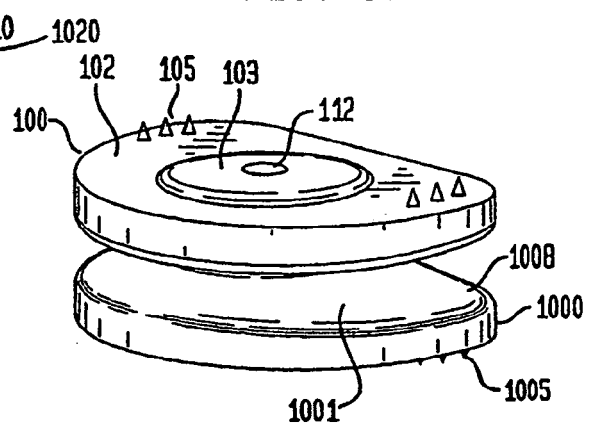


FIG. 7A

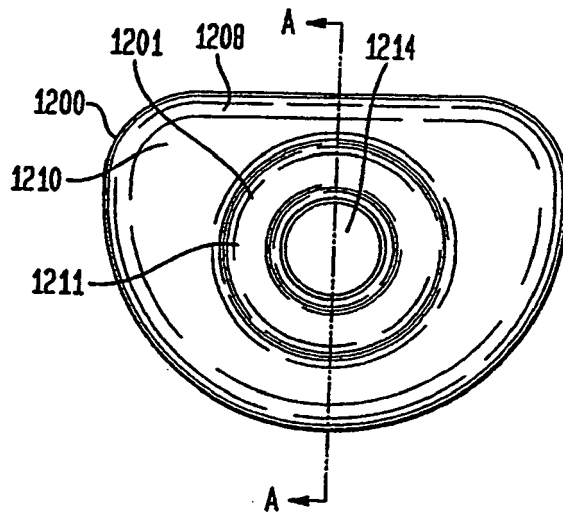


FIG. 7C

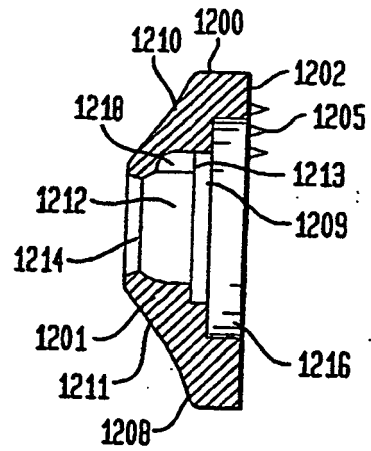


FIG. 7B

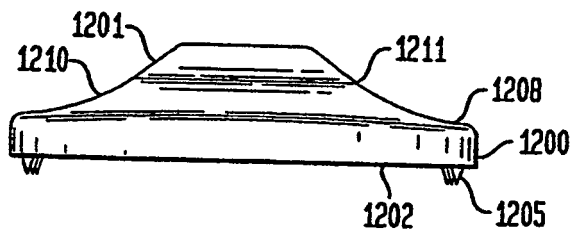


FIG. 7D

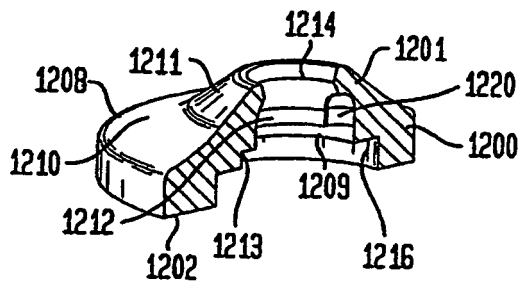


FIG. 7E

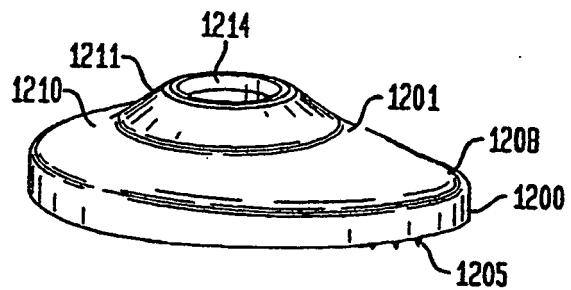


FIG. 7F

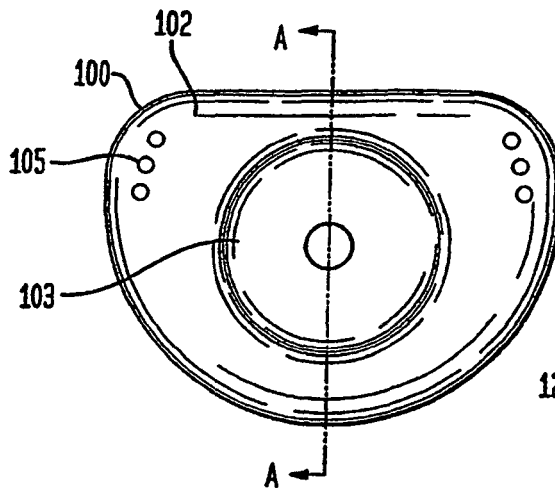


FIG. 7H

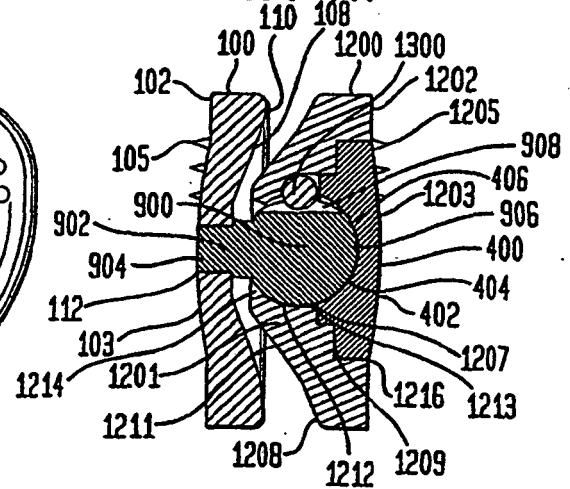


FIG. 7G

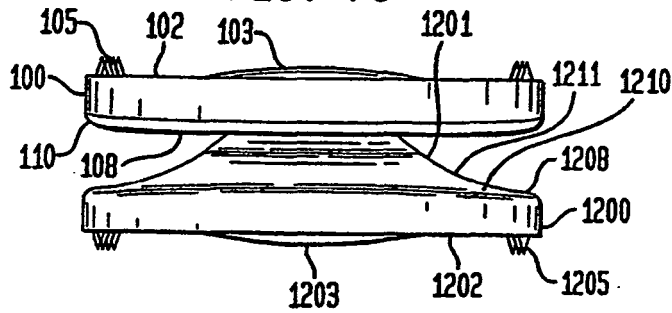


FIG. 7I

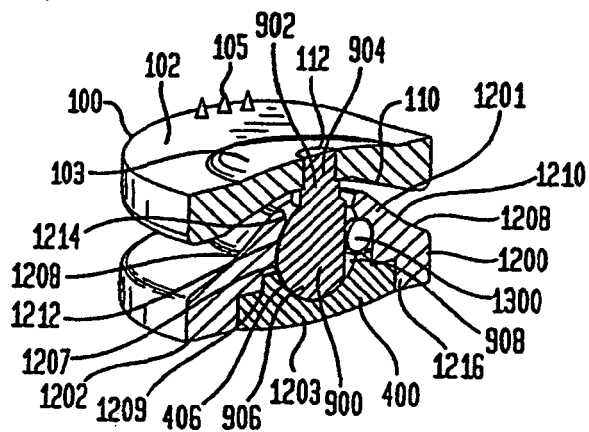


FIG. 7J

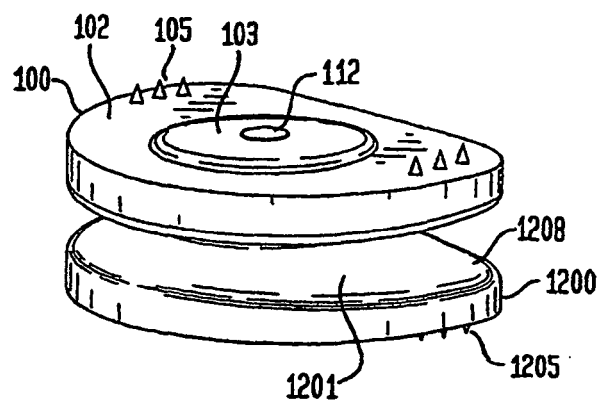


FIG. 8A

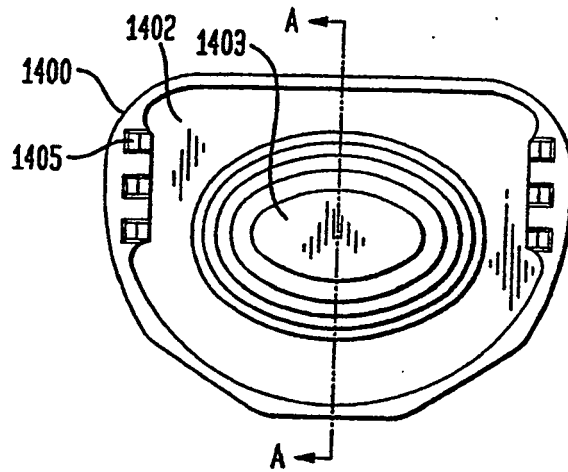


FIG. 8C

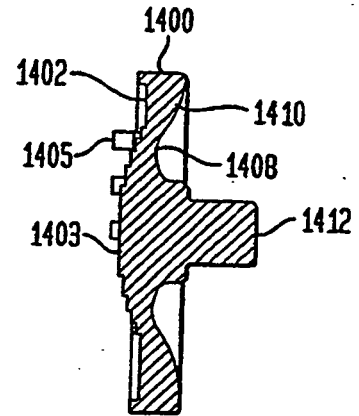


FIG. 8B

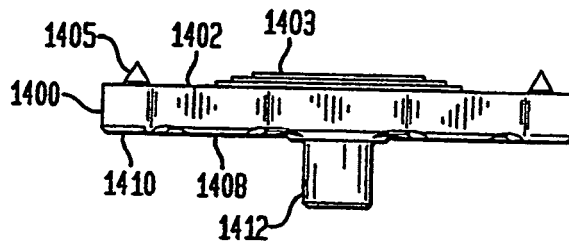


FIG. 8D

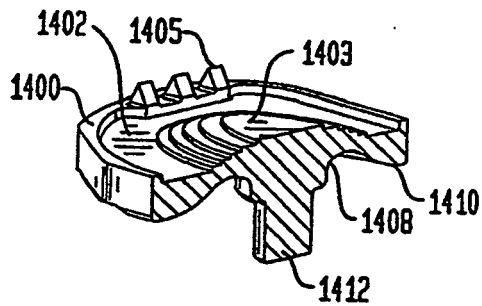


FIG. 8E

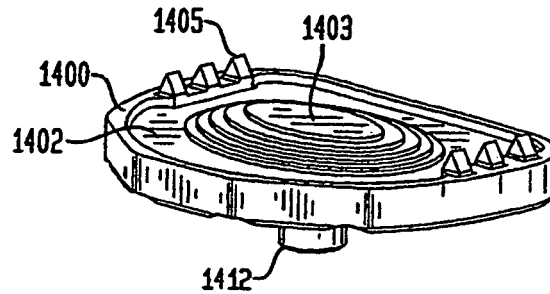


FIG. 8F

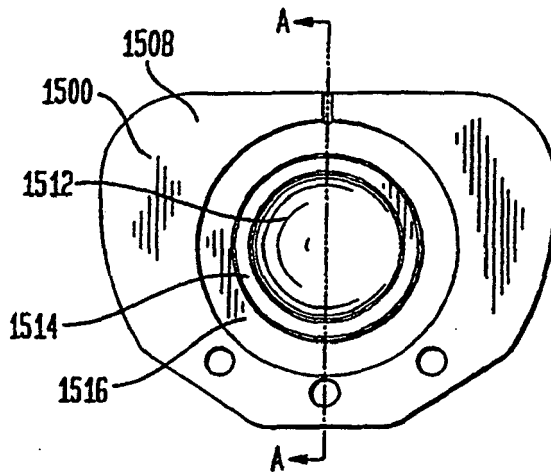


FIG. 8H

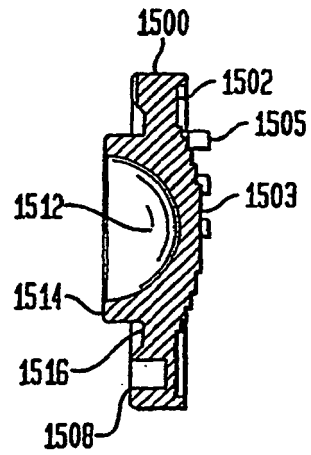


FIG. 8G

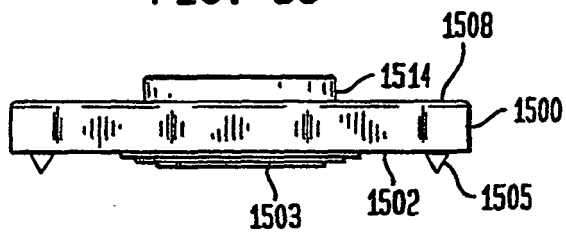


FIG. 8I

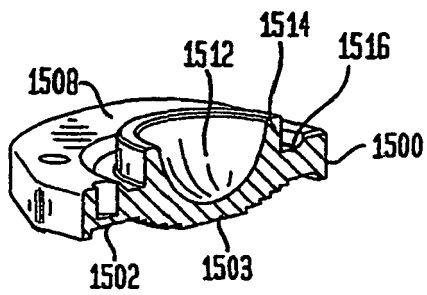


FIG. 8J

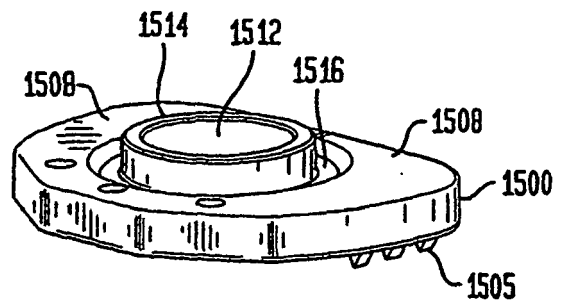


FIG. 8K

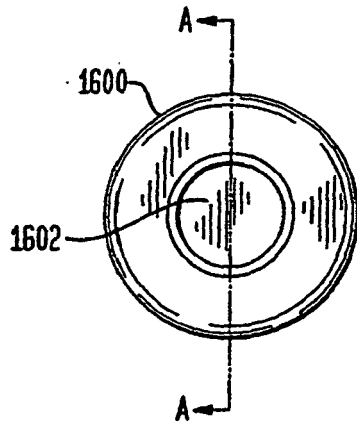


FIG. 8M

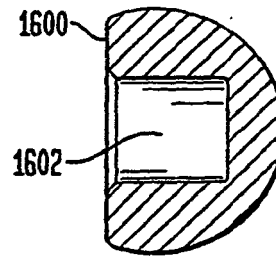


FIG. 8L

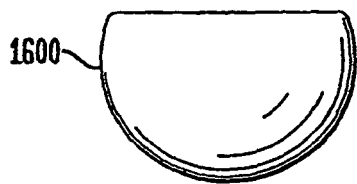


FIG. 8N

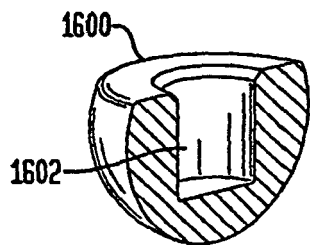


FIG. 8O

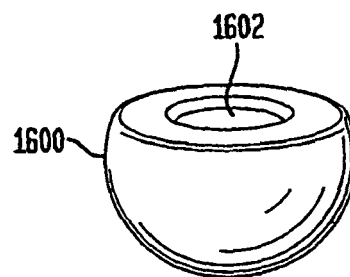


FIG. 8P

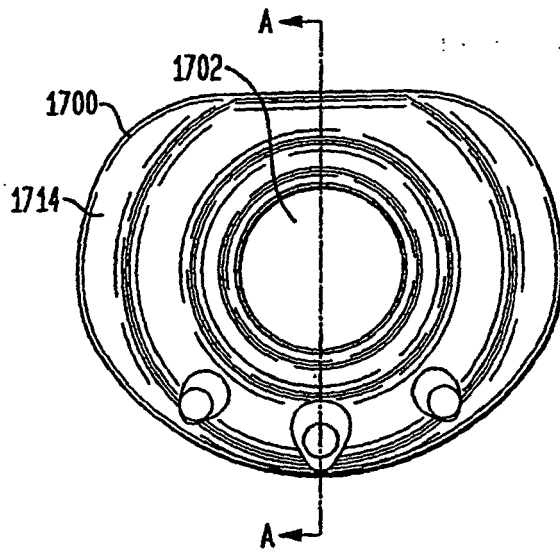


FIG. 8R

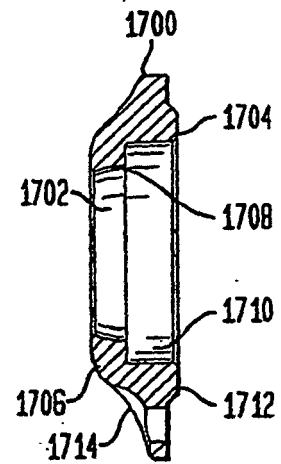


FIG. 8Q

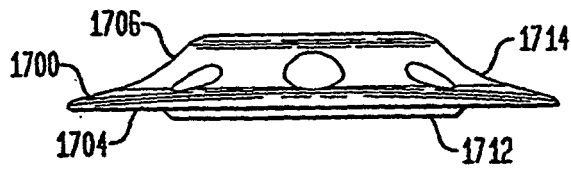


FIG. 8S

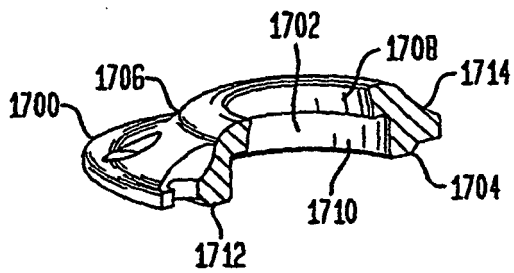


FIG. 8T

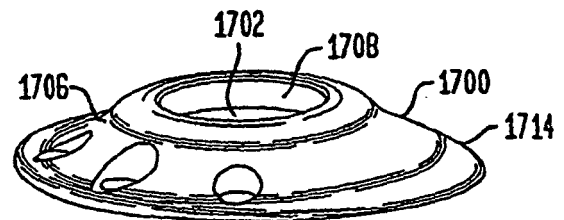


FIG. 8U

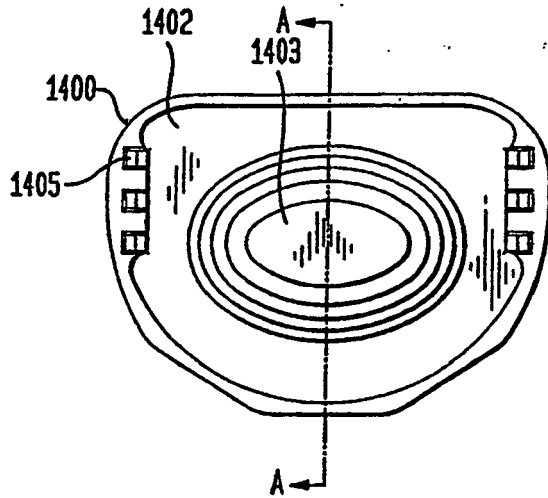


FIG. 8W

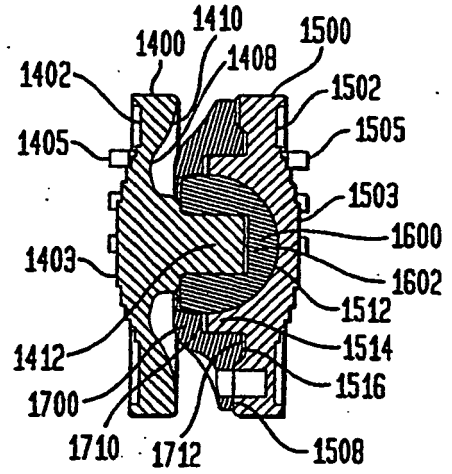


FIG. 8V

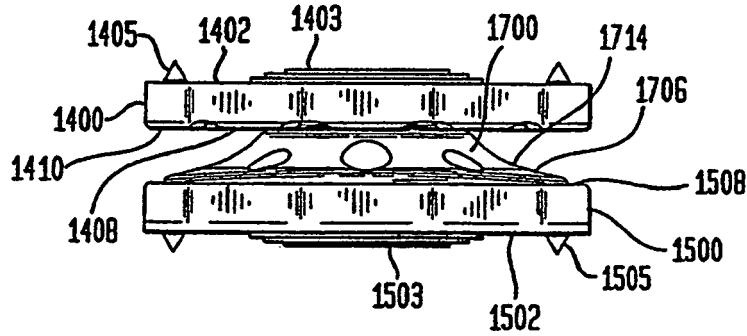


FIG. 8X

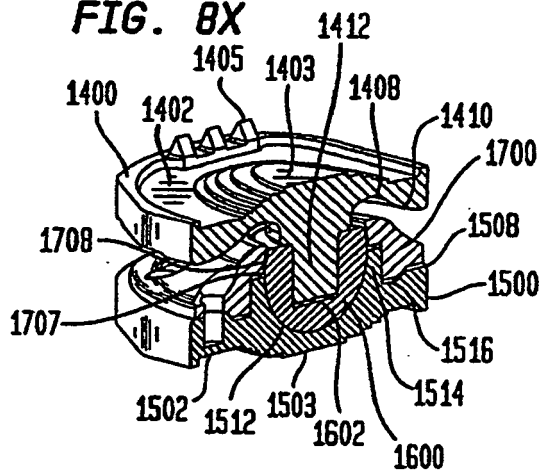


FIG. 8Y

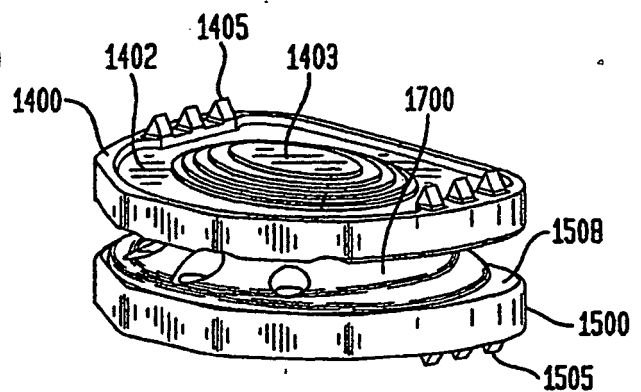


FIG. 9A

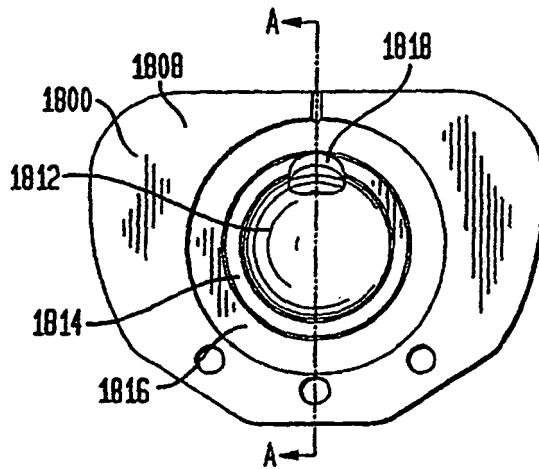


FIG. 9C

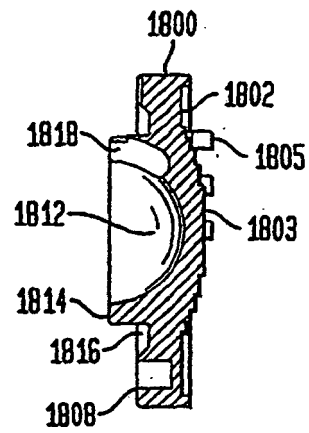


FIG. 9B

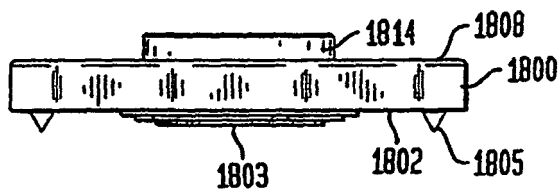


FIG. 9D

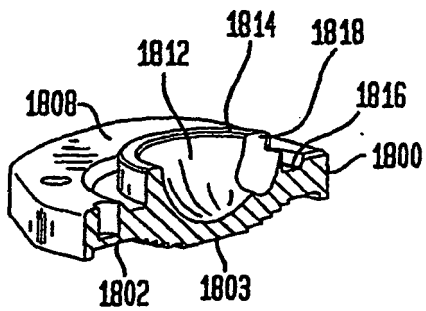


FIG. 9E

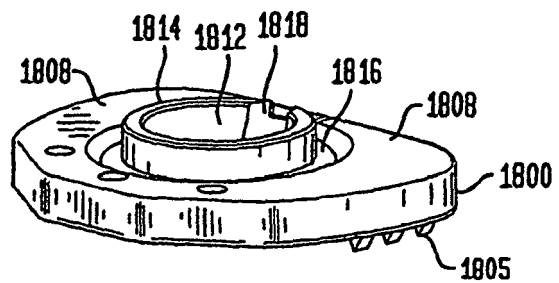


FIG. 9F

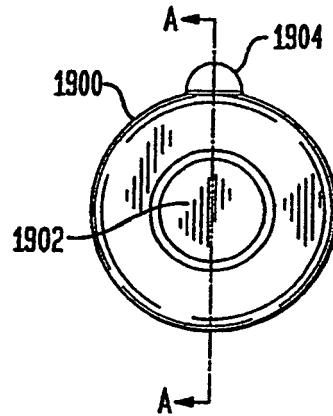


FIG. 9H

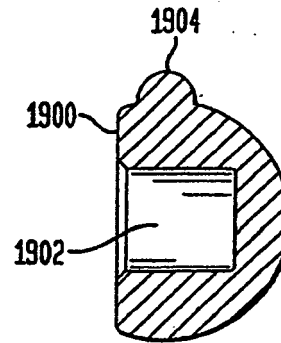


FIG. 9G

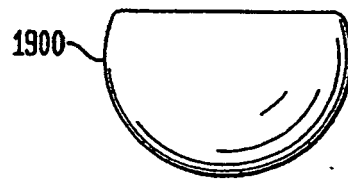


FIG. 9I

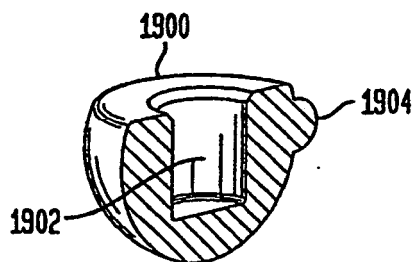


FIG. 9J

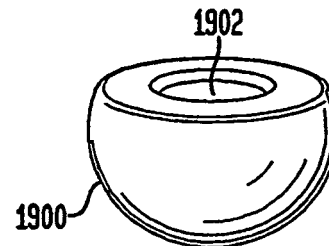


FIG. 9K

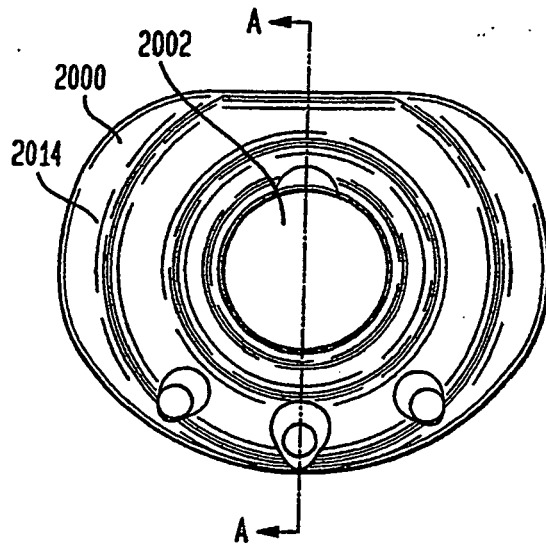


FIG. 9M

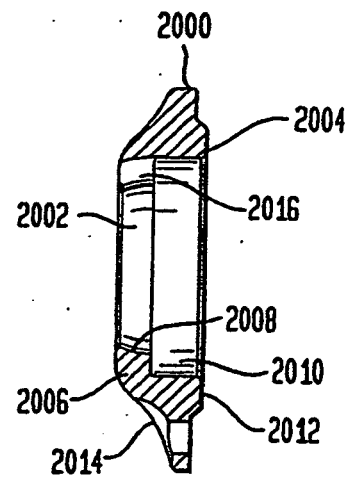


FIG. 9L

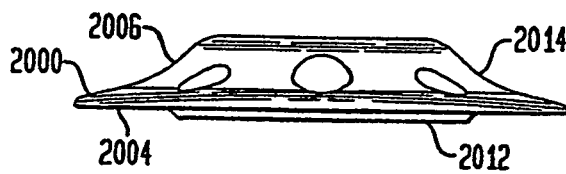


FIG. 9N

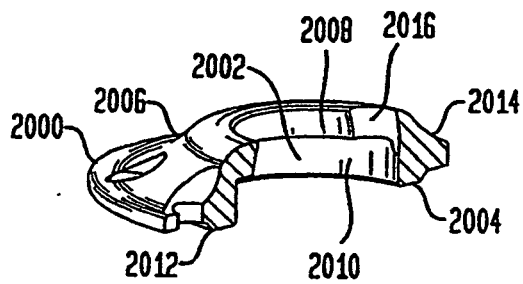


FIG. 9O

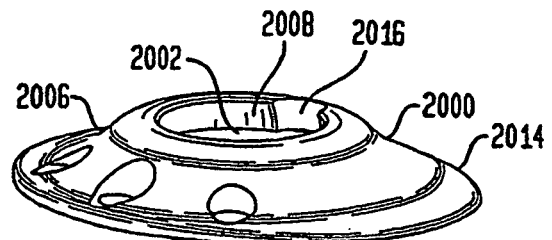


FIG. 9P

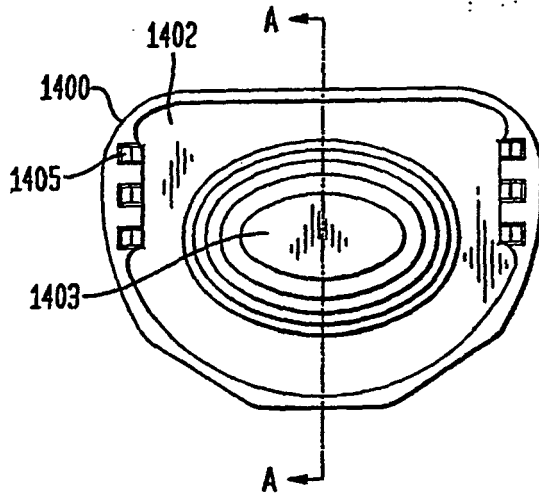


FIG. 9R

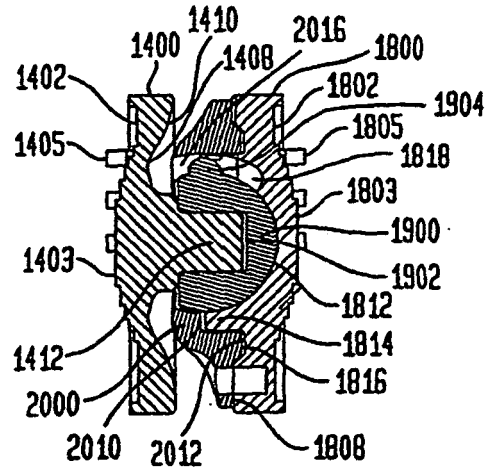


FIG. 9Q

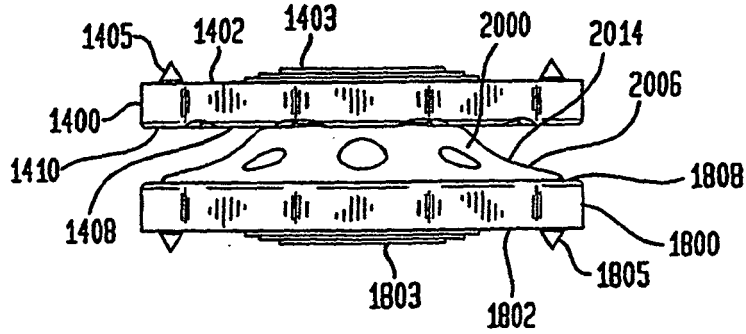


FIG. 9S

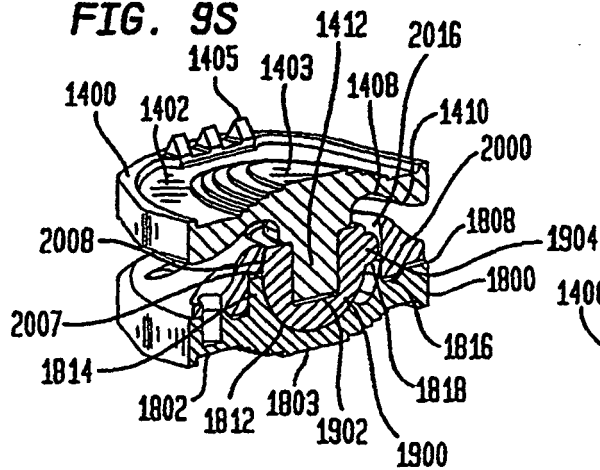


FIG. 9T

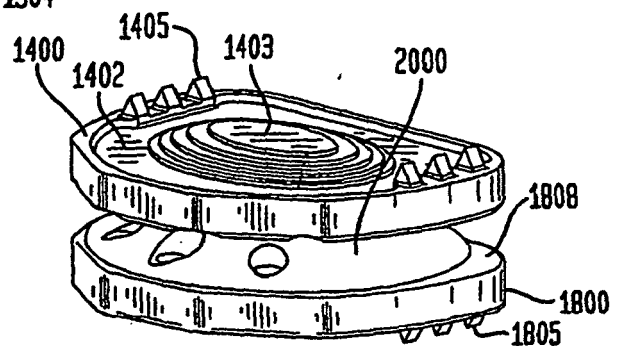


FIG. 10A

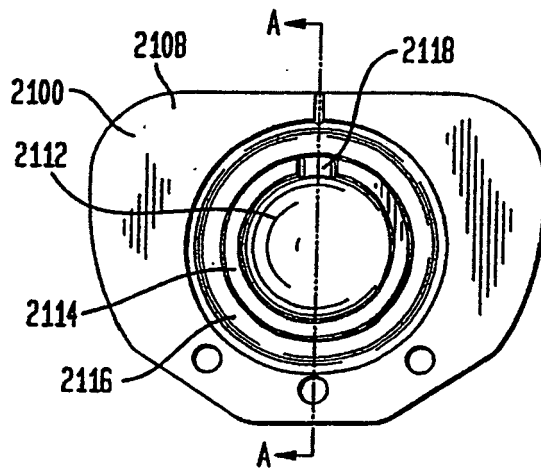


FIG. 10C

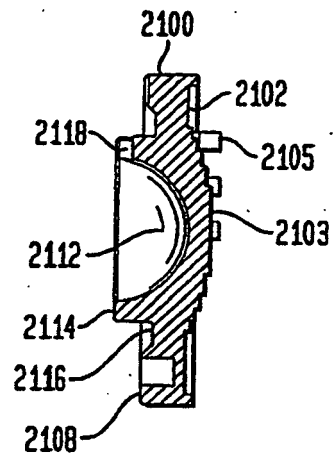


FIG. 10B

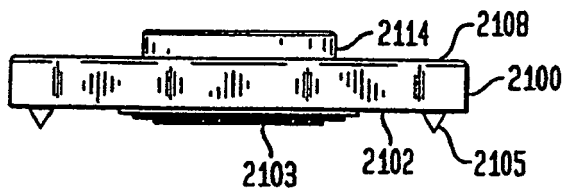


FIG. 10D

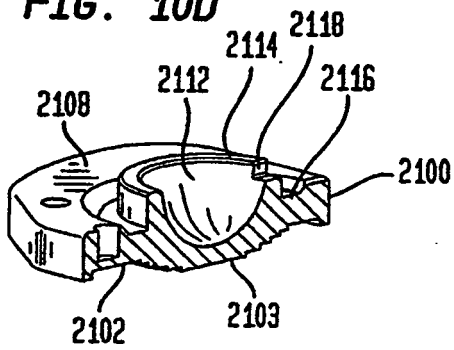


FIG. 10E

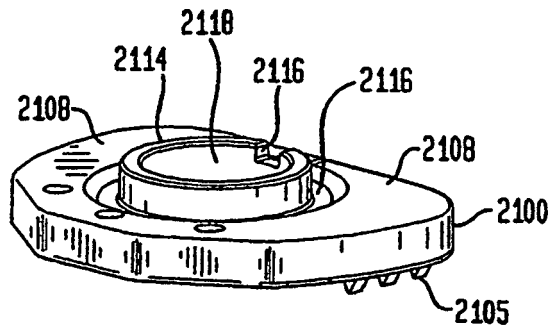


FIG. 10F

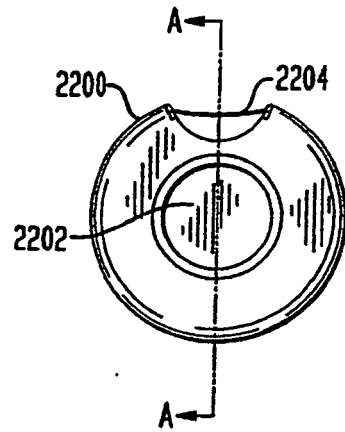


FIG. 10H

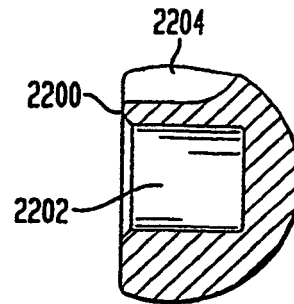


FIG. 10G

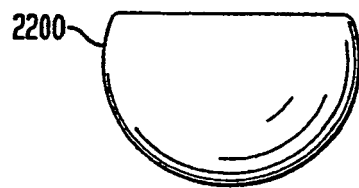


FIG. 10I

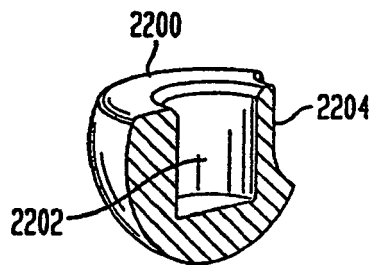


FIG. 10J

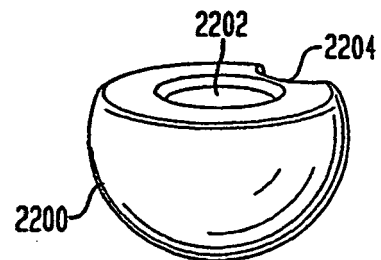


FIG. 10K

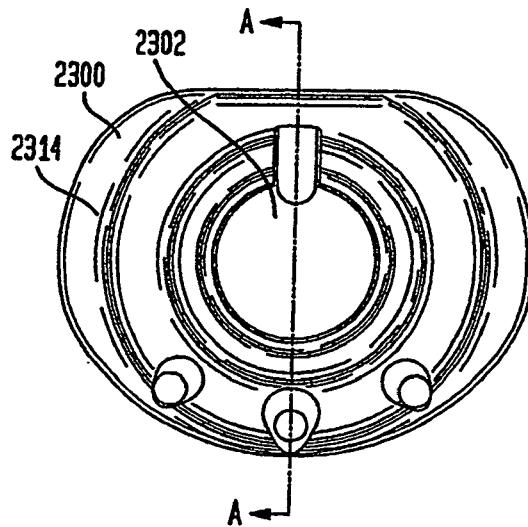


FIG. 10M

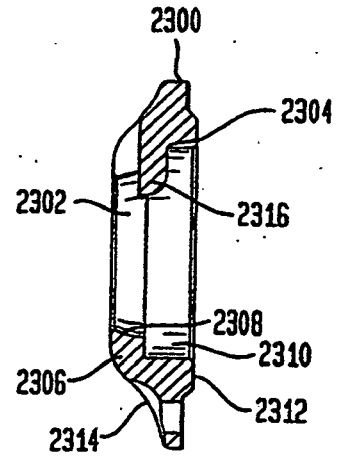


FIG. 10L

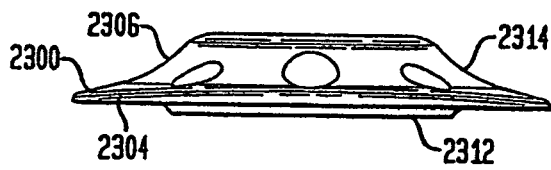


FIG. 10N

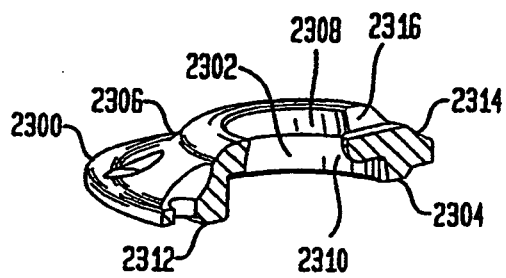


FIG. 10O

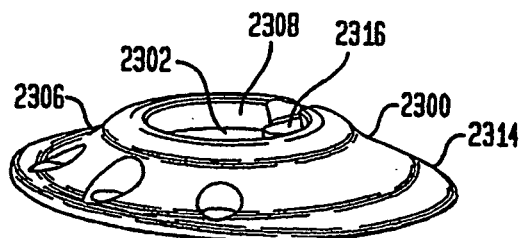


FIG. 10P

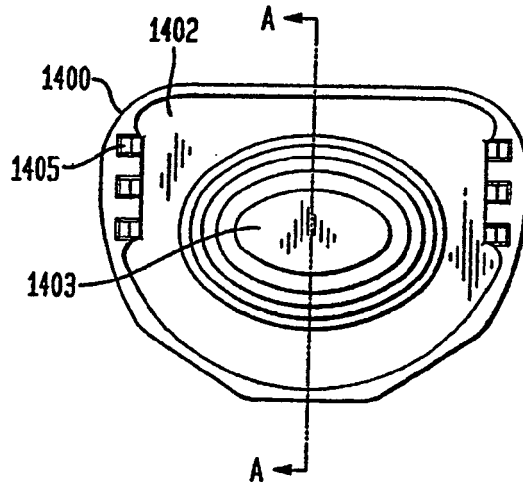


FIG. 10R

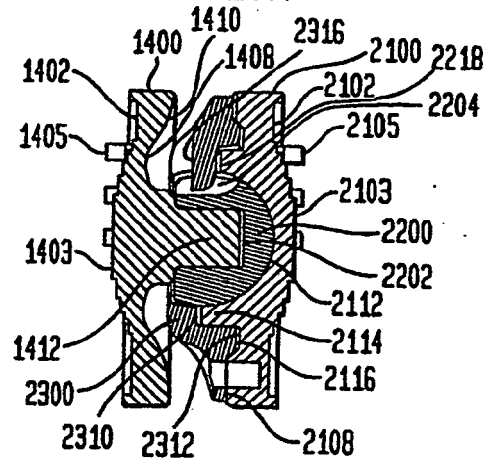


FIG. 10Q

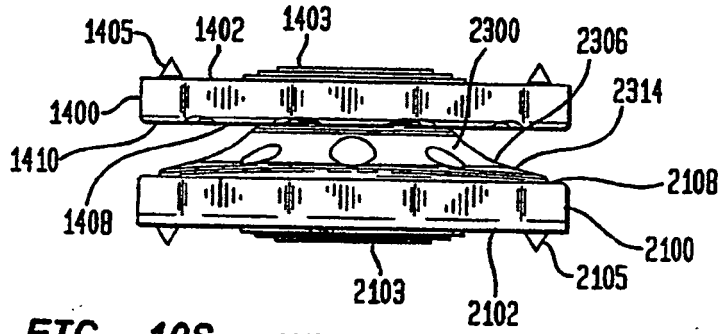


FIG. 10S

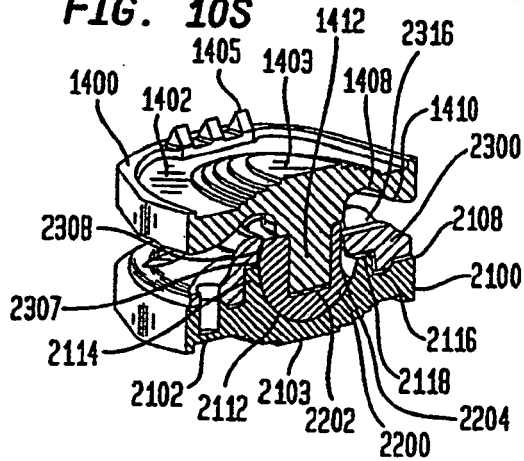


FIG. 10T

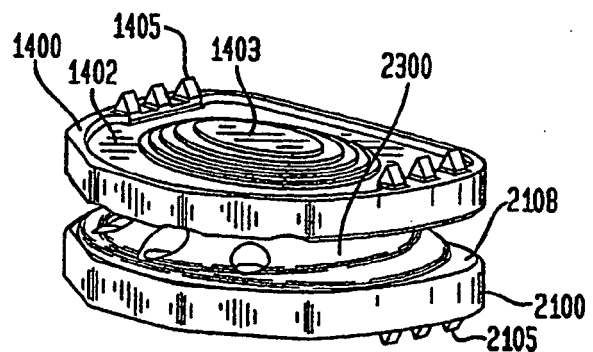


FIG. 11A

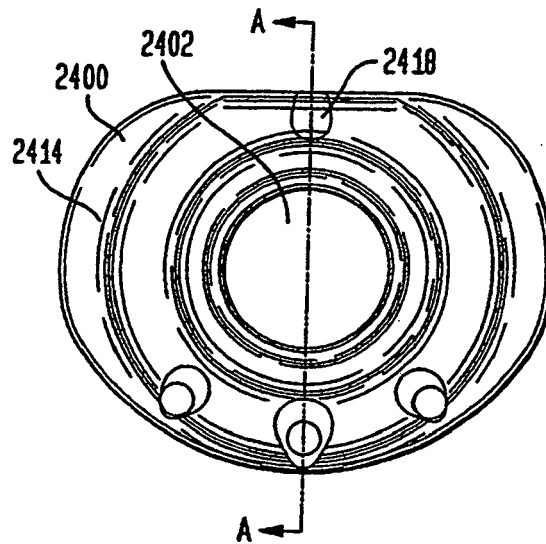


FIG. 11C

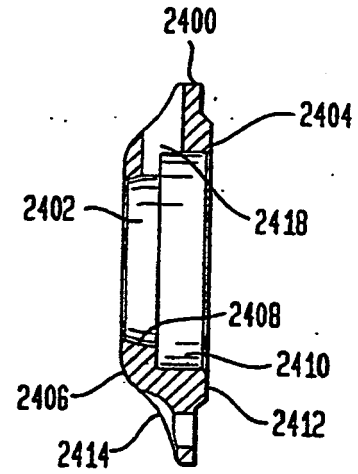


FIG. 11B

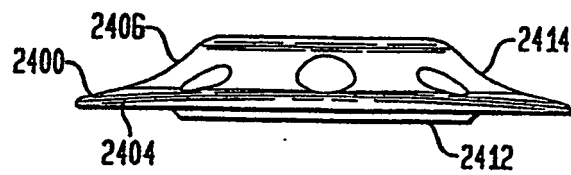


FIG. 11D

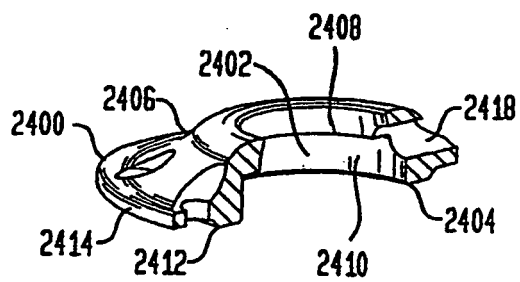


FIG. 11E

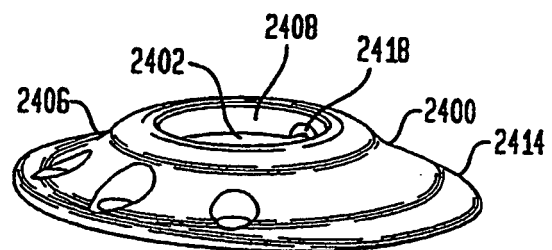


FIG. 11F

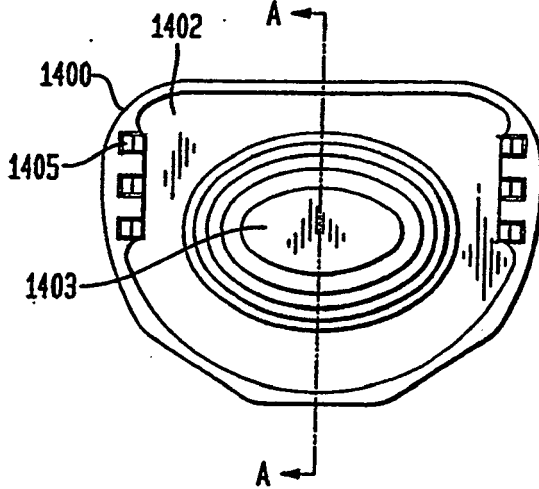


FIG. 11H

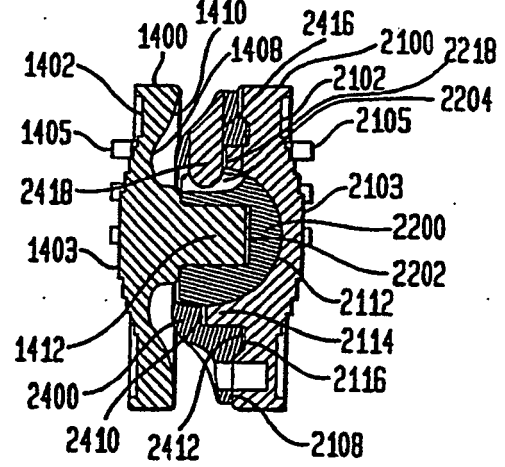


FIG. 11G

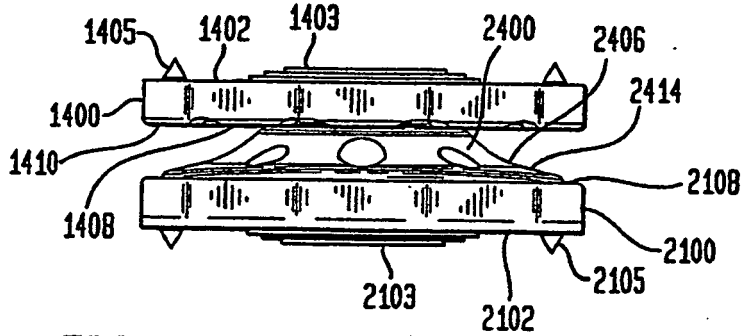


FIG. 11I

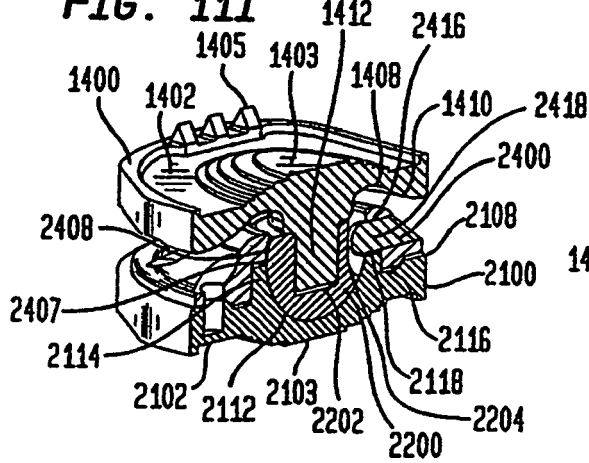


FIG. 11J

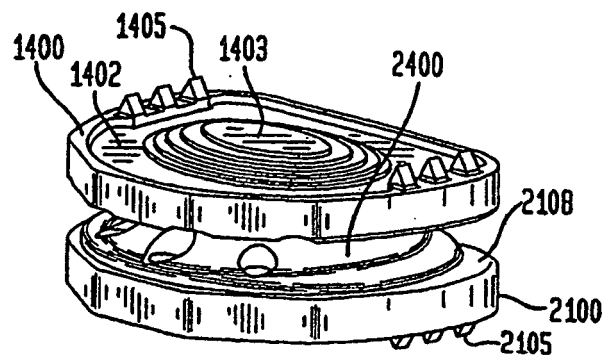


FIG. 12A

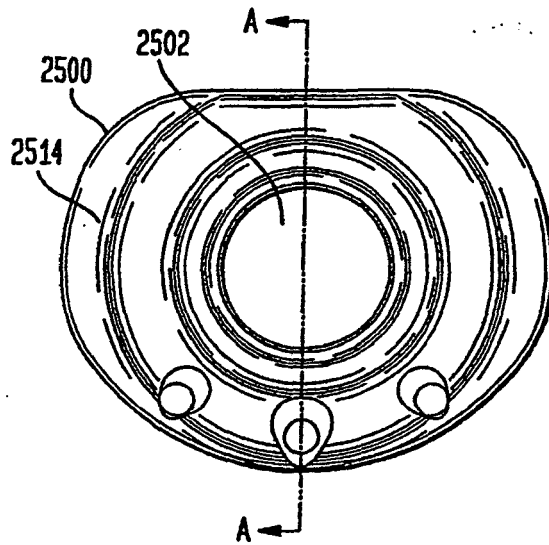


FIG. 12C

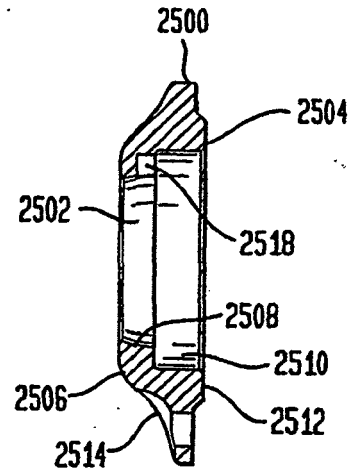


FIG. 12B

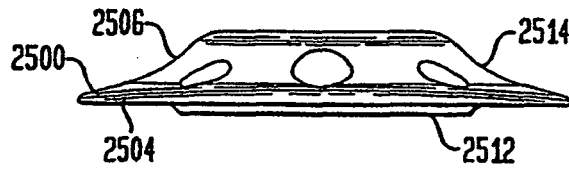


FIG. 12D

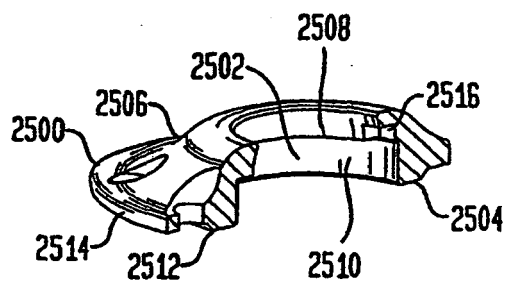


FIG. 12E

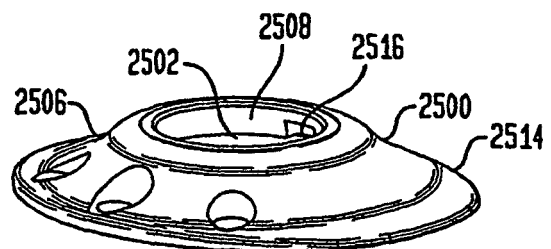


FIG. 12F

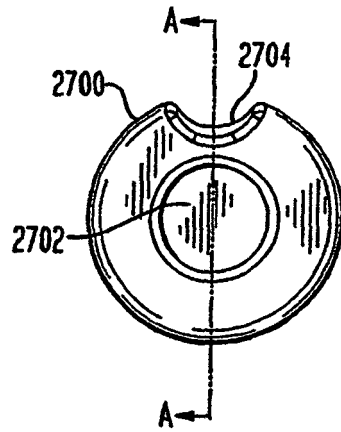


FIG. 12H

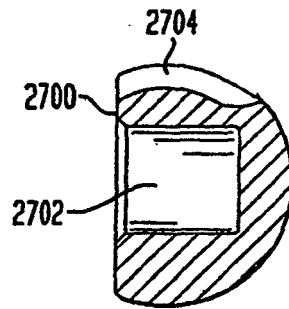


FIG. 12G

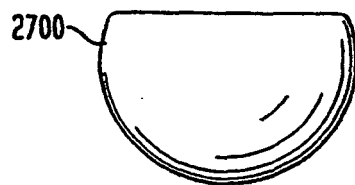


FIG. 12I

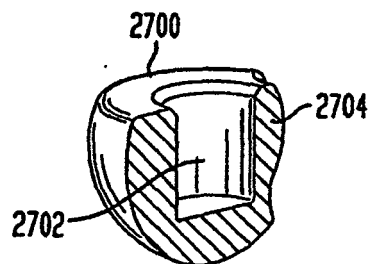
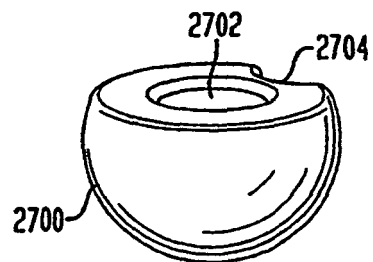


FIG. 12J



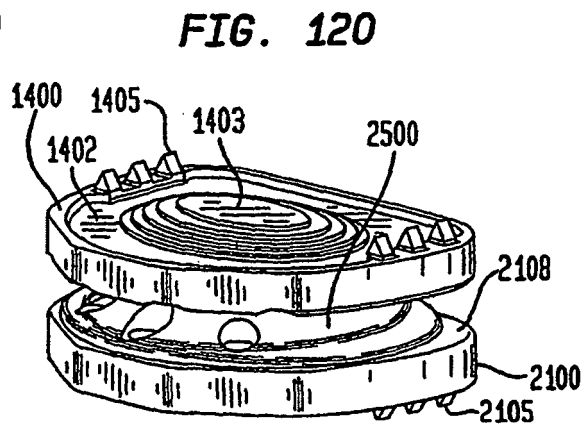
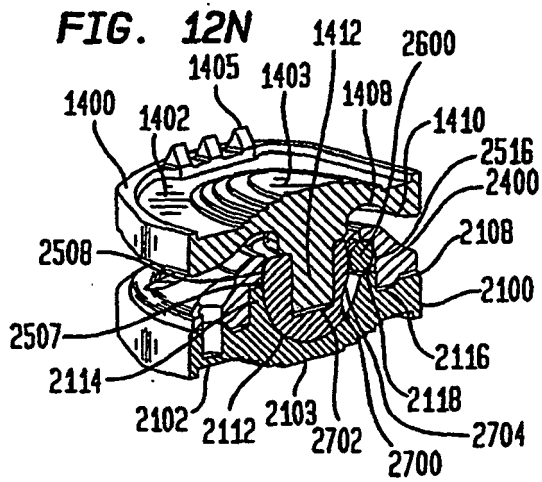
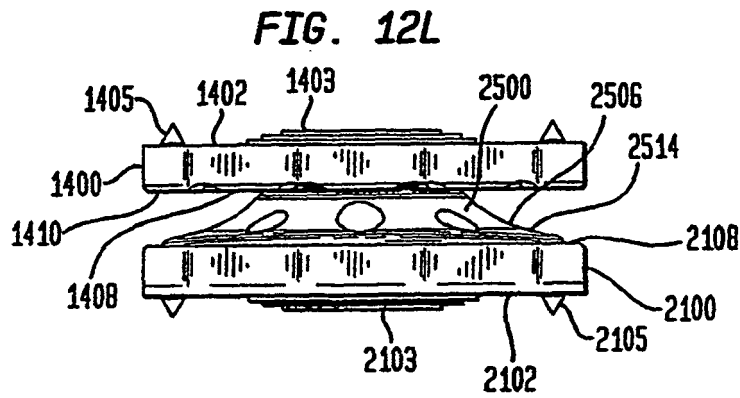
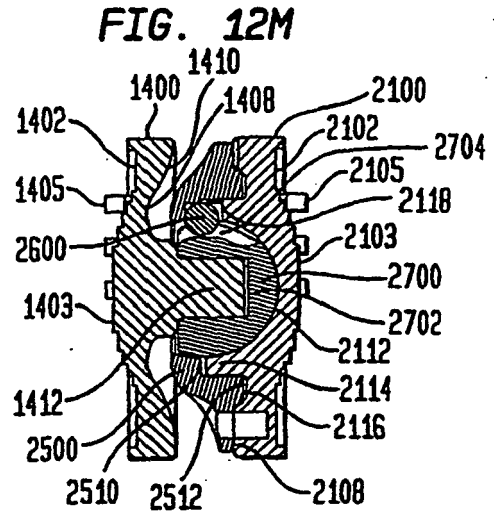
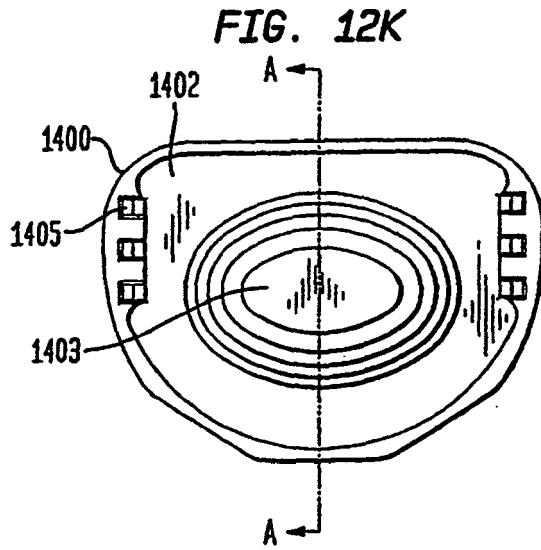


FIG. 13
(PRIOR ART)

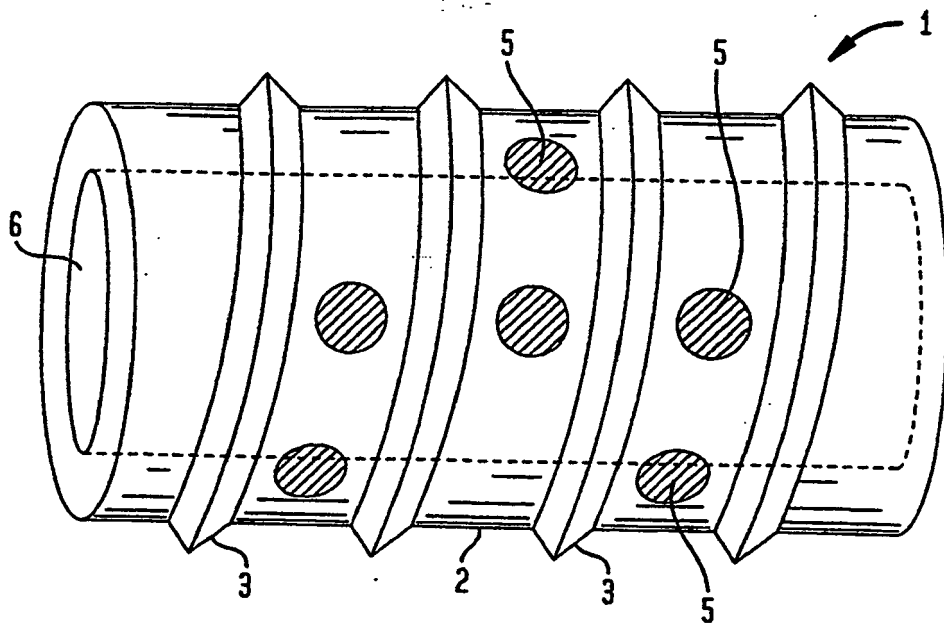


FIG. 14
(PRIOR ART)

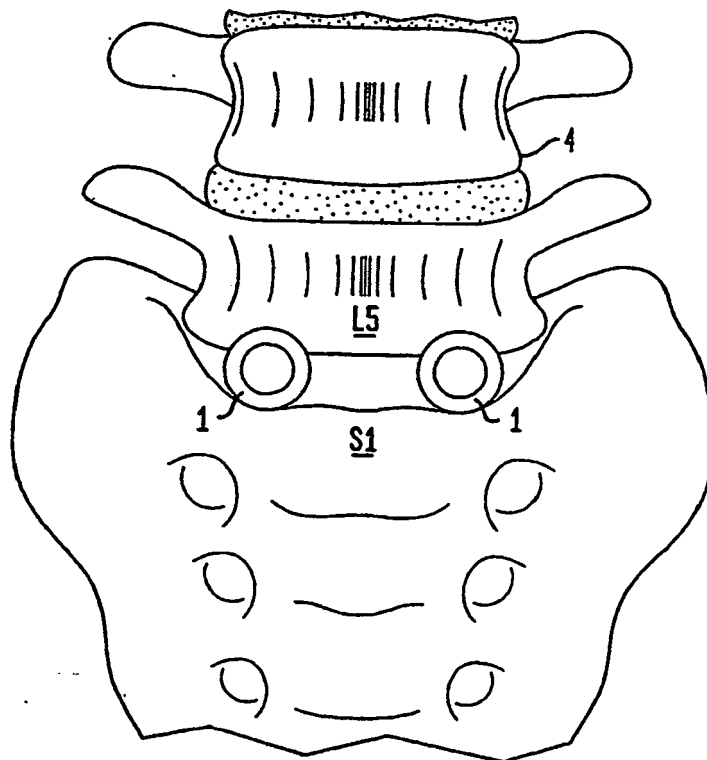


FIG. 3Z

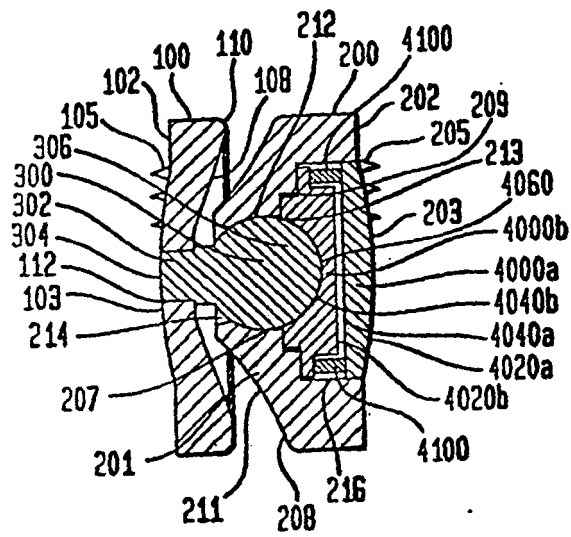


FIG. 4U

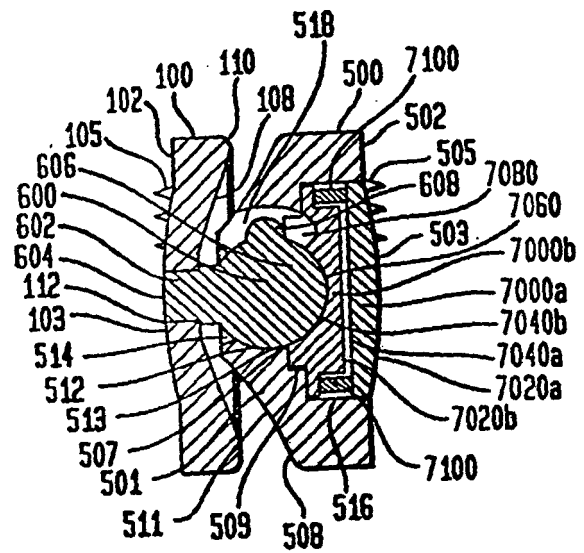


FIG. 5P

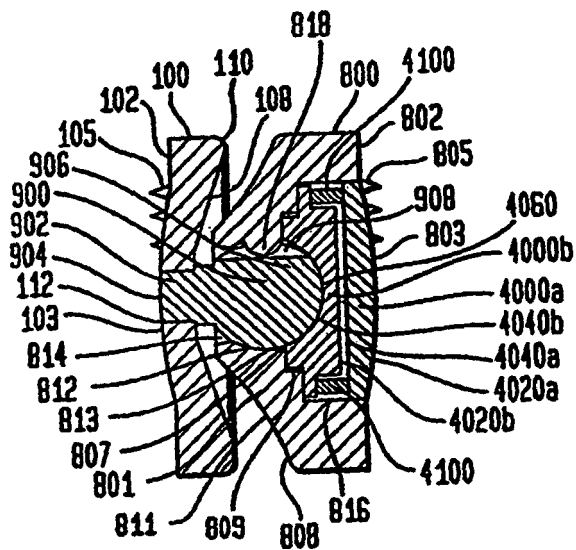


FIG. 6K

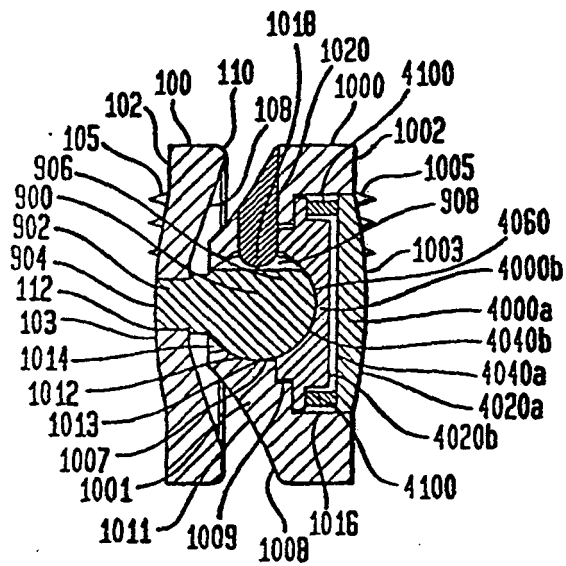


FIG. 7K

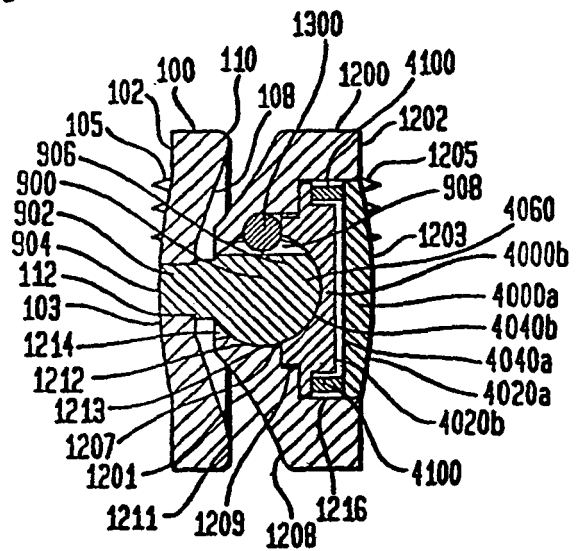


FIG. 8Z

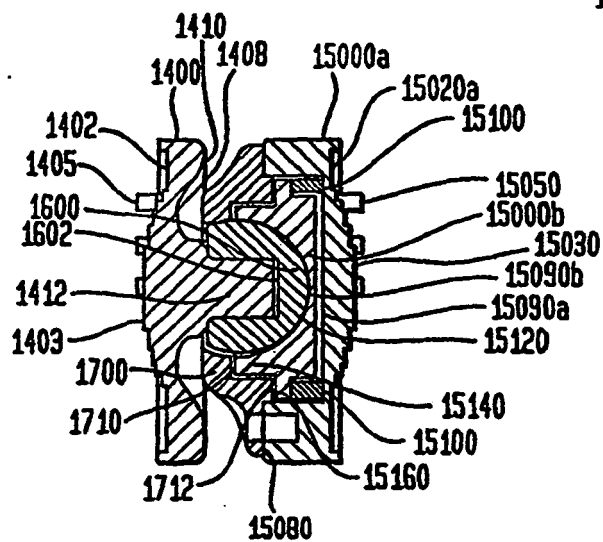


FIG. 9U

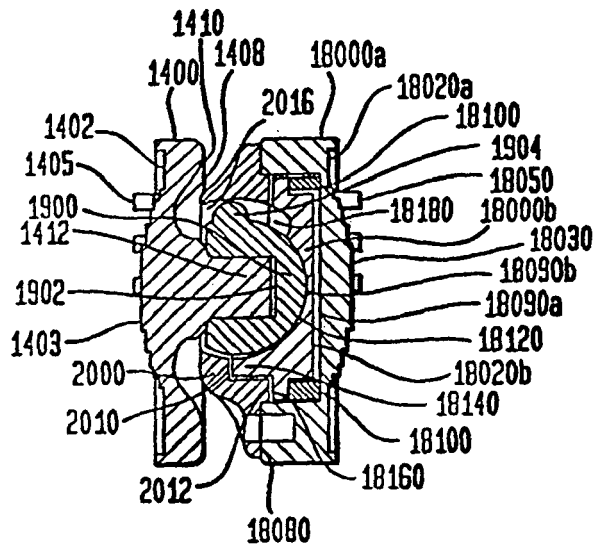


FIG. 10U

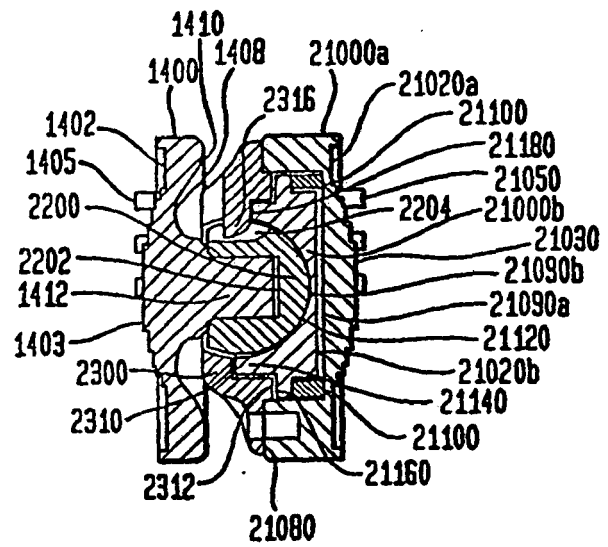


FIG. 11K

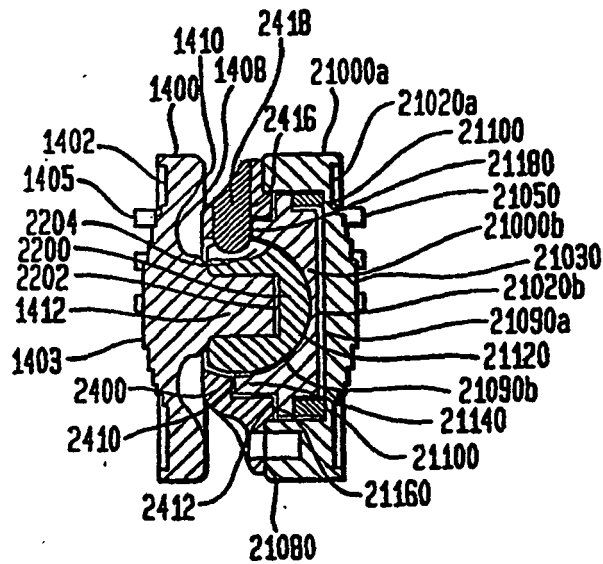


FIG. 12P

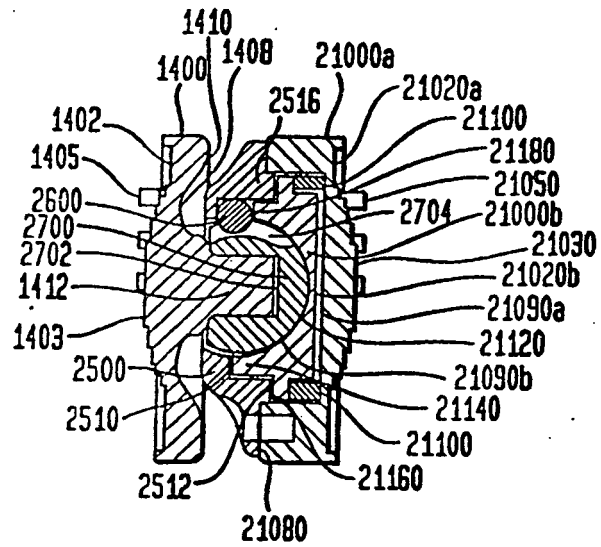


FIG. 8AA

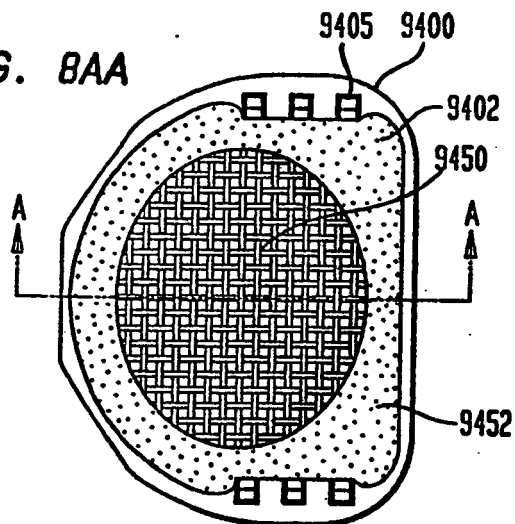


FIG. 8BB

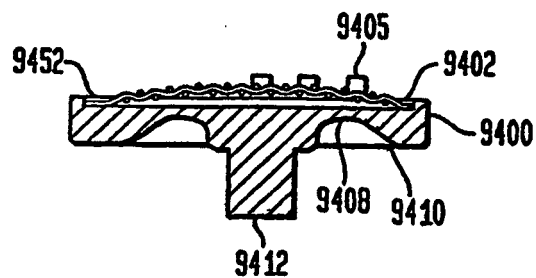


FIG. 8CC

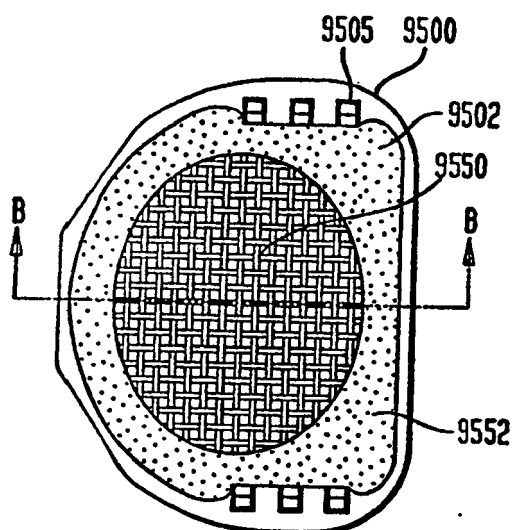
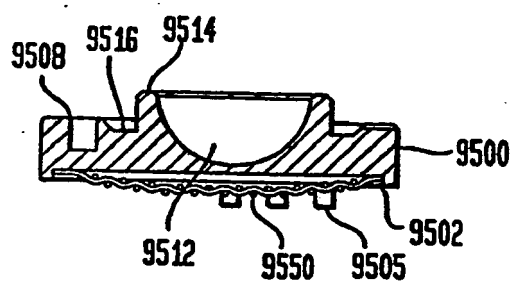


FIG. 8DD



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Patent documents cited in the description

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