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(54) **SYSTEM FOR DETECTING SHEATHING AND UNSHEATHING OF LOCALIZATION ELEMENTS**
SYSTEM ZUR ERKENNUNG VON UMHÜLLUNG UND ENTHÜLLUNG VON ORTUNGSELEMENTEN
SYSTÈME DE DÉTECTION DE GAINAGE ET DÉGAINAGE D'ÉLÉMENTS DE LOCALISATION

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US-A1- 2008 255 470 US-A1- 2009 262 109</p> |
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Description

BACKGROUND

a. Field of the Invention

[0001] The instant disclosure relates to localization systems, such as those used in cardiac diagnostic and therapeutic procedures. In particular, the instant disclosure relates to systems, apparatuses and methods for detecting when a localization element(s), such as an electrode(s), emerges from and/or is retracted into an introducer sheath or other enveloping instrument.

b. Background Art

[0002] US 2008/0255470 A1 relates to an electrode catheter and a method for using the catheter for tissue mapping, guidance and/or tissue ablation, wherein a localisation signal is not resolved into an in-phase component and a quadrature component.

[0003] US 2009/262109 A1 relates to illustrating a three-dimensional nature of a data set on a two-dimensional display, wherein no quadrature component of a demodulated signal is used for detecting a change of state of an electrode.

b. Background Art

[0004] Catheters are used for an ever-growing number of procedures. For example, catheters are used for diagnostic, therapeutic, and ablative procedures, to name just a few examples. Typically, the catheter is manipulated through the patient's vasculature and to the intended site, for example, a site within the patient's heart. In many instances, the catheters are inserted into the body and navigated to the target location with the aid of an introducer sheath (sometimes referred to as simply an "introducer" or a "sheath"). As the ordinarily skilled artisan will appreciate, an introducer is a catheter with a central lumen through which other medical devices can be passed.

[0005] It is also known to track the three-dimensional coordinates of a catheter or other medical device moving within a patient's body using a localization system (sometimes also referred to as a "mapping system," "navigation system," or "positional feedback system"). These devices typically use magnetic, electrical, ultrasound, and other radiation sources to determine the coordinates of these devices. For example, impedance-based localization systems determine the coordinates of the medical device by interpreting a voltage measured by the medical device (more particularly, the voltages measured by one or more electrodes carried on the medical device) as a location within an electrical field.

[0006] One drawback of an impedance-based system, however, is that the impedance measurements become unreliable when the medical device is withdrawn into the

introducer. This is because the introducer is normally made of an insulating material, such that the voltage gradient in the vicinity of localization electrodes within the sheath becomes non-linear and erratic. Indeed, a localization electrode within a sheath may appear to wander widely, making it difficult for the localization system to accurately and precisely render an image of the medical device for the practitioner. Although visual recognition of this condition is possible, there is no extant system or method to do so analytically.

BRIEF SUMMARY

[0007] Among other things, the disclosure provides an analytical method(s) to detect a localization element/sheath state change (e.g., the emergence of a localization electrode from or withdrawal of a localization electrode into an introducer).

[0008] The disclosure also provides an analytical method(s) to identify the position of a localization element(s) relative to an introducer (e.g., whether the localization element(s) is/are within, or outside of, the introducer).

[0009] Further, a localization system is disclosed that analytically detects localization element/sheath state changes.

[0010] Also disclosed herein is a localization system that analytically determines the relative position of a localization element(s) to an introducer sheath.

[0011] In one aspect, a method of detecting a localization element/sheath state change with a localization system includes the following steps: establishing a localization field using a plurality of localization field generators; obtaining at least one localization signal from at least one catheter-borne localization element positioned within the localization field via an introducer sheath, the at least one localization signal including an in-phase component and a quadrature component; and detecting a localization element/sheath state change for the at least one catheter-borne localization system based on the quadrature component of the at least one localization signal. The method optionally further includes establishing a baseline quadrature component with the at least one localization element outside of the introducer sheath. In some embodiments, the baseline quadrature component is established by adjusting a demodulation delay for the localization signal until the quadrature component remains substantially constant at a calibration value as the at least one localization element moves. Movement of the localization element can be imparted by patient (e.g., cardiac) motion and/or by catheter motion.

[0012] In certain aspects, withdrawal of the at least one localization element into the introducer sheath is detected based upon the quadrature component of the at least one localization signal deviating from the calibrated value by more than a preset amount. Similarly, re-emergence of the at least one localization element from the introducer sheath can be detected based upon the quadrature com-

ponent of the at least one localization signal returning to within the preset amount of the calibrated value.

[0013] Upon detecting withdrawal of the at least one localization element into the introducer sheath, an alert can be generated.

[0014] In another aspect, the baseline quadrature component can be established by making a plurality of complex impedance measurements and determining least squares parameters in a linear model. Withdrawal of the at least one localization element into the introducer sheath can then be detected based upon the quadrature component of the at least one localization signal deviating from the linear model by more than a preset amount.

[0015] It is also contemplated that the localization signal is measured along an axis defined by a first localization field generator and a second localization field generator, relative to a reference point substantially aligned with the axis, where the at least one catheter-borne localization element is spaced apart from the reference point along the axis. For example, the first localization generator can be positioned on a patient's neck, the second localization field generator can be positioned on the patient's leg, the reference point can be on the patient's belly, and the at least one catheter-borne localization element can be positioned within the patient's heart.

[0016] In a further aspect, a method of conducting a cardiac electrophysiology study includes: establishing an impedance-based localization field encompassing a patient's body; obtaining a localization signal from at least one localization element on at least one medical device positioned in the patient's body via an introducer sheath, the localization signal including an in-phase component reflecting a position of the at least one localization element within the localization field and a quadrature component; and detecting whether the at least one localization element is within or outside of the introducer sheath based upon the quadrature component of the localization signal.

[0017] The method can also include suspending data collection from the at least one localization element if the at least one localization element is detected within the introducer sheath. Alternatively, the method can include discarding data collected by the at least one localization element when the at least one localization element is detected within the introducer sheath. As still another option, the method can include generating an alert if the at least one localization element is detected within the introducer sheath.

[0018] The method typically includes establishing a baseline quadrature component with the at least one localization element positioned outside of the introducer sheath. This can be accomplished, for example, by adjusting a demodulation delay for the localization signal until the quadrature component remains substantially constant at a calibration value as the at least one localization element moves. Then, whether the at least one localization element is within or outside of the introducer sheath can be determined by detecting that the at least

one localization element is outside of the introducer sheath when the quadrature component falls within a preset range about the calibration value and detecting that the at least one localization element is within the introducer sheath when the quadrature component falls outside of a preset range about the calibration value.

[0019] A device according to the invention is defined in claim 1.

[0020] An exemplary advantage of the present disclosure is that it provides an analytical method of detecting a localization element/sheath state change, reducing the burden on the practitioner to visually recognize such conditions.

[0021] A representative advantage of the present invention is that it provides a localization system with an analytical capability to suspend an electrophysiology study when a localization element is withdrawn into the introducer, thereby rendering its measurements less reliable.

[0022] Still another representative advantage of the present invention is that it provides a localization system with an analytical capability to discard electrophysiology study data collected by a localization element within the introducer, thereby rendering its measurements less reliable.

[0023] The foregoing and other aspects, features, details, utilities, and advantages of the present invention will be apparent from reading the following description and claims, and from reviewing the accompanying drawings.

BRIEF DESCRIPTION OF THE DRAWINGS

[0024]

Figure 1 is a schematic diagram of a localization system, such as may be used in an electrophysiology study.

Figure 2 depicts an exemplary catheter used in an electrophysiology study.

Figures 3A through 3C are exemplary perspective views of relative positions of localization electrodes and an introducer sheath.

Figure 4 depicts the in-phase and quadrature components of the localization signals for four localization electrodes.

Figure 5 is a flowchart depicting representative steps according to the teachings herein.

DETAILED DESCRIPTION

[0025] The present disclosure provides methods, apparatuses and systems for detecting when a localization element, such as a localization electrode, emerges from and/or is withdrawn into another device such as an introducer sheath (referred to herein as a "localization element/sheath state change"). For purposes of illustration, embodiments of the invention will be described in detail

herein in the context of a localization system utilized in a cardiac electrophysiology procedure. It is contemplated, however, that the present invention may be practiced to good advantage in other contexts.

[0026] Figure 1 shows a schematic diagram of a localization system 8 for conducting cardiac electrophysiology studies by navigating a cardiac catheter and measuring electrical activity occurring in a heart 10 of a patient 11 and three-dimensionally mapping the electrical activity and/or information related to or representative of the electrical activity so measured. System 8 can be used, for example, to create an anatomical model of the patient's heart 10 using one or more electrodes. System 8 can also be used to measure electrophysiology data at a plurality of points along a cardiac surface and store the measured data in association with location information for each measurement point at which the electrophysiology data was measured, for example to create a diagnostic data map of the patient's heart 10.

[0027] As one of ordinary skill in the art will recognize, and as will be further described below, localization system 8 determines the location, and in some aspects the orientation, of objects, typically within a three-dimensional space, and expresses those locations as position information determined relative to at least one reference.

[0028] For simplicity of illustration, the patient 11 is depicted schematically as an oval. In the embodiment shown in Figure 1, three sets of surface electrodes (e.g., patch electrodes) are shown applied to a surface of the patient 11, defining three generally orthogonal axes, referred to herein as an x-axis, a y-axis, and a z-axis. In other embodiments the electrodes could be positioned in other arrangements, for example multiple electrodes on a particular body surface. As a further alternative, the electrodes do not need to be on the body surface, but could be positioned internally to the body.

[0029] In Figure 1, the x-axis surface electrodes 12, 14 are applied to the patient along a first axis, such as on the lateral sides of the thorax region of the patient (e.g., applied to the patient's skin underneath each arm) and may be referred to as the Left and Right electrodes. The y-axis electrodes 18, 19 are applied to the patient along a second axis generally orthogonal to the x-axis, such as along the inner thigh and neck regions of the patient, and may be referred to as the Left Leg and Neck electrodes. The z-axis electrodes 16, 22 are applied along a third axis generally orthogonal to both the x-axis and the y-axis, such as along the sternum and spine of the patient in the thorax region, and may be referred to as the Chest and Back electrodes. The heart 10 lies between these pairs of surface electrodes 12/14, 18/19, and 16/22.

[0030] An additional surface reference electrode (e.g., a "belly patch") 21 provides a reference and/or ground electrode for the system 8. The belly patch electrode 21 may be an alternative to a fixed intra-cardiac electrode 31, described in further detail below. It should also be appreciated that, in addition, the patient 11 may have most or all of the conventional electrocardiogram ("ECG")

system leads in place. This ECG information is available to the system 8, although not illustrated in Fig. 1.

[0031] A representative catheter 13 having at least one electrode 17 (e.g., a distal electrode) is also shown. This representative catheter electrode 17 is referred to as the "roving electrode," "moving electrode," or "measurement electrode" throughout the specification. Typically, multiple electrodes on catheter 13, or on multiple such catheters, will be used. In one embodiment, for example, localization system 8 may comprise sixty-four electrodes on twelve catheters disposed within the heart and/or vasculature of the patient. Of course, this embodiment is merely exemplary, and any number of electrodes and catheters may be used within the scope of the present invention. Likewise, it should be understood that catheter 13 (or multiple such catheters) are typically introduced into the heart and/or vasculature of the patient via one or more introducers (not shown in Figure 1, but readily understood by the ordinarily skilled artisan).

[0032] For purposes of this disclosure, a segment of an exemplary catheter 13 is shown in Figure 2. In Figure 2, catheter 13 extends into the left ventricle 50 of the patient's heart 10 through an introducer 35, the distal-most segment of which is shown in Figure 2. The construction of introducers, such as introducer 35, are well known and will be familiar to those of ordinary skill in the art, and need not be further described herein.

[0033] Catheter 13 includes electrode 17 on its distal tip, as well as a plurality of additional measurement electrodes 52, 54, 56 spaced along its length in the illustrated embodiment. Typically, the spacing between adjacent electrodes will be known, though it should be understood that the electrodes may not be evenly spaced along catheter 13 or of equal size to each other. Since each of these electrodes 17, 52, 54, 56 lies within the patient, location data may be collected simultaneously for each of the electrodes by localization system 8.

[0034] Figures 3A through 3C illustrate three relative positions of the distal end of catheter 13 relative to introducer 35. As shown in Figure 3A, catheter 13 is fully withdrawn into sheath 35 (e.g., electrodes 17, 52, 54, and 56 are all within sheath 35). In Figure 3B, catheter 13 has been advanced such that electrode 17, but not electrodes 52, 54, and 56, have emerged from sheath 35. In Figure 3C, catheter 13 has been advanced further, such that electrodes 17 and 52, but not electrodes 54 and 56, have emerged from sheath 35. As discussed in further detail below, the teachings herein can be applied to good advantage to detect the localization element/sheath state changes of electrode 17 from Figure 3A to Figure 3B, and of electrode 52 from Figure 3B to Figure 3C (and, as the ordinarily skilled artisan will appreciate, vice versa).

[0035] Returning now to Figure 1, an optional fixed reference electrode 31 (e.g., attached to a wall of the heart 10) is shown on a second catheter 29. For calibration purposes, this electrode 31 may be stationary (e.g., attached to or near the wall of the heart) or disposed in a

fixed spatial relationship with the roving electrodes (e.g., electrodes 17, 52, 54, 56), and thus may be referred to as a "navigational reference" or "local reference." The fixed reference electrode 31 may be used in addition or alternatively to the surface reference electrode 21 described above. In many instances, a coronary sinus electrode or other fixed electrode in the heart 10 can be used as a reference for measuring voltages and displacements; that is, as described below, fixed reference electrode 31 may define the origin of a coordinate system.

[0036] Each surface electrode is coupled to the multiplex switch 24, and the pairs of surface electrodes are selected by software running on a computer 20, which couples the surface electrodes to a signal generator 25. Alternately, switch 24 may be eliminated and multiple (e.g., three) instances of signal generator 25 may be provided, one for each measurement axis (that is, each surface electrode pairing).

[0037] The computer 20, for example, may comprise a conventional general-purpose computer, a special-purpose computer, a distributed computer, or any other type of computer. The computer 20 comprises a localization processor and a localization element/sheath state change detection processor, optionally in a parallel processing environment, which may execute instructions to practice the various aspects of the present invention described herein.

[0038] Generally, three nominally orthogonal electric fields are generated by a series of driven and sensed electric dipoles (e.g., surface electrode pairs 12/14, 18/19, and 16/22) in order to realize catheter navigation in a biological conductor. Alternatively, these orthogonal fields can be decomposed and any pairs of surface electrodes can be driven as dipoles to provide effective electrode triangulation. Likewise, the electrodes 12, 14, 18, 19, 16, and 22 (or any number of electrodes) could be positioned in any other effective arrangement for driving a current to or sensing a current from an electrode in the heart. For example, multiple electrodes could be placed on the back, sides, and/or belly of patient 11. Additionally, such non-orthogonal methodologies add to the flexibility of the system. For any desired axis, the potentials measured across the roving electrodes resulting from a predetermined set of drive (source-sink) configurations may be combined algebraically to yield the same effective potential as would be obtained by simply driving a uniform current along the orthogonal axes.

[0039] Thus, any two of the surface electrodes 12, 14, 16, 18, 19, 22 may be selected as a dipole source and drain with respect to a ground reference, such as belly patch 21, while the unexcited electrodes measure voltage with respect to the ground reference. The roving electrodes 17, 52, 54, 56 placed in the heart 10 are exposed to the field from a current pulse and are measured with respect to ground, such as belly patch 21. In practice the catheters within the heart may contain more or fewer electrodes than the four shown, and each electrode potential may be measured. As previously noted, at least

one electrode may be fixed to the interior surface of the heart to form a fixed reference electrode 31, which is also measured with respect to ground, such as belly patch 21, and which may be defined as the origin of the coordinate system relative to which localization system 8 measures positions. Data sets from each of the surface electrodes, the internal electrodes, and the virtual electrodes may all be used to determine the location of the roving electrodes 17, 52, 54, 56 within heart 10.

[0040] The measured voltages may be used to determine the location in three-dimensional space of the electrodes inside the heart, such as roving electrodes 17, 52, 54, 56, relative to a reference location, such as reference electrode 31. That is, the voltages measured at reference electrode 31 may be used to define the origin of a coordinate system, while the voltages measured at roving electrodes 17, 52, 54, 56 may be used to express the location of roving electrodes 17, 52, 54, 56 relative to the origin. Preferably, the coordinate system is a three-dimensional (x, y, z) Cartesian coordinate system, though the use of other coordinate systems, such as polar, spherical, and cylindrical coordinate systems, is within the scope of the invention.

[0041] As should be clear from the foregoing discussion, the data used to determine the location of the electrode(s) within the heart is measured while the surface electrode pairs impress an electric field on the heart. The electrode data may also be used to create a respiration compensation value used to improve the raw location data for the electrode locations as described in U.S. Patent Application Publication No. 2004/0254437 (now United States patent no. 7,263,397). The electrode data may also be used to compensate for changes in the impedance of the body of the patient as described in United States patent no. 7,885,707.

[0042] Therefore, in one representative embodiment, the system 8 first selects a set of surface electrodes and then drives them with current pulses. While the current pulses are being delivered, electrical activity, such as the voltages measured at least one of the remaining surface electrodes and *in vivo* electrodes, is measured and stored. Compensation for artifacts, such as respiration and/or impedance shifting, may be performed as indicated above.

[0043] In some embodiments, the localization/mapping system is the EnSite™ Velocity™ cardiac mapping system of St. Jude Medical, Inc., which generates electrical fields as described above, or another localization system that relies upon electrical fields. Other localization systems, however, may be used in conjunction with such electrical-field based localization systems in connection with the present teachings, including for example, the CARTO navigation and location system of Biosense Webster, Inc., the AURORA® system of Northern Digital Inc., or Sterotaxis' NIOBE® Magnetic Navigation System, all of which utilize magnetic fields rather than electrical fields. The localization and mapping systems described in the following patents can also be used with the

present invention: United States Patent Nos. 6,990,370; 6,978,168; 6,947,785; 6,939,309; 6,728,562; 6,640,119; 5,983,126; and 5,697,377.

[0044] Thus, the present invention will be described in the context of a localization system that generates an electrical field. The fields generated by localization system 8 will be referred to generically as "localization fields," while the elements generating the fields, such as surface electrodes 12, 14, 16, 18, 19, and 22 will be generically referred to as "localization field generators." As described above, surface electrodes 12, 14, 16, 18, 19, and 22 may also function as detectors to measure the characteristics of the localization field (e.g., the voltages measured at roving electrodes 17, 52, 54, 56, or a current from roving electrodes 17, 52, 54, 56), and thus may also be referred to generically as "localization elements" (or, in the case of an impedance-based localization system, more specifically as "localization electrodes"). Further, the measurements of each localization element can be referred to generically as "localization signals."

[0045] As previously described, surface electrodes 12, 14, 16, 18, 19, 22 generate electric fields that are in turn sensed by electrodes 17, 52, 54, and 56 on catheter 13. Signal generator 25 provides an excitation signal to any pair of surface electrodes in the form of a sinusoidal alternating current at, for example, a frequency of 8 kHz, although the ordinarily skilled artisan will appreciate that a broad range of frequencies can be used without departing from the teachings herein.

[0046] To determine the electric field intensity at each catheter electrode, the sensed signals are first frequency limited by low-pass filter 27, then converted to a digital value by analog to digital converter 26. Synchronous demodulation is then applied to determine the resulting electric field intensity for each electrode and, in turn, each surface electrode pair. Synchronous demodulation is an established method of determining the intensity of a signal at a particular frequency by multiplying the sensed signal (from analog-to-digital converter 26) with an in-phase copy of the excitation signal from signal generator 25. This in-phase copy is known as the sine reference. Before multiplication, the sine reference is time delayed to phase align it with the sensed signal. The sensed signal has a natural time delay relative to the sine reference due to the electrical path the sensed signal must traverse from signal generator 25, through surface electrodes, body tissue, catheter electrodes, and sensing electronics. The product of the multiplication is averaged over a time period to provide a value that is proportional to the electric field at each catheter electrode. This is the in-phase component and is used to calculate the relative location of each catheter electrode.

[0047] By multiplying the same sensed signal with a signal that is 90 degrees out-of-phase with the sine reference (by definition, a cosine reference) signal, an out-of-phase component is determined. This out-of-phase component is also known as the quadrature component.

[0048] In a properly tuned localization system (i.e., a

system where the demodulation delay time is optimized), the in-phase component will dominate over the quadrature component. The quadrature component, however, will still be measurable. Moreover, provided the localization elements remain outside the introducer sheath, the quadrature component will be substantially constant, regardless of localization element location.

[0049] When a localization element is withdrawn into the introducer sheath, however, the quadrature component changes measurably. This is due to the impedance change in the vicinity of the localization element. The impedance change results not only from the constricted space and insulating material construction of the introducer sheath, but also from changes in complex impedance (e.g., a combination of resistance and capacitance).

[0050] As the ordinarily skilled artisan will appreciate, changes in capacitance change the delay time of a signal sensed by a localization element. It follows that the demodulation delay time is no longer optimized, leading to position sensitivity in the quadrature component. The same lack of optimization renders the in-phase signal unreliable, leading, for example, to difficulties in rendering an image of catheter 13 within the patient's heart. In one embodiment, when a localization element has been withdrawn into the sheath, it may be desirable to detect this transition to enable the transitioning localization element to be temporarily turned off or otherwise disabled as described further below.

[0051] A method for detecting a localization element/sheath state change based on the quadrature component will now be described with reference to Figures 4 and 5. Figure 4 depicts both the in-phase and quadrature components of the localization signals for four electrodes (e.g., 17, 52, 54, and 56) along the neck-leg axis defined by patch electrodes 18 and 19. The top window of Figure 4 illustrates the respective in-phase components (100, 102, 104, 106) for these electrodes, while the bottom window illustrates their respective quadrature components (200, 202, 204, 206). At the left-most edge of Figure 4 (e.g., time t_0), all four electrodes 17, 52, 54, 56 are outside of introducer sheath 35. As can be seen in the lower window of Figure 4, the quadrature component for each of electrodes 17, 52, 54, 56 is non-zero, relatively small, and substantially constant.

[0052] At time t_1 , approximately 4 seconds later, catheter 13 is partially withdrawn into introducer sheath 35. The top window of Figure 4 shows the displacement change for each electrode, but, because all four electrodes remain outside of introducer sheath 35, the lower window of Figure 4 shows no change in the quadrature component for any of the electrodes.

[0053] At time t_2 , approximately 2 seconds later, catheter 13 is withdrawn further into introducer sheath 35 to such an extent that electrode 56 re-enters introducer sheath 35. The top window of Figure 4 shows the displacement, and further shows an unreliable in-phase component for electrode 56 (line 106). The bottom window of Figure 4 also shows a measurable change in the

quadrature component for electrode 56 (line 206). This measurable change in the quadrature component for electrode 56 is indicative of the localization element/sheath state change for electrode 56.

[0054] At time t_3 , approximately 2 seconds later, catheter 13 is withdrawn further into introducer sheath 35 to such an extent that electrode 54 also re-enters introducer sheath 35. The top window of Figure 4 shows the displacement, and further shows an unreliable in-phase component for electrode 54 (line 104). The bottom window of Figure 4 also shows a measurable change in the quadrature component for electrode 54 (line 204), as well as a further change in the quadrature component for electrode 56. This measurable change in the quadrature component for electrode 54 is indicative of the localization element/sheath state change for electrode 54.

[0055] At time t_4 , approximately 1.5 seconds later, catheter 13 is withdrawn further into introducer sheath 35 to such an extent that electrode 52 also re-enters introducer sheath 35. The top window of Figure 4 shows the displacement, and further shows an unreliable in-phase component for electrode 52 (line 102). The bottom window of Figure 4 also shows a measurable change in the quadrature component for electrode 52 (line 202), as well as further changes in the quadrature components for electrodes 56, 54. This measurable change in the quadrature component for electrode 52 is indicative of the localization element/sheath state change for electrode 52.

[0056] At time t_5 , approximately 1 second later, catheter 13 is withdrawn further into introducer sheath 35 to such an extent that electrode 17 also re-enters introducer sheath 35. The top window of Figure 4 shows the displacement, and further shows an unreliable in-phase component for electrode 17 (line 100). The bottom window of Figure 4 also shows a measurable change in the quadrature component for electrode 17 (line 200), as well as further changes in the quadrature components for electrodes 56, 54, 52. This measurable change in the quadrature component for electrode 17 is indicative of the localization element/sheath state change for electrode 17.

[0057] Finally, at time t_6 , approximately 1 second later, catheter 13 is advanced back out of introducer sheath 35 such that only the most proximal electrode 56 remains within introducer sheath 35. The top window of Figure 4 shows the displacement, with the in-phase components for electrodes 17, 52, and 54 (lines 100, 102, 104, respectively) returning to reliable signals. Likewise, the bottom window of Figure 4 shows that the quadrature components for electrodes 17, 52, and 54 (lines 200, 202, 204, respectively) return to approximate their initial, substantially stable values, indicative of their state change (e.g., re-emergence from introducer sheath 35). Only electrode 56 remains subject to an unreliable in-phase component (line 106) and a measurably changed quadrature component (line 206) because only electrode 56 remains within introducer sheath 35.

[0058] Figure 5 is a flowchart of representative steps that can be performed in order to detect localization element/sheath state changes. In step 500, catheter 13 is introduced into the localization field generated by localization system 8 (e.g., introduced into the patient's heart). In optional step 502, the delay time of the demodulation signal is optimized. These steps are sufficiently well understood by those of ordinary skill in the art that they need not be further discussed herein.

[0059] In step 504, a baseline quadrature component is set, such that localization element/sheath state changes can be detected from the quadrature component of the localization signal for a catheter-borne localization element by comparisons between the real time quadrature component and the baseline quadrature component. The baseline is established with the localization element outside of the introducer sheath.

[0060] In one embodiment, the baseline quadrature component will follow from the optimization of the demodulation delay time in step 502. Typically, in a properly calibrated (that is, optimized) system, the quadrature component of the localization signal will remain substantially constant at a calibration value as the localization element moves. Localization element movement during calibration can be due to the patient's natural motion (e.g., the beating of the heart). Alternatively, it can be induced, such as by the practitioner making small movements of the catheter. The calibration value for the quadrature component is depicted, for example, in the lower window of Figure 4 from time t_0 to time t_2 .

[0061] As described above, optimization step 502 is optional. Thus, in certain embodiments, the demodulation delay is calculated using a calibration procedure *ex vivo*. One manner for sufficiently calibrating or "tuning" the localization system involves performing a standard calibration that approximates the delays experienced by the signals in the body, obtaining impedance measurements for both in-phase and out-of-phase with simulated patient impedances, until the out-of-phase signal shows minimal change with simulated location change. As described above, the "location change" can result from normal cardiac rhythm, manual movements of the catheter, and the like. Simulated location changes can be created by invoking small changes in the simulated patient impedance.

[0062] Once the baseline quadrature component (e.g., the calibration value) is established, localization element/sheath state changes can be detected from a received localization signal (step 506) by monitoring the quadrature component (step 508) thereof.

[0063] For example, the withdrawal of a localization element into the introducer sheath can be detected when the quadrature component for the localization element deviates from the calibration value by more than a preset amount (path 510). This preset amount can be user-adjustable or user-selectable.

[0064] Conversely, when the quadrature component returns to within a preset amount of the calibration value

(path 512), the re-emergence of the localization element from the introducer sheath can be detected.

[0065] Similarly, if no change in the quadrature component is detected (path 514), then no localization element/sheath state change is detected.

[0066] In response to detecting that a localization element/sheath state change, a number of steps (referred to generally as "corrective actions") can optionally be taken in step 516, either independently or in concert. For example, an alert (e.g., an audible, visual, and/or haptic signal) can be generated to call the practitioner's attention to the withdrawal of a localization element into, or emergence of a localization element from, the introducer sheath.

[0067] As another example, data collection can be gated to the in- or out-of-sheath state of a given localization element. That is, when the localization element is within the sheath, data collection therefrom can be suspended; when the localization element is outside of the sheath, data collection therefrom can proceed (step 518).

[0068] As still another example, data collected with the localization element within the sheath can simply be discarded.

[0069] Although several embodiments of this invention have been described above with a certain degree of particularity, those skilled in the art could make numerous alterations to the disclosed embodiments without departing from the scope of this invention which is defined in the claims.

[0070] For example, the invention has been described above with reference to the neck-leg axis. The use of the neck-leg axis is desirable because it helps ensure that the quadrature component will be non-zero, because there will be an offset between the location of catheter 13 (e.g., within the heart) and the coordinate reference point for the localization system (e.g., belly patch 21) that will be larger than on other axes. It should be understood, however, that the teachings herein could be applied to any or all measurement axes of localization system 8.

[0071] As another example, in another embodiment, the calibration process (502) does not change the demodulation delay time, but rather invokes a linear relationship between the in-phase and quadrature components of localization elements that are not in sheaths. When measuring complex impedance components, any calibration delay offset manifests as a quadrature component that is linearly dependent on the in-phase component. In addition, some constant current may be present in the instrumentation which is out of phase with the localization field generation, resulting in a position-independent quadrature measurement. The plurality of localization elements disposed within the localization field provides a plurality of co-located in-phase and quadrature measurements to which a linear model is fit, such as by using least-squares or another suitable model fitting technique. Alternately, a single localization element may be moved to a plurality of locations in order to acquire a number of co-located in-phase and quadrature meas-

urements to determine the linear model parameters. Once the linear model parameters have been determined, a localization element can be identified as entering the sheath when its in-phase and quadrature measurements no longer fit the parameters, as evidenced by a residual between modeled and measured quadrature values rising above a critical threshold. An ordinarily skilled artisan would be able to extend the described technique to non-linear and multivariate models.

[0072] All directional references (e.g., upper, lower, upward, downward, left, right, leftward, rightward, top, bottom, above, below, vertical, horizontal, clockwise, and counterclockwise) are only used for identification purposes to aid the reader's understanding of the present invention, and do not create limitations, particularly as to the position, orientation, or use of the invention. Joinder references (e.g., attached, coupled, connected, and the like) are to be construed broadly and may include intermediate members between a connection of elements and relative movement between elements. As such, joinder references do not necessarily infer that two elements are directly connected and in fixed relation to each other.

[0073] It is intended that all matter contained in the above description or shown in the accompanying drawings shall be interpreted as illustrative only and not limiting. Changes in detail or structure may be made without departing from scope of the invention as defined in the appended claims.

Claims

1. A localization system, comprising:

a localization processor configured to receive as input a localization signal from at least one localization element (17, 52, 54, 56) and to resolve the localization signal into an in-phase component reflective of a position of the at least one localization element (17, 52, 54, 56) and a quadrature component;
a localization element/sheath state change detection processor configured to receive as input the quadrature component and detect when the at least one localization element (17, 52, 54, 56) emerges from and/or is withdrawn into another device based on the quadrature component.

2. The localization system according to claim 1, wherein the another device is an introducer sheath (35).

3. The localization system according to claim 2, wherein the at least one localization element (17, 52, 54, 56) is adapted for establishing a baseline quadrature component outside of the introducer sheath (35).

4. The localization system according to claim 3, wherein establishing a baseline quadrature component

- comprises adjusting a demodulation delay for the localization signal until the quadrature component remains substantially constant at a calibration value as the at least one localization element (17, 52, 54, 56) moves.
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5. The localization system according to claim 4, wherein movement of the localization element (17, 52, 54, 56) during establishing a baseline quadrature component is attributable to patient motion.
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6. The localization system according to claim 4, wherein movement of the localization element (17, 52, 54, 56) during establishing a baseline quadrature component is attributable to catheter motion.
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7. The localization system according to claim 4, wherein the localization element/sheath state change detection processor is adapted to detect withdrawal of the at least one localization element (17, 52, 54, 56) into the introducer sheath (35) based upon the quadrature component of the at least one localization signal deviating from the calibrated value by more than a preset amount.
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8. The localization system according to claim 7, wherein the localization element/sheath state change detection processor is further adapted to detect re-emergence of the at least one localization element (17, 52, 54, 56) from the introducer sheath (35) based upon the quadrature component of the at least one localization signal returning to within the preset amount of the calibrated value.
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9. The localization system according to claim 7, wherein an alert is generated regarding the withdrawal of the at least one localization element (17, 52, 54, 56) into the introducer sheath (35).
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10. The localization system according to claim 3, wherein the localization element/sheath state change detection processor is adapted to detect that the at least one localization element (17, 52, 54, 56) is outside of the introducer sheath (35) when the quadrature component falls within a preset range about the calibration value and to detect that the at least one localization element (17, 52, 54, 56) is within the introducer sheath when the quadrature component falls outside of the preset range about the calibration value.
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11. The localization system according to claim 3, wherein establishing a baseline comprises making a plurality of complex impedance measurements and determining least squares parameters in a linear model.
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12. The localization system according to claim 11,
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- wherein the localization element/sheath state change detection processor is adapted to detect withdrawal of the at least one localization element (17, 52, 54, 56) into the introducer sheath (35) based upon the quadrature component of the at least one localization signal deviating from the linear model by more than a preset amount.
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13. The localization system according to claim 1, comprising:
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- a first localization field generator and a second localization field generator defining an axis along which the localization signal is measured, wherein
- the localization signal is measured relative to a reference point substantially aligned with the axis; and at least one catheter-borne localization element is spaced apart from the reference point along the axis.
14. The localization system according to claim 13, wherein:
- the first localization field generator is positioned on a patient's neck;
- the second localization field generator is positioned on the patient's leg;
- the reference point is located on the patient's belly; and
- the at least one catheter-borne localization element is positioned within the patient's heart.
- Patentansprüche**
1. Lokalisierungssystem mit:
- einem Lokalisierungsprozessor, der ausgebildet ist zum Empfangen eines Lokalisierungssignals als Eingabe von mindestens einem Lokalisierungselement (17, 52, 54, 56) und zum Auflösen des Lokalisierungssignals in eine In-Phasen-Komponente, die eine Position des mindestens einen Lokalisierungselements (17, 52, 54, 56) widerspiegelt, und in eine Quadratur-Komponente;
- einem Lokalisierungselement/Schaftzustandsänderungs-Detektionsprozessor, der ausgebildet ist zum Empfangen der Quadratur-Komponente als Eingabe, und zum Erkennen, ob mindestens ein Lokalisierungselement (17, 52, 54, 56) aus einer anderen Vorrichtung heraus ragt und/oder hinein gezogen ist, basierend auf der Quadratur-Komponente.
2. Lokalisierungssystem nach Anspruch 1, bei dem die andere Vorrichtung ein Einführerschaft (35) ist.

3. Lokalisierungssystem nach Anspruch 2, bei dem das mindestens eine Lokalisierungselement (17, 52, 54, 56) ausgebildet ist zum Bilden einer Basisquadratur-Komponente außerhalb des Einführerschafts (35).
4. Lokalisierungssystem nach Anspruch 3, bei dem das Bilden einer Basisquadratur-Komponente ein Einstellen einer Demodulationsverzögerung für das Lokalisierungssignal aufweist, bis die Quadratur-Komponente im Wesentlichen konstant bei einem Kalibrierungswert bleibt, wenn sich das mindestens eine Lokalisierungselement (17, 52, 54, 56) bewegt.
5. Lokalisierungssystem nach Anspruch 4, bei dem die Bewegung des Lokalisierungselements (17, 52, 54, 56) während der Bildung einer Basisquadratur-Komponente einer Patientenbewegung zuordbar ist.
6. Lokalisierungssystem nach Anspruch 4, bei dem die Bewegung des Lokalisierungselements (17, 52, 54, 56) während der Bildung einer Basisquadratur-Komponente einer Katheterbewegung zuordbar ist.
7. Lokalisierungssystem nach Anspruch 4, bei dem der Lokalisierungselement/Schaftzustandsänderungs-Detektor ausgebildet ist zum Detektieren eines Zurückziehens des mindestens eines Lokalisierungselements (17, 52, 54, 56) in den Einführerschaft (35) basierend auf der Quadratur-Komponente des mindestens einen Lokalisierungssignals, die von dem kalibrierten Wert um mehr als eine vorbestimmte Größe abweicht.
8. Lokalisierungssystem nach Anspruch 7, bei dem der Lokalisierungselement/Schaftzustandsänderungs-Detektor ferner ausgebildet ist zum Detektieren eines erneuten Herausragens des mindestens einen Lokalisierungselements (17, 52, 54, 56) aus dem Einführerschaft (35) basierend auf der Quadratur-Komponente des mindestens einen Lokalisierungssignals, die zu der vordefinierten Größe des kalibrierten Werts zurückkehrt.
9. Lokalisierungssystem nach Anspruch 7, bei dem ein Alarm erzeugt wird bezüglich des Zurückziehens des mindestens einen Lokalisierungselements (17, 52, 54, 56) in den Einführerschaft (35).
10. Lokalisierungssystem nach Anspruch 3, bei dem der Lokalisierungselement/Schaftzustandsänderungs-Detektor ausgebildet ist zum Detektieren, dass sich das mindestens eine Lokalisierungselement (17, 52, 54, 56) außerhalb des Einführerschafts (35) befindet, wenn die Quadratur-Komponente innerhalb eines vorbestimmten Bereichs um den Kalibrierungswert herum liegt, und detektiert, dass das mindestens eine Lokalisierungselement (17, 52, 54, 56) sich in dem Einführerschaft befindet,
- wenn die Quadratur-Komponente außerhalb des vorbestimmten Bereichs um den Kalibrierungswert herum liegt.
11. Lokalisierungssystem nach Anspruch 3, bei dem das Bilden einer Basis das Durchführen einer Mehrzahl von Messungen einer komplexen Impedanz und Bestimmen von Parametern kleinster Quadrate in einem linearen Modell aufweist.
12. Lokalisierungssystem nach Anspruch 11, bei dem der Lokalisierungselement/Schaftzustandsänderungs-Detektor ausgebildet ist zum Detektieren eines Zurückziehens des mindestens einen Lokalisierungselements (17, 52, 54, 56) in den Einführerschaft (35) basierend auf der Quadratur-Komponente des mindestens einen Lokalisierungssignals, die von dem linearen Modell um mehr als eine vorbestimmte Größe abweicht.
13. Lokalisierungssystem nach Anspruch 1, mit:
- einem ersten Lokalisierungsfeldgenerator und einem zweiten Lokalisierungsfeldgenerator, die eine Achse definieren, entlang der das Lokalisierungssignal gemessen wird,
- wobei das Lokalisierungssignal relativ zu einem Referenzpunkt gemessen wird, der im Wesentlichen mit der Achse ausgerichtet ist; und mindestens ein kathetergelagertes Lokalisierungselement von dem Referenzpunkt entlang der Achse beabstandet ist.
14. Lokalisierungssystem nach Anspruch 13, bei dem der erste Lokalisierungsfeldgenerator sich auf dem Hals eines Patienten befindet; der zweite Lokalisierungsfeldgenerator sich auf einem Bein des Patienten befindet; der Referenzpunkt sich auf dem Bauch des Patienten befindet; und das mindestens eine kathetergelagerte Lokalisierungselement sich innerhalb des Herzens des Patienten befindet.

Revendications

1. Système de localisation, comprenant :
- un processeur de localisation configuré pour recevoir comme entrée un signal de localisation provenant d'au moins un élément de localisation (17, 52, 54, 56) et pour résoudre le signal de localisation en une composante en phase réfléchissant une position de l'au moins un élément de localisation (17, 52, 54, 56) et en une com-

- posante en quadrature ;
un processeur de détection de changement d'état de gaine/d'élément de localisation configuré pour recevoir comme entrée la composante en quadrature et détecter le moment où l'au moins un élément de localisation (17, 52, 54, 56) émerge d'un autre dispositif et/ou est extrait de celui-là sur la base de la composante en quadrature.
2. Système de localisation selon la revendication 1, dans lequel l'autre dispositif est une gaine d'introduction (35).
 3. Système de localisation selon la revendication 2, dans lequel l'au moins un élément de localisation (17, 52, 54, 56) est adapté pour établir une composante en quadrature de ligne de base à l'extérieur de la gaine d'introduction (35).
 4. Système de localisation selon la revendication 3, dans lequel l'établissement d'une composante en quadrature de ligne de base comprend l'ajustement d'un délai de démodulation pour le signal de localisation jusqu'à ce que la composante en quadrature reste pour l'essentiel constante à une valeur d'éta- lonnage quand l'au moins un élément de localisation (17, 52, 54, 56) se déplace.
 5. Système de localisation selon la revendication 4, dans lequel le déplacement de l'élément de localisation (17, 52, 54, 56) durant l'établissement d'une composante en quadrature de ligne de base est imputable à un mouvement du patient.
 6. Système de localisation selon la revendication 4, dans lequel le déplacement de l'élément de localisation (17, 52, 54, 56) durant l'établissement d'une composante en quadrature de ligne de base est imputable à un mouvement du cathéter.
 7. Système de localisation selon la revendication 4, dans lequel le processeur de détection de changement d'état de gaine/d'élément de localisation est adapté pour détecter l'extraction de l'au moins un élément de localisation (17, 52, 54, 56) dans la gaine d'introduction (35) sur la base de la composante en quadrature de l'au moins un signal de localisation s'écartant de la valeur étalonée de plus d'une quantité prédéfinie.
 8. Système de localisation selon la revendication 7, dans lequel le processeur de détection de changement d'état de gaine/d'élément de localisation est en outre adapté pour détecter la ré-émergence de l'au moins un élément de localisation (17, 52, 54, 56) de la gaine d'introduction (35) sur la base de la composante en quadrature de l'au moins un signal de localisation retournant dans la quantité prédéfinie de la valeur étalonée.
 9. Système de localisation selon la revendication 7, dans lequel une alerte est générée concernant l'extraction de l'au moins un élément de localisation (17, 52, 54, 56) dans la gaine d'introduction (35).
 10. Système de localisation selon la revendication 3, dans lequel le processeur de détection de changement d'état de gaine/d'élément de localisation est adapté pour détecter que l'au moins un élément de localisation (17, 52, 54, 56) est à l'extérieur de la gaine d'introduction (35) quand la composante en quadrature tombe dans une plage prédéfinie concernant la valeur d'éta- lonnage et pour détecter que l'au moins un élément de localisation (17, 52, 54, 56) est dans la gaine d'introduction quand la composante en quadrature tombe à l'extérieur de la plage prédéfinie concernant la valeur d'éta- lonnage.
 11. Système de localisation selon la revendication 3, dans lequel l'établissement d'une ligne de base comprend la réalisation d'une pluralité de mesures d'impédance complexes et la détermination de paramètres des moindres carrés dans un modèle linéaire.
 12. Système de localisation selon la revendication 11, dans lequel le processeur de détection de changement d'état de gaine/d'élément de localisation est adapté pour détecter l'extraction de l'au moins un élément de localisation (17, 52, 54, 56) dans la gaine d'introduction (35) sur la base de la composante en quadrature de l'au moins un signal de localisation s'écartant du modèle linéaire de plus d'une quantité prédéfinie.
 13. Système de localisation selon la revendication 1, comprenant :
un premier générateur de champ de localisation et un second générateur de champ de localisation définissant un axe le long duquel le signal de localisation est mesuré, dans lequel
le signal de localisation est mesuré par rapport à un point de référence sensiblement aligné sur l'axe ; et
au moins un élément de localisation porté par le cathéter est espacé du point de référence le long de l'axe.
 14. Système de localisation selon la revendication 13, dans lequel :
le premier générateur de champ de localisation est positionné sur le cou d'un patient ;
le second générateur de champ de localisation est positionné sur la jambe du patient ;

le point de référence se situe sur le ventre du patient ; et
l'au moins un élément de localisation porté par le cathéter est positionné dans le cour du patient.

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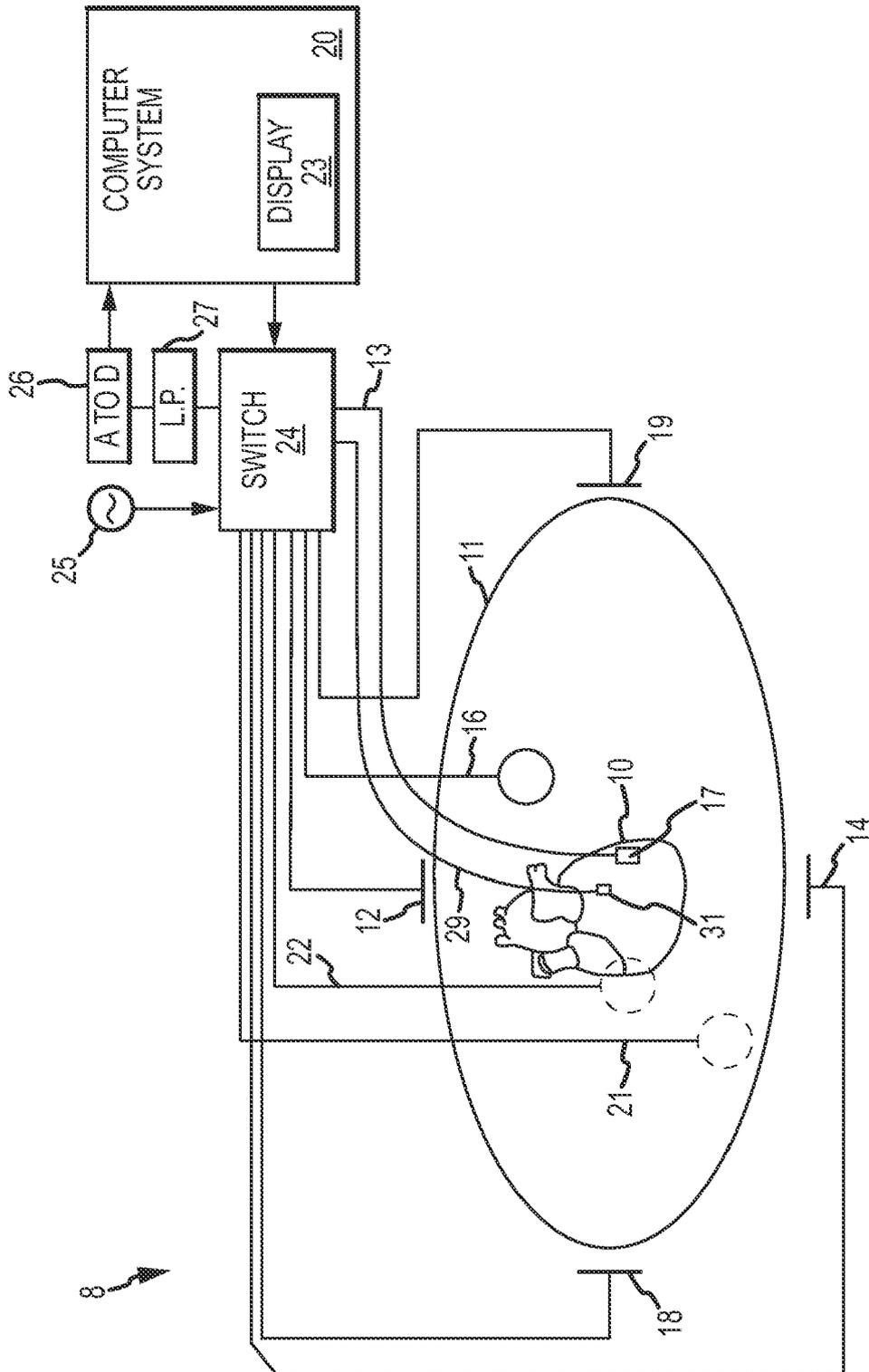


FIG.1

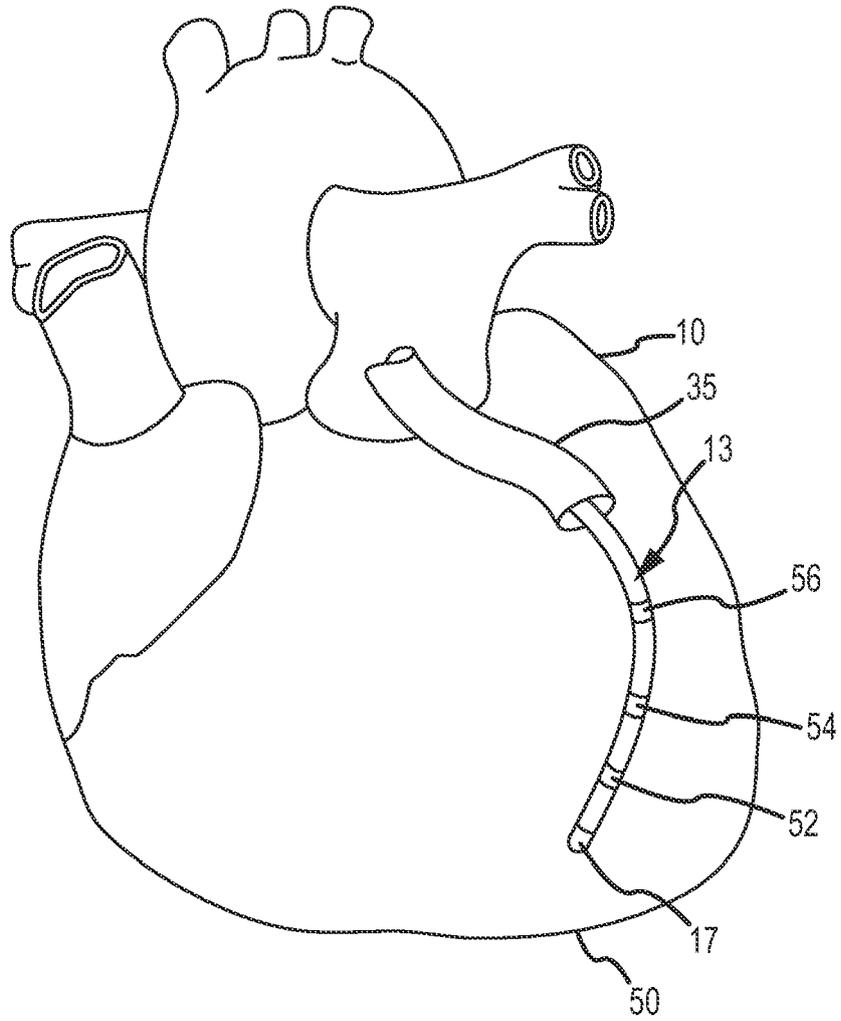


FIG.2

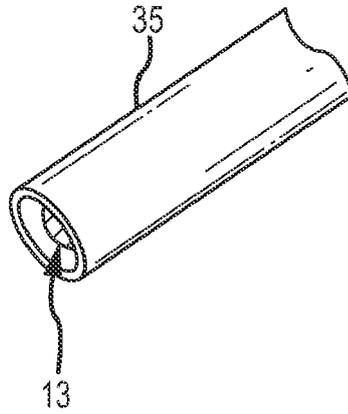


FIG. 3A

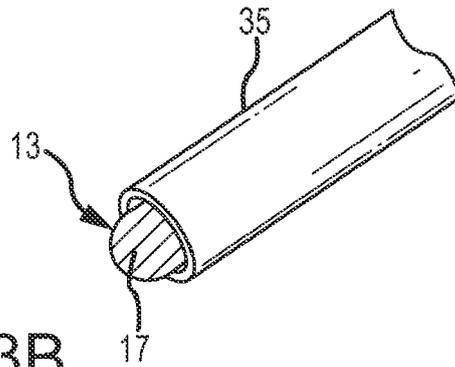


FIG. 3B

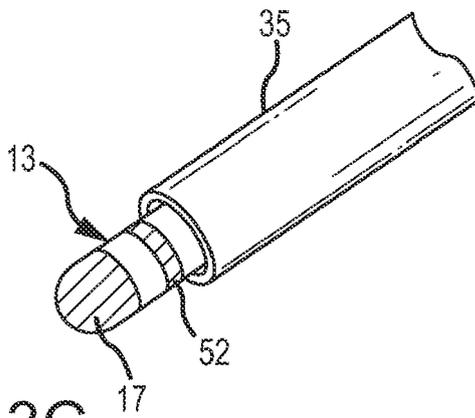


FIG. 3C

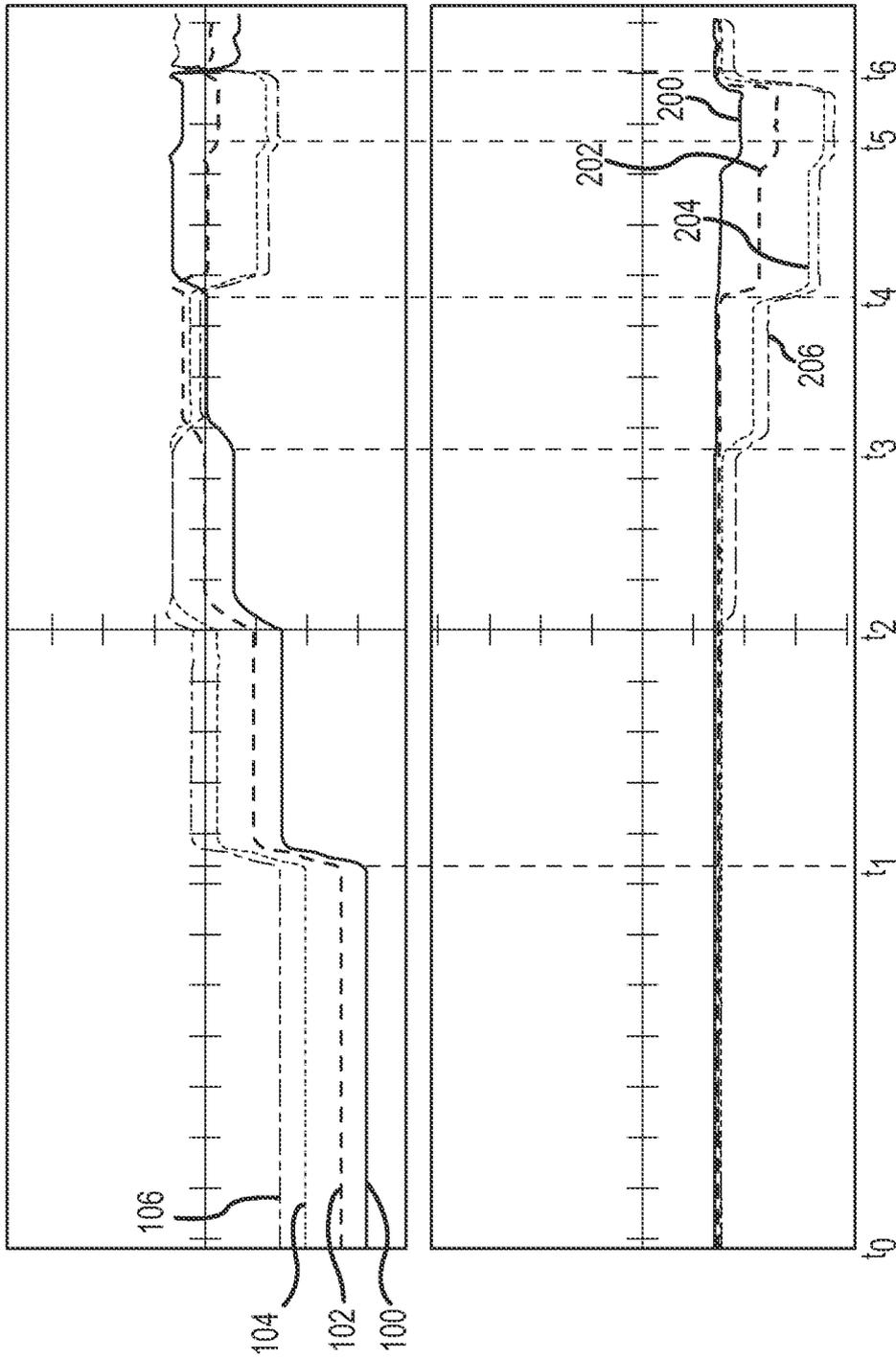


FIG.4

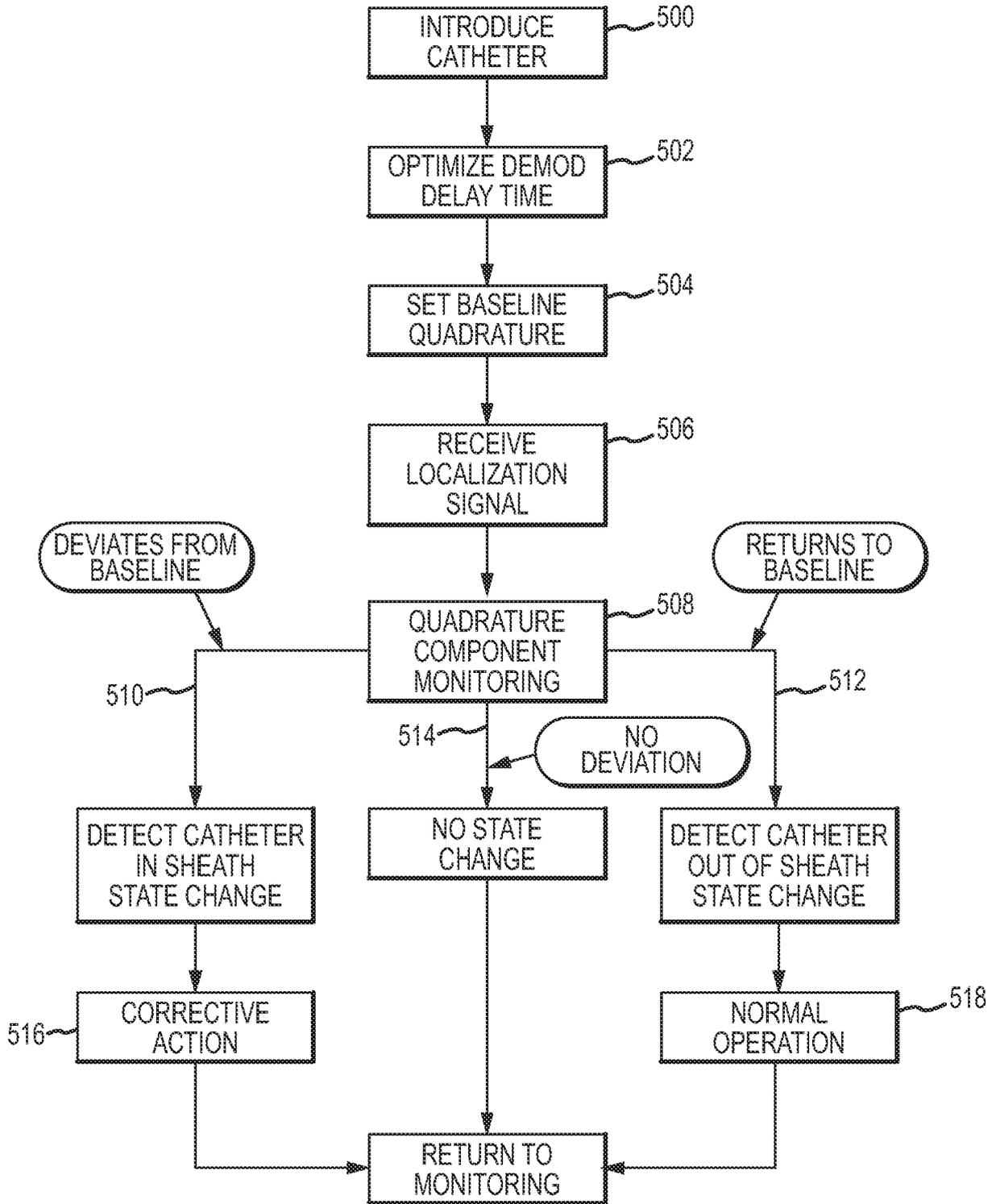


FIG.5

REFERENCES CITED IN THE DESCRIPTION

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